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Mapping Regional Homogeneity and Functional Connectivity of the Visual Cortex in Resting-State fMRI --Manuscript Draft--

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Additional Information:	
Question	Response
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Please indicate the city, state/province, and country where this article will be filmed . Please do not use abbreviations.	Wuhan, Hubei Province, China

Dear editor:

We would like to submit the enclosed manuscript '**Mapping regional homogeneity and functional connectivity of visual cortex in resting-state fMRI**', which we wish to be considered for publication in *JoVE*. The presented procedure is based on previously published data in Dan *et.al*, *Vision Research* (2019).

A combined regional homogeneity (ReHo) and functional connectivity (FC) methods, a non-invasive fMRI method was conducted to evaluate synchronous neuronal activity changes in RP group. Our study highlights that the visual network disconnection and reorganization of retino-thalamocortical pathway and dorsal visual stream occurred in the RP patients.

To share this experience and to support the dissemination of this expertise, this work describes our setup and protocol of processing the fMRI data.

Best regards,

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TITLE:**Mapping Regional Homogeneity and Functional Connectivity of the Visual Cortex in Resting-State fMRI****AUTHORS AND AFFILIATIONS:**

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KEYWORDS:

retinitis pigmentosa, visual loss, regional homogeneity, resting-state fMRI, visual cortex, functional connectivity

SUMMARY:

We present a protocol for analyzing functional magnetic resonance imaging data to investigate spontaneous neural activity alterations in retinitis pigmentosa patient using a combined regional homogeneity and functional connectivity method.

ABSTRACT:

A combined regional homogeneity (ReHo) and functional connectivity (FC) method, a type of noninvasive functional magnetic resonance imaging (fMRI) method, has been used to evaluate synchronous neuronal activity changes in retinitis pigmentosa (RP). The purpose of this study is to describe our method for analysis of intra- and interregional synchronizations of changes in neuronal activity in RP patients. The advantages of the combined ReHo and FC method are that it is both noninvasive and sufficiently sensitive to investigate changes in cerebral synchronous neuronal activity changes in vivo. Here, 16 RP patients and 14 healthy controls closely matched in age, sex, and education underwent resting-state fMRI scans. Two sample t-tests were conducted to compare ReHo and FC across groups. Our results showed that visual network disconnection and reorganization of the retino-thalamocortical pathway and dorsal visual stream occurred in the RP patients. Here, we describe the details of this method, its use, and the impact of its key parameters in a step-by-step manner.

INTRODUCTION:

Functional magnetic resonance imaging (fMRI) is a noninvasive method that can be used to investigate alterations in brain function and structure in vivo. Regional homogeneity (ReHo) and functional connectivity (FC) are often used to assess intra-and interregional synchronizations of brain activity. ReHo, a resting-state fMRI methodology, is used to calculate similarity between the time series of a given voxel and its nearest neighbors, which reflects the local synchronization of brain activities¹. FC is used to investigate the similarity between spatially remote regional time series².

fMRI technology can offer an objective assessment of visual function in the context of eye disease management. Here, we present a methodological protocol that combines ReHo and FC methods to share this experience and support the dissemination of our expertise. In the present work, we used the ReHo and FC protocol in retinitis pigmentosa (RP) subjects and healthy controls (HCs) to elaborate the details of the procedure. RP is a serious hereditary eye disease characterized by impaired night vision and the progressive loss of vision^{3,4}. Genetic mutation is the main risk factor for RP. The death of rod and cone photoreceptor cells leads to the loss of peripheral vision and finally blindness in RP patients. Previous neuroimaging studies have shown structural and functional abnormalities in the visual cortex and visual pathway of RP patients⁵⁻⁷. Moreover, diffusion tensor imaging was used to investigate the integrity of white matter fiber bundles. RP patients showed significantly higher apparent diffusion coefficient, principal eigenvalue, and orthogonal eigenvalue, as well as significantly lower fractional anisotropy in the optic nerves, relative to HCs⁸.

Here, our aim was the exploration of intra- and interregional synchronizations of neuronal activity. We investigated whether the mean ReHo values and mean FC values were correlated with clinical variables in RP patients. Our method might enable researchers to obtain important insights into the neural mechanism of peripheral vision loss in RP patients.

PROTOCOL:

The research protocol was approved by the medical ethics committee of the Renmin Hospital of Wuhan University. All participants completed a written consent form.

1. Participant classification and screening

1.1. Enroll RP subjects and HCs closely matched in age, gender, and education.

1.2. Ensure that all participants meet the following criteria: 1) able to be scanned with an MRI scanner (e.g., no cardiac pacemakers or implanted metal devices); 2) no claustrophobia; 3) no heart disease, hypertension, or cerebral diseases.

2. Acquisition of fMRI data

NOTE: A 3 T MRI scanner with eight-channel head coil is used in this protocol.

2.1. Ask each participant to remove metal objects before entering the MRI scanner room after a final safety check.

2.2. Instruct the participant to lie down on the bed and ensure that the orbitomeatal line is perpendicular to the bed. Then place foam pads in the bilateral temporal region of the head to prevent head movement and provide earplugs to reduce the noise of the scanner.

2.3. Instruct the participant to lie at rest, to keep his/her eyes closed without falling asleep, and not think of anything in particular during scanning.

2.4. Adjust the participant's head position through the positioning light. Make sure that the axis positioning cursor is parallel to the lateral canthus and the sagittal positioning cursor coincides with the midline of the face. Next, move the bed to make the axis positioning cursor stay 2 cm above or below the participant's eyebrows.

2.5. Notify the participant of the start of the scanning session. Using the scanning console, start the structural localizer scanning to determine the position of the participants' head in the scanner and allow planning for subsequent structural and functional scans.

2.6. Perform fMRI with the following sequences and parameters.

2.6.1. Perform three-dimensional brain volume imaging (3D-BRAVO) MRI with the following parameters: repetition time (TR)/echo time (TE) = 8.5 ms/3.3 ms; thickness = 1.0 mm; no intersection gap; acquisition matrix = 256 x 256; field of view = 240 x 240 mm²; and flip angle = 12°.

2.6.2. Obtain functional images using gradient echo-planar imaging blood oxygenation level-dependent (EPI-BOLD) imaging with the following parameters: TR/TE = 2,000 ms/25 ms; thickness = 3.0 mm; gap = 1.2 mm; acquisition matrix = 256 x 256; field of view = 240 x 240 mm²; voxel size = 3.6 x 3.6 x 3.6 mm³; and 35 axial slices.

2.7. Keep an eye on the condition of the participant during the duration of the scan, instruct them to move as little as possible, and stop scanning if the participant has any discomfort.

2.8. Remove the participant from the scanner and ask the participant to sit up carefully at the end of the experiment.

3. Data preprocessing and software preparation

NOTE: The functional images analyzed in this protocol are preprocessed by SPM8 and the toolbox for Data Processing & Analysis for Brain Imaging (DPABI, <http://rfmri.org/dpabi>)⁹ based on MATLAB 2013a. Perform the following preprocessing steps separately for each fMRI session.

3.1. Open the DPABI software in the MATLAB terminal by clicking **dpabi**, then choose **DPARSE 4.3 Advanced Edition** and import the folder "**FunRaw**" (**Figure 1**).

NOTE: The FunRaw folder contains the DICOM file for each participant.

3.2. Click **FunRaw** to import the fMRI scan files into DPABI with a consistent numbering scheme (e.g., "sub0001", "sub0002", etc.). Select the working directory and the initial EPI and T1 directories and continue to select all desired parameters in steps 3.3–3.9 before clicking **Run** in section 4.

3.3. Type the parameters: Timing points = 240 and TR = 2 (**Figure 2**). Select the **EPI DICOM to NIFTI** to convert the functional images from DICOM to NIFTI format and remove the first 10 volumes of each function images.

3.4. Check the boxes for **Slice Timing** and **Realign** in the DPABI software to correct the remaining 230 volumes of functional blood oxygenation level-dependent images for slice timing effects and head motion corrected.

NOTE: For head motion, the data of participants with head movement >2 mm or rotation >2° during scanning should be excluded. For slice order, the sequence of numbers in the vector is the acquisition time order of these layers. The selected slice number is 40, slice order is [1:2:39,2:2,40], and the reference slice is 39.

3.5. Select **Normalize by DARTEL** with the DPABI software.

NOTE: By selecting this option, the software will automatically perform spatial normalization using individual T1-weighted structural images registered to the mean fMRI data. The resulting aligned T1-weighted images are segmented using the DARTEL toolbox for improved spatial precision during normalization of fMRI data. Normalized data (in Montreal Neurological Institute [MNI] 152 space) are resliced at a resolution of 3 x 3 x 3 mm³.

3.6. Remove the linear trend by selecting **Detrend** in the DPABI software.

3.7. Check the box for **Nuisance Covariates Regression** and select the following parameters: head motion model, white matter signal, global mean signal, and cerebrospinal fluid signal.

3.8. Check the box for **Scrubbing** to remove the bad time points due to head motion in the DPABI software.

3.9. Retain signals between 0.01–0.08 Hz by checking the box **Filter [0.01-0.08]** in the DPABI software to remove high-frequency physiological noise and low-frequency drift.

NOTE: After the data preparation, ReHo and FC analysis can be performed.

4. ReHo and FC analysis

4.1. For the ReHo computation, open the DAPABI software through MATLAB and select **27 voxels** in the cluster. Left click **ReHo** and **smooth [6*6*6]**, then select **Run**.

NOTE: A Kendall's coefficient of concordance is assigned to a given voxel by calculating the Kendall's coefficient of concordance of time series of 27 voxels and their nearest neighbors. To reduce the influence of individual variations on statistical comparisons between groups, ReHo maps of each voxel are z-transformed using Fisher's r-to-z transformation. The remaining z ReHo maps are spatially smoothed using a Gaussian kernel of 6*6*6 full width at half maximum.

4.2. For the FC computation, open the DAPABI software through MATLAB and define the altered ReHo brain regions between both groups as regions of interest (ROIs). Click on **Functional Connectivity** and define the ROI (centering at x = 0, y = -69, and z = -3 with radius = 10 mm), then select **Run**.

NOTE: Correlation analysis of the time course for each participant is performed between the spherical seed region and whole brain voxels. All FC maps are z-transformed by Fisher's r-to-z transformation to reduce the influence of individual variations on statistical comparison between groups. The radius of the ROIs around the coordinates should be 10 mm (X = 0, Y = -69, Z = -3).

5. Statistical analysis

5.1. Find the folders named ReHo and FC after processing the relevant file data. Sort the files of zReHo.nii and zFC.nii, classifying them into four subfolders: "RP-group-ReHo", "HC-group-ReHo", "RP-group-FC", and "HC-group-FC".

5.2. Open DPABI through MATLAB to perform a one sample t-test.

5.2.1. Left click **Statistical Analysis**, then click **one-Sample t-test**. Name the output result "one-sample-t-test-RP" and set the output directory.

5.2.2. Left click **Add Group Images** and open the "RP-group-ReHo" subfolder.

5.2.3. In the **Mask File** option, left click to open the "BrainMask-05-61*73*61" subfile in the "mask" folder.

5.2.4. Select **Compute** to run the program. Perform this same procedure for the "one-sample-t-test-HC" group.

NOTE: The one-sample t-test is used to analyze and display mean ReHo maps of each group in DPABI software.

5.3. Open DPABI through MATLAB to perform a two sample t-test.

5.3.1. Left click **Statistical Analysis**, then select **two-sample t-test**. Name the output result "two-sample-t-test-ReHo" and set the output directory.

5.3.2. Left click **Add Group Images** and open the "RP-group-ReHo" and "HC-group-ReHo" subfolders.

5.3.3. In the **Mask File** option, left click to open the "BrainMask-05-61*73*61" subfile in the "mask" folder.

5.3.4. Select **Compute** to run the program. Perform this same procedure for the "two-sample-t-test-FC". Click **Statistical Analysis** and **Gaussian random field (GRF) correction [two-tailed, voxel-level (0.01) and voxel-level (0.05)]** and then click **Run**.

NOTE: The differences between groups of zReHo maps and zFC maps are compared by two sample t-tests. GRF is used to correct for multiple comparisons and regressed covariates of age and sex with DPABI software.

5.4. Use BrainNet Viewer software (<https://www.nitrc.org/projects/bnv/>) to show the results.

5.4.1. Open BrainNet through MATLAB and click on **Load file**. For surface files, click **Browse** and select **BrainMesh-ICBM152-smoothed.nv**, then click **Ok**; for volume files, select **spm-T.nii** (this includes ReHo and FC results), then click **Ok**.

5.5. Use statistical software to process the data obtained from the previous step.

NOTE: The chi-squared test is used for sex comparisons, while independent-samples t-tests are used for other clinical variables. Continuous variables are represented by means and standard deviations.

5.6. Conduct Pearson correlation coefficient analysis to identify the relationships between zReHo values and zFC values of different brain regions and visual measurements data by using statistical software.

5.6.1. Obtain ROI signals of zReHo values and zFC values in each participant by DPABI software. Click **ROI signals extractor** and **Add directory with ROI mask.nii file**.

NOTE: P values of <0.05 should be considered statistically significant.

REPRESENTATIVE RESULTS:

In our study, 16 RP individuals and 14 healthy controls closely matched in age, sex, and education underwent resting-state fMRI scans. ReHo and FC methods were used to explore the intra-and intersynchronous neuronal activity in RP individuals. Significant differences in BCVA were

observed between the right eye ($P < 0.001$) and the left eye ($P < 0.001$), but the difference in gender, age, or weight between the groups was not significant.

The RP and HCs show similar spatial distribution in the ReHo maps. However, the ReHo value of the visual area in RP patients was significantly lower than that in the control group (**Figure 3A,B**). Compared with HCs, the ReHo values of the RP individuals were significantly lower in the bilateral LGG/CPL (BA 17,18) compared to the HCs (**Figure 4** and **Table 1**) (Two-tailed, voxel-level $P < 0.01$, GRF correction, cluster-level $P < 0.05$).

Compared with the HCs group, the RP group showed increased FC between the bilateral LGG/CPL and bilateral thalamus and decreased FC between the bilateral LGG/CPL and left postcentral (**Figure 5** and **Table 2**).

FIGURE AND TABLE LEGENDS:

Figure 1: The operation interface of the DEPASFA toolbox.

Figure 2: The operation interface of the DEPASFA toolbox with parameters entered.

Figure 3: The distribution pattern of ReHo values in the RP and HC participants in the typical frequency band (0.01–0.08 Hz). Within-group means ReHo maps within the RP participants (**A**) and the HCs (**B**). ReHo = regional homogeneity; RP = retinitis pigmentosa; HC = health control; L = left hemisphere; R = right hemisphere.

Figure 4: Comparisons of the ReHo values between the RP and HCs participants. There were significant regional differences in spontaneous activities between the two groups. ReHo values of RP participants were significantly lower in the bilateral LGG/CPL (BA 17,18) compared to those of HCs. The blue areas indicate lower ReHo values (two-tailed, voxel-level $P < 0.01$, GRF correction, cluster-level $P < 0.05$). GRF = Gaussian random field; LGG = lingual gyrus; CPL = cerebellum posterior lobe.

Figure 5: Comparisons of seed-based FC of the altered ReHo between the RP and HC groups. There were significant differences in seed-based FC activities between the two groups. The color-bars indicate the T-values. FC = functional connectivity; L = left hemisphere; R = right hemisphere; GRF = Gaussian random field; LGG = lingual gyrus; CPL = cerebellum posterior lobe.

Table 1: Significant differences in the ReHo values between the two groups. The GRF theory was used to set the statistical threshold at the voxel level for multiple comparisons ($P < 0.01$). ReHo = regional homogeneity; BA = Brodmann area; RP = retinitis pigmentosa; HC = health control; MNI = Montreal Neurological Institute; GRF = Gaussian random field.

Table 2: Comparison of seed-based FC values of the altered ReHo regions between the two groups. The GRF correction method was used to set the statistical threshold at the voxel level for multiple comparisons ($P < 0.01$). FC = functional connectivity; ReHo = regional homogeneity; ROI = region of interest; LGG = Lingual Gyrus; CPL = cerebellum posterior lobe; BA = Brodmann area;

RP = retinitis pigmentosa; HC = health control; MNI = Montreal Neurological Institute; GRF = Gaussian random field.

DISCUSSION:

This report describes a protocol for computing ReHo and FC values for RP and HC groups and showed significantly different ReHo and FC values between the two. Notably, an important step in this process is the classification and screening of samples before the experiment. When we applied this protocol for our own analysis, all RP subjects were diagnosed by two experienced ophthalmologists. We excluded RP patients with other eye diseases such as glaucoma, cataracts, and optic atrophy. In addition, HCs enrolled in our study have no heart disease, cerebral diseases, or hypertension. The results show that ReHo values of the visual cortex and FC between the visual cortices and motor cortices decreased significantly in RP participants, as well as increased FC between the visual cortices and thalamus. Qin et al. demonstrated that RP patients showed a decreased FC density in V1, which is consistent with our findings.¹⁰ These findings may indicate the disconnection and reorganization of the intrinsic visual network of the retino-thalamocortical pathway and dorsal visual stream, suggesting visuospatial and stereoscopic vision impairment.

Another important issue in this protocol is the statistical analysis. When a two-sample t-test was performed to compare the ReHo and FC indexes using DPABI software, the effects of nuisance covariates (age, sex, and head motion parameters) were removed during statistical analysis.

There are some limitations in this ReHo method. In particular, neuropsychiatric scaling is not conducted in RP patients. Mental state and physiological noise might influence the accuracy of the results. Furthermore, the protocol does not compare brain structure differences between the RP and HC groups.

In addition to the applications described here, our combined ReHo and FC-based method provides promising potential approaches for assessment of intra- and interregional brain activity synchronizations. This method provides an efficient and practical means for capturing the precise inceptions of fMRI signals and generating reliable results using our data postprocessing approach. In addition, amplitude of low-frequency fluctuation¹¹ and degree centrality¹² enable measurement of regional activity changes in the resting state. In the future, multimodal MRI technologies will be used to determine the functional and morphological changes in RP patients. This technique may be useful in the clinical realm as a diagnostic tool for RP patients as further understanding is achieved regarding the complexities of the human neuronal system.

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DISCLOSURES:

The authors have nothing to disclose.

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Data Processing Assistant for Resting-State fMRI

Advanced Edition **DPARSF A**

Working Directory: ...

Participants:

- sub1001
- sub1002
- sub1003
- sub1004
- sub1005
- sub1006
- sub1007

Time Points:

TR (s):

Blank ☐ EPI DICOM to NIFTI ☐ Apply Mats ☐ Remove First Time Points ☐ Slice Timing

Slice Number: Slice Order: Reference Slice: ☐ Realign ☐ Voxel-Specific Head Motion

☐ Reorient Fun* ☐ AutoMask ☐ T1 DICOM to NIFTI ☐ Crop T1 ☐ Reorient T1* ☐ Bet ☐ T1 Coreg to Fun

☐ Segment ☐ New Segment + DARTEL

☐ Nuisance Covariates Regression Polynomial trend: Head Motion model: ☐ Rigid-body 6 ☐ Derivative 12

☒ Friston 24 ☐ Voxel-specific 12 ☐ Head motion scrubbing regressors

Nuisance regressors (WM, CSF, Global) ☐ Other covariates ☐ Add mean back ☐ Filter (Hz): ~

☐ Normalize Bounding Box: Voxel Size:

☐ Normalize by using EPI templates ☐ Normalize by using T1 image unified segmentation ☐ Normalize by DARTEL

☐ Smooth ☐ Smooth by DARTEL FWHM:

☒ Default mask ☐ No mask ☐ User-defined mask Use Default Mask ... ☐ Warp Masks into Individual Space

☐ Detrend ☐ Nuisance Covariates Regression ☐ ALFF+1ALFF Band (Hz): ~ ☐ Filter

☐ Scrubbing ☐ ReHo Cluster: ☐ 7 ☐ 19 ☒ 27 voxels ☐ Smooth ReHo ☐ Degree Centrality

☐ Functional Connectivity ☐ Extract ROI time courses Define ROI ☐ Define ROI interactively* ☐ CWAS

☐ Normalize to Symmetric Template ☐ Smooth ☐ VMHC ☐ Normalize Derivatives ☐ Smooth Derivatives

Parallel Workers #: Functional Sessions #: Starting Directory Name:

Data Processing Assistant for Resting-State fMRI

Advanced Edition DPARSF A

Working Directory:

Participants:

sub1001

sub1002

sub1003

sub1004

sub1005

sub1006

sub1007

Time Points:
TR (s):

Blank ☐ ☒ EPI DICOM to NIFTI ☐ Apply Mats ☒ Remove First Time Points ☒ Slice Timing

Slice Number: Slice Order: Reference Slice: ☒ Realign ☐ Voxel-Specific Head Motion

☒ Reorient Fun* ☒ AutoMask ☒ T1 DICOM to NIFTI ☐ Crop T1 ☒ Reorient T1* ☒ Bet ☒ T1 Coreg to Fun

☐ Segment ☒ New Segment + DARTEL Affine Regularisation in Segmentation: ☐ East Asian ☒ European

☐ Nuisance Covariates Regression Polynomial trend: Head Motion model: ☐ Rigid-body 6 ☐ Derivative 12

☒ Friston 24 ☐ Voxel-specific 12 ☐ Head motion scrubbing regressors

Nuisance regressors (WM, CSF, Global) ☐ Other covariates ☐ Add mean back ☒ Filter (Hz): ~

☒ Normalize Bounding Box: Voxel Size:

☐ Normalize by using EPI templates ☐ Normalize by using T1 image unified segmentation ☒ Normalize by DARTEL

☐ Smooth ☐ Smooth by DARTEL FWHM:

☒ Default mask ☐ No mask ☐ User-defined mask Use Default Mask ☐ Warp Masks into Individual Space

☒ Detrend ☒ Nuisance Covariates Regression ☐ ALFF+IALFF Band (Hz): ~ ☐ Filter

☒ Scrubbing ☒ ReHo Cluster: ☐ 7 ☐ 19 ☒ 27 voxels ☒ Smooth ReHo ☐ Degree Centrality

☐ Functional Connectivity ☐ Extract ROI time courses Define ROI ☐ Define ROI interactively* ☐ CWAS

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Parallel Workers #: Functional Sessions #: Starting Directory Name:

Figure 3

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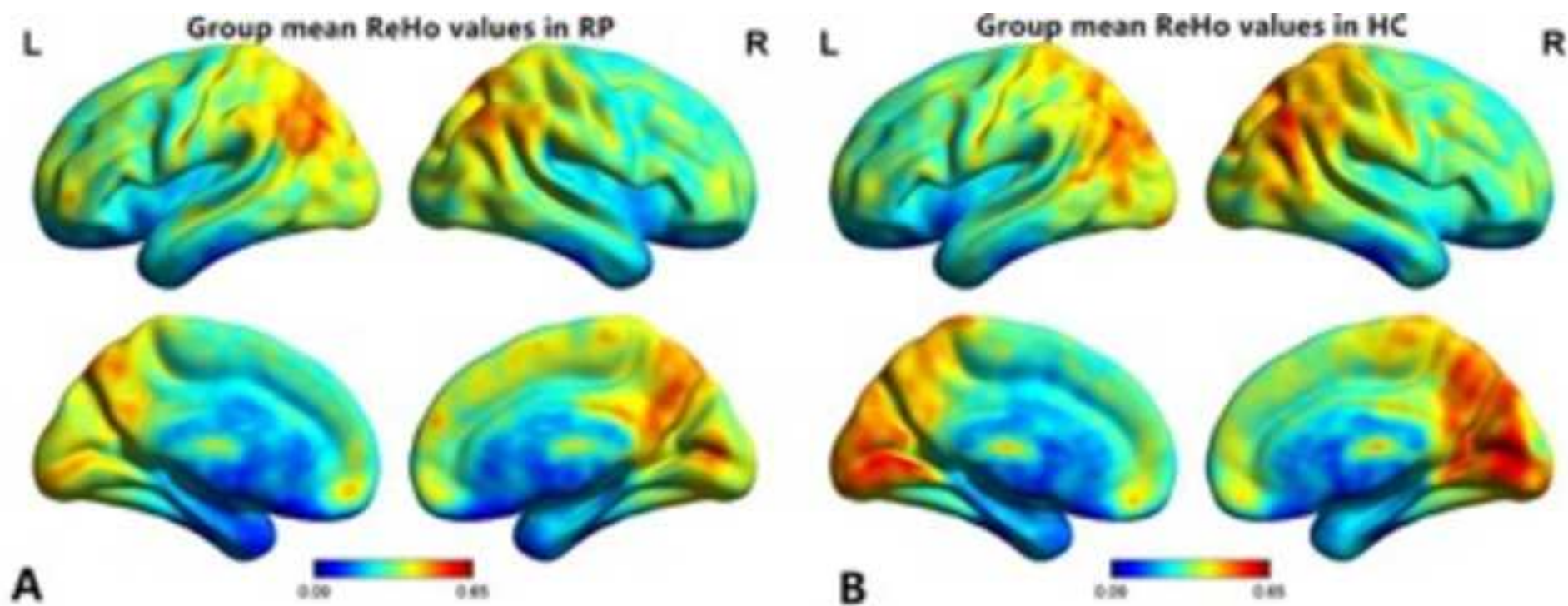


Figure 4

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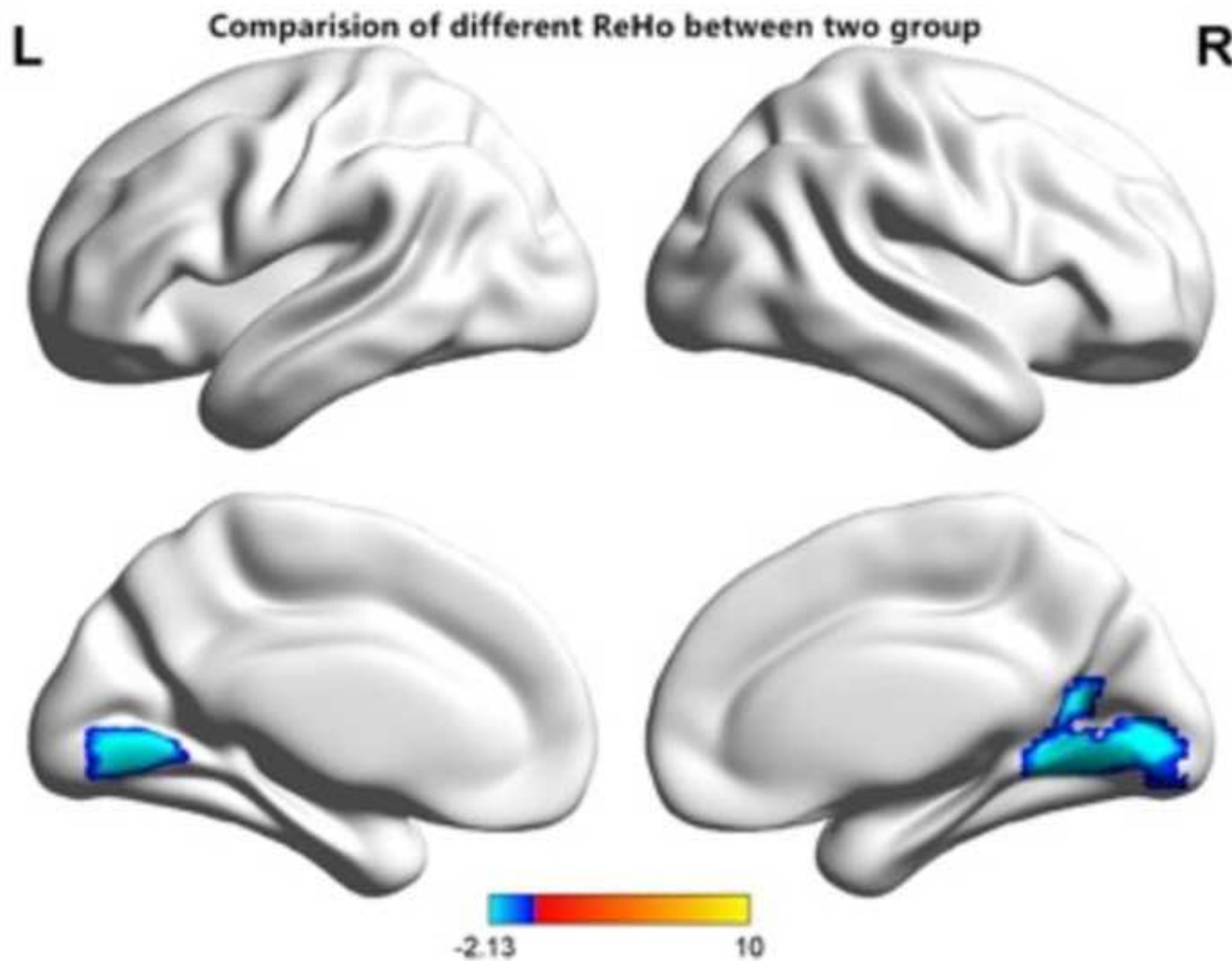
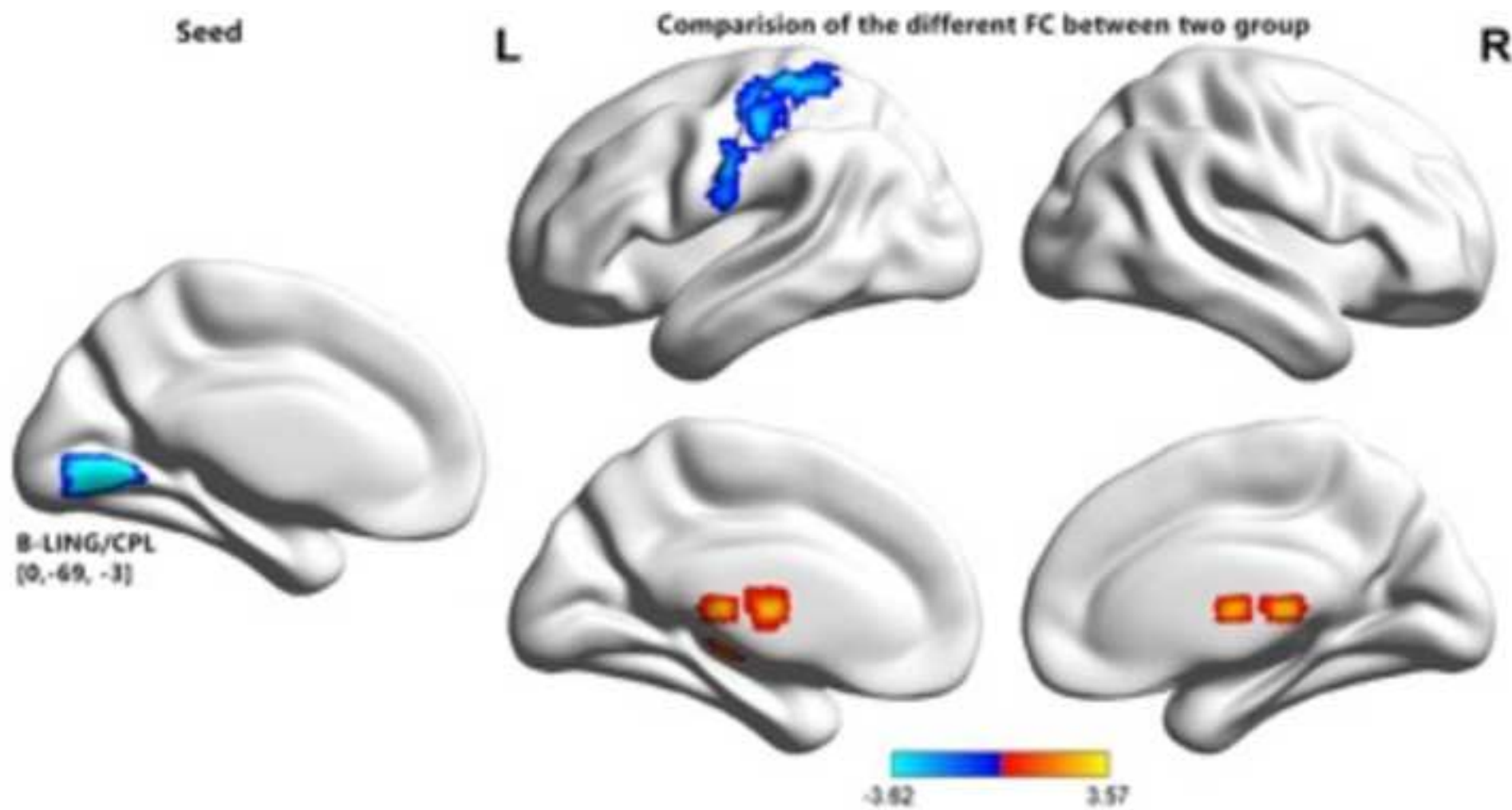


Figure 5

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Brain regions	BA	T-Peak scores (P-values)	MNI coordinate s (x, y, z)	Cluster size (voxels)
Bilateral Lingual Gyrus/Cerebellum Posterior Lobe	17,18	-5.12, (<0.01)	0, -69, -3	498

Conditio n	Brain regions	BA	Peak T scores	MNI coordinate s (x, y, z)	Cluster size (voxels)
ROI in bilateral LGG/CPL					
RP > HC	Left thalamus	-	3.1668	-21, -18, -3	70
RP > HC	Right thalamus	-	3.5733	18, -24, 21	219
RP < HC	Left Postcentral	-	-3.6226	-48, -21, 39	262

Name of Material/Equipment	Company	Catalog Number
BrainNet Viewer software	National Key Laboratory of Cognition Neuroscience and Learning, BNU	BrainNet Viwer 2013
DPABI software	Institute of Psychology, CAS, Beijing, China	DPABI 4.3
MATLAB	MathWorks, Natick, MA, USA	2013a
MRI scanner	GE Healthcare, Milwaukee	MRI 3.0
SPM software	Wellcome Centre for Human Neuroimaging, UCL	SPM8
SPSS	IBM, Chicago, IL, USA	SPSS version 20.0

Comments/Description

BrainNet Viewer is a brain network visualization tool to visualize structural and functional connectivity patterns
DPABI is a toolbox for data processing and analysis of brain imaging.

MATLAB is a high-level technical computing language and interactive environment for algorithm development, data visualization, data analysis, and numeric computation.

SPM8 is a major update to the SPM software, containing substantial theoretical, algorithmic, structural and interface enhancements over previous versions.

SPSS software platform offers advanced statistical analysis, text analysis, open-source extensibility, integration with big data and seamless deployment into applications.



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Author(s):

Xin Huang *, Yan Tong *, Chen-Xing Qi, Yang -Tao Xu, Han-Dong Dan, Qin-Qin Deng Yin Shen #

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Date:

21st May, 2019

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612542.6 For questions, please contact us at submissions@jove.com or +1.617.945.9051.

Responses to the reviewer's comments

RE: Manuscript ID: JoVE60305 "Mapping regional homogeneity and functional connectivity of visual cortex in resting-state fMRI."

Dear editor,

Thanks for your letter and the comments. We carefully revised our manuscript, and made changes according to your suggestions. Attached please find the revised version of the paper, with highlighting where changes have been made. Our point-to-point responses to the comments are also listed as below.

Editorial Comments:

Q1: Please note that the editor has formatted the manuscript to match the journal's style. Please retain the same. The updated manuscript is attached and please use this version to incorporate the changes that are requested.

R1: Thanks! We revised the manuscript based on the updated manuscript.

Q2: Please further revise the text to avoid text overlap with previously published text (see specific comments in the attached manuscript).

R2: Yes, we rephrased the text in the revised manuscript. Thanks!

Q3: Please carefully review the protocol and figures/screenfiles and make sure that all steps are clearly explained and can be reproduced (see specific comments in the attached manuscript).

R3: Yes, we revised the protocol and added more specific steps in figure/screenfiles in the rephrased manuscript.

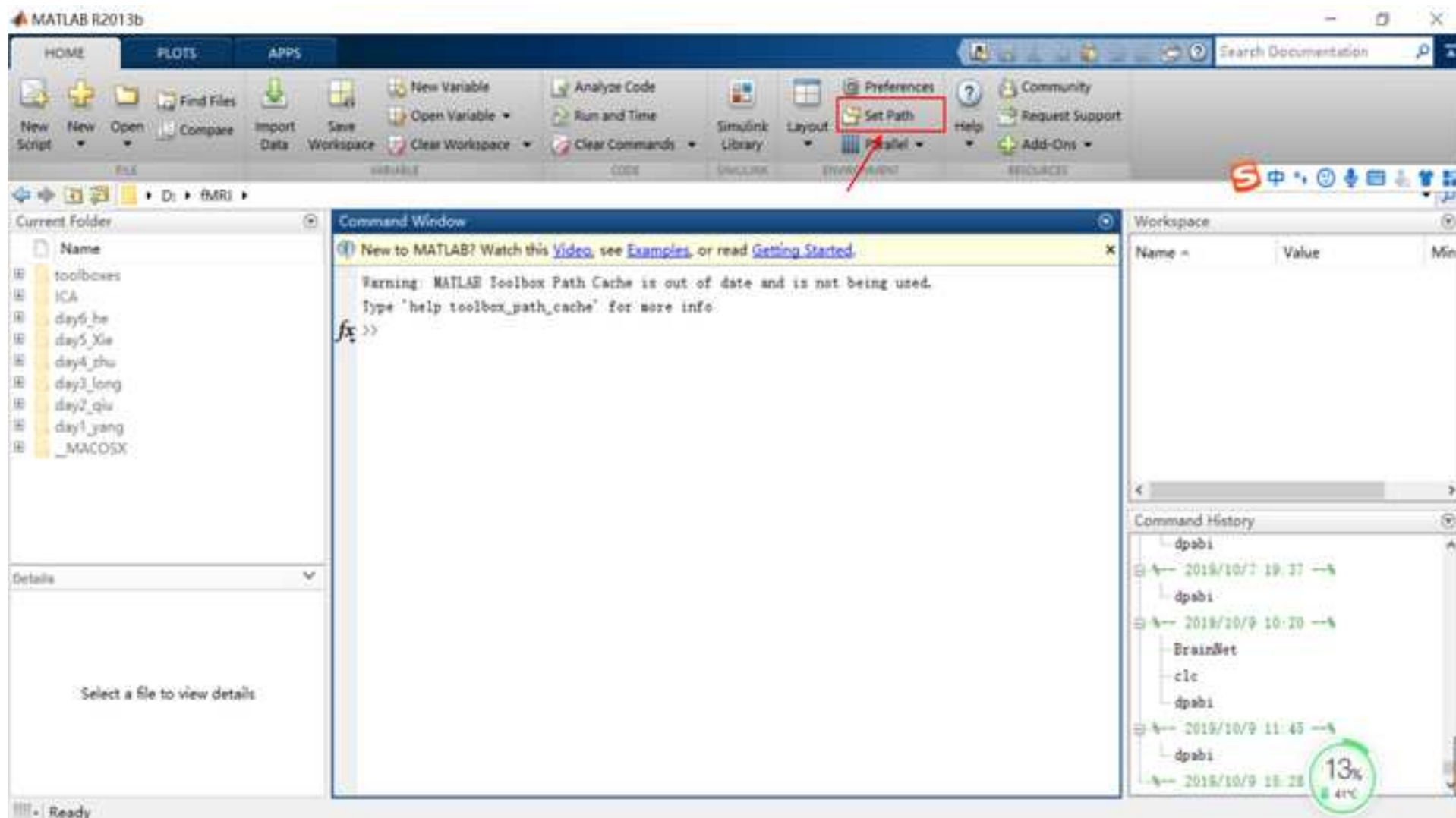
We appreciate editors/reviewer's comments and hope that our revision will meet with

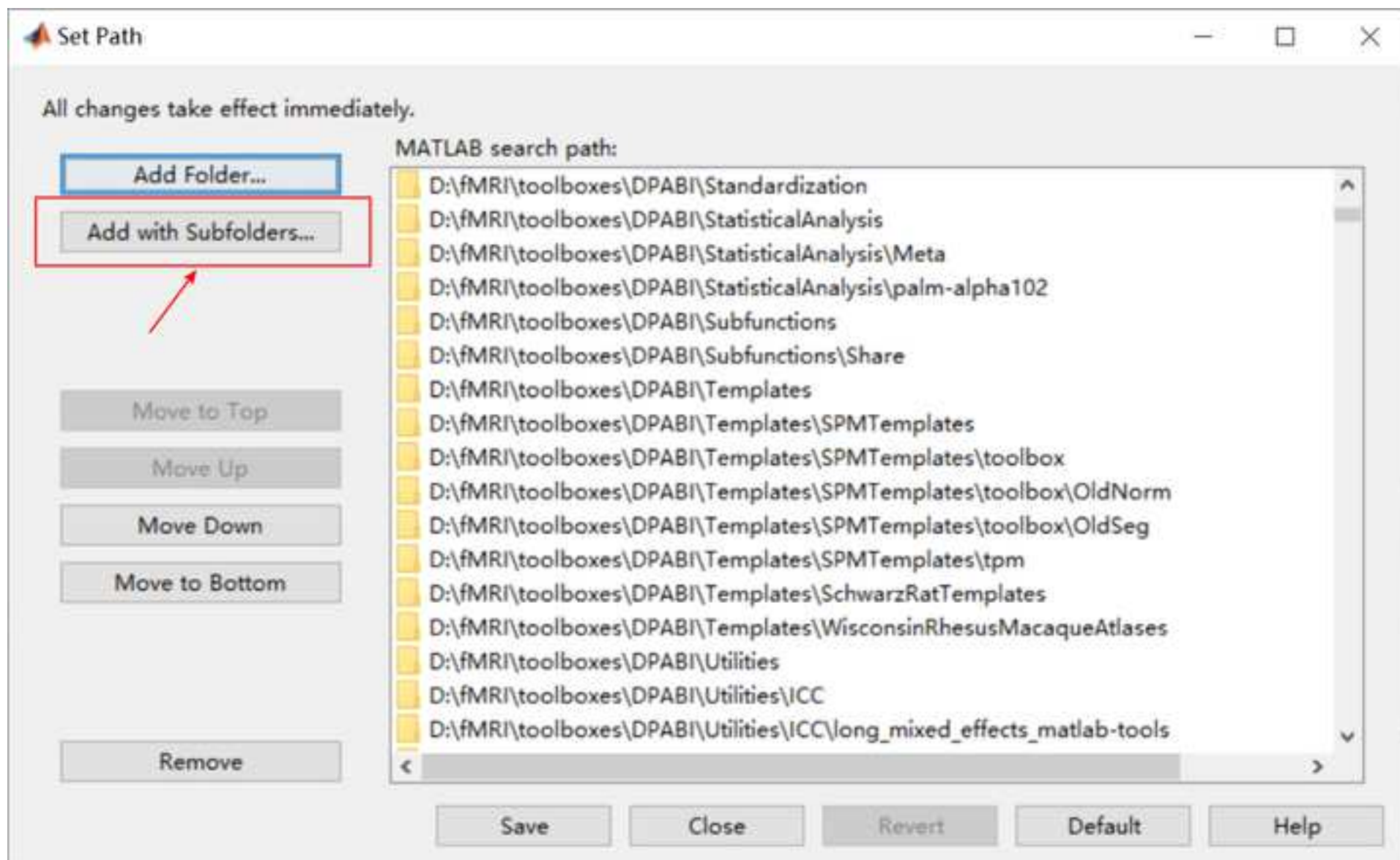
approval.

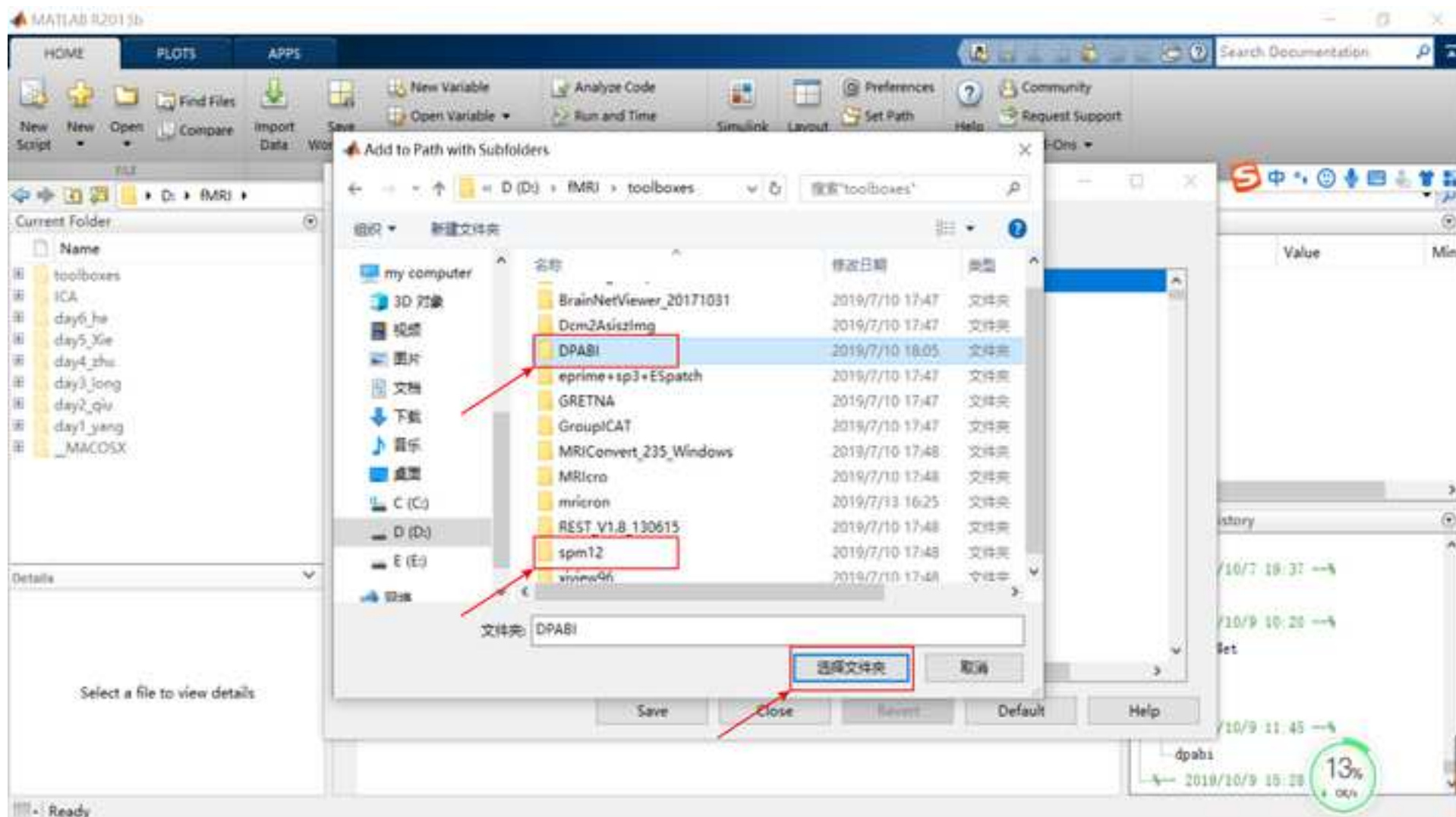
Yours sincerely,

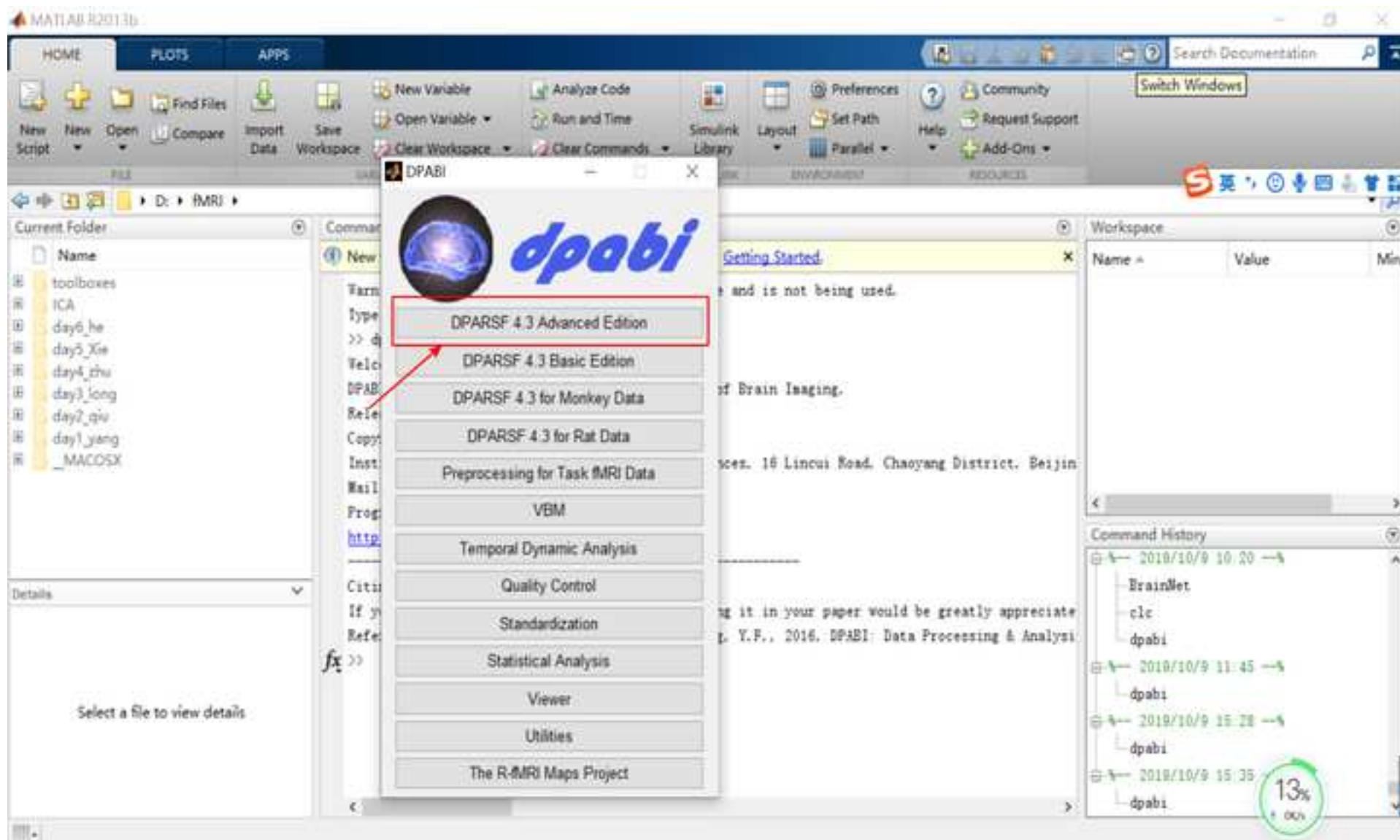
Yin Shen, M.D, Ph.D.

Eye Center, Renmin Hospital of Wuhan University









Data Processing Assistant for Resting-State fMRI

Advanced Edition**DPARSF A**

Working Directory: D:\fMRI

Participants:

Time Points: 240

TR (s): 2

Blank

☒ EPI DICOM to NIFTI☐ Apply Mats☒ Remove First

10

Time Points

☒ Slice Timing

Slice Number: 40

Slice Order: [1 3 5 7 9 11]

Reference Slice: 2

☒ Realign☐ Voxel-Specific Head Motion☒ Reorient Fun*☒ AutoMask☒ T1 DICOM to NIFTI☐ Crop T1☒ Reorient T1*☒ Bet☒ T1 Coreg to Fun☐ Segment☒ New Segment + DARTELAffine Regularisation in Segmentation: ☐ East Asian ☒ European☐ Nuisance Covariates Regression

Polynomial trend: 1

Head Motion model: ☐ Rigid-body 6☐ Derivative 12☒ Friston 24☐ Voxel-specific 12☐ Head motion scrubbing regressors

Nuisance regressors (WM, CSF, Global)

☐ Other covariates☐ Add mean back☐ Filter (Hz):

0.01

~ 0.1

☒ Normalize

Bounding Box: [-90 -126 -72 90 90]

Voxel Size: [3 3 3]

☐ Normalize by using EPI templates☐ Normalize by using T1 image unified segmentation☒ Normalize by DARTEL☒ Smooth☐ Smooth by DARTEL

FWHM: [4 4 4]

☒ Default mask☐ No mask☐ User-defined mask

Use Default Mask

☐ Warp Masks into Individual Space☒ Detrend☒ Nuisance Covariates Regression☐ ALFF+IALFF

Band (Hz):

0.01

~ 0.1

☐ Filter☐ Scrubbing☐ ReHoCluster: ☐ 7☐ 19☒ 27 voxels☐ Smooth ReHo☐ Degree Centrality☒ Functional Connectivity☐ Extract ROI time courses☒ Define ROI☐ Define ROI Interactively*☐ CWAS☐ Normalize to Symmetric Template☐ Smooth☐ VMHC☐ Normalize Derivatives☐ Smooth Derivatives

Parallel Workers #: 0

Functional Sessions #: 1

Starting Directory Name: FunRaw

Help

Save

Load

Utilities

Quit

Run

