# **Journal of Visualized Experiments**

# Rapid Encapsulation of Reconstituted Cytoskeleton inside Giant Unilamellar Vesicles --Manuscript Draft--

Article Type:	Invited Methods Article - JoVE Produced Video
Manuscript Number:	JoVE63332R1
Full Title:	Rapid Encapsulation of Reconstituted Cytoskeleton inside Giant Unilamellar Vesicles
Corresponding Author:	Allen Liu, Ph.D. University of Michigan Ann Arbor, MI UNITED STATES
Corresponding Author's Institution:	University of Michigan
Corresponding Author E-Mail:	allenliu@umich.edu
Order of Authors:	Yashar Bashirzadeh
	Nadab Wubshet
	Thomas Litschel
	Petra Schwille
	Allen Liu, Ph.D.
Additional Information:	
Question	Response
Please specify the section of the submitted manuscript.	Bioengineering
Please indicate whether this article will be Standard Access or Open Access.	Standard Access (\$1400)
Please indicate the <b>city, state/province, and country</b> where this article will be <b>filmed</b> . Please do not use abbreviations.	Ann Arbor, Michigan, USA
Please confirm that you have read and agree to the terms and conditions of the author license agreement that applies below:	I agree to the Author License Agreement
Please confirm that you have read and agree to the terms and conditions of the video release that applies below:	I agree to the <u>Video Release</u>
Please provide any comments to the journal here.	

1 TITLE: 2 Rapid Encapsulation of Reconstituted Cytoskeleton inside Giant Unilamellar Vesicles 3 4 **AUTHORS AND AFFILIATIONS:** Yashar Bashirzadeh<sup>1#</sup>, Nadab Wubshet<sup>1#</sup>, Thomas Litschel<sup>2</sup>, Petra Schwille<sup>3</sup>, Allen P. Liu<sup>1,4,5,6</sup>\* 5 6 7 <sup>1</sup>Department of Mechanical Engineering, University of Michigan, Ann Arbor, Michigan, 48109, 8 9 <sup>2</sup>John A. Paulson School of Engineering and Applied Sciences, Harvard University, Cambridge, 10 Massachusetts 02138, USA <sup>3</sup>Department of Cellular and Molecular Biophysics, Max Planck Institute of Biochemistry, 82152, 11 12 Martinsried, Germany 13 <sup>4</sup>Department of Biomedical Engineering, University of Michigan, Ann Arbor, Michigan, 48109, 14 USA 15 <sup>5</sup>Department of Biophysics, University of Michigan, Ann Arbor, Michigan, 48109, USA 16 <sup>6</sup>Cellular and Molecular Biology Program, University of Michigan, Ann Arbor, Michigan, 48109, 17 **USA** 18 19 Email addresses of the authors: 20 Yashar Bashirzadeh (ybash@umich.edu) (nadab@umich.edu) 21 Nadab Wubshet 22 Thomas Litschel (tlitschel@g.harvard.edu) 23 Petra Schwille (schwille@biochem.mpg.de) 24 Allen P. Liu (allenliu@umich.edu) 25 26 \*Email address of the corresponding author: 27 (allenliu@umich.edu) Allen P. Liu 28 29 \*These authors contributed equally

30 31

# **KEYWORDS:**

32 Emulsion transfer, cDICE, GUVs, bottom-up reconstitution, actin, fascin

33 34

35

36

37

# **SUMMARY:**

This article introduces a simple method for expeditious production of giant unilamellar vesicles with encapsulated cytoskeletal proteins. The method proves to be useful for bottom-up reconstitution of cytoskeletal structures in confinement and cytoskeleton-membrane interactions.

38 39 40

#### ABSTRACT:

Giant unilamellar vesicles (GUVs) are frequently used as models of biological membranes and thus are a great tool to study membrane-related cellular processes *in vitro*. In recent years, encapsulation within GUVs has proven to be a helpful approach for reconstitution experiments in cell biology and related fields. It better mimics confinement conditions inside living cells, as opposed to conventional biochemical reconstitution. Methods for encapsulation inside GUVs are often not easy to implement, and success rates can differ significantly from lab to lab. One technique that has proven to be successful for encapsulating more complex protein systems is called continuous droplet interface crossing encapsulation (cDICE). Here, a cDICE-based method is presented for rapidly encapsulating cytoskeletal proteins in GUVs with high encapsulation efficiency. In this method, first, lipid-monolayer droplets are generated by emulsifying a protein solution of interest in a lipid/oil mixture. After being added into a rotating 3D-printed chamber, these lipid-monolayered droplets then pass through a second lipid monolayer at a water/oil interface inside the chamber to form GUVs that contain the protein system. This method simplifies the overall procedure of encapsulation within GUVs and speeds up the process, and thus allows us to confine and observe the dynamic evolution of network assembly inside lipid bilayer vesicles. This platform is handy for studying the mechanics of cytoskeleton-membrane interactions in confinement.

### **INTRODUCTION:**

Lipid bilayer compartments are used as model synthetic cells for studying enclosed organic reactions and membrane-based processes or as carrier modules in drug delivery applications<sup>1,2</sup>. Bottom-up biology with purified components requires minimal experimental systems to explore properties and interactions between biomolecules, such as proteins and lipids<sup>3,4</sup>. However, with the advancement of the field, there is an increased need for more complex experimental systems that better imitate the conditions in biological cells. Encapsulation in GUVs is a practical approach that can offer some of these cell-like properties by providing a deformable and selectively permeable lipid bilayer and a confined reaction space. In particular, *in vitro* reconstitution of cytoskeletal systems, as models of synthetic cells, can benefit from encapsulation in membrane compartments<sup>5</sup>. Many cytoskeletal proteins bind and interact with the cell membrane. As most cytoskeletal assemblies form structures that span the entirety of the cell, their shape is naturally determined by cell-sized confinement<sup>6</sup>.

Different methods are used to generate GUVs, such as the swelling<sup>7,8</sup>, small vesicle fusion<sup>9,10</sup>, emulsion transfer<sup>11,12</sup>, pulsed jetting<sup>13</sup>, and other microfluidic approaches<sup>14–18</sup>. Although these methods are still utilized, each has its limitations. Thus, a robust and straightforward approach with a high yield of GUV encapsulation is highly desirable. Although techniques such as spontaneous swelling and electroswelling are widely adopted for the formation of GUVs, these methods are primarily compatible with specific lipid compositions<sup>19</sup>, low salt concentration buffers<sup>20</sup>, smaller encapsulant molecular size<sup>21</sup>, and require a high volume of the encapsulant. Fusing multiple small vesicles into a GUV is inherently energetically unfavorable, thus requiring specificity in charged lipid compositions<sup>9</sup> and/or external fusion-inducing agents, such as peptides<sup>22</sup> or other chemicals. Emulsion transfer and microfluidic methods, on the other hand, may require droplet stabilization through surfactant and solvent removal after bilayer formation, respectively<sup>21,23</sup>. The complexity of experimental setup and device in microfluidic techniques such as pulsed jetting impose an additional challenge<sup>24</sup>. cDICE is an emulsion-based method derived from similar principles governing emulsion transfer<sup>25,26</sup>. An aqueous solution (outer solution) and a lipid-oil mixture are stratified by centrifugal forces in a rotating cylindrical chamber (cDICE chamber) forming a lipid saturated interface. Shuttling lipid monolayered

aqueous droplets into the rotating cDICE chamber results in zipping of a bilayer as droplets cross the lipid-saturated interface into the outer aqueous solution<sup>25,27</sup>. The cDICE approach is a robust technique for GUV encapsulation. With the presented modified method, not only the high vesicle yield typical for cDICE with a significantly shorter encapsulation time (a few seconds) is achieved but GUV generation time that allow for the observation of time-dependent processes (e.g., actin cytoskeletal network formation) is significantly reduced. The protocol takes about 15-20 min from the start to GUV collection and imaging. Here, GUV generation is described using the cDICE method for encapsulating actin and actin-binding proteins (ABPs). However, the presented technique is applicable for encapsulating a wide range of biological reactions and membrane interactions, from the assembly of biopolymers to cell-free protein expression to membrane fusion-based cargo transfer.

# **PROTOCOL:**

# 1. Preparation of oil-lipid-mixture

NOTE: The step needs to be performed in a fume hood following all the safety guidelines for handling chloroform.

1.1. Take 0.5 mL of chloroform in a 15 mL glass vial. Add 88  $\mu$ L of 25 mg/mL dioleoylphosphocholine (DOPC), 9.3  $\mu$ L of 50 mg/mL cholesterol, and 5  $\mu$ L of 1 mg/mL dioleoylphosphoethanolamine-lissamine rhodamine B (rhodamine PE) (see **Table of Materials**) into the 15 ml glass vial.

NOTE: The final mole fractions of DOPC and cholesterol in silicone oil/mineral oil are 69.9% and 30%, respectively. It was established that 20-30 mol% cholesterol is an optimized concentration for membrane fluidity and stability of GUVs generated using the presented technique<sup>28,29</sup>. Physiologically, these values are well within the cholesterol concentration range found in mammalian cell plasma membranes<sup>6</sup>. Lipid stocks are acquired as solutions in chloroform and stored at -20 °C. Lipid stock vials should be acclimated to room temperature before they are opened.

1.2. Pipette 7.2 mL of silicone oil and 1.8 mL of mineral oil in a second 15 mL vial (see **Table of Materials**). Generally, this needs to be done in a low-humidity glove box, mainly if the mineral oil is reused.

1.3. Mix the oils by vortexing at the maximum rotational speed (3200 rpm) for 10 s, add the mixture to the vial containing the lipid-in-chloroform mixture and immediately place it on the vortex mixer. Vortex for 10-15 s at the maximum rotational speed (3200 rpm). The resulting lipids-in-oil mix should be slightly cloudy, as the lipids are not fully dissolved in the oil but rather dispersed as small aggregates<sup>27</sup>.

1.4. Put the lipid-in-oil dispersion in a bath sonicator (see **Table of Materials**) with ultrasonic power of 80 W and operating frequency of 40 kHz at room temperature for 30 min. Use the

mixture immediately or store at 4 °C for a maximum of 24 h.

134135

# 2. Vesicle generation

136

Mount the 3D-printed shaft (Supplementary File 1) made from black resin (see Table of
 Materials) on the benchtop stir plate and set rotational speed to 1200 rpm.

139

Mount the 3D-printed cDICE chamber (Supplementary File 2) made from clear resin (see
 Table of Materials) on the shaft (Figure 1A,B).

142

2.3. Prepare actin and actin-binding proteins (ABP) solutions separately in a total volume of
 20 μL.

145

2.3.1. Prepare 1-10 μM of actin in globular actin buffer (G-buffer), including 10% ATTO 488 actin
 (see Table of Materials).

148

NOTE: 1x G-buffer comprises 5 mM of Tris-HCl, pH 8.0, and 0.2 mM of CaCl<sub>2</sub>.

150

2.3.2. Add filamentous actin polymerization buffer (F-buffer) to begin actin polymerization on ice. Keep the solutions on ice to slow down actin polymerization before the addition of a crosslinker.

154

NOTE: The 1x F-buffer contains 50 mM of KCl, 2 mM of MgCl<sub>2</sub>, and 3 mM of ATP in 100 mM of Tris, pH 7.5.

157 158

2.3.3. Wait for 15 min to allow for initiation of actin polymerization on ice before adding crosslinkers of interest at the desired molar ratio. Keep the solution on ice until encapsulation.

160 161

159

2.3.4. Prepare actin-binding proteins (ABPs) separately in a microtube (Figure 1C).

162163

164

165

166 167 NOTE: This step is performed when a combination of ABPs (e.g., myosin,  $\alpha$ -actinin, fascin, Arp2/3 complex) encapsulates with actin<sup>28–30</sup>. In such cases, the desired amount of each ABP is drawn from its stock and added into the microtube designated for ABPs. As the total solution is to be 20  $\mu$ L, stock aliquots of ABPs must be prepared so that the desired amount of the total ABP mixture does not exceed 5-6  $\mu$ L. The only ABP used in the representative results here is fascin, the preparation of which is mentioned below.

168169

2.3.4.1. Aliquot 1.57  $\mu$ L of fascin from a 1.75 mg/mL of fascin stock (see **Table of Materials**), and directly to the actin solution in step 2.7. This corresponds to 2.5  $\mu$ M of fascin in the solution.

173

2.4. Add 7.5% of density gradient medium (see **Table of Materials**) into the actin solution to create a density gradient between the outer and the inner aqueous phase to facilitate GUV sedimentation.

2.5. Dispense 700 μL of the outer solution of 200 mM of glucose into the chamber (**Figure 1D**, left).

NOTE: The osmolarity of the inner solution determines the concentration of glucose. For these experiments, the osmolarity of the inner solution is ~200 mOsm, so a 200 mM glucose solution is used as the outer solution.

2.6. Add a sufficient amount of lipid-oil mixture (>3 mL based on the chamber size) into the chamber until 60%-80% of the chamber is filled (**Figure 1D**, right). An interface will be formed between the lipid-oil mixture and the outer solution.

2.7. Transfer ABPs (prepared in step 2.3.4) into the actin solution. Using a regular 100-1000  $\mu$ L pipette, immediately transfer the 700  $\mu$ L of the lipid-oil mixture into the actin-ABP mixture (**Figure 1E**, left). Pipette up and down 8 times to generate cell-sized lipid-monolayer droplets with diameter in the range of 7-100  $\mu$ m (**Figure 1E**, middle).

NOTE: Step 2.7 needs to be completed in a few seconds to avoid any actin network assembly before encapsulation. Thus, before performing the step, ensure that pipette tips are already inserted into the pipettes and ready to transfer the mixtures.

2.8. Using the same 100-1000  $\mu$ L pipette, immediately dispense the entire emulsion into the rotating chamber. Droplets will acquire a second leaflet of lipids by crossing the lipid monolayer at the oil-outer solution interface, thereby forming GUVs (**Figure 1E**, right).

2.9. Remove the chamber from the stir plate and discard most of the lipid-oil mixture by tilting the chamber in the waste container so that a large portion of the lipid-oil mixture is drained from the large opening at the center of the chamber.

NOTE: This way, the lipid-oil mixture is drawn off the chamber, avoiding mixing of lipid-oil mixture with the outer solution in the next step.

2.10. Hold the chamber with its lid facing towards the user. Open the chamber lid and slightly tilt the chamber towards the user. The interface between the outer solution containing GUVs and the lipid-oil mixture is visible from the chamber opening (where the lid is located).

2.11. Using a pipette, collect enough outer solution containing GUVs and dispense 50-300 μL of the outer solution into a 96-well plate to obtain an appropriate density of GUVs.

NOTE: Following this protocol, a total of about 2 x  $10^5$  GUVs are released in the outer solution inside the chamber. The GUV dispersity was not quantified; however, the diameter of about 90% of GUVs is in the range of 12-25  $\mu$ m. GUVs with any diameter in the range of 7-50  $\mu$ m can be found in the population. Depending on the encapsulated density gradient medium, GUV size, and solution depth in the well plate, it takes 2-15 min for GUVs to settle down on the surface. The

yield of GUVs with reconstituted actin bundles is about 90%.

# 3. Imaging and 3D image reconstruction

3.1. Set up the 96 well plate on the stage of an inverted microscope equipped with a spinning disk (or laser scanning) confocal unit, an EMCCD or an sCMOS camera, and an oil immersion 60x objective lens (see **Table of Materials**).

3.2. Focus on any region of interest (ROI) and take a z-stack image sequence from the ROI with a z-step interval of  $0.5 \mu m$ .

NOTE: Because GUVs can be slightly displaced on the surface over time, it is recommended to capture a multi-wavelength set of images at each z-plane if multiple fluorophores are being imaged, i.e., take a group of 561 nm and 488 nm images at each z-lane at a time to capture ATTO 488 actin and Rhod PE images.

3.3. Save each z-stack image sequence in .tiff format.

3.4. Open an image sequence of interest in an image processing software (ImageJ/Fiji). Identify the image with the highest intensity. Hold "ctrl+shift+c" to open the Brightness & Contrast window and click on **Reset**.

3.5. From the ImageJ/Fiji menu, go to **Analyze > Set Scale** and enter the known physical distance and its unit for each image pixel.

3.6. From the ImageJ/Fiji menu, go to Image > Stacks > 3D project to reconstruct a 3D image from the z-stack. Set "Projection method" as Brightness Point, "Slice Spacing ( $\mu$ m)" as 0.5, and checkmark Interpolate. The default options can be used for the rest of the settings.

NOTE: z-intervals in some microscopes might not be calibrated, and the actual movement in z-direction might slightly differ from the entered z-interval (i.e.,  $0.5~\mu m$ ). In such cases, a 3D calibration specimen such as fluorescent microspheres with a known diameter can be used to obtain the actual z-interval. This value will thus be used as "Slice Spacing ( $\mu m$ )" for 3D projection.

# **REPRESENTATIVE RESULTS:**

To demonstrate the successful generation of cytoskeletal GUVs using the current protocol, fascinactin bundle structures in GUVs were reconstituted. Fascin is a short crosslinker of actin filaments which forms stiff parallel-aligned actin bundles and is purified from *E. coli* as Glutathione-S-Transferase (GST) fusion protein<sup>29</sup>. 5  $\mu$ M of actin was first reconstituted, including 0.53  $\mu$ M of ATTO488 actin in the actin polymerization buffer and 7.5% of the density gradient medium. Upon adding fascin at a concentration of 2.5  $\mu$ M and encapsulating the fascin-actin mixture, actin bundle structures were formed in GUVs. z-stack confocal image sequences of the encapsulated actin bundle structures in the Rhod PE-labeled GUVs were captured 1 h post-encapsulation (**Figure 2A**). Using this protocol, inherent competition and sorting of the encapsulated actin

crosslinkers,  $\alpha$ -actinin, and fascin, which, together, form different actin bundle patterns in a GUV-size dependent manner, was previously demonstrated<sup>29</sup>.

Like the modified inverted emulsion approach presented here, the traditional cDICE process generates cytoskeletal GUVs with high yield yet requires a syringe pump and tubing setup for controlled injection of protein solution into the rotating chamber at low flow rates the order of nanoliters per second<sup>25,31</sup>. In this approach, the emulsion is directly generated in the rotating cDICE chamber; a thin capillary is inserted in the oil phase. The protein solution is injected through a syringe pump. Droplets form and are sheared off at the capillary tip before they travel towards the aqueous outer phase, where they turn into GUVs, similar to the method described above. **Figure 2B** shows vesicles that encapsulate a reaction mixture using this approach. The reaction mix contains 6  $\mu$ M of actin which is bundled by 0.9  $\mu$ M of fascin. Here, the two methods and their results are not being compared but note that they both generate a high yield of GUVs.

#### FIGURE LEGENDS:

**Figure 1: Experimental setup for generating GUVs.** (A) Top view and side section view of the cDICE chamber. (B) Photos of the setup for the spinning chamber. (C-E) Schematic illustrations of stepwise procedures for generation of GUVs.

**Figure 2: Encapsulation of actin bundle structures**. (A) The images show representative fluorescence confocal slices of GUVs (left) and maximum projections of a confocal z-stack of actin and lipid channels (right). Fascin, 2.5 μM; actin, 5 μM (including 10% ATTO 488 actin). Scale bar =  $10 \, \mu m$ . (B) Encapsulation of actin bundle structures using conventional cDICE. The image shows a representative maximum projection of confocal fluorescence images of encapsulated actin bundles formed in the presence of fascin. Fascin, 0.9 μM; Actin, 6 μM. Scale bar =  $10 \, \mu m$ .

Supplementary File 1: 3D printed shaft design.

Supplementary File 2: Design for the 3D-printed cDICE chamber.

# **DISCUSSION:**

Different methods of generating GUVs have been explored for the creation of synthetic cells<sup>7-18</sup>. However, the complexity of the procedures, extended time to attain encapsulation, restriction of lipid types and molecular composition of the encapsulant, need for non-physiological chemicals to facilitate encapsulation, low GUV yield, and inconsistencies in encapsulation efficiency have continued to challenge researchers in this field. Considering the wide range of potential studies that can be embarked in bottom-up synthetic biology, a seamless high throughput GUV encapsulation approach that is compatible with different lipid compositions and can encapsulate any molecules regardless of size may spur new opportunities to study complex biomimicking synthetic systems. The cDICE method has eliminated most challenges and limitations inherent to prior GUV generation methods.

The approach and governing principles to generate GUVs using the cDICE method predates the

platform and have been implemented in earlier techniques such as the inverted emulsion transfer<sup>12</sup>. However, the inverted emulsion transfer method has limitations such as low vesicle yield and heterogeneity of vesicles. For the cDICE method presented here, lipids are dispersed in oil in the form of aggregates of tens of nanometers (size of lipid aggregate is dependent upon the overall concentration of lipids)<sup>27</sup>. Dispersion of lipids is in two miscible oils, where one (mineral oil) can dissolve lipids and a second oil (silicon oil) that is not miscible with lipids. This creates lipid aggregate coacervates by way of solvent-shifting<sup>32</sup>. This particular dispersion approach facilitates instant monolayer saturation of aqueous droplets, faster renewal of lipids at the oilaqueous interface as aqueous droplets continuously cross the lipid-saturated oil-aqueous interface. This also subsequently improves bilayer zipping to form GUVs and increases GUV throughput. The centrifugal forces generated by the rotating chamber are optimal for shuttling polydispersed droplets across the lipid-saturated interface. The original version of the cDICE method utilizes a microcapillary nozzle to inject the inner solution into the oil-lipid mixture. In this approach, shearing forces created by the rotating oil-lipid mixture generate aqueous droplets, eventually transforming into GUVs as described. However, with the intent to reduce the time taken to prepare injection platform, especially critical for fast reactions, such as actin network assembly and potential clogging of the microcapillary, aqueous droplets with lipid monolayers are now generated by adding the inner solution directly to the oil-lipid mixture and pipetting up and down. This approach eliminates the time lag in GUV encapsulation for a fast reaction experiment.

328 329 330

331

332

333

334

335

336

337

338

339

340

341

342

343

344

345

346

347

348

349

350

351

352

309

310

311

312

313314

315

316317

318

319

320

321

322

323

324

325

326

327

Amongst the challenges caused by earlier GUV generation methods is the restriction of lipid types (charge of lipid and phase of lipid) depending on the technique of GUV generation. Multiple lipid types, including DOPC, dioleoyl-glycero-hosphoserine (DOPS), DGS (dioleoyl-glycero-succinate), dimyristoyl-glycero-phosphocholine (DMPC), and combinations of different lipids and cholesterol at varying concentrations were tested. For all conditions, the cDICE method is shown to form GUVs with a high encapsulation efficiency at a consistently high GUV yield. Furthermore, the cDICE method has also been shown to effectively encapsulate different cellular components, including cytoskeletal proteins, cell-free expression reactions, crowding agents, dyes, and other cellular molecules of different sizes without a loss of encapsulation efficiency or decreased throughput. Furthermore, like some microfluidic GUV generation methods<sup>33</sup>, the modified cDICE can potentially permit the generation of asymmetric GUVs for future work. Different lipid compositions can be used for the inner leaflet and the outer leaflet since monolayer droplets are formed separately (inside a microtube by pipetting up and down) before zipping the bilayer inside the cDICE chamber. It was also confirmed that the lipid-oil mixture could last up to 3 weeks if kept in tight seal glass vials at 4 °C while maintaining high yield and high GUV encapsulation efficiency. Sedimentation of lipids is observed when the lipid-oil mixture is kept for long; however, one can simply vortex the lipid-oil mixture before encapsulation to re-disperse lipid aggregates. It is important to note that encapsulation quality can become compromised when the lipid-oil mixtures are kept longer, as indicated by more significant than usual lipid aggregates in the lipid-oil mix. Although not tested, these aggregates could potentially result in imperfection in bilayer zipping, and the aggregates may also end up being encapsulated with inner solution compromising the desired chemical environment.

The limitation of the presented modified approach to form aqueous droplets is in generating uniformity in the size of droplets. Although this can be improved by using microcapillary injection of inner solution at different flow rates to regulate GUV sizes, it is less desirable to monitor fast reactions like actin assembly in encapsulated GUVs. By making droplets by pipetting up and down that results in different GUV sizes, one can analyze populations of similar size vesicles. Concerns about possible oil retention in bilayers impede the adoption of most GUV generation techniques, including emulsion-based GUV generation techniques such as cDICE<sup>24</sup>. However, the amount of oil remaining in the membrane may be reduced by using organic agents such as 1-octanol, which can be removed after generating the vesicles<sup>34, 35</sup>. Future modifications to the method, possibly by changing solvent composition, need to be investigated.

There are many areas in bottom-up synthetic biology that are yet to be investigated and perhaps require cell-mimicking confinements of GUVs. Such experimental endeavors necessitate GUV generation platforms like cDICE to generate GUVs robustly while efficiently encapsulating various molecules of interest. Many cellular processes occur faster than the time it takes to encapsulate molecules using prior GUV generation techniques. As described here, actin solutions are encapsulated quickly enough to observe vesicle deformation resulting from actin network assembly. Such synthetic cells with reconstituted actin cytoskeleton have revealed features of actin network organization in the presence of different crosslinkers<sup>5,28,36</sup> and membrane remodeling<sup>28,30,31</sup>. They will inspire future work to create more sophisticated synthetic cells.

#### **ACKNOWLEDGMENTS:**

APL acknowledges support by a Humboldt Research Fellowship for Experienced Researchers and from the National Science Foundation (1939310 and 1817909) and National Institutes of Health (R01 EB030031).

## **DISCLOSURES:**

 The authors declare no conflicts of interest.

# **REFERENCES:**

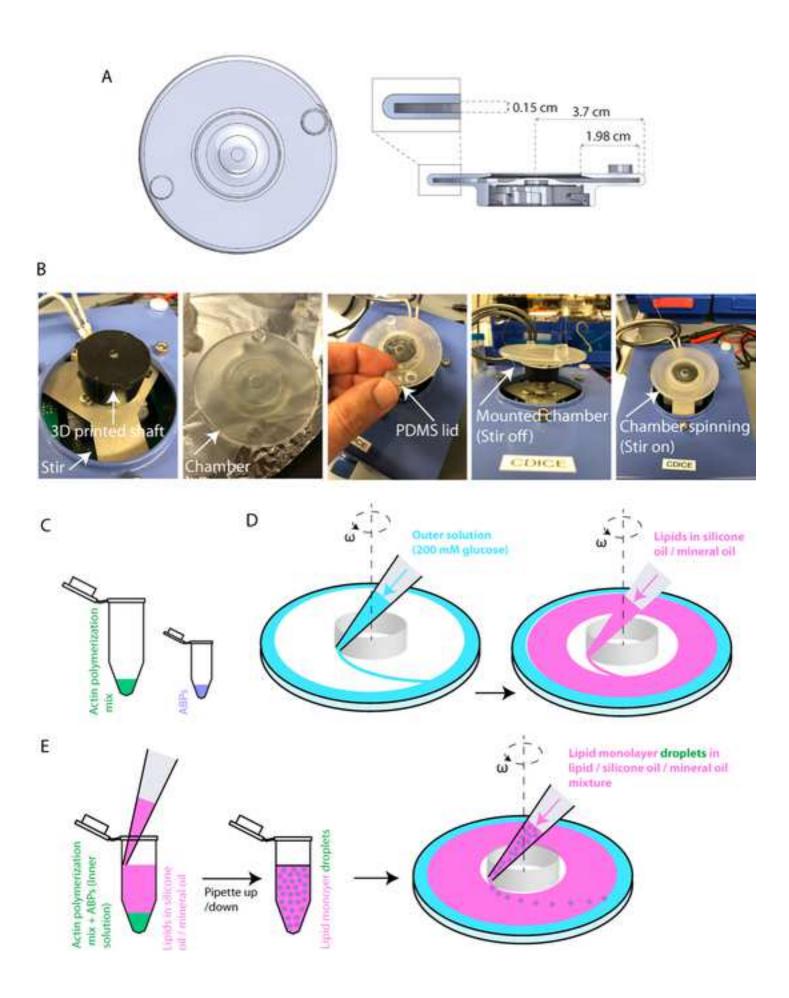
- 383 1. Groaz, A. et al. Engineering spatiotemporal organization and dynamics in synthetic cells.
- Wiley Interdisciplinary Reviews: Nanomedicine and Nanobiotechnology. **13** (3), e1685 (2021).
- Diltemiz, S. E. et al. Use of artificial cells as drug carriers. *Materials Chemistry Frontiers*. **5**, 6672-6692 (2021).
- 38. Liu, A. P., Fletcher, D. A. Biology under construction: In vitro reconstitution of cellular function. *Nature Reviews Molecular Cell Biology*. **10** (9), 644–650 (2009).
- Ganzinger, K. A., Schwille, P. More from less bottom-up reconstitution of cell biology.
   Journal of Cell Science. 132 (4), jcs227488 (2019).
- 5. Bashirzadeh, Y., Liu, A. P. Encapsulation of the cytoskeleton: Towards mimicking the mechanics of a cell. *Soft Matter.* **15** (42), 8425–8436 (2019).
- Blanchoin, L., Boujemaa-Paterski, R., Sykes, C., Plastino, J. Actin dynamics, architecture, and mechanics in cell motility. **94** (1), 235–263 (2014).
- 7. Angelova, M. I., Dimitrov, D. S. Liposome electroformation. *Faraday Discussions of the Chemical Society.* **81**, 303–311 (1986).

- 397 8. Tsumoto, K., Matsuo, H., Tomita, M., Yoshimura, T. Efficient formation of giant liposomes
- 398 through the gentle hydration of phosphatidylcholine films doped with sugar. Colloids and
- 399 *Surfaces B: Biointerfaces.* **68** (1), 98–105 (2009).
- 400 9. Bailey, A. L., Cullis, P. R. Membrane fusion with cationic liposomes: Effects of target
- 401 membrane lipid composition. *Biochemistry*. **36** (7), 1628–1634 (1997).
- 402 10. Haluska, C. K., Riske, K. A., Marchi-Artzner, V., Lehn, J. M., Lipowsky, R., Dimova, R. Time
- 403 scales of membrane fusion revealed by direct imaging of vesicle fusion with high temporal
- resolution. *Proceedings of the National Academy of Sciences*. **103** (43), 15841–15846 (2006).
- 405 11. Nishimura, K., Suzuki, H., Toyota, T., Yomo, T. Size control of giant unilamellar vesicles
- prepared from inverted emulsion droplets. Journal of Colloid and Interface Science. 376 (1), 119–
- 407 125 (2012).
- 408 12. Pautot, S., Frisken, B. J., Weitz, D. A. Production of unilamellar vesicles using an inverted
- 409 emulsion. *Langmuir*. **19** (7), 2870–2879 (2003).
- 410 13. Stachowiak, J. C., Richmond, D.L., Li, T. H., Liu, A. P., Parekh, S. H., Fletcher, D. A.
- 411 Unilamellar vesicle formation and encapsulation by microfluidic jetting. Proceedings of the
- 412 *National Academy of Sciences.* **105** (12), 4697–4702 (2008).
- 413 14. Bennett, M. K., Calakos, N., Scheller, R. H. Syntaxin: A synaptic protein implicated in
- docking of synaptic vesicles at presynaptic active zones. *Science*. **257** (5067), 255–259 (1992).
- 415 15. Lee, Y. L., Burke, B. LINC complexes and nuclear positioning. Seminars in Cell and
- 416 *Developmental Biology*. **82**, 67–76 (2018).
- 417 16. Noireaux, V., Liu, A. P. The new age of cell-free biology. Annual Review of Biomedical
- 418 Engineering. **22**, 51-77 (2020).
- 419 17. Berhanu, S., Ueda, T., Kuruma, Y. Artificial photosynthetic cell producing energy for
- 420 protein synthesis. *Nature Communications*. **10** (1), 1–10 (2019).
- 421 18. Ho, K. K. Y., Murray, V. L., Liu, A. P. Engineering artificial cells by combining HeLa-based
- 422 cell-free expression and ultrathin double emulsion template. Methods in Cell Biology. 128, 303-
- 423 318 (2015).
- 424 19. Akashi, K., Miyata, H., Itoh, H., Kinosita Jr, K. Preparation of giant liposomes in
- 425 physiological conditions and their characterization under an optical microscope. Biophysical
- 426 *Journal.* **71** (6), 3242–3250 (1996).
- 427 20. Méléard, P., Bagatolli, L. A., Pott, T. Giant unilamellar vesicle electroformation: From lipid
- 428 mixtures to native membranes under physiological conditions. Methods in Enzymology. 465,
- 429 161–176 (2009).
- 430 21. Walde, P., Cosentino, K., Engel, H., Stano, P. Giant vesicles: Preparations and applications.
- 431 ChemBioChem. **11** (7), 848–865 (2010).
- 432 22. Pécheur, E. I., Martin, I., Ruysschaert, J. M., Bienvenüe, A., Hoekstra, D. Membrane fusion
- induced by 11-mer anionic and cationic peptides: A structure– function study. Biochemistry. 37
- 434 (8), 2361–2371 (1998).
- 435 23. Morigaki, K., Walde, P. Giant vesicle formation from oleic acid/sodium oleate on glass
- 436 surfaces induced by adsorbed hydrocarbon molecules. *Langmuir*. **18** (26), 10509–10511 (2002).
- 437 24. Majumder, S., Wubshet, N., Liu, A. P. Encapsulation of complex solutions using droplet
- 438 microfluidics towards the synthesis of artificial cells. Journal of Micromechanics and
- 439 *Microengineering.* **29** (8), 83001 (2019).
- 440 25. Abkarian, M., Loiseau, E., Massiera, G. Continuous droplet interface crossing

- encapsulation (cDICE) for high throughput monodisperse vesicle design. Soft Matter. 7 (10),
- 442 4610-4614 (2011).
- 443 26. Cauter, L. Van de et al. Optimized cDICE for efficient reconstitution of biological systems
- in giant unilamellar vesicles. ACS Synthetic Biology. 10 (7), 1690–1702 (2021).
- 27. Claudet, C., In, M., Massiera, G. Method to disperse lipids as aggregates in oil for bilayers
- 446 production. *The European Physical Journal E.* **39** (1), 1–6 (2016).
- 447 28. Bashirzadeh, Y., Wubshet, N. H., Liu, A. P. Confinement Geometry tunes fascin-actin
- bundle structures and consequently the shape of a lipid bilayer vesicle. Frontiers in Molecular
- 449 *Biosciences.* **7**, 610277 (2020).
- 450 29. Bashirzadeh, Y. et al. Actin crosslinker competition and sorting drive emergent GUV size-
- dependent actin network architecture. *Communications Biology*. **4**, 1136 (2021).
- 452 30. Bashirzadeh, Y., Moghimianavval, H., Liu, A. P. Encapsulated actomyosin patterns drive
- 453 cell-like membrane shape changes. *bioRxiv*. doi: 10.1101/2021.10.20.465228 (2021).
- 454 31. Litschel, T. et al. Reconstitution of contractile actomyosin rings in vesicles. *Nature*
- 455 *Communications.* **12** (1), 1–10 (2021).
- 456 32. Vitale, S. A., Katz, J. L. Liquid droplet dispersions formed by homogeneous liquid liquid
- 457 nucleation: "The Ouzo effect." Langmuir. 19 (10), 4105–4110 (2003).
- 458 33. Pautot, S., Frisken, B. J., Weitz, D. A. Engineering asymmetric vesicles. *Proceedings of the*
- 459 *National Academy of Sciences.* **100** (19), 10718–10721 (2003).
- 460 34. Deshpande, S., Dekker, C. On-chip microfluidic production of cell-sized liposomes. *Nature*
- 461 *Protocols.* **13** (5), 856–874 (2018).

466

- 462 35. Deshpande, S., Caspi, Y., Meijering, A. E. C., Dekker, C. Octanol-assisted liposome
- assembly on chip. *Nature Communications*. **7**, 10447 (2016).
- 464 36. Wubshet, N. H., Bashirzadeh, Y., Liu, A. P. Fascin-induced actin protrusions are suppressed
- by dendritic networks in GUVs. *Molecular Biology of the Cell.* **32** (18), 1634-1640 (2021).



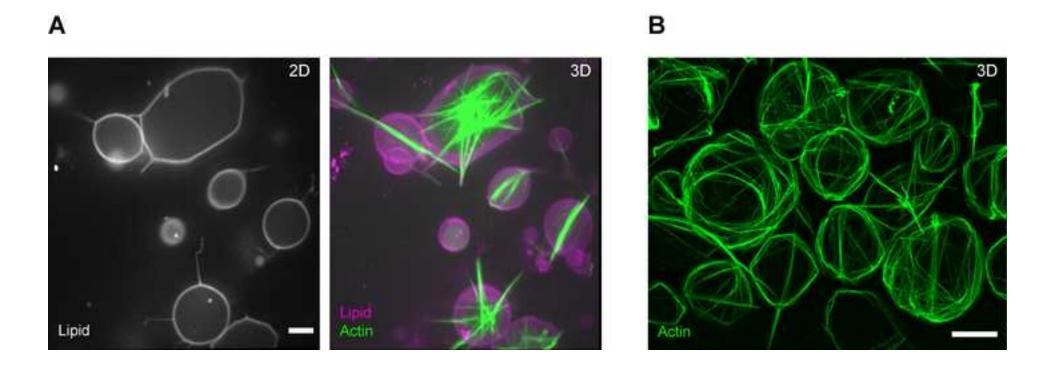


Table of Materials

Click here to access/download **Table of Materials**63332\_R1\_Table of Materials\_FINAL.xlsx

We thank the reviewers for their constructive feedback and recognizing the utility of cDICE for encapsulating cytoskeletal proteins to be useful to the scientific community. We have addressed the reviewers' comments point-by-point below.

#### Reviewer #1:

Manuscript Summary:

The manuscript describes a variation of the traditional cDICE method, where the authors dispense pre-formed water-in-oil droplets to the setup and obtain GUVs. Overall, the manuscript is clearly written and contains enough information to reproduce the method. This variation can be definitely useful to the scientific community. I have a few suggestions and comments for the authors to address, after which the manuscript can be accepted for publication.

#### Comments:

\* Introduction (line 66): There is a considerable amount of new microfluidic techniques that have been recently developed to generate GUVs. The two references currently given are relatively old. I would suggest adding some new relevant references.

Response: Relevant articles were added as suggested.

\* Introduction (line 76): The authors have mentioned the problem of oil retention with certain methods. However, the same oil retention problem can also be valid for cDICE. Authors should expand on this and explain why oil-in-the-bilayer is not a problem for cDICE, if indeed that is the case.

Response: The review's point is correct. Oil retention could be a potential issue in many GUV encapsulation techniques including cDICE. We modified the statement as our method does not offer an advantage over other techniques regarding oil retention.

"We corrected the statements as follow: "The complexity of experimental setup and device in microfluidic techniques such as pulsed jetting impose an additional challenge <sup>20</sup>. Further, concerns about possible oil retention in bilayers impede the adoption of microfluidic jetting and emulsion-based GUV generation techniques <sup>20</sup>. Continuous droplet interface crossing encapsulation (cDICE) is a method derived from similar principles governing emulsion transfer and may also have some oil retention<sup>21, 22</sup>."

\* Protocol (line 109): I assume that the design of the 3D-printed shaft be shared during the final publication?

Response: We added a subpanel, Fig.1E, to show the design and dimensions of the chamber. A bottom view of the chamber, where it connects to the 3D printed shaft is shown in the panel. The design of the shaft depends on the stir plate. We now include a statement that the design of both the shaft and chamber in .SLDPRT format will be provided upon request.

\* Protocol (line 140): Dispense using what? Just a regular pipette? How much volume at a time and at what speed? I think this is a crucial part of the experiment and this is where it differs from the traditional cDICE, so this should be explained very clearly.

Response: In steps 7 and 8, we added the necessary information suggested by the reviewer.

"6. Transfer ABPs into the actin solution and, using a regular 100-1000  $\mu$ L pipette, immediately transfer the 700  $\mu$ L of lipid-oil mixture into the actin-ABP mixture (Fig. 1D, left). Pipette up and down 8 times to generate cell-sized lipid-monolayer droplets with diameter in the range of 7-100  $\mu$ m (Fig. 1D, middle).

Note: Step 6 should take place in a few seconds to avoid any actin network assembly taking place before encapsulation. Thus, prior to performing step 6, make sure that pipette tips are already inserted into the pipettes and ready to transfer the mixtures.

- 8. Using the same 100-1000  $\mu$ L pipette, immediately dispense the entire emulsion into the rotating chamber. Droplets will acquire a second leaflet of lipids, by crossing the lipid monolayer at the oil-outer solution interface, thereby forming GUVs (Fig. 1D, right)."
- \* Protocol: Step 10 is not very clear, but I guess this becomes clear to the users after watching the video.

Response: We will demonstrate and explain this step clearly during the video production.

\* Representative results (line 200): Does 'this' approach mean traditional cDICE? Please make it clear because it is a bit confusing. Fig. 3 is then added purely for the comparison with modified cDICE (Fig. 2)? In that case, why is not the same experiment (actin-fascin) carried out so that it can be compared better? Right now, it is a bit hard to compare these two images.

Response: We replaced the image in Fig. 3 with actin images of fascin-actin bundles encapsulated using the traditional cDICE technique. It should be noted that the advantage of the modified technique over the traditional technique is rapid encapsulation of reconstituted actin and actin bundling reactions in GUVs. The yield using either technique is high. We actually did not intend to compare these methods or the results and have modified the text to not draw such comparison.

\* Fig. 1: The image resolution is quite low and will be necessary to have it in a higher resolution for the final print.

Response: We improved the resolution of images in Fig. 1A

\* Fig. 2: While the third image is labelled 3D, it basically seems to be a maximum intensity projection, summing up all the z-planes. The image construction should be properly explained to avoid confusion.

Response: We agree with the reviewer that our description was confusing. We now explain better what we mean by 2D (confocal z-slice) and 3D (maximum projection of a stack of confocal z-slices).

\* General remark: The manuscript is devoid of any analyses. For example, the authors talk about expeditious production of GUVs but there is no mention on the total number of GUVs produced, efficiency of production, the rate of production, etc. Also, there is a mention of polydisperse samples, but without any quantification. I am not sure if this is necessary for a JoVE publication, but authors should consider quantifying these important aspects of their variation and comparing it with the traditional setup.

Response: We thank the reviewer for the suggestions. We added the information about the number, size, and yield of GUVs as a note in the last step of 'Vesicle generation': "Note: Following this protocol, a total of about  $2\times10^5$  GUVs are released in the outer solution inside the chamber. We have not quantified GUV dispersity, however, the diameter of about 90% of GUVs is in the range of 12-25  $\mu$ m. GUVs with any diameter in the range of 7-50  $\mu$ m can be found in the population. Depending on the amount of encapsulated OptiPrep, GUV size, and solution depth in the well plate, it takes 2-15 minutes for GUVs to settle down on the surface. The yield of GUVs with reconstituted actin bundles is about 90%".

It should be noted that the modified method of GUV generation presented in this protocol significantly speeds up both the encapsulation of actin bundling reactions and production of GUVs. Both the traditional and modified methods (as shown in the figure below) can generate cytoskeletal GUVs with high yield.

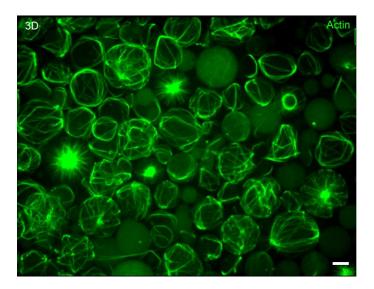


Figure 1. A high yield of actin bundle networks is obtained using the modified cDICE technique presented in the current protocol.

#### Reviewer #2:

Manuscript Summary:

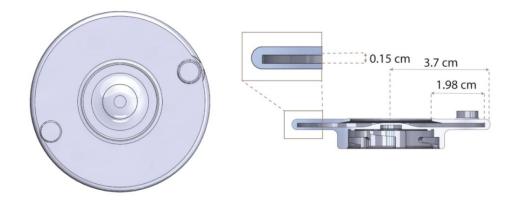
The authors describe efficient encapsulation method of cytoskeletal proteins in giant unilamellar vesicles (GUVs). They simplify the conventional method, called continuous droplet interface crossing encapsulation (cDICE) method, without loss of vesicle yield. The revised method

significantly shortens the vesicle formation time, which will enable us to observe the assembly process of the cytoskeletal networks within the vesicles under an optical microscope. Overall, the manuscript is well-organized and clearly describes the protocols. I would highly recommend publication in JoVE, but the following concerns should be addressed before publication.

# Major Concerns:

1) Spinning chamber: I think the most innovative part of this study is engineering of the spinning chamber. It will be worth to describe detailed information of the chamber, in particular, the inner diameter and height, and the resin (cat. no., company name) used for fabrication. I would highly recommend including diagrams of the spinning chamber (top view and cross section) to show dimensions in Figure 1.

Response: We thank the reviewer for the suggestions, and we have included Figure 1E showing the top view and the section view with key dimensions included. The chamber is designed with these dimensions so they are compatible with the volumes used for the inner solution, the outer solution and the oil-lipid mix used to make GUVs. Other details are subject to change by user depending on specific spinner used and will not affect GUV generation.



We also included the information about the resins in the text.

- " 1. Mount the 3D-printed shaft made from black resin (Formlabs, catalogue# RS-F2-GPBK-04) on the benchtop stir plate and set rotational speed to 1200 rpm.
- 2. Mount the cDICE chamber, 3D-printed from clear resin (Formlabs, catalogue# RS-F2-GPCL-04), on the shaft."
- 2) Lines 193-202: The authors show the representative image of actin-encapsulated GUVs prepared by the traditional cDICE method in Figure 3, then briefly explain and compare the encapsulation method with the newly proposed one. I cannot find any reasons why the authors include this image, because ABPs used for Figure 2 and Figure 3 are different and the actin concentration is not identical between two figures. Aster-like bundles are formed in Figure 2, but ring-shaped bundles are formed in Figure 3. Therefore, it is hard to discuss encapsulation efficiency of the two methods by comparing these images. If the authors want to compare the methods, they should provide images of GUVs prepared by the same molecular components.

Response: We thank the reviewer for the suggestion. We have now removed figure 3 and added image of fascin bundled actin network GUVs generated using the traditional cDICE method. We do not intend to compare these methods or the results and have modified the text to not draw such comparison.

#### Minor Concerns:

1) Line 117: Doesn't F-buffer contain any buffer solutions such as Tris-HCl like G-buffer? Please provide complete composition of F-buffer.

Response: The buffer used for F-Buffer is 100 mM Tris, pH 7.5 and we have now included this information.

2) Lines 137 and 138: "Step 6" should be "Step 7".

Response: We have made changes to, previously, Step 6 and Step 7 for better clarity.

3) Line 187: Please describe how to prepare fascin in the main text, or put the catalog number and company name if it was purchased.

Response: Fascin was purchased and we have added details including catalog number in the table of materials.

4) Reference 10: Please provide the journal name, and the volume and page numbers.

Response: We thank the author for spotting the error in the reference. We corrected the reference.

5) Table of Materials: The catalog numbers of DOPC and Rhodamine-PE include garbled characters. Please revise them.

Response: We thank the reviewer for flagging the error. We have made the correction and all characters should appear correctly.

6) Table of Materials: Sucrose will not be used in the protocol. Please check again and remove from the table if it is not necessary.

Response: It is correct that sucrose is not used anywhere in the process and we have now removed sucrose from the table of materials.

#### Reviewer #3:

Manuscript summary:

This manuscript titled "Rapid encapsulation of reconstituted cytoskeleton inside giant unilamellar vesicles" from Bashirzadeh et. al, describes in detail a very efficient method to generate GUVs that encapsulate cytoskeletal proteins. It has been a great challenge to generate GUVs with

desired lipids and physiologically relevant salt buffers while at the same time fill with proteins of interests. This manuscript and the video will thus be a great advance for the scientific community. The manuscript describes a method based on cDICE. In this method, proteins of interests are first encapsulated in water-in-oil emulsions covered with lipids; then, these emulsions are passed through a lipid monolayer by centrifugation to obtain the second lipid layer, resulting in the formation of cell-sized unilamellar vesicles. Overall, the experimental details provided by the manuscript is sufficient.

# Comments

1. Line 49, it should be "allows us to observe the dynamic evolution of the time-sensitive reactions".

Response: We thank the reviewer for the suggestion. We modified the sentence as follow: "This method not only simplifies the overall procedure of encapsulation within GUVs, but also speeds up the process and thus allows us to confine and observe the dynamic evolution of network assembly inside lipid bilayer vesicles."

2. Line 76-77, the issue of oil being trapped in the membranes is not only for the jet-based method but for all the emulsion-based method, including the current cDICE method. This should be clearly stated.

Response: The review's point is correct. Oil retention could be a potential issue in many GUV generation techniques including cDICE. We corrected the statements as follow: "The complexity of experimental setup and device in microfluidic techniques such as pulsed jetting impose an additional challenge <sup>20</sup>. Further, concerns about possible oil retention in bilayers impede the adoption of microfluid jetting and emulsion-based GUV generation techniques <sup>20</sup>. Continuous droplet interface crossing encapsulation (cDICE) is a method derived from similar principles governing emulsion transfer and may also have some oil retention <sup>21, 22</sup>."

3. Along the same line as in 2, recent studies have showed that by using octanol as an agent, one can limit the amount of oil present in the membranes. It would be information for the readers if the authors could mention these studies.

DOI: 10.1038/ncomms10447

https://doi.org/10.1038/nprot.2017.160

Response: We thank the author for the suggestion. This is indeed a useful information for readers. We added the following statement to address it: "However, the amount of oil remained in the membrane may be reduced by the use of organic agents such as 1-octanol, which have been used for generation of vesicles<sup>13, 21</sup>, although this has not been tested in cDICE."

4. Line 85, the time required to perform the current cDICE method should be specified.

Response: We revised the statement and included the suggested information as follow: "With our modified method, we combine the high vesicle yield typical for cDICE with a significantly shorter encapsulation time (a few seconds) and GUV generation time that allow for the observation of time-dependent processes (e.g., actin cytoskeletal network formation). The protocol takes about 15-20 min from the start to GUV collection and imaging".

5. Line 92, it is important to mention that chloroform must be handled in a chemical hood.

Response: We thank the author for reminding this important note. We modified the beginning of the step 1 as follow, "1. Inside a fume hood and following other safety guidelines for handling chloroform, put 0.5 ml chloroform in a 15 ml glass vial."

6. Line 93, what is the reason to have cholesterol in the mixture?

Response: We use several methods for generation of GUVs in our lab and established that 20-30 mol% cholesterol is an optimized concentration for membrane fluidity and GUV stability. We have used 30 mol% cholesterol, as described in the protocol, for consistency across our experiments. Physiologically, this value is well within the range of cholesterol concentration found in plasma membranes of mammalian cells.

We provided this information at the end of the step 1 of 'oil-lipid-mixture' section.

7. Line 102, what is the speed?

Response: The maximum speed of the vortexer is 3,000 rpm. We added this value in the text as well.

8. Line 104, is this step done by a bath sonicator or a tip sonicator. It would be informative to specify the speed/strength of the sonication step. Or if possible, provide the company name and category number of the sonicator.

Response: This information was added to text.

- "4. Put the lipid-in-oil dispersion in a bath sonicator (FS20, Fisher Scientific) with ultrasonic power of 80 W and operating frequency of 40 kHz at room temperature for 30 minutes. Use the mixture immediately or store at 4°C."
- 9. Line 104, at which temperature the sonication step is done?10. Line 104, should be "Use the mixture immediately..."

Response: Sonication step is done at room temperature. We added this information in the text.

- "4. Put the lipid-in-oil dispersion in a sonicator at room temperature for 30 minutes. Use the mixture immediately or store at 4°C."
- 11. Line 109, it would be very helpful to provide the dimensions of the shaft and the chamber. Or even better, with the design drawings if possible.

Response: We added a subpanel, Fig.1E, to show the design and dimensions of the chamber. A bottom view of the chamber, where it connects to the 3D printed shaft is shown in the panel. The design of the shaft depends on the stir plate. We included the design of both the shaft and chamber in .SLDPRT format in the supplementary information.

12. Line 114, conventionally, G-buffer states for "Globular actin buffer".

Response: We corrected our mistake. We should point out that Cytoskeleton market G-buffer general actin buffer.

13. Line 117, it should be mentioned that performing this step in ice is to slow down actin polymerization

Response: We thank the reviewer for the suggestion, and we have added a sentence to describe the need for the addition of F-buffer in ice.

"Keeping solutions on ice will help slow down actin polymerization prior to addition of a crosslinker".

14. Line 122, any specific reason for using a PCR tube here?

Response: Volumes of ABPs are very small and easier to handle in small micro test tubes. We now however refer to them more generally as "microtubes" in the manuscript, which might be a better description of the tubes we use.

15. Line 123, is it known if the OptiPrep solution influence actin polymerization and ABPs binding to actin?

Response: Multiple actin network encapsulation in GUVs with and without Optiprep showed no difference in the assembly of networks. Optiprep is only used to induce density gradient for fast sedimentation of GUVs. In vitro cell studies using similar contrast media has also shown that Optiprep does not affect cellular cytoskeleton <sup>1</sup>. Reference below.

- 1. Franke, R.-P., Scharnweber, T., Fuhrmann, R., Mrowietz, C., Jung, F. Effect of radiographic contrast media (Iodixanol, Iopromide) on the spectrin/actin-network of the membranous cytoskeleton of erythrocytes. *Clinical hemorheology and microcirculation*. **54** (3), 273–285 (2013).
- 2. Pautot, S., Frisken, B.J., Weitz, D.A. Engineering asymmetric vesicles. **100** (19), at <a href="https://www.pnas.orgcgidoi10.1073pnas.1931005100">www.pnas.orgcgidoi10.1073pnas.1931005100</a> (2003).

16. Line 137 and 138, it should be step "7"

Response: We have made changes to, previously, Step 6 and Step 7 for better clarity as shown below.

17. Line 145, it is not clear to me where the "large opening" is. It is hard to image how this step is done.

Response: We thank the reviewer for their comment. We have rephrased this to better clarify the sentence as quoted below. Furthermore, the newly added Figure 1E may better demonstrate what is referred to as "large opening".

"Remove the chamber from the stir plate and discard most of the lipid-oil mixture in the chamber by tilting the chamber in the waste container so that a large portion of lipid-oil mixture is drained from the large opening at the center of the chamber".

We will also demonstrate and explain this step clearly during video production.

18. Line 184, what did the authors want to say when mentioned that fascin is a "short" crosslinker? What does "short" refer to?

Response: this is a rather common description and refers to the length of the crosslinker and indicates how closely filaments are bundled. We have clarified this in the manuscript.

19. Line 212, for 3D image, is it maximum intensity projection? It should be specified.

Response: We thank the reviewer for the suggestion. We have now revised the figure caption as follow:

"(A) Encapsulation of actin bundle structures using the presented protocol. The images show representative fluorescence confocal slices of GUVs (left) and maximum projections of a confocal z-stack of actin and lipid channels (right). Fascin, 2.5  $\mu$ M; actin, 5  $\mu$ M (including 10% ATTO 488 actin). Scale bar, 10  $\mu$ m. (B) Encapsulation of actin bundle structures using conventional cDICE. The image shows a representative maximum projection of confocal fluorescence images of encapsulated actin bundles formed in the presence of fascin. Fascin, 0.9  $\mu$ M; Actin, 6  $\mu$ M; Scale bar, 10  $\mu$ m."

20. Line 216, it says "2D" in the figure. This should be corrected to the right one

Response: Per other reviewer's comments, we have now replaced actin images of encapsulated talin-vinculin-actin bundles with fascin-actin bundles generated using the traditional cDICE method. We also combined Figures 2 and 3 into one figure.

21. In the Discussion, the authors should comment on the potential oil being trapped in the membranes for this modified cDICE method.

Response: Emulsion-based methods suffer from potential oil retention in bilayers and we have explicitly mentioned it in the introduction and discussion per reviewer's suggestions. Quoted below.

"Furthermore, the cDICE method, as an emulsion-based technique, does not eliminate potential bilayer oil retention. Future modifications to the method, possibly by changing solvent composition, need to be investigated."

22. In the Discussion, the authors should discuss how "rapid" their method is compared to the others, especially this is one of the key points in the title of this manuscript

Response: We thank the reviewer for the suggestion. We believe that we have sufficiently discussed how rapid our method by eliminating the need for using microfluidic nozzle to generate aqueous droplets. We have quoted part of the section where this is discussed below

"However, with the intent to reduce the time taken to prepare injection platform, especially critical for fast reactions, such as actin network assembly, and potential clogging of the microcapillary, we now generate aqueous droplets with lipid monolayers by adding the inner solution (created by pipetting up and down) directly to the oil-lipid mixture. This approach eliminates the time lag in GUV encapsulation for a fast reaction experiment."

We also quote a part of the introduction that is now added to address the reviewer's point.

"The cDICE approach is, in our experience, a robust technique for GUV encapsulation. With our modified method, we combine the high vesicle yield typical for cDICE with a significantly shorter encapsulation time (a few seconds) and GUV generation time that allow for the observation of time-dependent processes (e.g., actin cytoskeletal network formation). The protocol takes about 15-20 min from the start to GUV collection and imaging."

23. In the Discussion, could the authors comment on the potential application of the cDICE method in generating asymmetric membranes?

Response: We agree with the reviewer's comment, and we have added this to the discussion to elaborate.

"Furthermore, like some microfluidic GUV generation methods <sup>28</sup>, our modified cDICE can potentially permit the generation of asymmetric GUVs. Different lipid composition can be used for the inner leaflet and the outer leaflet since monolayer droplets are formed separately (inside a microtube by pipetting up and down) before zipping the bilayer inside the cDICE chamber."

Supplementary File 1-Shaft design

Click here to access/download **Supplemental Coding Files**cDICE\_base\_v2-2\_nS (1).SLDPRT

Supplementary File 2-Chamber design

Click here to access/download **Supplemental Coding Files**finalcdice (1).SLDPRT