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TITLE:

Measuring Cardiac Output in a Swine Model

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SUMMARY:

Thermodilution, pressure-volume loop catheters, and contrast ventriculography are reliable and accurate methods for determining cardiac physiology such as stroke volume and cardiac output in a laboratory setting in swine.

ABSTRACT:

Swine are frequently used in medical research given their similar cardiac physiology to that of humans. Measuring cardiac parameters such as stroke volume and cardiac output are essential in this type of research. Contrast ventriculography, thermodilution, and pressure-volume loop (PV-loop) catheters can be used to accurately obtain cardiac performance data depending on which resources and expertise are available. For this study, five Yorkshire swine were anesthetized and intubated. Central venous and arterial access was obtained to place the necessary measurement instruments. A temperature probe was placed in the aortic root. A cold saline bolus was delivered to the right atrium and temperature deflection curve was recorded. Integration of the area under the curve allowed for the calculation of the current cardiac output. A pigtail catheter was percutaneously placed in the left ventricle and 30 mL of iodinated contrast was power injected over 2 seconds. Digital subtraction angiography images were uploaded to volumetric analysis software to calculate the stroke volume and cardiac output. A pressure volume-loop catheter was placed into the left ventricle (LV) and provided continuous pressure

45 and volume data of the LV, which allowed the calculation of both stroke volume and cardiac
46 output. All three methods demonstrated good correlation with each other. The PV-loop catheter
47 and thermodilution exhibited the best correlation with a 3% error and a Pearson coefficient of
48 0.99, with 95% CI=0.97 to 1.1, (p=0.002). The PV-loop catheter against ventriculography also
49 showed good correlation with a 6% error and a Pearson coefficient of 0.95, 95% CI=0.96 to 1.1
50 (p=0.01). Finally, thermodilution against ventriculography had a 2% error with r=0.95, 95%
51 CI=0.93 to 1.11, (p=0.01). In conclusion, we state that the PV-loop catheter, contrast
52 ventriculography, and thermodilution each offer certain advantages depending on the
53 researcher's requirements. Each method is reliable and accurate for measuring various cardiac
54 parameters in swine such as the stroke volume and cardiac output.

55

56 **INTRODUCTION:**

57 Swine are frequently used in hemorrhage control and resuscitation research due to their similar
58 physiology to humans. Integral to resuscitation research is continuous cardiac output monitoring
59 to assess the physiological response to interventions. Several clinical systems exist such as
60 pulmonary artery (PA) catheters and pulse contour analysis-based systems¹. Additionally,
61 echocardiography (echo), computed tomography (CT) and magnetic resonance imaging (MRI) can
62 all be used to capture hemodynamic data. Images obtained during end-diastole and systole can
63 be used to determine the volume of blood ejected during that cardiac cycle. While these
64 techniques are minimally invasive, they only present data acquired at the time of imaging and do
65 not provide continuous measures². They are also either largely operator dependent (echo) or
66 require advanced, expensive equipment (CT and MRI). Given different laboratories' capabilities
67 and resources, there are various alternative methods to measure the cardiac output optimally in
68 each instance.

69

70 Thermodilution is a common method of measuring cardiac output in the clinical setting using a
71 Swan-Ganz catheter³. This method can be recreated in a laboratory setting in swine to directly
72 measure the cardiac output. Contrast ventriculography can also be utilized if the fluoroscopic
73 capability is readily available⁴. Finally, pressure-volume loop catheters offer a means of directly
74 measuring the ventricular pressure and volume on a beat-to-beat basis and can generate more
75 nuanced data⁵. This method utilizes electrical admittance and Wei's equation to measure the
76 chamber volume. Compared to older conductance-based catheters, admittance catheters
77 eliminate the parallel conductance phenomenon between the blood and the cardiac muscle,
78 thereby producing more accurate measurements without requiring repeated calibration⁶.

79

80 The aim of this study is to validate the accuracy of these three methods against each other in
81 terms of measuring cardiac stroke volume and output in a healthy swine model. Ultimately, each
82 investigator can choose which approach suits their needs the best, depending on their study
83 requirements and what resources are available to them.

84

85 **PROTOCOL:**

86 Procedures were approved by the University of Maryland, Baltimore Institutional Animal Care
87 and Use Committee (Approval #0320017) and conformed to National Institutes of Health
88 guidelines for ethical animal research. Five adult male Yorkshire swine weighing between 50 and

89 70 kg were enrolled into the study. This study utilized a digital data collection system and paired
90 software to record all hemodynamic and temperature data. Measuring cardiac parameters in the
91 swine model consisted of the following steps: preparation, thermodilution, ventriculography, PV-
92 loop catheter insertion, and finally euthanasia. All five animals underwent each of the three
93 cardiac output measuring protocols.

94

95 **1. Animal selection and housing**

96

97 1.1. Use adolescent male Yorkshire swine (*Sus Scrofa*) weighing 50-70 kg.

98

99 1.2. House animals in caging at least 30 square feet in area with high-carbon bedding such as hay,
100 straw, or pine shavings. House the animal individually, the night prior to the procedure.

101

102 1.3. Allow acclimation period for new animals as per institution guidelines.

103

104 NOTE: This is typically 48-72 h for large mammals⁷.

105

106 1.4. Feed animals a standard diet and provide free access to water until the night before the
107 experiment.

108

109 1.5. Fast the animals the night before the procedure to minimize aspiration risk during
110 endotracheal intubation.

111

112 1.6. Monitor animals' health weekly by inspecting the skin for signs of injury such as scabs,
113 scrapes, or abrasions. Ensure normal work of breathing (15-30 breaths/min) and proper,
114 interactive behavior. Ensure that the oral mucosa is pink, moist, and without discharge.

115

116 1.6.1. Weigh animals regularly to confirm that they have adequate nutrition. Report any
117 abnormalities to the veterinary staff and then exclude the animal from the protocol.

118

119 **2. Sedation and induction of general anesthesia**

120

121 2.1. Sedate the animal in its housing area by intramuscular injection of Telazol (4-5 mg/kg)/
122 Xylazine (1.8-2.2 mg/kg) in the fat pad caudal to the ear.

123

124 2.2. Wait until the animal is fully sedated and there is minimal to no response to stimulation to
125 ensure safe handling and transport of the animal.

126

127 2.3. Transport the animal from the housing area to the procedure room and place it in dorsal
128 recumbency on the operating table.

129

130 2.4. Place a pulse oximetry probe on the animal's ear and begin ventilating the animal with a
131 snout mask using a mechanical ventilator with 100% O₂. Ensure proper seal of rubber gasket of

132 the mask around the snout. Once a proper seal is ensured, administer 3-4% isoflurane until
133 general anesthesia is induced and the jaw is relaxed.

134
135 NOTE: Be sure to follow institutional guidelines for inhaled volatile agent use. In general, the
136 procedure room must be well ventilated, and a proper scavenging/ventilation mechanism must
137 be used to eliminate inhalation exposure.

138
139 2.5. Place an orotracheal tube using a laryngoscope by turning off the isoflurane vaporizer and
140 removing the snout mask. Have a second person hold the jaws open while the operator inserts
141 the laryngoscope and displaces the epiglottis ventrally away from the soft palate. Once the vocal
142 cords are visualized, insert an 8-0 endotracheal (ET) tube through vocal cords by at least 5 cm.

143
144 2.6. Inflate the ET cuff with 10 mL of air and secure the ET tube to the animal's snout using
145 umbilical tape. Confirm the tube placement by the chest rise, end-tidal CO₂, and/or chest
146 auscultation.

147
148 2.7. Connect the ET tube to the anesthetic machine with a heat and moisture exchanger.

149
150 2.8. Adjust the mechanical ventilator settings to deliver an inspired O₂ fraction of 30%, with a
151 tidal volume 7-10 mL/kg, and a respiratory rate of 10-16 breaths/min, to maintain an end-tidal
152 CO₂ tension of 38-42 mmHg.

153
154 2.9. Return and maintain inhaled anesthetic using 1.5-3% isoflurane. Monitor the animal for signs
155 of pain and discomfort such as involuntary movements or tachycardia. Adjust isoflurane until
156 movements extinguish or tachycardia resolves.

157 158 **3. Surgical site sterilization and preparation**

159
160 3.1. Clip the hair overlying and percutaneous access sites (bilateral ventral neck) by using an
161 electric hair clipper.

162
163 3.2. Prepare and scrub all percutaneous puncture sites with betadine and isopropyl alcohol and
164 allow to dry completely.

165
166 3.3. Place sterile drapes around the operative sites to preserve the sterile surgical fields and
167 prevent contamination. Secure these in place with staples.

168
169 3.4. Secure the animal to the operating table by restraining forelimbs and hindlimbs to the table
170 using either tape or rope. Place the heating pad underneath the animal and set to 37 °C.

171
172 3.5. Apply a water-based lubricant to the tip of the temperature probe and insert the probe into
173 the rectum to provide continuous body temperature data.

174

175 3.6. Place the ECG adhesive electrodes on the right and left lateral chest wall. Attach the ECG
176 leads to the adhesive electrodes and connect ECG leads to the data collection unit.

177
178 3.7. Carefully, flip the animal to ventral recumbency, ensuring that the airway tubing and ECG
179 leads are controlled during transfer.

180 181 **4. External jugular vein cannulation**

182
183 NOTE: Jugular venous access is obtained for the right atrial venous cannula insertion during the
184 thermodilution procedure.

185
186 4.1. Use ultrasound (US) guidance to locate the external jugular vein in the jugular furrow located
187 in the lateral neck region. Puncture the skin with an 18 G needle placed at a 45° angle to the skin
188 and advance the tip into the venous lumen under US guidance.

189
190 4.2. Pass an 0.035" Seldinger guidewire through the needle and into the venous lumen. Remove
191 the needle while leaving the guidewire in place within the venous lumen.

192
193 4.3. Make a 5 mm skin incision adjacent to the wire using a #11 blade scalpel, and thread a 15
194 cm, 7 Fr sheath with a dilator into the vein over the guidewire. Remove the guidewire and the
195 dilator. Ensure that the sheath remains in position. Stitch the sheath in place by suturing it to the
196 skin with 3-0 silk sutures.

197
198 4.4. Repeat steps 4.1 through 4.3 to cannulate the contralateral external jugular vein.

199 200 **5. Carotid artery cannulation**

201
202 NOTE: The carotid artery cannulation is performed to provide access to the LV and aortic root
203 during thermodilution, contrast ventriculography, and PV-loop catheter insertion.

204
205 5.1. Locate the carotid artery lateral to the trachea using an US probe. Ensure pulsatile flow using
206 color Doppler imaging if available.

207
208 5.2. Puncture the skin with an 18 G needle placed at a 45° angle to the skin and advance it into
209 the arterial lumen under US vision. Advance an 0.035" Seldinger guidewire through the needle
210 and into the arterial lumen. Remove the needle while leaving the guidewire in position within
211 the arterial lumen.

212
213 5.3. Make a 5 mm skin incision adjacent to the wire with a #11 blade scalpel, and thread a 20 cm
214 7 Fr sheath with a dilator into the artery over the guidewire. Leave 5-10 cm of the sheath outside
215 of the skin. Remove the guidewire and the dilator and ensure that the sheath remains in position.
216 Secure the sheath in place by suturing it to the skin with 3-0 silk sutures⁸.

217 218 **6. Cardiac output measurement**

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NOTE: All of the following methods are performed sequentially in each of the 5 animals used in this study.

6.1. Thermodilution

6.1.1. Insert a T-type thermocouple probe via the carotid arterial sheath and guide the probe into the aortic root using fluoroscopic guidance.

6.1.2. Attach the probe to the data collection system. Allow several minutes of data collection to establish a confident baseline aortic temperature. A confident baseline temperature is achieved when the temperature stays within 1 °C of the central value over 2-3 min of data collection.

6.1.3. Next, insert a 5 Fr, 110 cm catheter via the external jugular vein sheath and navigate the catheter to the right atrium using fluoroscopy.

6.1.4. Once the position is verified, forcefully flush 20 mL of 12 °C saline into the catheter.

6.1.5. Observe the temperature deflection curve on the data collection software. Highlight this region and use the cardiac output function of the software to calculate cardiac output (**Figure 1**).

6.1.6. Repeat this process 3-5 times as needed to obtain an average value across these measurements.

6.2. Ventriculography

6.2.1. Using portable x-ray fluoroscopic guidance, insert a 0.035" guidewire via the carotid arterial sheath and into the left ventricle. Advance the sheath so that the tip traverses the aortic valve. Remove the 0.035" guide wire and insert an 80-cm marker pigtail catheter via the carotid arterial sheath so that the pigtail is resting in the LV apex. Withdraw the sheath 5 cm while leaving the pigtail in place so that the sheath is no longer within the LV.

6.2.1.1. Ensure that all personnel in the room are wearing 0.5 mm lead apron equivalents. Have anyone within 1 m of the emitter wear leaded glasses.

6.2.1.2. Minimize the beam-on time and ensure that the emitter is well collimated to reduce exposure to lab personnel.

6.2.1.3. Ensure that all personnel stand as far away from emitter as possible while still being able to perform the procedure in order to reduce exposure.

6.2.2. Attach the catheter to a contrast power injector with at least 30 mL of iodinated contrast loaded. Note the current heart rate of the animal.

263 6.2.3. Configure the power injector to deliver 15 mL/s of contrast for a total of 30 mL and arm
264 the device.

265
266 6.2.4. Configure the fluoroscope for digital subtraction angiography (DSA) at 30 frames/s at 30°
267 left anterior obliquity.

268
269 6.2.5. Start DSA on the fluoroscope and wait for the image to subtract. Begin the power injection
270 as soon as the subtraction image is shown by the fluoroscopy machine. Do this by pressing the
271 injector button as soon as the fluoroscopy machine subtracts the radio-opaque material from the
272 image so that only the LV chamber is opacified during the image series (**Figure 2A**).

273
274 NOTE: Alternatively, classical fluoroscopy can be used for ventriculography if DSA is unavailable.

275
276 6.2.6. Upload these images to a picture archiving and communication system (PACS).

277
278 6.2.7. Import the ventriculogram images into a quantitative imaging software.

279
280 6.2.8. Using the left ventricular analysis function, calibrate the software to the image using the 1
281 cm marks on the marker pigtail as a reference.

282
283 6.2.9. Click on the **End Diastole** button and search the DSA images for the frame depicting the
284 largest LV volume indicating end-diastole. Then, trace the LV border using the mouse in small
285 increments to ensure accuracy.

286
287 6.2.10. Next click on the **End Systole** button and search for the frame depicting end systole where
288 LV volume is the least. Again, trace the LV border in the same manner as the previous step.

289
290 6.2.11. Click the **Analyze** button. The program then performs quantitative volumetric analysis
291 using the Dodge-Sandler area-length method⁹ to calculate end-systolic volume, end-diastolic
292 volume, as well as stroke-volume. The data is then output in an LV analysis document.

293
294 6.2.12. Determine the cardiac output by multiplying the measured stroke volume by the
295 previously recorded heart rate.

296
297 6.3. Pressure-volume loop catheter

298
299 6.3.1. Presoak the PV-loop catheter in normal saline for at least 20 min prior to the use. Connect
300 the catheter to the data collection system.

301
302 6.3.2. Insert the tip of the PV-loop catheter containing the pressure transducer into a syringe of
303 saline and hold the pressure transducer just underneath the meniscus. Using the coarse and fine
304 adjustment buttons on the catheter module, adjust the output pressure signal until it reads 0
305 mmHg on the data collection software.

306

307 6.3.3. Calibrate the PV-loop catheter blood resistivity and stroke volume per the manufacturer's
308 instructions.

309
310 NOTE: The manufacturer suggests using a blood resistivity of 1.5 mΩ and a stroke volume of 60
311 mL for large animal models.

312
313 6.3.4. As in step 6.2.1, insert a 0.035" guidewire into the carotid arterial sheath and advance it
314 into the LV using fluoroscopic guidance. Advance the sheath until it traverses the aortic valve.
315 Remove the guidewire leaving the sheath in place and insert the PV-loop catheter under
316 fluoroscopic guidance via the carotid arterial sheath until the pigtail portion is resting in the LV
317 apex (Figure 2B). Withdraw the sheath ~5 cm so that it is no longer within the LV while leaving
318 the pigtail in place.

319
320 6.3.5. Per manufacturer instructions, perform a baseline scan prior to collecting data by
321 navigating to the **Baseline scan** option on the data acquisition screen and press the **Enter** button.
322 A baseline scan is taken using the PV-loop catheter system to confirm accurate heart rate
323 measurement. Press the **Enter** button again to begin pressure and volume data acquisition. The
324 volume segments can be scrolled through to acquire the best volume waveform.

325
326 6.3.6. Check the pressure volume curve being output to the data collection software. Ensure that
327 the PV-loop is recorded adequately, which should be rectangular with smooth edges. (Figure 2C).
328 If not, gently reposition the catheter either by twisting, or moving back and forth until an
329 adequate loop is recorded. Calculate stroke volume and cardiac output by multiplying the heart
330 rate by the difference between the end-diastolic and end-systolic volume.

331
332 6.3.7. Secure the catheter in place either with tape or suture to ensure adequate positioning
333 throughout.

334 335 **7. Euthanasia**

336
337 7.1. Euthanize the animal using >2 mEq/kg potassium chloride (50-70 mL of 2 mEq/mL KCl)
338 injection via the jugular vein sheath.

339
340 7.2. Continue general anesthesia and cardiac monitoring until ECG tracing shows no cardiac
341 electrical activity and end-tidal CO₂ tension reaches 0 mmHg.

342
343 NOTE: Hemodynamic monitoring was maintained throughout the experiment.

344 345 **REPRESENTATIVE RESULTS:**

346 The weight of the swine ranged from 51.4 kg to 61.5 kg with a mean weight of 56.6 ± 3.6 kg. The
347 average stroke volumes measured by PV-loop catheter, ventriculography, and thermodilution
348 across all five subjects were 58.0 ± 12.0 mL, 57.6 ± 8.5 mL, and 53.0 ± 9.8 mL, respectively. The
349 average cardiac outputs measured by a PV-loop catheter, ventriculography, and thermodilution
350 across all five subjects were 5.0 ± 1.1 L/min, 5.3 ± 1.2 L/min, and 5.2 ± 1.0 L/min, respectively

351 (Table 1). Figure 3 shows the scatter plots of cardiac output measurements by each of the three
352 methods compared with the other two. The line of identity demonstrates where all points would
353 fall if there was perfect agreement between each test. The line of identity for all three methods
354 falls within the 95% confidence interval range. When measuring cardiac output, the PV-loop
355 catheter compared to thermodilution demonstrated the best correlation with a Pearson
356 coefficient of $r=0.99$ (Figure 3A). The slope of the regression line was 1.03 indicating a 3% error
357 with 95% CI=0.97 to 1.1, $p=0.002$. As seen in Figure 3B, the PV-loop catheter compared against
358 ventriculography also exhibited good correlation with a Pearson coefficient $r=0.95$ The slope of
359 the regression line was 1.06 indicating a 6% error with 95% CI=0.96 to 1.1, $p=0.01$. Lastly,
360 ventriculography compared to thermodilution demonstrated agreement as well with a Pearson
361 coefficient of $r=0.93$ (Figure 3C). The slope of the regression line was 1.02, indicating a 2% error
362 with 95% CI=0.93 to 1.1 and $p=0.01$.

363

364 FIGURE AND TABLE LEGENDS:

365

366 **Figure 1: Example of thermodilution curve.** An example thermodilution curve in a single
367 representative animal demonstrating the deflection of temperature curve as a cold saline bolus
368 is delivered. The area under the curve is used to calculate the cardiac output.

369

370 **Figure 2: Ventriculogram and PV Loops.** (A) Left ventriculogram. (B) Successful PV-loop catheter
371 placement in the apex of the LV. (C) Example of high-quality PV loops.

372

373 **Figure 3: Linear regression of cardiac output measurements.** Linear regression of cardiac output
374 measurements in five different animals using (A) PV-loop catheter versus thermodilution, (B) PV-
375 loop catheter versus ventriculography, and (C) thermodilution versus ventriculography. The line
376 of identity (red) falls within the 95% confidence range (dotted) of the best-fit-line (black) among
377 all three methods.

378

379 **Table 1: Average results of cardiac parameters using PV loop, contrast ventriculography, and**
380 **thermodilution.**

381

382 DISCUSSION:

383 This study details a standardized method of three different ways to accurately measure cardiac
384 output in swine. Swine has analogous cardiovascular anatomy and physiology to humans and is
385 commonly used as a model for human cardiac physiology, specifically for pre-clinical evaluations
386 of surgical and interventional processes¹⁰. This allows swine to serve as the primary model for
387 cardiovascular physiology, pathology, and emerging biotechnology¹¹. In order to assess these
388 concepts, hemodynamic monitoring must be an accessible and reliable tool for swine models.

389

390 PV-loop catheters are not commonly used in human medicine due to inherent risks of prolonged
391 ventricular cannulation (i.e., arrhythmia, thrombus formation, and myocardial injury). Despite
392 this, they are occasionally used for short durations during cardiac catheterization procedures to
393 measure stroke volume and stroke work¹³. However, in healthy non-survival animal studies, the
394 benefit and versatility of PV-loop catheters generally outweigh the aforementioned risks. Other

395 clinical tools include pulmonary artery catheters. However, this technique assumes the right
396 heart output matches the left heart output and ignores beat-to-beat variations in output
397 between the two chambers¹². The thermodilution method described in this study mitigates these
398 variations by measuring thermodilution across both ventricles of the heart simultaneously rather
399 than just the right ventricle¹⁴. Given these limitations, contrast ventriculography, PV-loop
400 catheter, or thermodilution can be used to reliably obtain cardiac performance data in the
401 laboratory setting.

402
403 In terms of vascular cannulation, this study employed the Seldinger technique rather than a
404 vascular cutdown. The Seldinger technique was used due to its rapid vascular access with novice
405 level skill and few complications. Conversely, open vascular dissection requires a larger skillset
406 and carries larger risk for complications that can either delay or even prohibit further experiment
407 on the animal¹⁵. Additionally, this study utilizes carotid cannulation rather than femoral
408 cannulation. This is largely due to the ease of accessing the heart chambers precluding the need
409 to navigate the aortic arch for LV access. These protocol choices allowed for more efficient
410 vascular access and endovascular navigation that give these methods versatility and ease of use
411 in various protocols in the laboratory setting.

412
413 This study demonstrates that in healthy swine, there is a good correlation of cardiac parameters
414 among different measurement methods including contrast ventriculography with quantitative
415 volumetric analysis, thermodilution, and a PV-loop catheter. When measurement data between
416 two methods are compared directly, the line of identity indicates where all the measurements
417 would fall if perfect agreement existed between the two methods¹⁶. The PV-loop catheter,
418 ventriculography, and thermodilution each produced measurements where the line of identity
419 falls within the confidence interval range, which indicates accurate measurements by each
420 method when compared to each other.

421
422 Based upon which resources and expertise are available, the optimal method can be chosen. If
423 there is an access to a suite of measurement probes and data acquisition, PV-loop catheters or
424 thermodilution are ideal choices depending on the protocol needs. PV-loop catheters offer real
425 time, continuous data acquisition throughout the experimental protocol and provides a myriad
426 of cardiac parameters including stroke volume, ejection fraction, end-diastolic volume, end-
427 systolic volume, and stroke work. Thermodilution offers quick and easy, snap-shot
428 measurements whenever needed, and avoids the need for ventricular cannulation. The method
429 described in this study also has the advantage of measuring cardiac output across both ventricles
430 of the heart. Finally, if there is a limited access to advanced measurement tools contrast
431 ventriculography with volumetric analysis software is readily available and require comparatively
432 little expertise to employ.

433
434 There are several limitations to each of these methods. Namely, they will all require readily
435 available fluoroscopy to confirm various catheter positions when obtaining measurements.
436 Choice of anesthetic will also influence cardiac performance, but each method will provide
437 consistent measurements as long as the same anesthetic is used. Finally, this study is targeted
438 towards healthy animals without cardiac pathology. The agreement and accuracy amongst these

439 methods may diverge given different chronic disease states such as heart failure, valvular
440 regurgitation, or cardiomyopathy. Nevertheless, these three methods offer researchers flexibility
441 in choosing whichever method is the most ideal for a given experiment while providing reliable
442 and accurate measurements of cardiac performance in healthy swine specimens.

443

444 **ACKNOWLEDGMENTS:**

445 None

446

447 **DISCLOSURES:**

448 The authors declare that there is no conflict of interest.

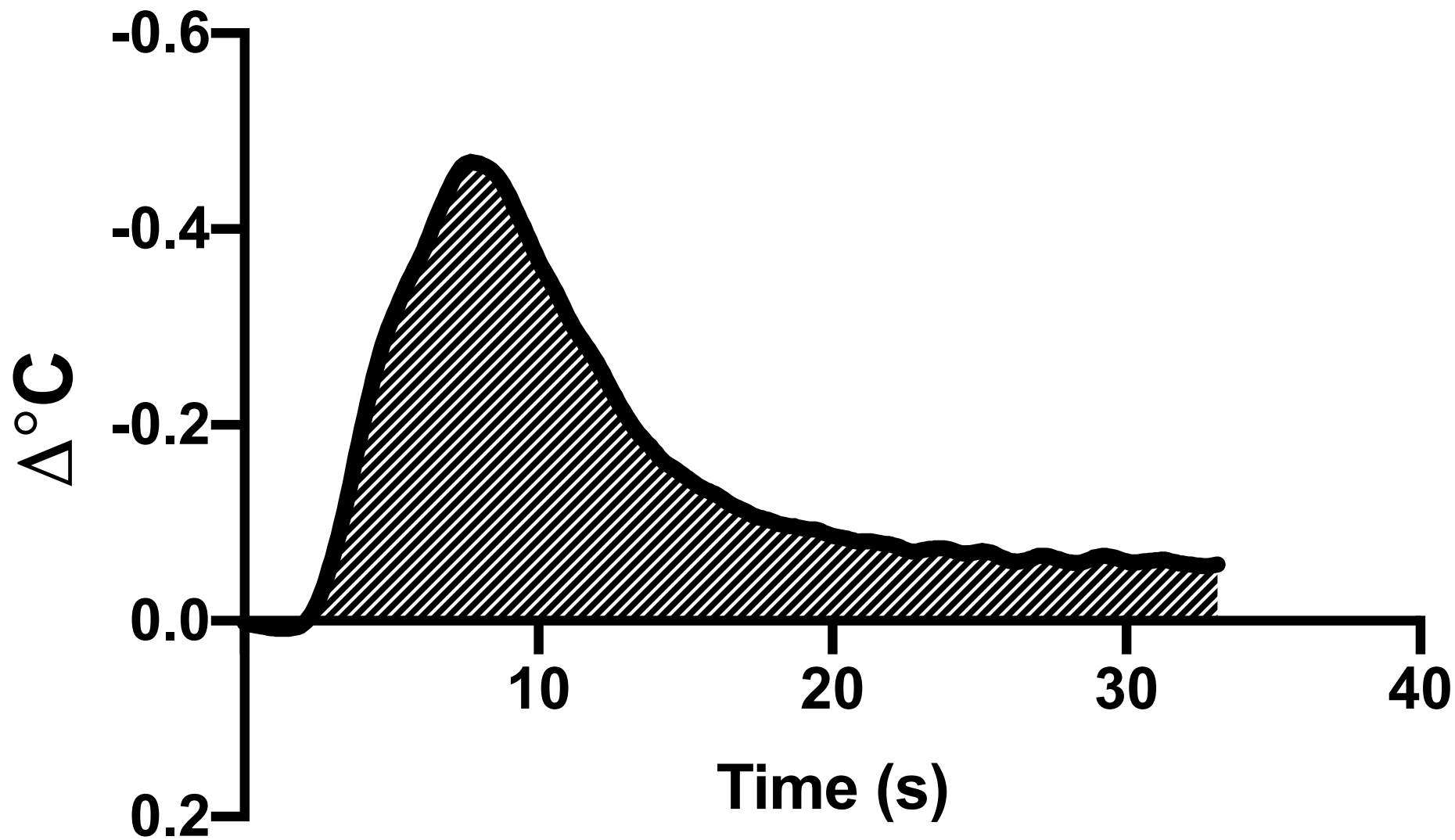
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450 **REFERENCES:**

- 451 1. Pinsky, M. R., Payen, D. Functional hemodynamic monitoring. *Critical Care London. England.*
452 **9**, 566–572 (2005).
- 453 2. Geerts, B. F., Aarts, L. P., Jansen, J. R. Methods in pharmacology: Measurement of cardiac
454 output. *British Journal of Clinical Pharmacology.* **71**, 316–330 (2011).
- 455 3. Argueta, E. E., Paniagua, D. Thermodilution cardiac output: A concept over 250 years in the
456 making. *Cardiology in Review.* **27**, 138–144 (2019).
- 457 4. Higgins, C. B. et al. Quantitation of left ventricular dimensions and function by digital video
458 subtraction angiography. *Radiology.* **144**, 461–469 (1982).
- 459 5. Abraham, D., Mao, L. Cardiac pressure-volume loop analysis using conductance catheters in
460 Mice. *Journal of Visual Experiments.* (103), e52942 (2015).
- 461 6. Porterfield, J. E. et al. Dynamic correction for parallel conductance, G_p , and gain factor, α , in
462 invasive murine left ventricular volume measurements. *Journal of Applied Physiology.* **107**,
463 1693–1703 (2009).
- 464 7. Obernier, J. A., Baldwin, R. L. Establishing an appropriate period of acclimatization following
465 transportation of laboratory animals. *Institution of Laboratory Animal Research Journal.* **47**, 364–
466 369 (2006).
- 467 8. Madurska, M. J. et al. Development of a selective aortic arch perfusion system in a porcine
468 model of exsanguination cardiac arrest. *Journal of Visualized Experiments.* (162), e61573 (2020).
- 469 9. Dodge, H. T., Sandler, H., Ballew, D. W., Lord, J. D. The use of biplane angiocardigraphy for the
470 measurement of left ventricular volume in man. *American Heart Journal.* **60**, 762–776 (1960).
- 471 10. Crick, S. J., Sheppard, M. N., Ho, S. Y., Gebstein, L., Anderson, R. H. Anatomy of the pig heart:
472 comparisons with normal human cardiac structure. *Journal of Anatomy.* **193**, 105–119 (1998).
- 473 11. Smith, A. C., Swindle, M. M. Preparation of Swine for the Laboratory. *Institution of Laboratory*
474 *Animal Research Journal.* **47**, 358–363 (2006).
- 475 12. Franklin, D. L., Van Citters, R. L., Rushmer, R. F. Balance between right and left ventricular
476 output. *Circulation Research.* **10**, 17–26 (1962).
- 477 13. Borlaug, B. A., Kass, D. A. Invasive hemodynamic assessment in heart failure. *Cardiology*
478 *Clinics.* **29**, 269–280 (2011).
- 479 14. Thrush, D., Downs, J. B., Smith, R. A. Continuous thermodilution cardiac output: Agreement
480 with fick and bolus thermodilution methods. *Journal of Cardiothoracic and Vascular Anesthesia.*
481 **9**, 399–404 (1995).

- 482 15. Izer, J., Wilson, R., Herson, K., Ündar, A. Ultrasound-guided vessel catheterization in adult
483 Yorkshire cross-bred pigs. *Veterinary Anesthesia and Analgesia*. **44**, 133–137 (2017).
- 484 16. Hanneman, S. K. Design, analysis, and interpretation of method-comparison studies. *AACN*
485 *Advanced Critical Care*. **19**, 223–234 (2008).
- 486

Figure 1
Figure 1



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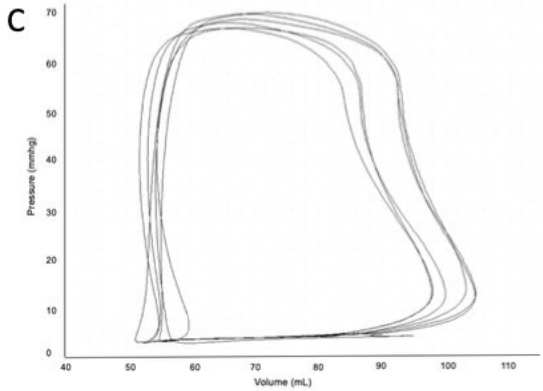
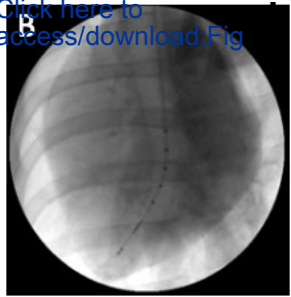


Figure 3

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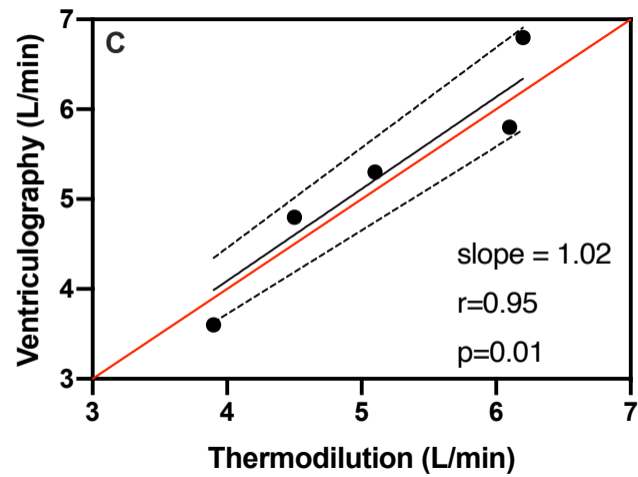
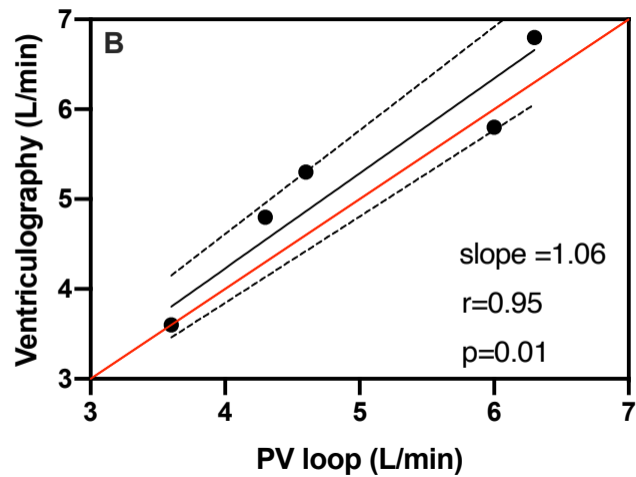
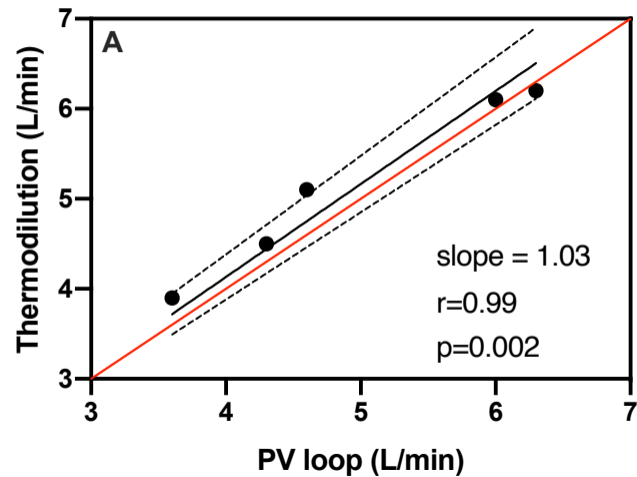


Table 4

Method	Stroke Volume (mL)	Cardiac Output (L/min)
PV-loop	58.0 ± 12.0	5.0 ± 1.1
Contrast Ventriculography	57.6 ± 8.5	5.3 ± 1.2
Thermodilution	53.0 ± 9.8	5.2 ± 1.0

Name of Material/ Equipment	Company	Catalog Number	Comments/Description
0.9% sodium chloride injection	Hospira	0409-4888-50	
7 Fr Introducer Kit	Terumo	RCFW-5.0-35	
Anesthesia Machine	Drager	Fabius Tiro	
Contrast Power Injector	GEHealthcare	E8004N	
Fluoroscope	GEHealthcare	OEC 9800	
Heating/Cooling T/pump	Gaymar	Tp-700	
Isoflurane	Baxter	10019-360-40	
Jackie catheter	Terumo	40-5023	
Omnipaque	GEHealthcare	559289	
PowerChart	ADinstruments	ML866/P	Software
PowerLab	ADinstruments	PL3516	
PV-loop catheter	Transonic		Prefer pigtail tip to straight tip
PV-loop module	Transonic	FFS-097-A004	
Surgical suture, black braided silk, 3.0	Corp.		
Thermocouple probe	ADinstruments	MLT1401	
Ultrasound probe	Philips	L12-4	
Various-sized syringes			
ViewPlus	Sanders Data Systems		Software



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March 31, 2021

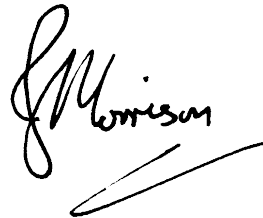
Dear Editors,

On behalf of all the authors we thank the reviewers for their comments on our manuscript and have made revisions to address their concerns.

We specifically added steps in the protocol to detail animal and laboratory worker welfare as well as discussed some of the nuances of the pressure-volume loop catheter uses in the introduction and discussion.

We anticipate that our manuscript will be acceptable for publication in JoVE. Please see the attached document for responses to each of the reviewers' comments.

Yours Sincerely,



Jonathan J Morrison, PhD, FRCS, FEBVS, FACS,
Assistant Professor of Surgery,
School of Medicine, University of Maryland,

Attending Trauma and Vascular Surgeon,
R Adams Cowley Shock Trauma Center

Reviewer #4:

Manuscript Summary:

The manuscript describes potentially useful, albeit quite sophisticated methods to assess cardiac output in a porcine model. While the measurements are interesting and worth the publication of a standardized method, there are some methodical concerns regarding animal handling, animal welfare and workplace safety that have to be specified before publication.

Concerns:

Introduction

Sources and references are completely missing.

We apologize for this error. The introduction has been revised to include all sources and references.

Preparation

3. Specific housing requirements/cage sizes etc. are missing

Housing requirements can vary upon institutional guidelines and availability. I have added the specifications of our institution to the methods section of our manuscript.

4. Not specific enough. What exactly is monitored. Are there exclusion criteria and if so, who, when and how often where they assessed?

Thank you for pointing this out. We specifically monitor oral and nasal mucosa for signs of infection such as discharge. We note respiratory effort as well as swine are prone to pneumonia. Signs of injury on the skin such as large or deep cuts, scrapes, and abrasions are also noted. Any abnormalities are reported to the veterinary staff and excluded from the study. This has been added to the methods section.

Sedation and induction of general anesthesia

3. Induction of anesthesia with volatile agents in pigs is not a standard procedure. Aside from workplace safety considerations of gas concentrations in the lab, why not establish i.v. access prior to intubation? Explain and specify, if safety measures are taken to prevent lab worker exposure to isoflurane.

Animal and laboratory staff safety is of utmost concern. To that end, our IACUC has allowed sedation by intramuscular injection of Telazol/xylazine and rapid induction of general anesthesia by Isoflurane to facilitate quick airway securement by endotracheal intubation. This eliminates the need to obtain IV access under time-limited light sedation without a secure airway. For lab worker safety, the volatile agent vaporizer is only active when the snout mask is securely placed around the snout of the animal or connected to the ET tube.

The procedure room must be well ventilated and a scavenging/ventilation system must be used to eliminate inhalation exposure. Any time the mask is removed, the vaporizer is turned off and purged with pure oxygen for 5-10 seconds. Additionally, minimal isoflurane fraction is used to maintain surgical plane anesthesia.

4. Intubating pigs can be difficult. Which tube size is used?

We use an 8-0 endotracheal tube. This detail has been added to the methods section.

8. Analgesic qualities of isoflurane are debatable and no other analgesics are given to the animals. Specify if and how exactly animal distress would be detected and adequately treated to prevent unnecessary pain and suffering.

We again agree that animal welfare is a top priority. Given that our only invasive procedure in these animals are two points of percutaneous vascular access our IACUC (Institutional animal care and use committee) has deemed the procedure minimally stimulating. Therefore, we manage animal pain (typically noted by animal movement during cannulation) and distress (tachycardia on ECG) by titrating the percent Isoflurane given through the airway circuit between 1.5-3%.

Ventriculography

4. What kind of fluoroscope? Are there any measures necessary to prevent lab worker harm during DSA imaging?

We use a GEHealthcare OEC 9800 X-ray fluoroscope as noted in the materials list. Thank you for pointing out lab worker protection during this protocol. All personnel in the room must wear 0.5 mm equivalent lead apron shielding as well as thyroid shielding. Any personnel working within 1 m of the emitter must also wear leaded eye-protection. All personnel must stand as far away from the emitter as possible while still being able to perform the steps in the protocol. We also minimize beam-on time as much as possible and collimate the emitter as much as possible. This has all been added to the methods section of the manuscript.

Euthanasia

1. Which concentration? Which volume? How is the animals death confirmed? Is sedation provided until the confirmed death of the animals?

We use a 2 mEq/mL solution of KCl and use a rapid intravenous dose of 2 mEq/kg (typically requiring 50-70 mL volume of injection depending on animal weight) to induce cardiac arrest. Death is confirmed by absence of ECG activity as well as drop in end-tidal CO₂ value to zero. This has been added to the methods section of the manuscript. General anesthesia is maintained until death is confirmed. This has been added to the methods section of the manuscript.

Manuscript Summary:

This manuscript aims to compare three different methods of cardiac output measurements - transpulmonary thermodilution, DSA derived ventriculography, and LV PV loop. When correlated in 5 animals, all three methods are reported comparable with only a small difference between them (2, 3, and 6%).

The study has a short introduction summarizing the need for hemodynamic monitoring in animal model research, simple methodology, and a brief discussion.

Based on the methodology described, I am afraid that the results in CO measurements can be influenced by multiple errors. First PV loop method in the way that is used here cannot provide realistic measurement. Second, I am very surprised by the highly precisely correlating results of ventriculographic measurements.

Furthermore, the result values are reported different between the abstract/figures and the text.

The work needs major revisions before it can be considered for publication.

Major Concerns:

The study was performed on 5 healthy young pigs. Are the presented methods of CO measurements being used also in human medicine? Please comment on that. What are pros and cons of each of those three methods?

Thank you for the insightful questions. All of these methods are used to an extent in human medicine to some degree. Thermodilution is most commonly used in the form of a pulmonary artery catheter that uses a heating electrode and temperature sensor to perform thermodilution measurements on the right side of the heart. Ventriculography is commonly used in the cardiac catheterization suite to measure cardiac output and ejection fraction. Pressure-volume loops are less commonly used in human medicine due to inherent risks of prolonged ventricular cannulation (ie. Arrhythmia, thrombus formation, and myocardial injury) however, they are occasionally used for short durations during cardiac catheterization procedures to measure stroke volume and stroke work. This was added to the discussion section of the manuscript.

PV-loop allows real-time, continuous measurements of cardiac performance in addition to providing additional data compared to other methods such as end-diastolic and end-systolic volumes, ejection fraction, and stroke work. Risks include cardiac arrhythmia, thrombus formation, and potential myocardial injury during prolonged cannulation.

Ventriculography does not require specialized acquisition equipment other than a fluoroscope. Limitations include operator variability during LV border tracing, and only snapshot data acquisition.

Finally, thermodilution accounts for cardiac output across both chambers of the heart simultaneously. It provides snapshot information but is easily repeatable if catheters and probes are left in place during experiments. Downsides include potential error introduced by heat exchange with inspired air in the pulmonary vascular bed.

Thermodilution - the sensor is placed in the aortic root. Can this setting result in values different from a S-G catheter placed in the PA?

Yes, agreed. This different placement of the temperature probe can result in different values measured compared to Swan-Ganz catheters. The cold bolus infusion must traverse the pulmonary vascular bed before reaching the temperature probe in our case. There may be heat exchanging effects with inspired air that can skew results. However, we have demonstrated that these effects if there are fairly minute. Additionally, Swan-Ganz catheters only measure right sided output which can change quickly with sudden changes in circulation (exercise) or blood distribution (change in posture, respiratory variation). Left ventricular output must then adjust several cycles later to accommodate this increase or decrease in right ventricular output. This discrepancy is largely avoided when performing thermodilution across both the right and left side of the heart as we have done in this manuscript.

It would be nice to have a correlation to real cardiac output, why didn't you measure invasively with a flow probe to have a CO reference?

Agreed this information would be very helpful. Unfortunately, at this time our lab is not equipped for open thoracic procedures. We aim to tackle this in the near future.

What was the mean difference in repeated cardiac output measurements by thermodilution for each of the animals?

The results reported are averaged over three measurements. They are as follows: 3.9 ± 0.23 L/min, 4.5 ± 0.34 L/min, 5.1 ± 0.29 L/min, 6.1 ± 0.41 L/min, 6.2 ± 0.35 L/min.

What was the SV which the PV system was calculating with during measurements? How does the PV loop catheter estimate the actual SV? Without proper SV calculation, the PV system cannot give correct results.

The average SV calculated by PV-loop was 58.0 ± 12.0 mL. There are different types of PV loop catheters namely electrical conductance and admittance systems. Our system uses the difference in electrical admittance of blood and cardiac muscle and Wei's equation to estimate chamber size. This system is considered to have certain advantages over traditional

conductance type catheters by eliminating parallel conductance between blood and muscle tissue. This allows the catheter to remain accurate despite acute changes in cardiac performance.

Minor Concerns:

How was the body temperature controlled during the prep?

Temperature was monitored using a rectal temperature probe. The animal was kept warm by placing a heating pad underneath it set to 37° C. This has been added to the methods section.

How can remodeling or dilation of the LV affect ventriculographic measurements? Is DSA necessary for the acquisitions or would a classic fluoroscopy serve good as well?
Language corrections are needed.

Indeed, LV remodeling or dilation can affect ventriculographic measurements. The Dodge-Sandler method of ventriculography assumes an elliptical shape of the LV to provide accurate measurements. Of course, this is not always the case especially in diseased or remodeled hearts and would therefore introduce error to the measurements. However, for labs using healthy swine as their model, this method remains useful. Classic fluoroscopy will can be used in ventriculographic measurements as well as DSA. These comments have been added to the discussion and method section respectively.