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## In-vivo protocol of controlled subconcussive head impacts for validation of field study data --Manuscript Draft--

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INDIANA UNIVERSITY  
Department of Kinesiology  
Bloomington

**Aaron Berard, PhD**

**Science Editor**

*Journal of Visualized Experiments*

11-10-18

Dear Dr. Berard,

Please accept our submission entitled, “*In-vivo* protocol of controlled subconcussive head impacts: validation of field study data” for publication in the Journal of Visualized Experiments. The manuscript has not been submitted for publication elsewhere. This manuscript outlines a subconcussive soccer heading model (SSHM) which is emerging as a reliable and leading methodology for examining the neural impact of subconcussive hits to the head. Our manuscript details a stepwise explanation of the SSHM, as well as the background and necessity for researching subconcussion. Furthermore, we supplement the efficacy of the SSHM by presenting results from a previous study of ours, in which the SSHM was utilized. Lastly, we show how the SSHM exhibits vast clinical relevance and implications, which will undoubtedly intrigue the scientific community.

Thank you for the invitation to submit.

Sincerely,

Keisuke Kawata, PhD, ATC

**TITLE:**

In Vivo Protocol of Controlled Subconcussive Head Impacts for the Validation of Field Study Data

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**KEYWORDS:**

Subconcussion, soccer heading, chronic traumatic encephalopathy, repeated measures, methodology, concussion

**SUMMARY:**

The subconcussive soccer heading model is a safe and concise methodological approach to isolate and measure the effects of subconcussive head impacts.

**ABSTRACT:**

Subconcussive hits pose a threat to neuronal health as they have shown to induce neuronal structural damage and functional impairment without causing outward symptomology and appear to be a key contributor to an irreversible neurodegenerative disease, chronic traumatic encephalopathy (CTE). In addition, athletes can incur more than 1,000 of these hits per season. The subconcussive soccer heading model (SSHM) is a relevant, reproducible, and leading method of isolating and examining the effects of these subconcussive head impacts. By controlling variables such as ball traveling speed, the frequency of impacts, interval, ball placement to the head, as well as by measuring head impact magnitude, the SSHM provides the scientific community with a superior avenue of investigating the acute subconcussive effects on neuronal health. In this paper, we demonstrate the utility of SSHM in studying a time-course expression of neurofilament-light polypeptide (NF-L) in plasma in a repeated measures fashion. NF-L is an axonal injury marker that has previously been shown to be elevated in boxers and football players following subconcussive head trauma. Thirty-four adult aged soccer players were recruited and randomly assigned to either a soccer heading ( $n = 18$ ) or kicking ( $n = 16$ ) group. The heading group executed 10 headers with soccer balls projected at a velocity of 25 mph over 10 min. The kicking

group followed the same protocol with 10 kicks. Plasma samples were obtained before and at 0 h, 2 h, and 24 h after heading/kicking and assessed for NF-L expressions. The heading group showed a gradual increase in plasma NF-L expression and peaked at 24 h after the heading protocol, whereas the kicking group remained consistent across the time points. These results confirmed the NF-L data from clinical field studies, encouraging the use of SSHM to validate clinical subconcussion data.

## **INTRODUCTION:**

Long-term, repetitive exposure to subconcussive head impacts has been proposed as one of the key contributors for developing the neurodegenerative disease CTE<sup>1-5</sup>. Each year, approximately 2.5 million high school and college athletes engage in contact sports that frequently induce these subconcussive insults through rapid acceleration-deceleration of the body and head<sup>6,7</sup>. Specifically, contact sport athletes may experience several 100 up to a 1,000 of such impacts per season<sup>6,8,9</sup>. Additionally, other populations, such as military men and women, have registered more than 300,000 head injuries since 2001, which has manifested into the recent diagnosis of CTE within a retired military veteran<sup>10</sup>. This diagnosis parallels with 110 postmortem CTE brains of American football players and four postmortem soccer players to present a burgeoning public health issue<sup>11,12</sup>. In light of the staggering prevalence, head impact research must shift its gaze to incorporate sound, precise methods of analyzing the acute debt subconcussive hits are inducing in a variety of arenas.

The SSHM presented here is one that satisfies the current methodological need to safely induce common mechanical stresses placed upon neural tissue during contact sport activities. The implementation of this model allows investigators to meticulously manage ball traveling speed, the frequency of impacts, interval, ball placement to the head, as well as measurements of head impact magnitude<sup>13,14</sup>. While these factors are virtually impossible to control in the field setting, the SSHM provides an outlet for researchers to isolate the effects of subconcussive head impacts. Furthermore, through the elimination of confounding variables seen during play (e.g., effects from vigorous exercise, body damage, body temperature change, and hydration/perspiration), the SSHM provides a superior method of validating clinical observations.

The SSHM has direct parallels to head impacts seen specifically within the realm of sport. As such, the literature has already begun to show its utility and corroborate the findings of cumulative head impact burden from other investigators. For example, we have demonstrated that the burden of subconcussive head impacts significantly drive neuro-ophthalmologic dysfunction amongst soccer athletes<sup>13,15</sup>. In addition, as few as 10 subconcussive impacts have been shown to immediately perturb vestibular function which can be normalized after 24 h of resting<sup>16</sup>. In this methodological report, we describe the application of SSHM to safely study the effects of subconcussive head impacts and introduce one of our findings that repetitive subconcussive head impacts gradually increase the concentration of a neuron-derived blood biomarker, namely NF-L<sup>14</sup>. This finding not only substantiates previous results of NF-L presence due to repetitive subconcussive blows to the head<sup>17,18</sup> but also validates that the SSHM can reproduce such findings in a controlled clinical manner.

## **PROTOCOL:**

The authors verify that the Indiana University Institutional Review Board approved the study (protocol # 1610743422) and written informed consent was obtained.

NOTE: The SSHM was integrated into a repeated measures design that is intended to investigate changes among dependent variables within subjects at 0 h, 2 h, and 24 h post-intervention compared to individual pre-intervention values. This study design allows researchers to track changes for a 24 h period, which is the typical timeframe between athletic practices. In the present study, soccer players were randomly assigned to either a soccer heading ( $n = 18$ ) or a soccer kicking group ( $n = 16$ ).

### **1. Setup**

1.1. Following baseline measurement collection (pre-intervention), begin the SSHM with the positioning of a soccer ball launcher approximately 40 ft away from the subject, as well as ensuring the soccer ball is inflated to 9 psi.

1.2. The face of the machine displays two identical dials, which regulate the speed of the left and right wheels, and an on/off switch in between them. Set both these dials to a standardized speed of choice.

NOTE: For this demonstration purpose, the ball traveling speed has been set to 30 mph. This speed was chosen as it simulates a soccer throw-in from the sideline to midfield. Soccer players frequently perform this maneuver during practice and games.

1.3. Place 3 inch blocks underneath the wheels of the ball launcher to allow for the desired trajectory (no blocks needed for kicking subjects). Once this is complete, the ball launcher is then angled to 40°, which is measured as the angle between the ground and the midline of the rotating wheels.

NOTE: The angle measurement is taken with a goniometer, and the machine can be adjusted after loosening a knob located along the blue rails where the soccer ball is loaded.

1.4. Once the soccer machine is properly set, fit the subjects with a triaxial accelerometer embedded within a head-band pocket and positioned directly below the external occipital protuberance (inion) to monitor linear and rotational head accelerations.

1.5. Start up the corresponding software for the accelerometer, and enter the subject's information accordingly. At this point, the subject is ready to begin the familiarization trials of the intervention (heading, kicking).

### **2. Familiarization trials**

2.1. Position the subject approximately 40 ft in front of the ball launcher.

2.2. Be sure to explain to the subject that the ball launcher will volley the soccer ball to them and that they simply need to simulate intervention contact with the ball (i.e., heading subjects will catch the ball with their hands in front of their forehead before head-to-ball contact is made, kicking subjects will “trap” the ball on the ground with their foot instead of volleying the ball back, and standing subjects will remain static and not make contact with the ball).

2.3. When the subject understands and feels ready, have the researcher turn the ball launcher on, load the soccer ball onto the blue rails, and finally push the ball into the rotating wheels after a 3-2-1 countdown.

2.4. After stopping the ball as described previously (step 2.2), have the subject roll the ball back.

2.5. Repeat steps 2.3 and 2.4 two to four additional times (no rest time required between) to ensure that the subject positioning is correct and interaction with the ball will be safe and controlled. This concludes the familiarization trials.

### **3. Intervention**

3.1. Verbally confirm that the subject is ready. Once confirmed, give instructions to the heading subjects to only make forehead contact with the ball; tell the subjects to avoid potential impacts to the crown, parietal, and temporal lobes. Instruct the kicking subjects to kick the ball only while it is in flight as ball contact with the ground will attenuate the subsequent impact to the foot.

3.2. Instruct both heading and kicking subjects to volley the ball to a target (additional researcher) approximately half the distance between them and the machine. As best they can, ask subjects to do this in a manner that will mimic the arched trajectory the ball took during its flight toward the subject.

3.3. Activate the triaxial accelerometer and begin the recording.

3.4. Load the soccer ball onto the blue rails, push the ball into the rotating wheels after a 3-2-1 countdown, and make sure appropriate contact is made.

3.5. Repeat step 3.4 nine more times with a 60 s rest in between bouts. If the subject forgoes interaction with the ball (due to inopportune placement or suspected contact with the body in an area that must be avoided), then volley the ball to the subject again promptly, without any rest period.

3.6. In between each head contact with the ball, verify that the triaxial accelerometer registered an impact (using triaxial software; kicking subjects should not register G-force).

3.7. Once the intervention is concluded, turn off the ball launcher and stop the triaxial recording (important, as the movement required to remove the headband could record another “impact”). Once the recording has stopped, remove the headband.

**REPRESENTATIVE RESULTS:**

The results represented here were interpreted from a previous article<sup>14</sup>, in which the SSHM was utilized as previously described. In this particular study, we aimed to show how the SSHM could induce changes in plasma levels of NF-L, which is an axonal injury marker that is hypothesized to filter out of the cranium and into the peripheral blood following head impacts.

**SSHM and head kinematics**

The present data were derived from 34 subjects who were eligible for analysis (heading group:  $n = 18$ , and kicking [control] group:  $n = 16$ ). There were no significant differences in any demographic characteristic between the groups. Demographics and head impact kinematics are detailed in **Table 1**. Head impact kinematic data showed that the heading group experienced a median linear head acceleration of 31.8  $g$  per head impact (IQR: 31.1–34.5  $g$ ) and a median rotational head acceleration of 3.56  $\text{krad/s}^2$  per head impact (IQR: 2.93–4.04  $\text{krad/s}^2$ ). In contrast, the kicking (control) group did not result in detectable levels of head acceleration (as expected) (**Table 1**).

**SSHM effects on NF-L biomarker levels**

The SSHM was able to produce the following outcomes. See **Figure 1** for the visual representation of the results<sup>14</sup>. (i) There was a gradual increase in plasma NF-L expression, as illustrated by a statistically significant time effect for the head impact group,  $F(1,31) = 9.17$ ,  $p = 0.0049$ . For example, 0.03  $\text{pg/mL}$  of NF-L is estimated to increase every hour after 10 headers ( $SE = 0.001$ ). (ii) There was no significant time effect for the kicking (control) group,  $F(1,31) = 1.20$ ,  $p = 0.28$ . (iii) Follow-up paired  $t$ -tests with Bonferroni correction within the heading group revealed that a significant difference appeared at 24 h post-heading ( $3.68 \pm 0.30 \text{ pg/mL}$ ) compared to pre-heading ( $3.12 \pm 0.29 \text{ pg/mL}$ ,  $p = 0.0013$ ; Cohen’s  $d = 1.898$ ). (iv) Linear regression, adjusting for the baseline NF-L level, was used to assess the between-group difference at the 24 h post-intervention time point and distinguished that the NF-L level in the heading group was significantly higher than the kicking (control) group with an estimated mean difference of 0.66  $\text{pg/mL}$  ( $SE = 0.22$ ,  $p = 0.0025$ ).

**FIGURE AND TABLE LEGENDS:**

**Table 1: Demographics and impact kinematics by group.**

**Figure 1: Changes in plasma NF-L levels before and after subconcussive impacts.** In the heading group, NF-L was elevated at 24 h post-heading compared with pre-heading and 0 h post-heading time points, but the kicking (control) group remained static across all time points. The heading group’s NF-L level at 24 h post-heading was higher than that of the kicking (control) group. Data are presented as the mean  $\pm$  SEM. NF-L = neurofilament light; SEM = standard error of the mean.

The figure is reproduced from Wirsching et al.<sup>14</sup> with permission from Mary Ann Liebert, Inc., New Rochelle, NY.

## DISCUSSION:

While contact sports like American football might appear to be driving the need for a concise research model to study subconcussive impacts, other sports like soccer may account for the dominant share of subconcussive exposure around the globe as approximately 265 million people participate in what is perhaps the world's most popular sport<sup>19</sup>. However, while the majority of the suspected long-term neurodegenerative effects of subconcussion have been autopsied in American football players, the resemblance of football head impacts to soccer headers is surprisingly large. For instance, 10 bouts of soccer heading in the current study induced approximately 300 *g* and 35 krad/s<sup>2</sup>, which were near identical to previous reports using similar subconcussion models<sup>20,21</sup>. These impact kinematics were comparable to the hits observed in American football, where the average college football player incurs 7.0–9.4 hits during practice and 25 hits during games, with a mean peak linear acceleration per hit of 28.8–32.0 *g*<sup>22–25</sup>. Furthermore, other contact sports, such as ice hockey, have displayed similar or greater peak linear head accelerations than these results. For example, a recent study examining both male and female collegiate ice hockey athletes revealed that, over the course of a season, these athletes would register peak linear accelerations of 41.6 *g* (36.6–49.5 *g*) and 40.8 *g* (36.5–49.9 *g*) for males and females, respectively (median [IQR])<sup>26</sup>. Additionally, the head impact telemetry system that was utilized in this ice hockey study revealed that nearly one-third of males (28.0% [21.2%–33.5%]) and females (29.3% [24.8%–32.1%]) (median [IQR]) were inflicted on the front of the head<sup>26</sup>. These results directly parallel to the head impacts induced by using the SSHM, which indicates the vast clinical utility of the current methodology.

There is, however, one limitation that should be addressed when attempting to extrapolate soccer and American football head impacts to other contact sports like ice hockey. Head impacts in ice hockey are not routine drills and are penalized, and they usually are the result of deliberate contact with another player. In fact, subconcussive head impact incidence for collegiate ice hockey athletes is known to be substantially low: 1.3 (1.0–1.7) per practice and 6.3 (3.5–9.0) per game for males and 0.9 (0.6–1.0) per practice and 3.7 (2.5–4.9) per game for females<sup>26</sup>.

The present study is not the first to explore the expression of NF-L following head trauma; however, it is the first to isolate head trauma as the cause for NF-L expression outside the central nervous system. Oliver et al. assessed for serum NF-L expression within American football athletes at eight different time points over the course of a season (~6 months)<sup>17</sup>. Players were categorized into two groups, starters and nonstarters, with an assumption that starter athletes will be exposed to larger quantities of head hits, whereas nonstarters will incur lower quantities of head hits than the starters. The authors identified significant increases in serum NF-L expressions in the starter group over time across the season<sup>17</sup>. Conversely, the nonstarter group remained consistent throughout the season. Similarly, Shahim et al. analyzed serum NF-L levels in boxers following a subacute phase of subconcussive head trauma (7–10 days prior)<sup>18</sup>. In their analysis, boxers were categorized into two groups (mild vs. severe head impact groups) based on an anecdotal threshold of <16 vs. ≥16 head hits during a boxing match, respectively. The serum



expression of NF-L was significantly elevated in the severe head impact group when compared to the mild impact group, suggesting a dose-dependent response to head impact and biomarker expression<sup>18</sup>. While the presented literature elicits strong reasoning for NF-L as a marker of axonal injury, neither study exhibits robust control of confounding variables seen throughout sport (thermogenesis, hydration status, body contacts, head kinematics, etc.). This gap in methodology underpins the need for the SSHM. By using the SSHM, Wirsching et al.<sup>14</sup> and Wallace et al.<sup>27</sup> were able to control aforementioned confounding variables, coupled with the monitoring location, magnitude, and quantity of head impacts, and study the head impact dose-response profile of NF-L levels in the blood. Therefore, the SSHM provides safe and standardized means to study the effect of subconcussive head impacts and validate clinical findings.

The SSHM shows promise as being a relevant, reproducible, and leading method of isolating and examining the effect of subconcussive head impacts irrespective of sport; however, there are a few limitations to consider when adopting this method. First, the SSHM has a strong ability to control for environmental covariates (previously described); however, this means that a temperature-controlled indoor facility is required. Second, in an effort to ensure safe and controlled head contacts, we set participant exclusion criteria to a minimum of 5 years of soccer heading experience. This cutoff was used to eliminate potential injurious head contacts due to novice heading technique. Finally, this protocol requires specific equipment and multiple researchers to conduct, which may not be accessible unanimously.

The SSHM provides an invaluable modality for researchers to confidently validate results found in field studies. This confidence stems from the ability of the SSHM to control for both internal and external confounding factors such as impact location and quantity, body damage, exercise effect, and perspiration, to mention a few. Furthermore, because the SSHM has shown similar head impact magnitudes as other sports like ice hockey and American football, the claim can be made that this methodology bears vast clinical relevance not only to soccer athletes but also to American football, ice hockey, rugby, and boxing athletes. Lastly, because the SSHM does not segregate populations, as do some unisex sports like American football, all genders and ethnicities can be studied.

#### **ACKNOWLEDGMENTS:**

The authors would like to acknowledge Ms. Angela Wirsching, who was a key contributor to the research we cite in the representative results section.

#### **DISCLOSURES:**

The authors have nothing to disclose.

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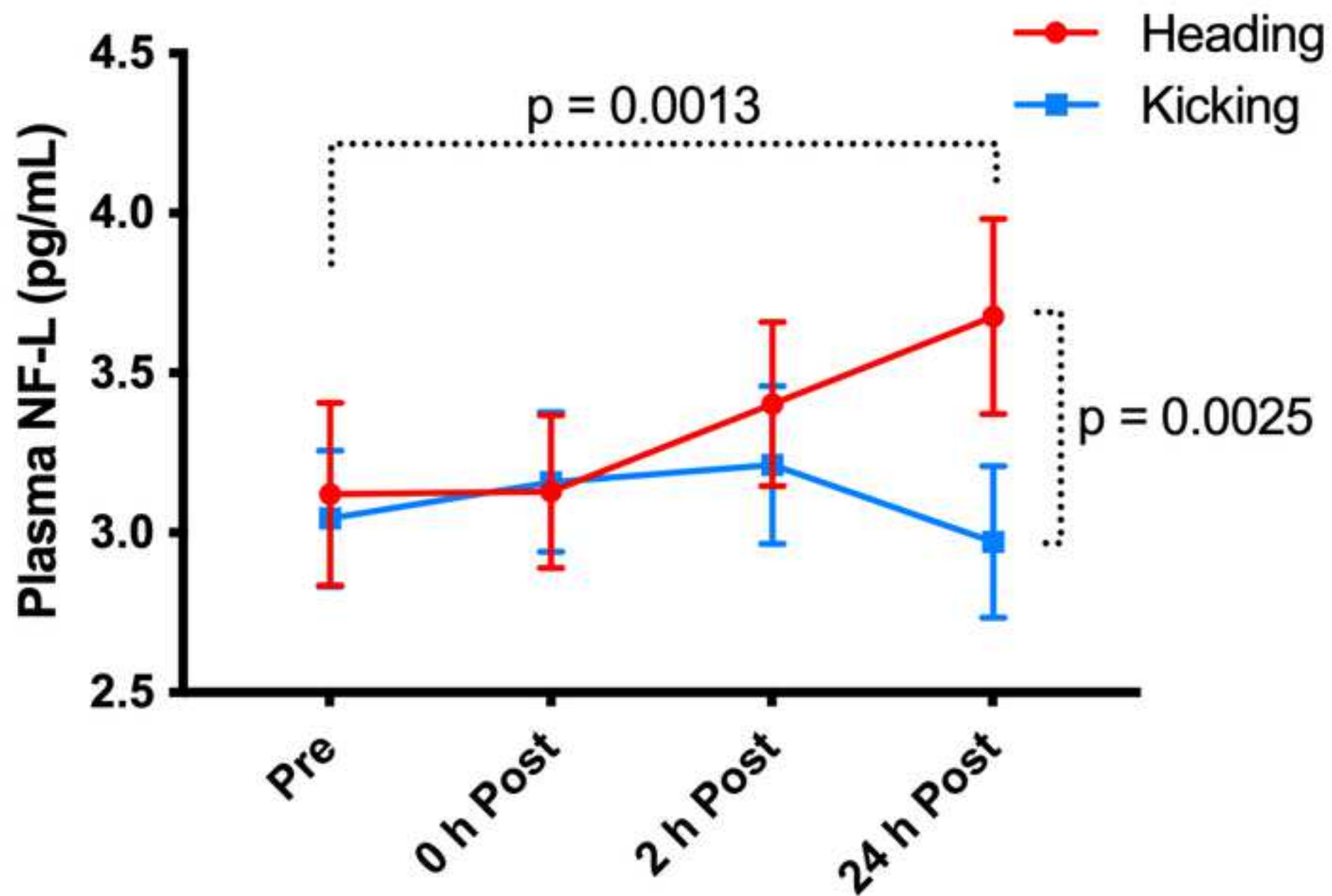
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Variables	Heading	Kicking Control	P-value
n	18	16	-
Sex	7M 11F	6M 10F	-
Age, y	20.3 ± 1.5	21.2 ± 1.4	0.089
BMI, kg/m <sup>2</sup>	23.2 ± 2.4	24.4 ± 3.2	0.236
No. of previous concussion	0.78 ± 1.0	0.63 ± 1.7	0.753
Soccer heading experience, y	9.5 ± 3.6	10.0 ± 4.5	0.725
Head impact kinematics, median (IQR), a			
PLA, g	31.8 (31.1 – 34.5)	- b	-
PRA, krad/s <sup>2</sup>	3.56 (2.93 – 4.04)	- b	-
Note: BMI, body mass index. IQR, interquartile range. PLA, peak linear acceleration. PRA, peak rotational acceleration. krad, kiloradian. a, Based on the sum of 10 soccer headers. b, Soccer kicking did not cause a detectable level of head acceleration.			

Name of Material/ Equipment		Company
JUGS Soccer Machine		JUGS Sports
SIM-G Triaxial Accelerometer		Triax Technologies

### **Catalog Number**

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*In-vivo* protocol of controlled subconcussive head impacts: validation of field study data

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### CORRESPONDING AUTHOR:

Name:	Keisuke Kawata		
Department:	Kinesiology		
Institution:	Indiana University Bloomington		
Article Title:	In-vivo protocol of controlled subconcussive head impacts: validation of field study data		
Signature:			Date: 11/11/18

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## Author Response:

We addressed and modified the following editorial comments in the revised manuscript. Thank you for the direct instruction.

### Editorial comments:

Changes to be made by the author(s) regarding the manuscript:

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and “would be” throughout the Protocol. Any text that cannot be written in the imperative tense may be added as a “Note.” Please include all safety procedures and use of hoods, etc. However, notes should be used sparingly and actions should be described in the imperative tense wherever possible. Please move the discussion about the protocol to the Discussion.

12. Discussion: Please also discuss the critical steps within the protocol.

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### **Reviewers' comments:**

Please note that the reviewers raised some significant concerns regarding your method and your manuscript. Please thoroughly address each concern by revising the manuscript or addressing the comment in your rebuttal letter.

#### **Reviewer #1:**

The Authors of this manuscript use an automated machinery to induce control head impacts in players. A cohort of "kickers" is used as a control. The manuscript is concisely written and reports results that were already published. The main and perhaps fatal flaw of the design is to use a marker (NF-L) which has been rarely studied in clinical context, while ignoring S`100B and GFAP which are better known. The reason for this comment is not this Reviewer's preference of one marker over another, but rather a concern in the space of general diagnostics. An elevation is meaningless unless a value for controls vs. injured is available. In a previous study with S100B in football players, subconcussive head hits were often associated with an increase of S100B above the published and validated control values. In other words, an elevation of a marker (e.g., blood glucose) within a normal clinical range is meaningless, and does not suggest a diabetic pathology.

### **Author Response:**

We thank the reviewer for his/her comments on the use of NF-L as a marker for brain injury. We would like to clarify the rationale of using the marker in this manuscript. As mentioned, extensive research has been conducted to better understand S100B and GFAP (along with UCH-L1 and Tau) in clinical studies, and indeed, NF-L has lesser volumes of evidence to date. This is exactly why our SSHM can be of paramount use in validating the clinical results. Shahim et al.<sup>1</sup> and Oliver et al.<sup>2,3</sup> have reported that blood levels of NF-L raise in concert with subconcussive head impacts in boxers and football players. However, as elaborated in our discussion section, these studies do not control any extraneous factors, and thus the effects of subconcussive head impact on NF-L is suggestive at best. In this manuscript, we demonstrated that using the laboratory subconcussion model we were able to validate their clinical findings by controlling for extraneous factors that are inherent to field studies (temperature change, exercise effect, body hit, and orthopedic stress). It is also important to emphasize that this manuscript is a methodological paper submitted to the JoVE (which introduces innovative methodologies).

While it is best to evaluate other markers (S100B, GFAP, Tau, UCH-L1, NF-H, NSE, SNTF: see our review papers<sup>4,5</sup> on their strength and clinical significance), that is not the intent of this manuscript. Also, the sentence on “an elevation is meaningless unless a value for controls vs. injured is available” is confusing to us. We demonstrate the elevation in NF-L which was significantly elevated within-group (heading) and between group (heading vs. kicking control). The clinical significance of such increase is yet to be delineated by follow-up studies, as with any other blood biomarkers. The reviewer’s logic is not clear to us. Could you please elaborate?

An additional factor relates to use of human subjects as experimental tools. If NF-L increases are in your opinion clinically important, were the volunteers aware of the risk of CTE, or brain/axonal damage? It is a hard for me to understand how your IRB committee approved this study. Was the risk of long-term consequences deemed acceptable?

**Author Response:**

Our apologies for not including an IRB statement. The study has been approved by Indiana University IRB and Temple University IRB (where Dr. Kawata currently and previous affiliate). Subconcussion poses a public health concern and it is important to understand the mechanism of head impact and physiological/biological response. Therefore, our protocol of 10 soccer headers (which is regularly performed in soccer players, as well as players in American football, ice hockey, rugby, and boxing incurring similar levels of head impacts per practice/game), is considered safe and advantageous means to study the subconcussive effect. Subjects were also told regarding risks of head impacts and signed informed consent. The ethical statement was added to the revised manuscript. Thank you for pointing this out.

Methods: "frontal lobe" is not a synonym of forehead and a forehead hit will affect other regions of the brain as well.

**Author Response:**

It is corrected in the revised manuscript.

**REFERENCES**

1. Shahim P, Zetterberg H, Tegner Y, Blennow K. Serum neurofilament light as a biomarker for mild traumatic brain injury in contact sports. *Neurology*. 2017;88(19):1788-1794.
2. Oliver JM, Jones MT, Kirk KM, et al. Serum Neurofilament Light in American Football Athletes over the Course of a Season. *Journal of neurotrauma*. 2016;33(19):1784-1789.
3. Oliver JM, Jones MT, Kirk KM, et al. Effect of Docosahexaenoic Acid on a Biomarker of Head Trauma in American Football. *Med Sci Sports Exerc*. 2016;48(6):974-982.
4. Kawata K, Tierney R, Langford D. Blood and cerebrospinal fluid biomarkers. *Handbook of clinical neurology*. 2018;158:217-233.

5. Kawata K, Liu CY, Merkel SF, Ramirez SH, Tierney RT, Langford D. Blood biomarkers for brain injury: What are we measuring? *Neuroscience and biobehavioral reviews*. 2016;68:460-473.

Reviewer #2:

**Manuscript Summary:**

In this manuscript, the authors describe a soccer heading protocol that provides a means to generate subconcussive head impacts under controlled circumstances. In particular, in a pre/post repeated measures design, participants headed a soccer ball 10 times in a 10 minute period. For the proof of concept purposes of this methods paper, the authors measured a blood biomarker (neurofilament light) which is associated with axonal injury. This was done immediately prior to and after the bout of soccer heading and then at 2 hours and 24 hours after the protocol. For comparison, a control group of participants did all the same procedures except instead of heading the ball they kicked it. Ball speed and trajectory were controlled by a JUGS soccer machine. The results showed a significant increase in NF-L in the heading but not the kicking group.

The manuscript is clearly written and addresses a new experimental manipulation that has been published on only a small number of times. All of the relevant methodological details are present in the manuscript that would allow another scientist to replicate the procedures. I only have a couple of suggestions for the authors.

**Major Concerns:**

1. Some discussion of the safety and ethics associated with the protocol appears warranted. Researchers wanting to implement this protocol will need to convince their local ethics panel that the injuries that are induced by the head impacts are temporary in nature. One approach is to have the participants come back for additional testing (e.g., by serving as their own controls) to demonstrate that the relevant dependent variable has returned to baseline.

**Author Response:**

Thank you for the pointer and our apologies for not including the ethical statement. We have included an "ethics statement" outlining our approval and compliance with IRB.

2. An additional paper by our group (Wallace et al., 2018. *BMJ Open Sport and Exercise Science*) examining NF-L changes following a more intense bout of heading has recently been published and may be worth including in the discussion regarding dose-response effects.

**Author Response:**

We included Wallace et al. paper in the discussion section.

3. The NF-L results are only different at the 24 hour time point between the heading and kicking groups. Although this is not the primary purpose of the manuscript, it might be worth discussing.

**Author Response:**

Although the reviewer's recommendation is important, we feel that elaborating upon NF-L specifically would detract from the primary goal of the manuscript, which is to showcase the SSHM, and not the biomarkers it can be used with. We believe that the NF-L finding has been discussed sufficiently in the discussion section; therefore, we respectfully choose not to further elaborate on the NF-L result. Readers should refer to Wirsching et al.

**Minor Concerns:**

1. The Alfonsi (2018) reference appears to be incomplete.

**Author Response:**

This was corrected.



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Thank you,

Keisuke Kawata, Ph.D., ATC.  
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I'm emailing to inquire permission to reproduce the Figure 2 of our [recent paper](#). We are preparing a methodological manuscript to [JoVE](#) (journal of visualized experiments), highlighting our soccer heading model that we used for J Neurotrauma paper. We'd like to reproduce the Figure 2 as an example finding derived from the soccer heading model. The title of the manuscript for the JoVE is: *In-vivo protocol of controlled subconcussive head impacts: validation of field study data*.

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