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# Development of a Noninvasive, Laser-Assisted Experimental Model of Corneal Endothelial Cell Loss --Manuscript Draft--

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1 TITLE: 2 Development of a Noninvasive, Laser-Assisted Experimental Model of Corneal Endothelial Cell 3 Loss 4 5 **AUTHORS AND AFFILIATONS:** Annekatrin Holzhev<sup>1,\*</sup>, Svenja Sonntag<sup>2,\*</sup>, Johannes Rendenbach<sup>1</sup>, Justus S. Ernesti<sup>1</sup>, Vinodh 6 7 Kakkassery<sup>2</sup>, Salvatore Grisanti<sup>2</sup>, Fred Reinholz<sup>3</sup>, Sebastian Freidank<sup>3</sup>, Alfred Vogel<sup>3</sup>, Mahdy Ranjbar<sup>1,2</sup> 8 9 10 <sup>1</sup>Laboratory for Angiogenesis and Ocular Cell Transplantation, University of Lübeck, Lübeck, 11 12 <sup>2</sup>Department of Ophthalmology, University of Lübeck, Lübeck, Germany 13 <sup>3</sup>Institute of Biomedical Optics, University of Lübeck, Lübeck, Germany 14 15 \*These authors contributed equally. 16 17 **Corresponding Author:** 18 Mahdy Ranjbar (eye.research101@gmail.com) 19 20 **Email Addresses of Co-Authors:** 21 Annekatrin Holzhev (annekatrin.holzhey@uksh.de) 22 Svenja Sonntag (svenja.sonntag@uksh.de) 23 Johannes Rendenbach (j.rendenbach@aol.de) 24 Justus S. Ernesti (justus-satoshi.ernesti@uksh.de) 25 Vinodh Kakkassery (vinodh.kakkassery@uksh.de) 26 Salvatore Grisanti (salvatore.grisanti@uksh.de) 27 Fred Reinholz (reinholz@bmo.uni-luebeck.de) 28 Sebastian Freidank (freidank@bmo.uni-luebeck.de) 29 Alfred Vogel (vogel@bmo.uni-luebeck.de) 30 31 **KEYWORDS:** 32 Nd:YAG laser, cornea, corneal endothelial cells, bullous keratopathy, cavitation bubble, disease 33 model 34 35 **SUMMARY:** 36 Here, we present a protocol to detach corneal endothelial cells (CEC) from Descemet's 37 membrane (DM) using a neodymium: YAG (Nd: YAG) laser as an ex vivo disease model for bullous 38 keratopathy (BK). 39 40 **ABSTRACT:** 41 Nd:YAG lasers have been used to perform noninvasive intraocular surgery, such as capsulotomy 42 for several decades now. The incisive effect relies on the optical breakdown at the laser focus.

Acoustic shock waves and cavitation bubbles are generated, causing tissue rupture. Bubble sizes

and pressure amplitudes vary with pulse energy and position of the focal point. In this study,

enucleated porcine eyes were positioned in front of a commercially available Nd:YAG laser. Variable pulse energies as well as different positions of the focal spots posterior to the cornea were tested. Resulting lesions were evaluated by two-photon microscopy and histology to determine the best parameters for an exclusive detachment of corneal endothelial cells (CEC) with minimum collateral damage. The advantages of this method are the precise ablation of CEC, reduced collateral damage, and above all, the non-contact treatment.

#### INTRODUCTION:

Transparency of the cornea is essential for the transmission of light to the retina and its photoreceptors<sup>1</sup>. In this regard, a relative state of dehydration is critical to keep the collagen fibers within the corneal stroma correctly aligned. This homeostasis is maintained by corneal endothelial cells (CEC) located on the Descemet's membrane (DM)<sup>2</sup>. The endothelium is the innermost corneal layer. It has an important barrier and pump function, which is crucial for corneal transparency<sup>3</sup>. In contrast to the epithelium, the endothelium is not able to self-renew<sup>4</sup>. Therefore, any cell damage caused by disease or trauma stimulates the remaining endothelial cells to enlarge and migrate, to cover resulting defects and to maintain corneal functionality<sup>5</sup>. However, if the CEC density falls below a critical threshold, decompensation of the endothelium leads to an edema, resulting in blurred vision and discomfort or even severe pain<sup>4</sup>. Despite the availability of drugs to relieve symptoms, currently the only definitive treatment in these cases is corneal transplantation, which can be performed in the form of a full-thickness graft or a lamellar endothelial transplantation. The latter procedure is available as Descemet's membrane endothelial keratoplasty (DMEK) as well as Descemet's stripping automated endothelial keratoplasty (DSAEK)<sup>6</sup>. However, the protection of remaining CEC and enhancing their survival could be an alternative target, which needs an adequate disease model to test potential therapeutic drugs.

Current CEC loss disease models focus on the destruction of the endothelium through the injection of toxic agents (e.g., benzalkonium chloride) into the anterior chamber or by mechanical abrasion of the cells using an invasive descemetorhexis technique<sup>7,8</sup>. While these models are well established, disadvantages such as general inflammatory response and imprecise collateral damage exist. Therefore, these models are more likely to represent final stages of the disease, when the above-mentioned surgical options are inevitable.

With advances in cellular treatment strategies such as stem cells and gene therapy, the application of these cellular therapies could be useful in early stages of CEC loss<sup>9</sup>. Subsequently, we need a model that represents these earlier stages of the disease more adequately. In this regard, cell culture models have improved over the last decade but are still limited in their validity, as cells in vitro cannot come close to replicating the complex interactions that occur between the different cell types within the cornea<sup>10</sup>. Therefore, ex vivo and in vivo disease models are still in high demand and improving the existing ones is of utmost interest.

Noninvasive, intraocular surgery by photodisruption using a neodymium:YAG (Nd:YAG) laser has become a routine procedure for ophthalmologists worldwide since its introduction in the late 1970s<sup>11</sup>. Photodisruption relies on nonlinear light absorption leading to the formation of plasma,

generation of acoustic shock waves, and creation of cavitation bubbles, whenever the application site is located in a liquid environment<sup>12</sup>. In general, these processes contribute to the intended effect of precise tissue cutting. However, they can also be the source of unnecessary collateral damage limiting the local confinement of laser surgery<sup>13</sup>.

The prediction of resulting mechanical effects has significantly improved through characterization of the shock wave propagation and cavitation course. It is our goal to target CEC with as little damage to surrounding tissue as possible to provide a noninvasive, laser-assisted experimental disease model for the early stages of CEC loss. For this purpose, it is necessary to determine the optimal pulse energies and positions of the focal spots of the laser.

## PROTOCOL:

All procedures involving animal tissue follow the guidelines of the local Animal Care and Ethics Committee.

## 1. Preparation of organ culture and laser treatment

1.1. Obtain freshly enucleated porcine eyes from the local abattoir. Keep them cool (4 °C) in Dulbecco's modified Eagle medium (DMEM) with high glucose, supplemented with L-glutamine, sodium pyruvate, penicillin/streptomycin (1%), and porcine serum (10%), henceforth referred to in this article as full medium.

1.2. Remove extracellular tissues with scissors and soak the eyes in 5% povidone-iodine ophthalmic solution for 5 min before placing them in sterilized phosphate-buffered saline (PBS) until use.

1.3. Screen eyes for major anterior segment pathologies, such as corneal scarring, edema, and other opacities with a spectral-domain optical coherence tomography device (**Table of Materials**).

1.4. Position the eyes in front of a slit-lamp unit equipped with a Nd:YAG laser (**Table of Materials**), which has a wavelength of 1,064 nm and a focal spot diameter of 10  $\mu$ m in air.

NOTE: For optimal positioning a 3D-printed holding apparatus is used, which was designed to hold the eye firm, without putting too much pressure on it (**Figure 1**).

126 1.5. Use a magnification of 12x and deflect the illumination to visualize the individual corneal layers.

1.6. Set the pulse energy (e.g., 1.6 mJ) and focus point (e.g., 0.16 mm) for selective ablation of endothelial cells.

1.7. Place a clear cornea paracentesis close to the limbus and inject viscoelastic (Table of Materials) to stabilize the anterior chamber.

1.8. Excise the laser-treated central cornea using an 8 mm trephine.

1.9. Place the excised cornea in a well of a 12-well plate with the endothelial site facing upwards and incubate the specimen in 3 mL of full medium at 37 °C for up to 3 days.

NOTE: Potential cytoprotective agents can be added to the medium during this step.

2. Preparation for histology

2.1. Prepare Sorensen's buffer with a pH of 7.4 containing 19.6 mL of 133 mM KH<sub>2</sub>PO<sub>4</sub> and 80.4 mL of 133 mM Na<sub>2</sub>HPO<sub>4</sub>.

2.2. Remove the medium from the cornea-containing well and fixate the tissue for 20 min at room temperature (RT) using methanol-free paraformaldehyde (4%) in Sorensen's buffer.

2.3. Place tissue in 20% sucrose in PBS until tissue sinks (1 h) and then in 30% sucrose in PBS overnight at RT. Take care to avoid contact with bubbles and the air surface interface. Embed tissue in optimal cutting temperature (OCT) compound and store at -80 °C.

2.4. Cut sections 10 μm thick using a cryostat at -27 °C.

NOTE: A camel hairbrush is useful to help guide the emerging section over the knife blade.

2.5. Transfer the section to a microscope slide by touching the slide to the tissue within 1 min of cutting it to avoid freeze-drying of the tissue. Store the slides at -80 °C.

3. Hematoxylin and eosin (H&E) staining

3.1. Air dry sections for several minutes to remove moisture.

3.2. Stain with filtered 0.1% Mayers hematoxylin for 10 min in a 50 mL tube. 

3.3. In a Coplin jar, rinse in cool running ddH<sub>2</sub>O for 5 min and dip in 0.5% eosin 10x. 

3.4. Dip in ddH<sub>2</sub>O until the eosin stops streaking and then dip in 50% (10x) as well as 70% (10x) EtOH.

3.5. Equilibrate in 95% EtOH (30 s) and 100% EtOH (60 s) before dipping in xylene several times.

3.6. Finally mount and coverslip the specimen before taking images using a light microscope.

#### REPRESENTATIVE RESULTS:

Using the procedure presented here, we treated eyes with a Nd:YAG laser, evaluating different pulse energies (1.0-4.6 mJ) and positions of focal points (distance from the posterior surface of the cornea: 0.0-0.2 mm) to find the optimal parameters. Multiple replicates (n = 3) were evaluated for each constellation of the laser parameters  $(12 \times 21)$ .

In addition to the above-mentioned protocol, specimen was analyzed with a two-photon microscope before fixation and H&E staining. The two-photon microscope used a solid-state, mode-locked 80 MHz Ti:sapphire laser with a tuning range of 690–1b040 nm and a mean laser output of >900 mW at 800 nm as light source. It delivered pulses with a width of approximately 150 fs to the sample. Images were taken with a microscope objective (20x/0.95) at a wavelength of 730 nm and 30 mW of laser power.

Two-photon as well as light microscopy images were independently reviewed by 3 reviewers, who were blinded to experimental settings and had to assign the images to three categories: (1) no damage, (2) too much damage, or (3) right amount of damage (Figure 2 and Figure 3). Based on their evaluation a heatmap was calculated (Figure 4). Using this heatmap it is possible to select the right constellation of laser parameters to selectively ablate CEC with minimal damage to surrounding tissue (green). Results show that the focal point of the laser must be at least 0.15 mm behind the corneal endothelium for the lowest pulse energy (1.0 mJ) tested. For pulse energies higher than 2.9 mJ, the longest focal distance tested (0.2 mm) is still too close to the endothelium.

### FIGURE LEGENDS:

**Figure 1: Experimental setup.** (A) Eyes were fixed in a partially 3D-printed holding apparatus, which allowed precise alignment with respect to the laser beam. (B) Before laser treatment, the tissue was evaluated with an anterior segment optical coherence tomography device to check for major anterior segment pathologies. Positions of focal laser points are indicated with exemplary for 0.0 mm (black asterisk), 0.1 mm (red asterisk), and 0.2 mm (blue asterisk).

**Figure 2: Two-photon microscopy.** Results ranged from no damage at all (**A**), extensive collateral damage (**B**) to selective ablation of endothelial cells (**C**). The red arrowhead shows a ruptured Descemet's membrane, and green arrowheads indicate selective ablation of CEC-clusters. Scale bar =  $100 \, \mu m$ .

**Figure 3: Histology.** Hematoxylin and eosin staining confirmed the damage range from no damage at all (**A**), extensive collateral damage (**B**) to selective ablation of endothelial cells (**C**). The red arrowhead shows a ruptured Descemet's membrane, and green arrowheads indicate selective ablation of CEC-clusters. Scale bar =  $100 \mu m$ .

**Figure 4: A heatmap showing the probability of selective CEC damage.** In this regard, the pulse energy as well as the position of the Nd:YAG laser focal point must be taken into account. Excessive damage is shown in red, and the desired portion of damage is shown in green.

#### DISCUSSION:

The results of this pilot study indicate that a Nd:YAG laser can be used to selectively ablate corneal endothelial cells when appropriate parameters for energy dose and focus point position are chosen.

As the endothelial function is important for corneal transparency and safeguarding the cornea from stromal edema, models of endothelial dysfunction play an important role in the development of anti-edematous drugs or surgical procedures. There are several established in vitro models for mimicking the in vivo situation<sup>10,14,15</sup>, but as generally known, in vitro models cannot completely imitate the influences of enzymes and cytokines or the effect of cell-cell-interaction. In contrast, this newly developed ex vivo model of endothelial cell loss offers the possibility to monitor different states of the disease and corneal decompensation in the natural environment.

As the cornea in our model is excised with a trephine after the laser procedure, the physiology of the cornea changes and similar to the in vitro situation, regional interactions are significantly hampered. However, the local interface remains intact and especially the cellular communication to other cells within the cornea persists. Our study revealed that under these circumstances the cornea maintains its function for three days in culture, which offers sufficient time to observe and evaluate potential therapeutic agents. On the other hand, longtime healing processes cannot be investigated.

In our model, we used porcine eyes as larger quantities of those can be easily obtained. Furthermore, porcine eyes mimic human eyes very well. In contrast to rabbits that are regularly used for experiment, porcine eyes have a Bowman's membrane. Nevertheless, the corneal thickness of the porcine eye differs considerably from the human eye. In particular, the porcine stroma is much thicker and there is no difference between central and peripheral thickness in porcine corneas<sup>16</sup>. It must also be considered that human CEC do not have any healing capability while this regenerative feature is reported in some animals, such as pigs and rabbits<sup>17,18</sup>. Our study did not focus on wound healing processes, but this difference should be kept in mind when translating results. As the wound healing of animal CEC does not exceed four days, it might still be observed in our cultured tissues even if they last only for three days.

Comparing our experimental setup with previous studies, the applied energy levels were similar<sup>19</sup>. Instead of focusing only on the endothelium, different locations of focal points were evaluated. Therefore, the main difference of our setup to earlier studies is its potential to induce specific endothelial damage without damaging either DM or stromal tissue. Accurate monitoring of energy dose and focus position enables selective CEC ablation without causing shock wave damage to other parts of the cornea. Also, we have not noticed stromal or subepithelial edema directly after laser treatment<sup>20</sup>.

A previous study showed that temperatures of ~40 °C can lead to CEC damage<sup>21</sup>. We did not measure the induced temperature, but it might be of interest for further studies. Moreover, the effect of different types of laser systems should be evaluated. Earlier studies showed a difference

between laser induced circumscribed CEC damage and other CEC injuries<sup>19,22</sup>. This might also limit the comparability to human tissue and diseases because laser induced damage seems to be followed by different disease development processes. Interestingly, the wound healing after laser application stopped at the burned DM in earlier studies<sup>19</sup>. The source of injury might be less important if the DM remains intact.

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Higher energy levels can pose a higher risk of extended injury<sup>22</sup>. Our results show that using higher energy levels (<2.9 mJ) for selective CEC damage requires a tighter focus range. While the damage to CEC was mechanically applied in previous studies<sup>17</sup>, laser-induced damage used here has a more precise dosing of the lesion and can be easily used in in vivo studies.

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It should be noted that only a small number of eyes have been treated and examined according to this protocol. As mentioned above, there might be interindividual differences in the response to the laser treatment as well as differences between the corneas of different animal species. Since CEC damage can be produced at different focal positions, certain thresholds should not be exceeded to avoid extended damage.

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Finally, the lesions generated in this study were placed in the central part. An earlier study of porcine eyes showed accelerated wound healing in the corneal periphery, which might be due to its proximity to limbal stem cells<sup>17</sup> as the corneal thickness in porcine eyes does not differ between regions. It should be evaluated in future studies whether laser parameters should be adjusted when switching from the center of the cornea to the periphery.

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In conclusion, our study introduces a noninvasive model for further investigations on CEC dysfunction. Limitations of ex vivo or in vivo studies in terms of usage of animal instead of human tissue remain and must be considered when interpreting the results.

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## **DISCLOSURES:**

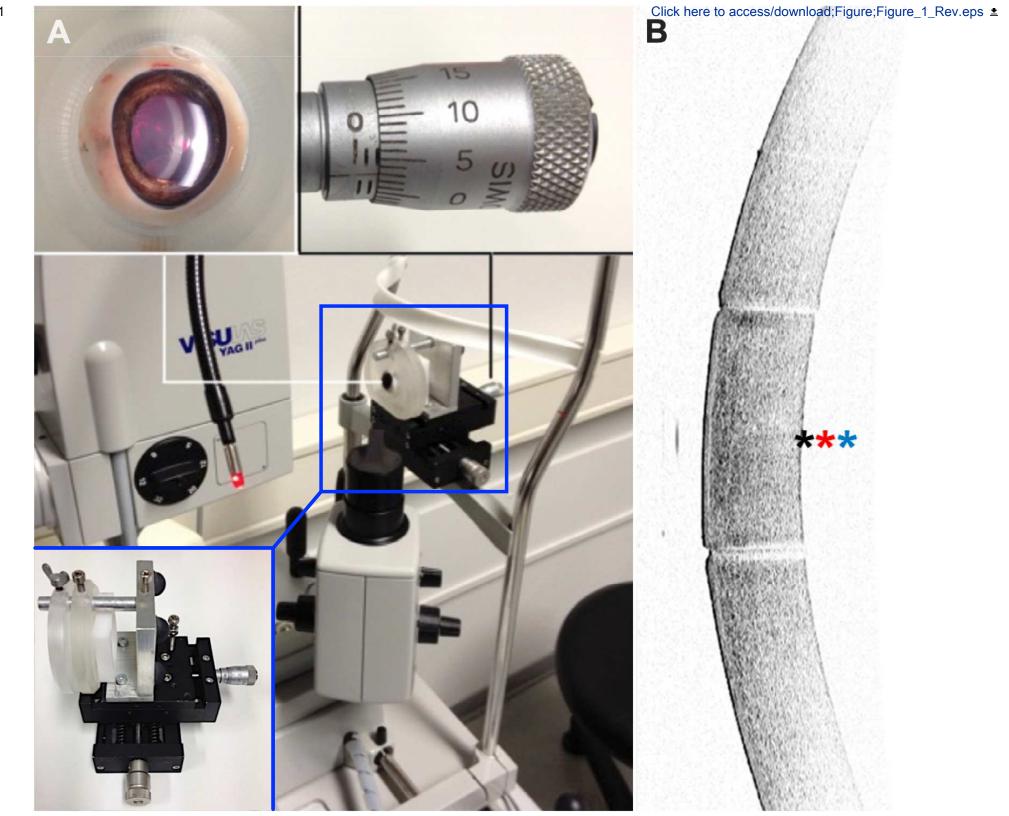
The authors have nothing to disclose.

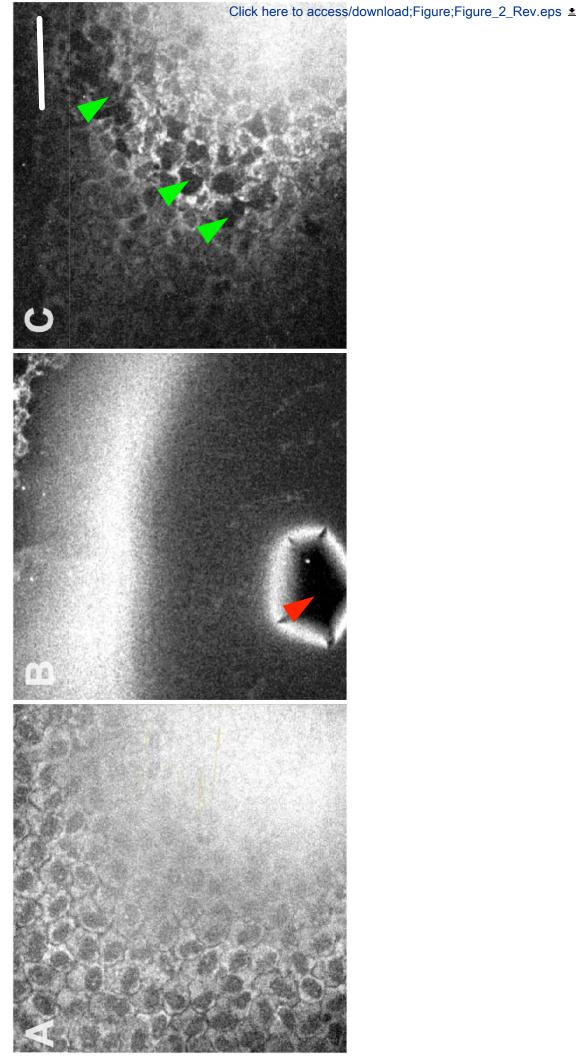
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## Name of Material/ Equipment

## **Company**

BARRON VACUUM TREPHINE Katena

Cryostat Leica

Dulbecco's Modified Eagle's Medium - high glucose PAA

Eye holder Self

Inverted Microscope Leica

KH<sub>2</sub>PO<sub>4</sub> Merck

Na<sub>2</sub>HPO<sub>4</sub> Merck

Nd:YAG laser Zeiss Meditec

OCT Tissue Tek Sakura Finetechnical

Penicillin-Streptomycin Sigma-Aldrich

Phosphate Buffered Saline (PBS) Gibco

Porcine serum Sigma-Aldrich

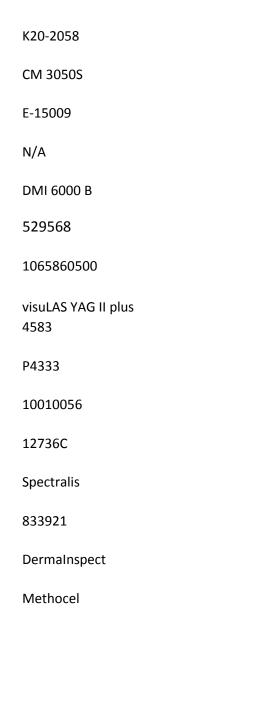
Spectral-domain optical coherence tomograph Heidelberg Engineering

Tissue culture plate 12-well Sarstedt

Two-Photon Microscope JenLab

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Dear Professor Cao, Dear Reviewers,

First of all, I'd like to thank you for your constructive revision, thoughtful comments, reasonable suggestions, and appreciation of our manuscript. We tried to answer all questions to the best of our knowledge and edited the manuscript.

Thank you for still considering our now revised manuscript for JoVE.

With best wishes and appreciation for your time,

Mahdy Ranjbar

### **Editorial comments:**

1. Please take this opportunity to thoroughly proofread the manuscript to ensure that there are no spelling or grammar issues. The JoVE editor will not copy-edit your manuscript and any errors in the submitted revision may be present in the published version.

R1: The manuscript has been proofread. Spelling as well as grammar issues were modified to the best of our knowledge.

2. Please revise lines 41-44 and 127-129 to avoid textual overlap with previously published work.

R2: Lines 41-44 have been revised. However, the technical description in lines 127-129 is difficult to rephrase as it simply states the characteristics of the device.

3. Authors and affiliations: Please provide an email address for each author in the manuscript.

R3: Email addresses have been added.

4. Please add a Summary section before the Abstract section to clearly describe the protocol and its applications in complete sentences between 10–50 words: "Here, we present a protocol to ..."

R4: The first sentence of our abstract, which summarizes our manuscript very well, has been moved to a separate summary section before the abstract section.

- 5. JoVE cannot publish manuscripts containing commercial language. This includes trademark symbols (TM), registered symbols (®), and company names before an instrument or reagent. Please remove all commercial language from your manuscript and use generic terms instead. All commercial products should be sufficiently referenced in the Table of Materials. You may use the generic term followed by "(Table of Materials)" to draw the readers' attention to specific commercial names. Examples of commercial sounding language in your manuscript are: Spectralis®, Heidelberg Engineering GmbH, Carl Zeiss Meditec AG, Methocel, Tissue Tek, JenLab GmbH, etc. R5: The manuscript has been modified accordingly.
- 6. All methods that involve the use of human or vertebrate subjects and/or tissue sampling must include an ethics statement. Please provide an ethics statement at the beginning of the protocol section indicating that the protocol follows the guidelines of your institution.

R6: The required statement has been added.

- 7. Please adjust the numbering of the Protocol to follow the JoVE Instructions for Authors. Step 1 followed by 1.1, followed by 1.1.1, etc. Each step should include 1–2 actions and contain 2–3 sentences. Use subheadings and substeps for clarity if there are discrete stages in the protocol. Please refrain from using bullets, dashes, or indentations. R7: The protocol has been reformatted.
- 8. Please add more details to your protocol steps. There should be enough detail in each step to supplement the actions seen in the video so that viewers can easily replicate the protocol. Alternatively, add references to published material specifying how to perform the protocol action. See examples below.

R8: The protocol has been modified.

9. Line 86: Please provide the composition of antiseptic solution. If it is purchased, please list it in the Table of Materials.

R9: The information has been added.

10. Line 96: Please describe how to adjust the pulse energy and focus point. What is the desired effect here?

R10: The sentence has been rephrased.

11. Line 100: Once cornea per well? Please also specify the incubation temperature and regenerative additives used in this step.

R11: The sentence has been rephrased.

12. Line 106: What container is used for fixation?

R12: The sentence has been rephrased.

13. Line 108: At what temperature is this done?

R13: The information has been added.

14. Line 117: Please describe how histological staining is done.

R14: The information has been added.

15. Please reference Figure 1 in the protocol.

R15: The reference has been added.

16. Please describe how to obtain data presented in Figure 4 in the protocol.

R16: The information has been added in the representative results section.

17. Figure 1: Please indicate what each color asterisk represents? Which focal length? R17: The description has been added.

18. Figure 2 and Figure 3: Please describe what the arrowheads point to in the figure legend.

R18: The description has been added.

19. Please submit each figure as a vector image file to ensure high resolution throughout production: (.psd, ai, .eps., .svg).

R19: Images have been reformatted to .eps

20. Table of Materials: Please ensure that it has information on all relevant supplies, reagents, equipment and software used, especially those mentioned in the Protocol. Please sort the materials alphabetically by material name.

R20: The materials have been reordered.

### **Reviewer 1:**

It would be useful if authors can provide a mechanical drawing of the porcine eye holder. The schematic could be part of Figure 1.

R: The porcine eye holder consists of different parts, which were partially 3D-printed and specifically arranged to hold the eye firm, without putting too much pressure on it. Instead of the suggested mechanical drawing we added a bigger image of the device to illustrate the setup.

Microscopy in Fig. 2 cannot be duplicated by many investigators since 2-photon microscopes are not commonly available in most research institutions. Perhaps authors could discuss alternative approaches to assess/tune the laser to ablate endothelial cells alone without damage to the adjacent cells and tissue.

R: We are aware that 2PM is not available everywhere. Therefore, we demonstrate in Figure 3 that the ablation of endothelial cells is also visible using common light microscopy after H&E staining.

Line 137 - How was the heat map calculated? Instead of graphical representation, is it more useful to provide the actual values of probability?

R: We used a single-blind review system, in which 3 reviewers who were blinded to the treatment parameters had to assign two-photon as well as histology images to three categories (no damage, too much damage, selective damage). Based on their evaluation the heatmap was calculated.

If possible, reproduce the histology micrographs at higher resolution in Fig. 3. R: The resolution has been upscaled.

### **Reviewer 2:**

1. In the abstract, the following phrase: "Precise application of lesions" is not self-explanatory. Please use a better phrase to relay your message.

R1: The sentence has been rephrased.

2. Line 48, it is better to state full corneal transplant, endothelial transplantation in the forms of DMEK and DSAEK rather stating lamellar graft.

R2: The sentence has been rephrased according to your suggestion.

3. Line 83, need to specify what DMEM abbreviation stands for.

R3: It has been written out in full.

4. Line 1010, what do you mean by regenerative additives of interest for up to 3 days? What do you mean? Did you already tell us what the regenerative additives of interests are?

R4: The sentence has been rephrased. We just wanted to state, that during these 3 days potential therapeutic agents can be added to the medium.

5. It is difficult to know how many eyes in total were used in this study based on the energy level and distance form the endothelium.

R5: In total we used 3 eyes for every constellation (12x21). 756 eyes in total were evaluated. This information has been added to the representative results section.

6. Was there any collateral damage to descemets membrane? Was the damage to descemet membrane unacceptable.? Only CEC without basement membrane insult was the target of your study?

R6: Yes, damage to Descemet's membrane (DM) ranged from small bumps to total rupture. During the review of the images minor damage to DM was acceptable, as long as there was no partial or complete rupture. Actually, minor damage to DM would be ideal for a disease model as this is common early stages of these diseases.

7. Author need to provide some range of energy and corresponding posterior distance from the endothelium that caused no damage except the desired specific insult to the CEC and nothing else. Please provide these in the result section instead of simply referring the reader to the figures.

R7: The range is illustrated in the heatmap, however we now added the required information also in the results section.

8. Was desired damage defined in terms of single cell damage or clusters of few cells without collateral damage?

R8: Clusters. We rephrased some passages for clarity.

9. Can author share some of the safe YAG laser setting in the discussion for other investigators who are interested in this field.

R9: Referring to R7.

10. Congratulate the authors on the great work. As mentioned in vivo animal study needs to verify the validity of their laser setting.

R10: Thanks for your appreciation of our efforts.

- 11. I think authors need to share their energy threshold and distance threshold that caused only CEC damage and then emphasize that the safety and validity of their work in the actual in vivo system needs to be cautiously performed.

  R11: Referring to R7+R9.
- 12. I am curious to know about your custom designed holding apparatus. Such detail in the method section needs published references or more detailed information in the method section about the apparatus.
- R12: The porcine eye holder consists of different parts, which were partially 3D-printed and specifically arranged to hold the eye firm, without putting too much pressure on it. We added a bigger image of the device to illustrate the setup.
- 13. For examples in the table of material, the holding apparatus company or manufacturing should be reflected.
  R13: Referring to R12.