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An automated counterflow centrifugal system for small scale downstream process

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TITLE:**Automated Counterflow Centrifugal System for Small-Scale Cell Processing****AUTHORS AND AFFILIATIONS:**

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SUMMARY:

Automation is key to upscaling and cost management in cell manufacturing. This manuscript describes the use of a counterflow centrifugal cell processing device for automating the buffer exchange and cell concentration steps for small-scale bioprocessing.

ABSTRACT:

Successful commercialization of gene and cell-based therapies requires manufacturing processes that are cost-effective and scalable. Buffer exchange and product concentration are essential components for most manufacturing processes. However, at the early stages of product development, these steps are often performed manually. Manual dead-end centrifugation for buffer exchange is labor-intensive, costly, and not scalable. A closed automated system can effectively eliminate this laborious step, but implementation can be challenging. Here, we describe a newly developed cell processing device that is suitable for small- to medium-scale cell processing and aims to bridge the gap between manual processing and large-scale automation.

This protocol can be easily applied to various cell types and processes by modifying the flow rate and centrifugation speed. Our protocol demonstrated high cell recovery with shorter processing times in comparison to the manual process. Cells recovered from the automated process also maintained their proliferation rates. The device can be applied as a modular component in a closed manufacturing process to accommodate steps such as buffer exchange, cell formulation, and cryopreservation.

INTRODUCTION:

The landscape of modern medicine has transformed rapidly through recent developments in gene and cell-based therapies (GCT). As one of the fastest growing fields in translational research, the GCT sector also faces unique and unprecedented challenges. In addition to robust clinical outcomes, efficient and cost-effective manufacturing processes are essential for the commercial success of GCT, which is particularly difficult to achieve in small-scale manufacturing¹. The cost of time, labor, and quality assurances are magnified when each batch of cells only produces a few doses for one patient instead of hundreds or thousands. Unlike allogeneic cell therapies in which the manufacturing processes are more akin to the production of antibodies and recombinant proteins, autologous cell therapies are typically produced as small-scale operations¹. As a relatively new phenomenon in biopharmaceutical manufacturing², options for small-scale cell processing are currently quite limited.

Buffer exchange is essential to cell manufacturing. It is one of the downstream processes where cells are removed from culture media and concentrated for cryopreservation or infusion. Currently, small-scale cell manufacturing often applies processes similar to those in the academic research setting and relies on specialized clean rooms to maintain sterility³. Manual downstream processes often use benchtop centrifuges to pellet and resuspend cells for volume reduction and buffer exchange. These open processes are costly (i.e., labor and clean room maintenance) and have limited manufacturing capacity, which are not ideal for commercial production^{2,3}.

Implementing automation has been proposed as a solution to improve manufacturing efficiency and achieving commercial scale productions². Sterility cannot be achieved in cell-based products through traditional methods used for biologics, such as gamma irradiation or terminal end filtration. Instead, an automated closed system is deployed to reduce risks of contamination and operators relying on clean rooms to maintain sterility⁴. Process automation also addresses the issue of scalability by either having multiple systems running in parallel (scale-out) or increasing the processing capacity of an individual device (scale-up), which in turn minimizes the variability between operators. Furthermore, cost modelling analysis of autologous therapies suggests that automation may reduce the cost of manufacturing^{5,6}. However, no cost benefit was found in an autologous stem cell clinical trial where an automated manufacturing platform was used⁷, suggesting that the cost benefit of automation may depend on the individual manufacturing process.

There are different strategies in which automation can be introduced into an existing manufacturing process. This can be achieved either by implementing a fully integrated platform or a modular-based processing chain. There are several fully integrated platforms commercially

available for autologous cell manufacturing, such as CliniMACS Prodigy (Miltenyi Biotec), Cocoon (Octane Biotech), and Quantum (Terumo BCT). These integrated platforms, which are often described as "GMP-in-a-box", have low demands on infrastructure and are easy to operate. However, the manufacturing capacity of a fully integrated setup may be restricted by the incubator attached to the system. For example, the culturing capacity of Prodigy is limited to its 400 mL chamber⁸ and the Quantum cartridge has a limiting surface area set to 2.1 m² (equivalent to 120 T175 flasks)⁷, which may not be sufficient for patients requiring higher cell doses^{9,10}. Additionally, Prodigy and Quantum have a common attribute that limits their use: the operational unit is occupied by a single batch of cells throughout the cell expansion period, thus limiting the number of batches that can be manufactured by each unit¹¹. The modular approach to automation is to create a manufacturing chain with multiple modular units that simulates the commercial manufacturing process^{12,13}. This approach, which separates the culture device from the cell washing device, can thereby maximize manufacturing efficiency. An ideal processing device would be one that is adaptable and scalable to manufacturing needs¹².

Counterflow centrifugation (CFC) technology, which dates back to the 1970s, has had a long history in cell processing¹⁴. It achieves cell concentration and separation by balancing centrifugal force with a counterflow force. Typically, a cell suspension enters from the narrow end of a cell chamber under a constant flow rate while subjected to a centrifugal force (**Figure 1A**). The flow of the fluid is exerted in the opposite direction to the centrifugal force. This is referred to as the counterflow force, which forms a gradient within the cell chamber. The counterflow force then decreases as the cell chamber widens away from the tip of the cone-shaped cell chamber. Cells with higher density and larger diameter have a higher sedimentation rate, and thus they reach force equilibrium towards the tip of the cone-shaped cell chamber. Smaller particles may reach equilibrium towards the base of the chamber or be too small to be retained in the chamber and will be washed away. The CFC technology is mostly known for its application in processing blood apheresis products, such as isolating monocytes for dendritic cell therapies^{15,16}. In terms of buffer exchange, the CFC technology has only been applied in large-scale manufacturing¹⁷ and has yet to be used for the smaller scale manufacturing of autologous cell therapies.

To address the need of a suitable device for small-scale cell manufacturing, an automated CFC device (See **Table of Materials**), was recently developed¹⁸. The automated cell processing device uses counterflow centrifugation technology to remove cell debris and facilitate buffer exchange. The device performs buffer exchange with a single-use kit that can be sterile-connected to a cell transfer bag, which allows the cells to be processed within a sterile, enclosed system. Here, we investigate the use of a counterflow centrifugal device to perform buffer exchange in mammalian cell cultures in automated protocols. In this study, we tested the buffer exchange protocol using Jurkat cells and mesenchymal stromal cells (MSCs) to model nonadherent and adherent cell types, respectively. Jurkat cells are immortalized T cells often used for the study of acute T cell leukemia^{19,20}. MSCs are adult stem cells that have been studied in human clinical trials for a wide range of diseases⁹.

PROTOCOL:

1. Preparation of reagents and cells for buffer exchange

1.1. Prepare buffers (see **Table of Materials**) in a class 2 laminar flow hood. Using a syringe and needle assembly, remove 50 mL of saline solution from a 500 mL saline bag. Replace this with 50 mL of 20% human serum albumin (HSA) to make 2% HSA in saline, which will serve as the wash buffer.

1.2. Remove the cells from the culture vessels and perform a cell count to determine the starting cell quantity and viability by trypan blue exclusion. Load the cells into a transfer bag.

NOTE: In this protocol Jurkat cells were cultured in RPMI and MSCs were cultured in DMEM:F12. Both media were supplemented with 10% fetal bovine serum (FBS) and 1% Antibiotic-Antimycotic solution. Cells were cultured at 37 °C with 5% CO₂. For MSCs or adherent cells, add a digestion enzyme (e.g., trypsin) into the culture vessels in order to detach the cells, and quench with culture media once the cells are detached. A transfer bag was used in this protocol because the cells were expanded in culture vessels. However, if the cells are cultured in a cell culture bag, it can be directly connected to the single-use kit via sterile tube welding. In this protocol, either 3×10^7 Jurkat cells or 1×10^7 MSCs were used for each run, where cells were suspended in 40 mL of culture media.

1.2.1. Load cells into a transfer bag (see **Table of Materials**) using a syringe and needle assembly if a sterile tube welder is available to connect the transfer bag to the single use processing kit.

1.2.2. Alternatively, use a pair of autoclaved scissors to cut the connecting tube with around 10 cm remaining attached to the transfer bag and add a female Luer connector to the end of the tubing. Use a syringe to aspirate cells and media, then connect the syringe to the Luer connector and load cells to the transfer bag.

1.3. Connect the bag containing the cells, wash buffer bag containing 500 mL of wash buffer prepared in step 1.1, waste bag, and collecting syringe to the single-use kit (**Figure 1B**).

NOTE: The connecting position of each bag depends on the settings in the program. In this protocol, we connected the waste bag at position A, wash buffer at position B, cell bag at positions D and F, and collection syringe at position H (**Figure 1C**).

2. Program for automated buffer exchange protocol

2.1. Open the Graphic User Interface (GUI) of the device and press the "**START**" button on a laptop PC or tablet. Then "**Open**" an existing protocol or press "**New**" to create a new one.

2.2. Use the "**Forward**" and "**Backward**" button to navigate through each step, select the valves to be opened/closed, centrifugal speed, pump speed, pump direction, and action triggers. The settings for each step are summarized in **Table 1**. Then save the protocol.

3. Setting up the machine

3.1. Place the single-use processing kit on the machine and hang the connected bags accordingly. Press the red **"Stop/Reset"** button to reset all valves into the default closed position.

NOTE: The machine will perform a test when the door is closed to ensure the kit has been placed correctly and that all the valves are functioning appropriately.

3.2. Connect the GUI to the processing device and press the **"Connect"** button. Then download the saved program. When the green **"Play"** button lights up, it indicates that the protocol is ready to start.

3.3. Open the manual clamps for the transfer bag tubing.

NOTE: If the operator forgets to open the clamps, the device will stop and the pressure sensor warning will appear. Press the **"Stop"** button to reset the device and open the clamps to start again.

4. Automated buffer exchange

4.1. Press **"Start"** to initiate the buffer exchange program.

NOTE: To manually alter the automated process, press the **"Next"** button to move to the next step before reaching the **"Trigger"** or press **"Pause"** to put the process on hold. This will recirculate the cells through the kit while keeping only valves J and K open (**Figure 1C**).

4.2. At the end of automation step 6 (**Table 1**), the process will pause when air in the now emptied bag triggers the bubble sensor. Press **"Start"** to move the process to the next step if the bag is indeed empty, or press **"Pause"** to resume the processing if the sensor was triggered by a bubble in the line.

5. Collecting and sampling the cells

5.1. When the automated process is finished, close all tubing clamps. Open the door and take the single-use kit out of the device. Disconnect the syringe to collect the cells for subsequent processes. Take a sample of the collected cells for a cell count and viability check (see step 6.2).

6. Process validation

6.1. Perform control experiments using a manual buffer exchange protocol.

6.1.1. Centrifuge cell suspension at 200 x g for 5 min. Discard the supernatant and resuspend the cells with 30 mL of cell wash buffer. Centrifuge the cell suspension again at 200 x g for 5 min. Discard the supernatant and resuspend the cells with 10 mL of cell wash buffer.

6.2. Perform cell counting via the trypan blue exclusion assay to assess cell viability using an automated cell counter.

6.3. Perform an MTS assay to quantify cell proliferation at 2, 24, and 48 h.

NOTE: The MTS assay was performed on a 96 well tissue culture plate according to the manufacturer's instructions. A 100 μ L aliquot of cell culture media (containing 10,000 Jurkat cells or 1,500) per well were plated after the buffer exchange process. At each time point, 20 μ L of MTS reagents were added into each well and incubated for 2 h at 37 °C. The absorbance was assessed at 490 nm using a plate reader.

6.4. Perform functional assays to compare the impact of the automated process versus the manual process on the Jurkat cells and MSC function.

6.4.1. Culture Jurkat cells in a 96-well plate at a density of 1×10^6 cells/mL stimulated with 50 ng/mL phorbol 12-myristate 13-acetate (PMA) and 1 μ g/mL ionomycin (cell stimulation cocktail) in DMEM:F12 media containing 10% fetal bovine serum (FBS) for 24 h. Incubate the cells at 37 °C with 5% CO₂.

6.4.2. Measure interleukin-2 production from culture supernatant using bead-based ELISA assay (see **Table of Materials**) according to the manufacturer's instructions.

6.4.3. Culture MSCs in a 12 well plate at the density of 10,000 cells/cm² in 1 mL of DMEM:F12 media containing 10% FBS supplemented with interferon- γ 50 units/mL for 48 h. Collect supernatant for the kynurenine concentration assay to measure indoleamine 2,3-dioxygenase (IDO) enzyme activity of MSCs as previously described²¹.

REPRESENTATIVE RESULTS:

In this protocol, we used Jurkat cells and MSCs as representative examples to demonstrate the automated buffer exchange process. During the process, Jurkat cells and MSCs shared the same processing steps with differences in centrifugal force and pump speed that control the flow rate (**Table 1**). **Figure 2** shows representative images captured by the camera of how the fluidized cell bed may appear during the buffer exchange process. Typically, the fluidized cell bed will resemble the image in **Figure 2A**, where cells accumulate in the middle and towards the front of the cone with a small space at the tip of the chamber, where cells do not accumulate and the opening of the cell loading inlet is visible. The fluidized cell bed may be compressed (**Figure 2B**) when introducing new buffer that is at a different viscosity or density. In this protocol, the pump speed was lowered from 30–35 mL/min to 20 mL/min at the start of the washing step. Once the chamber was filled with the new buffer, the pump speed was returned to normal to prevent pelleting cells at the tip of the chamber. A high flow rate (**Figure 2C**) may be applied to select for live cells because dead cells are smaller and lighter and can be forced out of the chamber by increasing the flow rate.

The automated process of buffer exchange was achieved by first concentrating the cells, then introducing the wash buffer, which was around 10x of the volume of the fluidized cell bed. The cells were then formulated to the desired volume. These three processing steps were designed to follow the same principles as a manual buffer exchange. Typically, a two-cycle centrifugation (200 x g, 5 min) is used to perform manual buffer exchange, in which cells are pelleted to concentrate, resuspended to wash, then centrifuged again and resuspended to the final volume. The processing time of the automated processes was shorter compared to the manual ones (Figure 3). The recovery rate between manual and automated processes were similar for both Jurkat cells and MSCs, and cell viability was not affected by the process (Figure 4). The cell quality was verified by cell proliferation (MTS assay) and cytokine/enzyme production. The recovered cells showed similar proliferation rates between the manual and the automated processes (Figure 5A). The level of interleukin-2 production from Jurkat cells and IDO activity of MSCs were also comparable between the two groups (Figure 5B and 5C).

FIGURE AND TABLE LEGENDS:

Table 1: Automated buffer exchange GUI setup for Jurkat cells and MSCs.

Figure 1: Counterflow centrifugal cell processing system. (A) A schematic diagram illustrating the principle of counterflow centrifugation. The counterflow force is present in a gradient within the cell chamber. While centrifuging (grey arrow), cells with larger diameters receive a higher sedimentation force, in which the cells reach force equilibrium towards the narrow end of the chamber, forming a fluidized cell bed. Cell debris and small particles that are too small to remain in the chamber are washed away. (B) The counterflow centrifugal processing system consists of the processing device and the single-use processing kit. (C) The single-use kit configuration for the buffer exchange protocol.

Figure 2: Fluidized cell bed in the cell chamber. Representative images of a fluidized cell bed under (A) medium, (B) low, and (C) high flow rate. The dotted line indicates the area of the fluidized cell bed within the chamber.

Figure 3: Comparison of cell processing time of Jurkat cells and MSCs with manual and automated processing (n = 3–4 in each group, data are presented as mean ± SD).

Figure 4: Comparison of cell viability and live cell recovery of Jurkat cells and MSCs with manual and automated processing. Cell viability (A) and live cell recovery (B) were measured by trypan blue exclusion assay using an automated cell counter. Live cell recovery was reduced in the absence of serum or when only 3×10^6 or 1×10^6 cells were processed. (n = 4–9 in each group, data are presented as mean ± SD).

Figure 5: Cell proliferation and cell function from manual and automated processing. (A) MTS assay of Jurkat cells and MSCs were performed at 2, 24, and 48 h after buffer exchange. The quality of recovered cells was quantified by Interleukin-2 production from Jurkat cells (B), and IDO activity in MSCs (C). (n = 4–8 in each group, data are presented as mean ± SD).

Figure 6: Fluidized cell bed stability at various flow rate. Two processes were performed for each cell type. In one process, either 3×10^7 Jurkat cells or 1×10^7 MSCs. In the second process, 10x the number of cells were used. In both processes, 10 mL of cell elutriate was collected from port A at various flow rates using the centrifuging speed indicated in this protocol ($1,600 \times g$ for Jurkat cells and $1,500 \times g$ for MSCs). The number of cells in the elutriate was determined and presented as percentage of the total amount of cells loaded in the chamber. ($n = 3$ for each group, data are presented as mean \pm SD).

DISCUSSION:

The automated buffer exchange protocol described is simple and user friendly. Nevertheless, there are a few key steps in this protocol that are critical and require particular attention. In our experience, when processing larger cells such as MSCs (average diameter 10–15 μm) each run should include at least 1×10^7 cells to achieve optimal cell recovery (**Figure 4B**). Processing smaller cells, such as Jurkat cells (average $\sim 10 \mu\text{m}$ diameter), requires around 3×10^7 cells to achieve a stable fluidized cell bed (**Figure 4B**). When the cell number is too low, cells are more likely to be removed from the fluidized bed, which will affect the final cell recovery. Additionally, we compared cell loss rates at different pump speeds when a constant centrifugal speed is applied. Here, we observed that the cell loss increased with the flow rate (**Figure 6**), which is due to the increasing instability of the fluidized bed at higher flow rates. However, the percentage of cell loss was lower when 10x the number of cells were loaded into the chamber, which suggests that a higher pump speed can be applied when processing a larger number of cells to allow faster processing. In step 5 of the process, 100 mL of culture media was recirculated from the chamber back to the cell transfer bag to allow the fluidized bed to form and stabilize prior to volume reduction and buffer exchange. If the cell concentration is low (e.g., below $0.2 \times 10^6/\text{mL}$), the recirculation step may need to be extended to allow enough cells to form the fluidized cell bed. Likewise, if the cell concentration is high, the recirculation step can be shortened.

The presence of serum in the wash buffer is also critical for cell recovery. Previous studies have shown that hydrodynamic stress can cause necrotic cell death in the absence of buffering proteins^{22,23}. The flow dynamic of the counterflow centrifugal system is quite complex. In this protocol, cell recovery rates dropped to around 70% when the process was performed in the absence of serum (**Figure 4B**). Although the exact mechanism is not clear, the presence of serum in culture media or albumin in wash buffers was able to mitigate the potential mechanical damage to the cells. For applications requiring serum-free buffers, hydroxyethyl starch and dextran 40 are examples of non-protein additives that are often used in cell manufacturing to protect against hydrodynamic stress^{24,25}.

Counterflow centrifugation technology has been used in large-scale biopharmaceutical manufacturing and blood product processing¹⁷. The applications of CFC technology in small-scale cell manufacturing (i.e., 0.1–10 L) are often limited to isolating mononuclear cells from apheresis products, such as the Elutra (Terumo BCT)²⁶, in which additional manual intervention is required to perform wash and concentrate steps. Other small-scale cell processing platforms include membrane filtration-based buffer exchange systems such as the LOVO (Fresenius Kabi)²⁷ and vertical centrifugation separation such as the Sepax (GE Healthcare)²⁸. Although it is difficult to

perform a direct comparison between devices, one of the advantages of this counterflow centrifugal device is its capacity to deliver very small output volumes (minimum 5 mL), which is the smallest among currently available cell processing platforms. The small output volume is suitable for applications such as formulating cells for local injections²⁹ or infusions for neonates³⁰. The camera embedded in the device is also a unique feature that provides visualization of the fluidized cell bed during the process development stage.

One of the limitations of the CFC technology is that it is sensitive to the size and density of the cells. When setting up a buffer exchange protocol for a different cell type, the protocol presented here should serve as a guideline for users to optimize according to their needs, keeping in mind the size of their cells of interest and the density of their cell suspension. Although the current protocol is usable for processing up to 5 L of media, the processing time will be substantially extended (i.e., 1–2 h). It is important to note that the impact of extended processing time on cell quality has not been examined in this current study.

Future studies will evaluate the impact of processing speed and processing time on cell function to determine the maximum processing capacity of the device. Furthermore, future studies may explore other applications such as the removal of dimethyl sulfoxide (DMSO) from cryopreserved products and selective removal of dead cells.

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DISCLOSURES:

SW, IF, and DJ are COO, CTO, and CEO of Scinogy Pty. Ltd. The access to the CFC device was also provided by Scinogy.

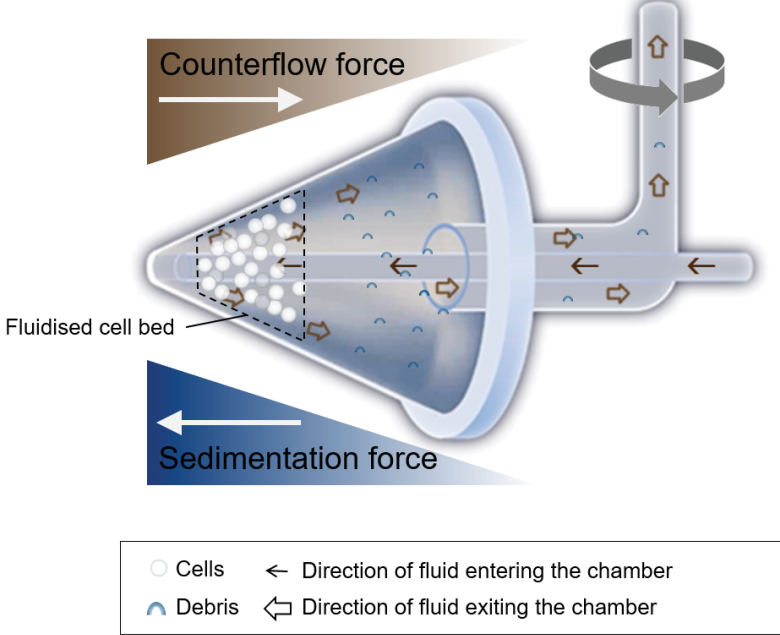
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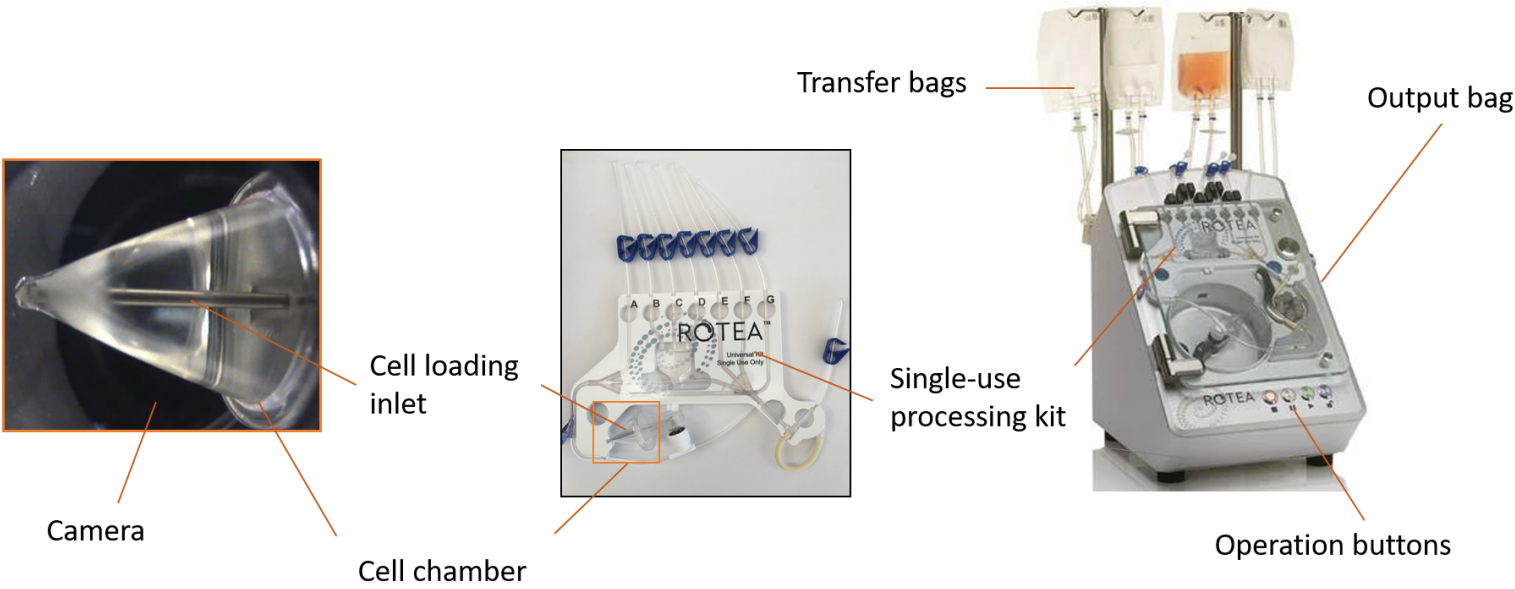
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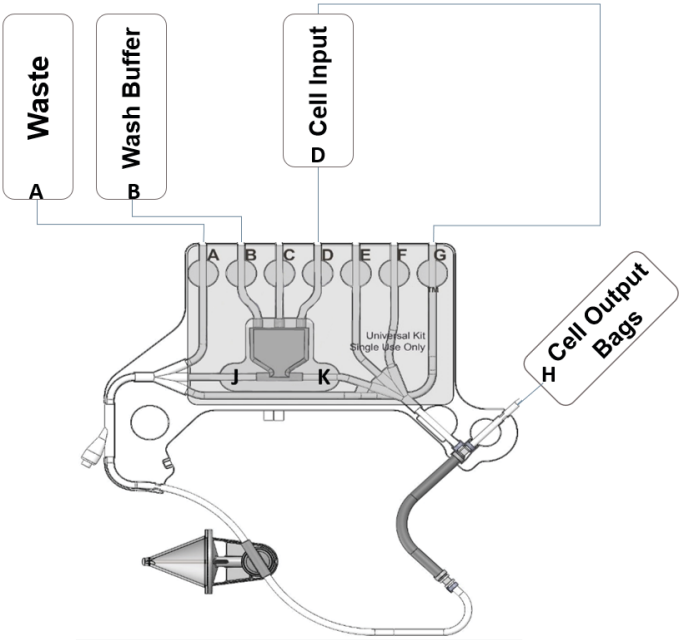
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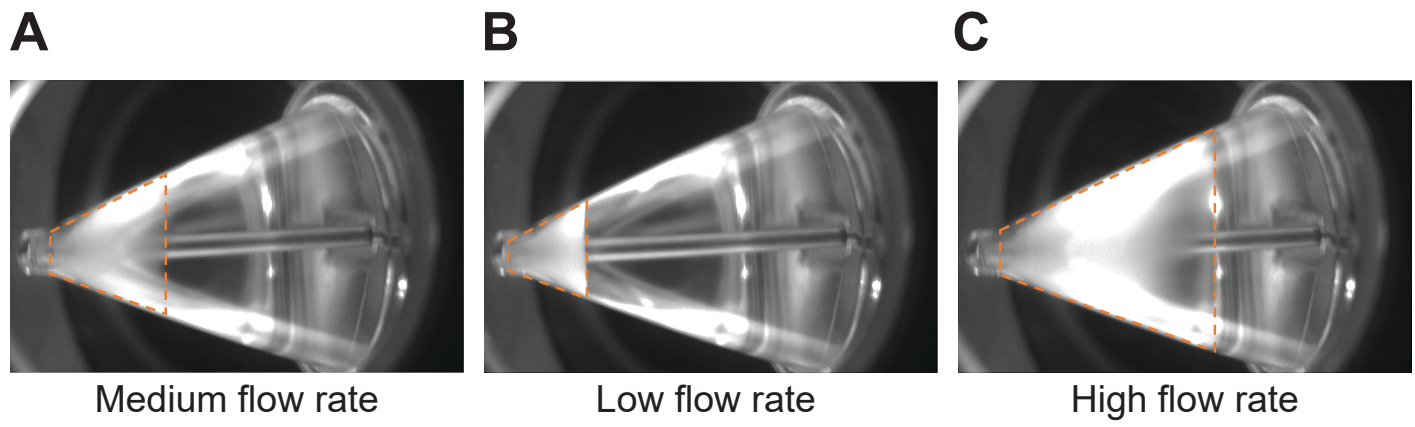


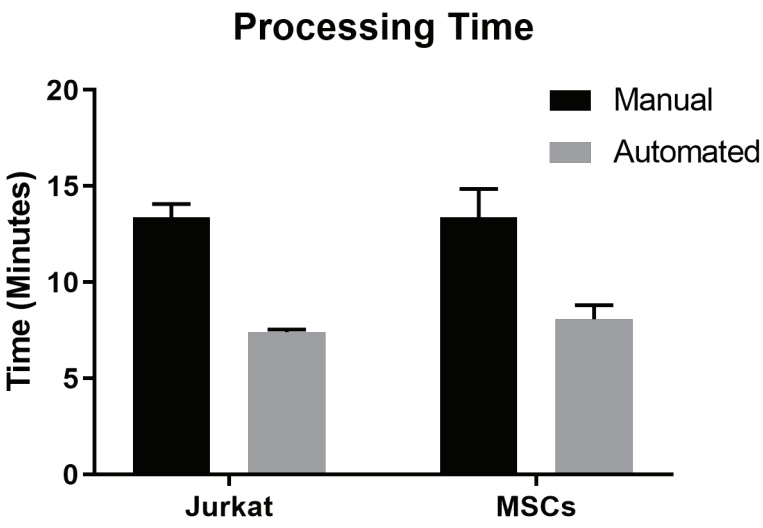
B



C



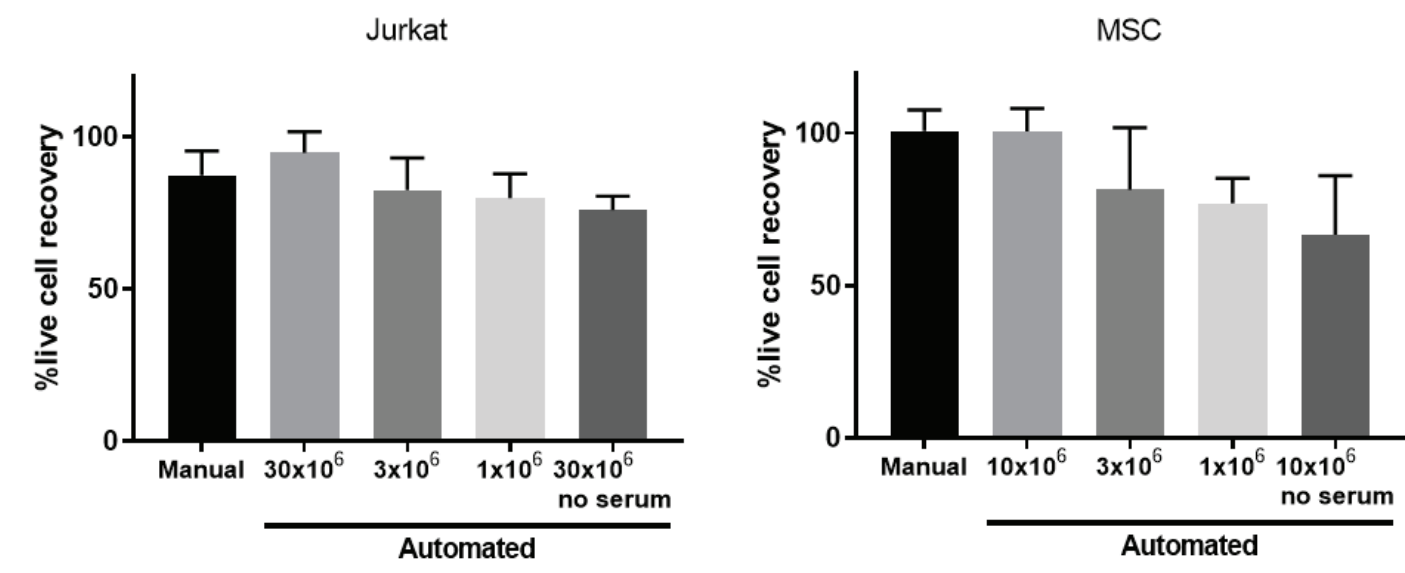




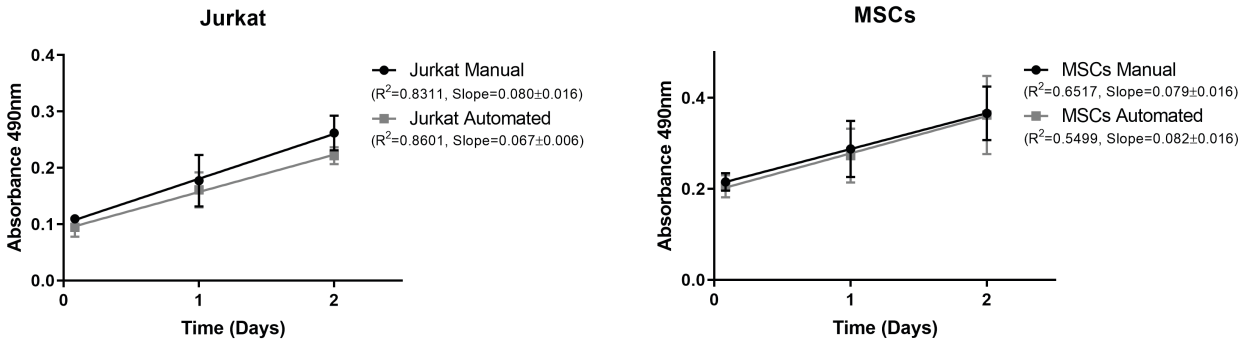
A

Cell type	<u>Jurkat</u>		MSC	
Processing method	Manual (n=4)	Automated (n=8)	Manual (n=6)	Automated (n=9)
Cell viability (before)	88.3 ±3.2%	85.6 ±5.5%	88.9 ±6.8%	93.3 ±4.2%
Cell viability (after)	86.9 ±5.8%	88.9 ±5.1%	94.3 ±3.1%	95.9 ±1.5%

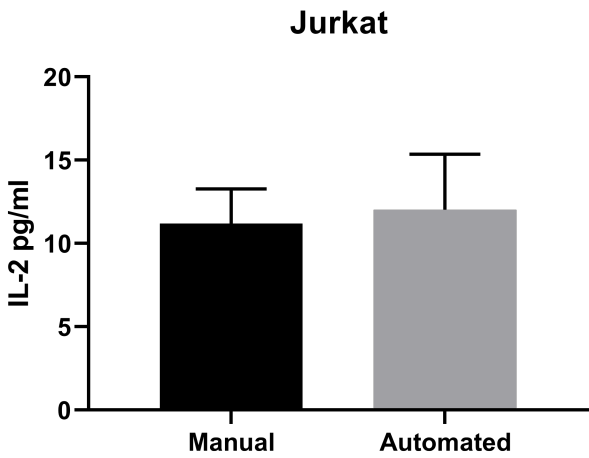
B



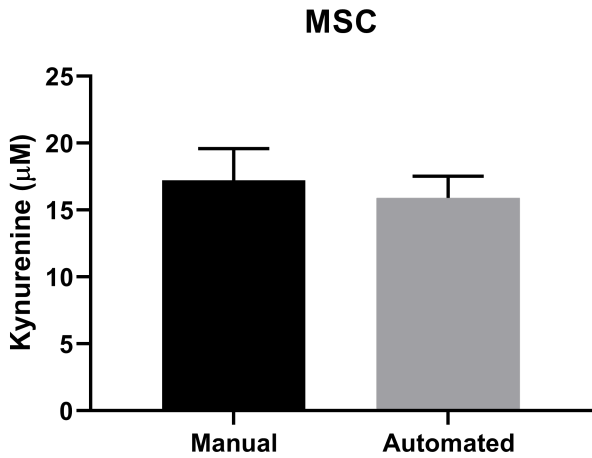
A

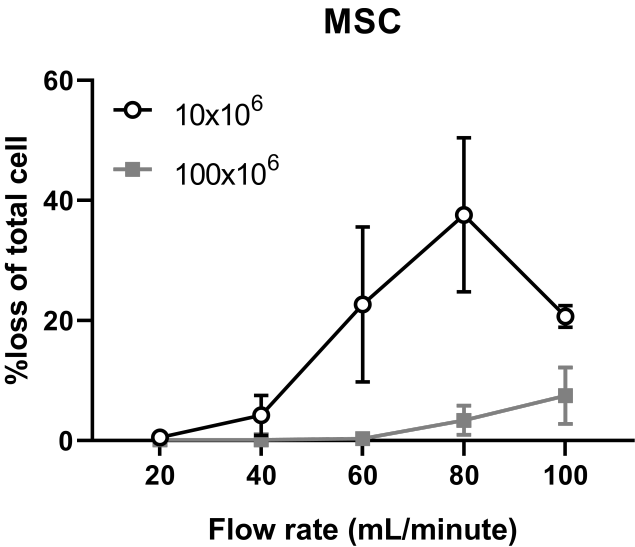
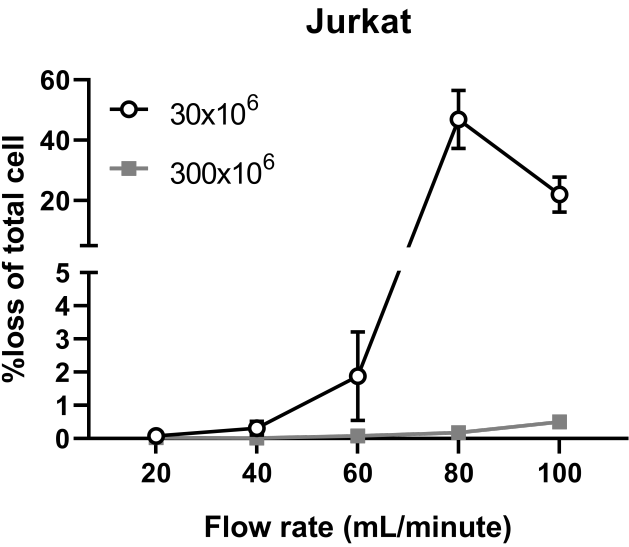


B



C





Step Number	Description	Open valves	Centrifuge speed (g)	Pump speed (ml/min)
1	Prime tubing from B to A	A, B, K	10	50
2	Fill bubble Trap from A to B	A, B, K	100	50 (reverse)
3	Prime tubing A to D	A, D, K	100	50 (reverse)
4	Prime tubing J to K	J, K	100	50
5	Load cells – initial start D to G	D, K, G	1600 (Jurkat)	25 (Jurkat) 30 (MSCs)
6	Load cells with bubble detect [At the detection of bubble/ empty tubing, the program will pause and wait for operator's command, press 'pause' or 'next']	A, D, K	= last step	30 (Jurkat) 35 (MSCs)
7	Empty remaining media on port D tube	A, D, K	= last step	= last step
8	Wash cells 1	A, B, K	= last step	20
9	Ramping up washing speed	A, B, K	= last step	35
10	Wash Cells 2	A, B, K	= last step	= last step
11	Prepare to harvest	J, K	= last step	= last step
12	Recover cells to output and dilute to target volume	B, J, K	= last step	60 (Reverse)

Note: '= last step' is a setting option for centrifuging speed and pump speed in the GU

Triggers
Volume: 45 ml
Volume: 10 ml
Volume: 2 ml
Volume: 3 ml
Volume: 100 ml
Bubble sensor D
Volume: 1.5 ml
Volume: 20 ml
Timer: 5 seconds speed ramping
Volume: 20 ml
Timer: 2 seconds
Volume: 10 ml

I.

Name	Company	Catalog Number
20 ml Luer lock syringes	BD	302830
20% Human serum albumin (HSA)	CSL Behring	AUST R 46283
4-(Dimethylamino)benzaldehyde	Sigma-Aldrich	156477-25g
500ml IV saline bag	Fresenius Kabi	K690521
Antibiotic-Antimycotic	Thermo Fisher Scientific	15240112
Automated cell counter (Countess)	Thermo Fisher Scientific	N/A
Cell counting chamber slides	Thermo Fisher Scientific	C10228
Cell stimulation cocktail (500x)	Thermo Fisher Scientific	00-4970-93
Cell transfer bags	Terumo	T1BBT060CBB
CellTiter AQueous One Solution Cell Proliferation Assay (MTS)	Promega	G3582
Centrifuge	Eppendorf	5810R
DMEM: F12 media	Thermo Fisher Scientific	11320082
EnVision plate Reader	Perkin Elmer	N/A
Fetal bovine serum (FBS)	Thermo Fisher Scientific	10099141
Human Interleukin 2 (IL2) Kit	Perkin Elmer	AI221C
Luer (female) fittings	CPC	LF41
PC laptop or PC tablet device	ASUS	N/A
Plate reader (SpectraMax i3)	Molecular Device	N/A
Recombinant Human IFN- γ	PeptoTech	300-02
Rotea counterflow centrifuge cell processing device	Scinogy	N/A
Rotea single-use processing kit	Scinogy	N/A
RPMI media	Thermo Fisher Scientific	11875119
Surgical scissors	ProSciTech	420SS
Trichloroacetic acide	Sigma-Aldrich	T6399-250g
Trypan Blue stain	Thermo Fisher Scientific	T10282
Trypsin digestion enzyme (TrypLE Express Enzyme)	Thermo Fisher Scientific	12604013

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Title of Article:	An automated counterflow centrifugal system for small scale downstream process
Author(s):	Anqi Li, Stephen Wilson, Ian Fitzpatrick, Mehri Barabadi, Siow Teng Chan, Mirja Krause, Gina Diamanta Kusuma, David James, Rebecca Lim

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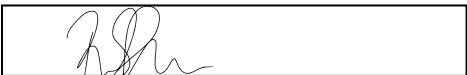
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CORRESPONDING AUTHOR

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Signature:		Date:	14th June 2019

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17th September 2019

Dear Editor-in-chief,

On behalf of my co-authors, I am pleased to submit the revision of our manuscript, “**An automated counterflow centrifugal system for small scale downstream process**” for publication in the Journal of Visualized Experiments.

We thank the editors and reviewers for their insights and the opportunity to respond to their comments. We appreciate the time taken to collectively improve this manuscript. We have addressed each concern as detailed in our response below.

Editorial Comments:

- Please take this opportunity to thoroughly proofread the manuscript to ensure that there are no spelling or grammatical errors.

[This manuscript has been subjected to more proof reading and all grammatical and syntax errors have been corrected.](#)

- **Protocol Numbering:** All steps should be lined up at the left margin with no indentations. There must also be a one-line space between each protocol step.

[One-line space has now been added between each protocol step.](#)

- **Protocol Highlight:** Please highlight ~2.5 pages or less of text (which includes headings and spaces) in yellow, to identify which steps should be visualized to tell the most cohesive story of your protocol steps.

1) The highlighting must include all relevant details that are required to perform the step. For example, if step 2.5 is highlighted for filming and the details of how to perform the step are given in steps 2.5.1 and 2.5.2, then the sub-steps where the details are provided must be included in the highlighting.

[Filming protocol has been highlighted, including the sub-steps and excluding notes](#)

2) Some of your shorter protocol steps can be combined so that individual steps contain 2-3 actions and maximum of 4 sentences per step.

[A few short protocol steps has been combined.](#)

3) The highlighted steps should form a cohesive narrative, that is, there must be a logical flow from one highlighted step to the next.

[The highlighted steps follow the operational order of the protocol.](#)

4) Please highlight complete sentences (not parts of sentences). Include sub-headings and spaces when calculating the final highlighted length.

[The total length of the highlight is around 1.5 pages.](#)

5) Notes cannot be filmed and should be excluded from highlighting.

[No notes were highlighted.](#)

- **Discussion:** JoVE articles are focused on the methods and the protocol, thus the discussion should be similarly focused. Please ensure that the discussion covers the following in detail and in paragraph form (3-6 paragraphs): 1) modifications and troubleshooting, 2) limitations of the technique, 3) significance with respect to existing methods, 4) future applications and 5) critical steps within the protocol.

The modifications and troubleshooting are discussed in 2 paragraphs, lines 260-276. Limitations of the technique are listed in line 302-306. Significance with respect to existing methods is discussed in lines 288-300. Future applications in lines 308-311. Critical steps within the protocol is lines 278-286.

- **Figure/Table Legends:** Define error bars in all figures.

All error bars are now defined.

- **References:** Please spell out journal names.

The spelling of journal names has been checked.

- **Commercial Language:** JoVE is unable to publish manuscripts containing commercial sounding language, including trademark or registered trademark symbols (TM/R) and the mention of company brand names before an instrument or reagent. Examples of commercial sounding language in your manuscript are Rotea™

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The commercial name of the product has been removed. The Rotea is now referred to as the 'CFC device'.

2) Please remove the name ROTEa from fig 1

The Rotea name in figure 1B has been removed.

- Please define all abbreviations at first use.

All abbreviations have been checked and defined.

- If your figures and tables are original and not published previously or you have already obtained figure permissions, please ignore this comment. If you are re-using figures from a previous publication, you must obtain explicit permission to re-use the figure from the previous publisher (this can be in the form of a letter from an editor or a link to the editorial policies that allows you to re-publish the figure). Please upload the text of the re-print permission (may be copied and pasted from an email/website) as a Word document to the Editorial Manager site in the "Supplemental files (as requested by JoVE)" section. Please also cite the figure appropriately in the figure legend, i.e. "This figure has been modified from [citation]."

Comments from Peer-Reviewers:

Reviewer #1:

Manuscript Summary:

The authors described the use of a counterflow centrifugal cell processing device for automating the buffer exchange and cell concentration steps for small-scale bioprocessing. The protocol is useful

and could be used for small-scale processes in a closed manner, compatible with GMP guidelines. My only concern is about the COG. Since the system is single-use, the COG will not be lower than the traditional method used (centrifugation), especially in a small-scale scenario. Please try to focus in the fact that the system is closed and automated, not of being cost-effective.

The benefit of automation in the introduction has been revised in Line 78-89, which includes improved sterility and scalability and minimisation of operator variation. Cost-effectiveness is discussed but is not the focus of the manuscript, as suggested by Reviewer 1.

Minor Concerns:

-Page 3, line 80: "A recent cost analysis report identified labour as the main cost in GCT, accounting for almost 50% of the cost of goods (CoG)"

Is this for autologous or allogeneic product? Which process are you referring? Please provide more details for this important information.

The cost analysis study was in reference to an autologous product and refers to the entire manufacturing process. Details have been added to the manuscript (lines 85-86).

-Page 3, line 90: The authors state that automated platforms commercially available for cell manufacturing include Cocoon and CliniMACS Prodigy that is not suitable for adherent cell cultures. However, the Quantum system (Terumo BCT) provides protocols for adherent or suspension cells in a fully automated system. Please revise.

We thank Reviewer 1 for pointing this out and we have now revised our manuscript to include the Quantum system (lines 95-103).

Cell viability after the process is the most important information. The results is presented in the table 2. How the authors measured the cell viability? Flow cytometry? Please add this information.

Cell viability was measured by trypan blue exclusion and an automated cell counter. This information has been added to the figure legend, lines 441-442.

As already mentioned, the authors describe that implementing automation, the COG can be reduced. However I am not sure if in this case, the costs will be truly reduced especially due to the fact that the method proposed is intended for small-scale. Could authors estimate the costs of the traditional method (centrifugation, etc.) and Rotea including labour, time, consumables, reagents? Just to justify and extol the work.

Reviewer 1 raises a valid point and in staying true to our claims, the emphasis of our protocol has been refocussed to closed and automated process.

Reviewer #2:

Manuscript Summary:

It appears sufficient work has been done to optimize the process. It may be useful to provide data demonstrating the observations noted in the discussion, such as minimum cell numbers, flow rates,

pump speeds, and presence of serum. For example, a graph showing recovery across multiple centrifuge and pump speed configurations.

We agree with Reviewer 2 that adding observations noted in the discussion would be useful. To this end, we have added cell recovery data from runs with a suboptimal number of cells and in the absence of serum (Figure 4b). Additionally, we have also added a new figure demonstrating the percentage cell loss across different flow rate (Figure 6).

Major Concerns:

The addition of at least one functional characterization assay to complement the viability and recovery data per cell type would be suggested.

We agree with Reviewer 2 that adding functional characterisation assays would complement our viability and recovery data. Accordingly, we have added the measurement of cytokine/enzyme production from each cell type as an additional assay to complement the protocol. The data have been provided in Figure 5.

More focus on both the advantages and limitations of the Rotea could be outlined in the discussion, in addition to suggested use cases.

We agree with Reviewer 2 that this would benefit the quality of our paper and have this included the advantages of Rotea in lines 299-304 and 306-309.

Lines 86-95: The highlighting of fully-automated platforms appears here, but the capabilities of these two options doesn't match with the function of the Rotea. Instead, the mention of more similar CFC processing technology was listed in lines 254-268 in the discussion. Comparison of these offerings is more pertinent to match the Rotea's functionality as demonstrated in this manuscript. Pros and cons of the device could be placed either completely in the introduction or discussion for comparison to other platforms.

The fully automated platforms discussed in the introduction part (line 90-101) was intended to inform the reader of the different ways of implementing automation, in particular, highlighting the need of the modular-based approach. However, we understand the concerns of Reviewer 2, and as such the wording in this paragraph has been updated to clarify our intention. Additionally, the significance of the protocol is discussed in the discussion in comparison to current existing technology (lines 292-298), in accordance to requirements of the journal.

Line 100-107: A figure or schematic illustrating the centrifugal force, opposite fluid flow, flow gradient, and separation of live cells and debris would be helpful here. This could also be supported by the current Figure 1, where an additional device schematic could show these concepts.

We have now included a schematic illustration is added in Figure 1 to describe all the forces.

Minor Concerns:

Line 90: Further elaborate on the types of operating protocol limitations here.

We have elaborated on the operating protocol limitations in lines 98-103 to describe how a fully integrated system may be restricted by its the culturing capacity.

Line 92: It would be useful here to identify examples of "typical adherent mammalian cell cultures" that are being used/investigated as cell therapies.

In our response to Reviewer 1, we have added Quantum (Terumo BCT) system to this paragraph and as such we have removed the statement in line 92.

Line 107-111: This use case of CFC seems to diverge from the focus of the paper. Specific cell population isolation isn't investigated for the protocol.

We have removed the statement around use of the CFC device for cell population isolation.

Line 132: It is unclear from the protocol only if the cultured cells were grown in flasks or culture bags. This would be important to identify at which step the open versus closed system processes take place for this protocol.

Thank you for pointing this out. Our protocol used cells cultured in flasks, and we have now clarified this in protocol step 1.2. line 142-149

Figure 4: Further elaboration in the figure caption would be recommended to accurately label what constitutes as the "cell bed" as described in the manuscript.

We have now updated this (now Figure 2) to include a dotted line to outline the area that is occupied by the 'cell bed'.

We thank the editor and reviewers again for taking time to review this re-submission and look forward to hearing from you in due course.

Kind regards,

A handwritten signature in black ink, appearing to read 'Rebecca Lim', with a stylized, flowing script.

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