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Corresponding Author:	Froylan Gomez-Lagunas Universidad Nacional Autonoma de Mexico Cd. Mexico , MEXICO
Corresponding Author's Institution:	Universidad Nacional Autonoma de Mexico
Corresponding Author E-Mail:	froylangl@yahoo.com
First Author:	Froylan Gomez-Lagunas
Other Authors:	Carolina Barriga-Montoya
	Araceli de la O-Martinez
	Beatriz Fuentes-Pardo
	Arturo Picones
	Arturo Hernandez-Cruz
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TITLE:

Desensitization and Recovery of Crayfish Photoreceptors upon Delivery of a Light Stimulus

AUTHORS:

Carolina Barriga-Montoya[1], Araceli de la O-Martínez[1], Arturo Picones[2], Arturo Hernández-Cruz[2], Beatriz Fuentes-Pardo[1], Froylán Gómez-Lagunas[1]

[1]Departamento de Fisiología, Facultad de Medicina, Universidad Nacional Autónoma de México, Ciudad de México, México

[2]Laboratorio Nacional de Canalopatías, Instituto de Fisiología Celular, Universidad Nacional Autónoma de México (UNAM), Ciudad de México, México

CORRESPONDING AUTHOR:

Froylán Gómez-Lagunas
Email: froylangl@yahoo.com
Tel: (5255)-56232263

EMAIL ADDRESSES:

Carolina Barriga-Montoya (carolina@ciencias.unam.mx)
Araceli de la O-Martínez (araceli_delao@yahoo.com.mx)
Arturo Picones (arturopicones@yahoo.com)
Arturo Hernández-Cruz (ahernan@ifc.unam.mx)
Beatriz Fuentes-Pardo (bfpardo@unam.mx)
Froylán Gómez-Lagunas (froylangl@yahoo.com)

KEYWORDS:

Light-elicited current, desensitization, recovery from desensitization, intracellular recording, voltage-clamp, two-pulse protocol, crayfish, circadian rhythms.

SHORT ABSTRACT:

A protocol for the study of desensitization and sensitivity recovery of crayfish photoreceptors as a function of circadian time is presented.

LONG ABSTRACT:

A method to study desensitization and recovery of crayfish photoreceptors is presented. We performed intracellular electrical recordings of photoreceptor cells in isolated eyestalks using the discontinuous single electrode-switched voltage-clamp configuration. First, with a razor blade we made an opening in the dorsal cornea to get access to the retina. Thereafter, we inserted a glass electrode through the opening, and penetrated a cell as reported by the recording of a negative potential. Membrane potential was clamped at the photoreceptor's resting potential and a light-pulse was applied to activate currents. Finally, the two light-flash protocol was employed to measure current desensitization and recovery. The first light-flash triggers, after a lag period, the transduction ionic current, which after reaching a peak amplitude decays towards a desensitized state; the second flash, applied at varying time intervals, assesses the state of the light-activated conductance. To characterize the light-elicited current, three parameters were measured: 1)

latency (the time elapsed between light flash delivery and the moment in which current achieves 10% of its maximum value); 2) peak current; and 3) desensitization time constant (exponential time constant of the current decay phase). All parameters are affected by the first pulse.

To quantify recovery from desensitization, the ratio p2/p1 was employed versus time between pulses. p1 is the peak current evoked by the first light-pulse, and p2 is the peak current evoked by the second pulse. These data were fitted to a sum of exponential functions. Finally, these measurements were carried out as function of circadian time.

INTRODUCTION:
In order to be perceived as a visual stimulus, light reaching the eyes must be transduced into an electrical signal. Hence, in all visual organisms, light triggers a transduction ion-current, which in turn produces a change in the membrane potential of photoreceptor cells, the so-called receptor potential. Due to this, the light sensitivity of the eye primarily depends on the state of the light activated conductance, which can be either available to be activated or desensitized.

In crayfish photoreceptors, light triggers a slow, transient, ionic current[1]. Upon illumination, the transduction current arises after a lag or latency before reaching its maximum; thereafter it decays, as the transduction channels fall into a desensitized state in which they are unresponsive to further light stimulus[2]. That is, light, in addition to activating the transduction current responsible of vision, also induces a transient decrement of the sensitivity of photoreceptor cells. Desensitization may represent a general protective mechanism against overexposure to an adequate stimulus. The eye's sensitivity to light is recovered as the transduction conductance recovers from desensitization.

Intracellular recording is a useful technique for measuring electrical activity of excitable cells[3-8]. Although intracellular recording has become less frequent with the advent of the patch-clamp technique[9], it is still a convenient approach when cells are either difficult to isolate, or present a geometry that makes the formation of the patch-clamping giga-seals difficult (*i.e.*, seals or tight-contacts between the patch electrode and membranes with electrical resistance of the order of 10^9 ohms). Examples of the latter are sperm cells[10] and the photoreceptor cells herein studied. In our experience, *Procambarus clarkii* photoreceptors are difficult to isolate and keep in primary culture; additionally, they are thin rods that make giga-seal formation difficult to achieve. In intracellular recordings, a sharp electrode is advanced into a cell that is kept in place by the surrounding tissue. The electrode is chopped by the high-speed switching circuitry of the amplifier, so current is sampled between voltage pulses. This mode is known as discontinuous single-electrode voltage clamp (dSEVC mode)[11]. The high resistance (small opening) of the electrode hinders the diffusional exchange between the cell and the pipette solutions, yielding a minimal disturbance of the intracellular milieu[3]. A potential drawback of this technique is that electrode insertion may produce a non-selective leak current; therefore, care must be taken to avoid recording from cells where the size of the leak current may interfere with the intended measurements[4,12].

Herein, we use isolated crayfish eyestalks to assess desensitization and recovery of the light-

activated ion conductance by performing intracellular electrical recordings of photoreceptor cells under voltage clamp conditions.

PROTOCOL:

Note: The experiments comply with the Laws of Animal Protection of Mexico.

1.1.   General connections

1.1.1.   Connect the amplifier to a suitable computer through an analog-to-digital converter and use an oscilloscope to monitor the experiment (**Figure 1**).

1.1.2.   Connect the photostimulator to the A/D converted.

1.2.   Recording chamber

1.2.1.   Place the recording chamber on top of an anti-vibration table and locate it inside a Faraday cage.

Note: This prevents mechanical vibration and electrical noise that may affect the recording. Our Faraday cage was made of darkened wire mesh. A homemade, 2 mL, acrylic recording chamber is used (**Figure 2**).

1.2.2.   Prepare the bath solution to keep the preparation alive[13]: 205 mM NaCl; 5 mM KCl; 2 mM $MgSO_4$; 13 mM $CaCl_2$; 5 mM Hepes-NaOH, pH 7.3.

Note: Solution does not include dextrose or any bubbling by 95% O_2, 5% CO_2 mixture because the experimental procedure is short enough to detect damage by the electrical recording (see step 4.2.3 for completeness).

1.3.   Electrodes

1.3.1.   Use a chloride-coated silver-wire electrode as the reference electrode

Note: Silver chloride coating is necessary to allow the electrode reaction: $AgCl(s) + e^- \leftrightarrow Ag(s) + Cl^-$.

1.3.1. Sand a silver wire (thickness ~ 1 mm, length ~ 10 cm) with a fine grade emery paper in order to clean its surface.

1.3.1. Rinse the silver wire with distilled water.

1.3.1. Immerse the clean silver-wire in a 4–6% sodium hypochlorite solution (NaClO) until it appears dark (approximately 20 min).

1.3.2.   Use thin glass pipettes filled with an electrolyte solution (2.7 M KCl) as the intracellular electrode.

1.3.2. Pull a glass capillary tube (internal diameter ≈ 1 mm) with a micro-pipette puller to obtain a thin tip with a small opening (0.01–0.1 μm)[14].

1.3.2. Fill the pulled capillary glass with a 2.7 M KCl solution. First fill it by capillarity (immerse the pipette tip into the 2.7 M KCl solution) and then fill the half of the pipette with a fine injection needle. If necessary, tap the electrode pipette to eliminate air bubbles.

1.3.3.   Connect the electrode to its holder. Connect the holder to the amplifier headstage with the amplifier. Position the electrode-holder-headstage with a stable 3-D micromanipulator. Lower the electrode until bath solution covers its tip.

Note: The electrode must have a vertical orientation

1.4.   Select the Bridge Mode of the amplifier (in the Mode section of the amplifier, press the Bridge button) and measure the electrode resistance. Make sure that the resistance is about 50 MΩ[11].

Note: This electrode size allows a good-quality electrical recording with limited damage to the cell.

1.5.   Null the offset current and compensate capacitive transients using the Holding Position button in the section Voltage Clamp of the amplifier, and the Capacitance Neutralization button in Microelectrode 1 section of the amplifier.

1.6.   Superfusion system

1.6.1.   Pour the bath solution (step 1.2.2) into a suitable receptacle (a 250 mL serum bottle) and connect it to an irrigation tubing set (3.2 mm of internal diameter), thus connecting the recording chamber. Use a gravity driven superfusion system. Regulate the flow rate to ~ 0.5 mL/s.

1.6.2.   Connect the chamber to a suction device. Regulate the solution suction system in such a way that the total volume of the recording chamber does not vary. Use a vacuum pump for suction.

Note: A constant volume in the recording chamber is important to keep stray capacitances constant throughout the experiment.

2.   Biological Material

Note: Use adult crayfishes *P. clarkii* (7–10 cm long) in the intermolt stage of indistinct sex.

2.1.   Circadian time

2.1.1. One month prior to the experiments, maintain 100 crayfishes under a 12-h light/12-h dark cycle[15] (white light, 2.4 kW/m^2).

Note: One month is sufficient time to synchronize the crayfish population.

2.1.2. Determine the circadian time of the crayfish population by assessing the amplitude of electroretinograms of five randomly chosen animals[15].

Note: 0 h circadian time (CT 0) indicates the beginning of a subjective day, *i.e.*, time during which an organism is normally active[16, 17, 18, 19] (**Figure 3**). The crayfish is a nocturnal animal, so under a 12-h light/12-h dark cycle, it is active during the dark phase.

2.2.   Eyestalk isolation procedure

2.2.1. At the desired circadian time, anesthetize a selected crayfish by immersion in tap water at 0–4 °C, for 15 min.

2.2.2. By means of a fine scissor, detach the eyestalk from the base.

2.2.3. Access the retina using a razor blade to make an opening (~ 1-mm^2) in the dorsal cornea.

2.2.4. Place the eyestalk in the center of the recording chamber (the hole covered with silicone) with the access opening to the retina on the top of the chamber.

2.3.   Keep the eyestalk under constant darkness for 20 min.

Note: 20 min is sufficient time for the photoreceptor cell to be fully dark adapted.

3.   **Photoreceptor Impaling**

3.1.   Put the microelectrode and the eyestalk's longitudinal axis parallel in such a way that the microelectrode is centered for access to the retina. Use a stereoscopic microscope (10X) to place the devices in the correct configuration.

3.2.   Monitor the voltage difference between the reference and recording electrodes by selecting the Bridge Mode[11] of the amplifier.

3.3.   Lower the electrode into the bath and thereafter place it right over the retina.

3.4.   Move away the microscope and position the photostimulator lamp parallel to the eyestalk's longitudinal axis.

Note: Distance between lamp and superfusion chamber is approximately 15 cm.

3.5.   Slowly lower the microelectrode until a sudden voltage drop is detected.

Note: A voltage drop of around −50 mV indicates the impalement of a healthy photoreceptor cell.

3.6.   Deliver a test light-flash (white light, 7.2 kW/m^2, 10 μs duration) to record the photoreceptor's receptor potential.

Note: The photoreceptor's receptor potential is a depolarizing potential of 10–15 mV amplitude and 300 ms duration (**Figure 4**).

4.   Electrical Recording

4.1.   Ensure that the photoreceptor cells are totally adapted to dark conditions (see step 2.3).

4.1.1.   Deliver a test-light flash every 2 min. Automate the time between flashes by choosing an adequate value (120 s) of "time between episodes" in the data acquisition software.

Note: 2 min is the necessary time to allow the total recovery of the currents underlying the photoreceptor's electrical response.

4.1.2.   Monitor the resting membrane potential, as well as the amplitude and duration of the receptor potential. Assume that the photoreceptor is completely adapted once the membrane potential, amplitude, and duration of the receptor potential remain unchanged. Eyestalks previously kept under constant darkness for 20 min (step 2.3) complete their adaptation in approximately 5 min.

4.1.3.   Stop stimulating the cell 2 min before recording the light-elicited current.

4.2.   Current recording

4.2.1.   Clamp the voltage at the measured resting membrane potential value of the cell by selecting "Holding amplitude" in the data acquisition software (in Waveform on the Analog Output Channel section).

4.2.2.   Select the dSEVC mode of the amplifier. In the Mode section of the amplifier, select the SEVC button and switch the lever to the Discont SEVC position.

4.2.3.   Set the switching rate to 500–1,000 Hz (by using the Rate Adjust button of the amplifier), as determined by the speed of the electrode[11].

4.2.4. Deliver a light-flash, and observe the evoked ion influx.

Note: This is the light-elicited or transduction current (**Figure 5**).

4.2.5. Return to the Bridge mode on the amplifier and record a receptor potential by sending a light flash (see section 3). Make sure that the photoreceptor cell is totally adapted to dark conditions. Measure the receptor potential characteristics (amplitude and duration) and compare with the first measurements. Assume that the impaled photoreceptor cell is a healthy cell if they have the same characteristics.

Note: After eyestalk ablation, biological preparation is viable during the following 2 h.

4.3.   Two pulse protocol: Measure the recovery from desensitization with a two light-flash protocol.

Note: The two light-flash protocol is similar to the standard two-pulse voltage protocol used to measure recovery from inactivation of voltage-gated channels[20]. The first light-flash causes a temporary change in the sensitivity of the photoreceptor cell and the second flash evaluates the state of the light-activated conductance.

4.3.1. Deliver a pair of light pulses. Apply the second flash after a desired time interval (from 300 ms to 2 min).

4.3.2. Digitize the currents at 10 KHz sampling with the data acquisition software and save the data for off-line analysis[11].

Note: A table with the configuration values of the software is included as supplementary material.

5.   Data Analysis

5.1.   Kinetics of the light-elicited current

5.1.1. Measure three current parameters: activation latency L, the time elapsed from the light-flash delivery until the current attains 10% of its maximal amplitude (**Figure 5**); peak or maximal current amplitude I_p; and desensitization time constant T. Measure the desensitization time constant (T) by fitting the current decay phase to:

$$i(t) = -Ae^{\frac{-t}{T}}$$

where, A = -I(t=0) is a positive constant (**Figure 5**).

5.2.   Desensitization and recovery

Note: Recovery from desensitization was assessed as the ratio p_2/p_1, where p_1 is the relevant parameter (either L, I_p, or T) of the control current, and p_2 is the corresponding parameter of the second test-current.

5.2.1.   Plot p_2/p_1 (either L, I_p, or T) as a function of time between pulses.

5.2.2.   Depending on the parameter, fit the points of each plot to:

$$\frac{p_2}{p_1} = \sum_{1}^{n} 1 - e^{\frac{-t}{\tau_n}}$$

or to:

$$\frac{p_2}{p_1} = \sum_{1}^{n} 1 + A_n e^{\frac{-t}{\tau_n}}$$

5.2.3.   Use an appropriate statistical test to determine the number of exponential terms required to fit the experimental data.

REPRESENTATIVE RESULTS:
First, a representative receptor potential of crayfish photoreceptor cells is obtained (**Figure 4**). Afterwards, a test light-flash was applied to trigger the light transduction current (**Figure 5**). The cationic transduction current[1] activates after a lag, reaching a maximal and thereafter slowly drops into an absorbing desensitized state from which it slowly recovers.

It is reasonable to suppose that the long latency L (tens of milliseconds) of the light-elicited current depends on the biochemical events triggered by light, which involve G-protein pathways. The amplitude of the peak current I_p depends on the fraction of channels available to be opened, and the relative rates of current activation and inactivation. The latter is assessed by the decay time constant T.

On the other hand, the L recovery should be related to the rate of recovery of the biochemical phototransduction cascade; I_p recovery depends both, on the intrinsic conformational changes of the proteins responsible for the ion conductance, and on the rate of recovery of the biochemical phototransduction cascade. The latter could also be related to the recovery of T. Furthermore, the parallel variation of L and T suggest that a common biochemical factor (or factors; *e.g.*, the phosphorylation state of the channel) can affect both parameters[1].

A two-flash protocol (**Figure 6**) was applied subsequently to determine the kinetics of recovery

from desensitization (**Figure 7**) at different moments in the circadian cycle (**Figure 8**).

FIGURE LEGENDS:
Figure 1. Line diagram of the equipment setup. Connections among personal computer (PC) (**A**), interface (**B**), oscilloscope (**C**), voltage-clamp amplifier (**D**), photostimulator (**E**), and the headstage/holder/microelectrode system of the equipment setup (**F**).

Figure 2. Recording chamber. (**A**) The recording chamber inside a Faraday cage with its superfusion-suction system. It is also shown the position of photostimulator, microscope, and micromanipulator-headstage-microelectrode system. (**B**) Diagram of the recording chamber.

Figure 3. Electroretinogram (ERG) amplitude. (**A**) Crayfish. (**B**) Representative plot of the ERG amplitude of crayfish photoreceptors (data were taken every 20 min) as a function of circadian time. The existence of a circadian rhythm can be clearly appreciated. Note that for each cycle, the beginning of activity coincides with circadian time 0.

Figure 4. Receptor potential. Representative receptor potential evoked by a light flash (white light, 7.2 kW/m^2, 10 µs duration). This figure has been modified from Barriga-Montoya, C, *et al.*[2].

Figure 5. Transduction current. Representative transduction current triggered by a light flash (white light, 7.2 kW/m^2, 10 µs duration) applied with the voltage kept constant at the photoreceptor resting potential. Current latency, peak amplitude, and desensitization phase are indicated. This figure has been modified from Barriga-Montoya, C, *et al.*[2].

Figure 6. Two-pulse protocol. Currents elicited by a pair of light flashes. Light stimuli were applied at 0 ms and 700 ms (indicated by arrows). This figure has been modified from [2].

Figure 7. Recovery from desensitization. (**A**) L: latency recovery, (**B**) I_p: peak current recovery, (**C**) T: Desensitization time constant T recovery. Experiments were performed at 0 h CT. This figure has been modified from Barriga-Montoya, C, *et al.*[2]. Results are expressed as the mean ± standard deviation of the number of experiments (n = 11).

Figure 8. Recovery from desensitization as a function of CT. (**A**) I_p recovery, (**B**) L recovery, (**C**) T recovery. (**D**) Weighted time constants. Biphasic processes are marked with an arrow. This figure has been modified from Barriga-Montoya, C, *et al.*[2]. Results are expressed as the mean ± standard deviation of the number of experiments (n = 11).

DISCUSSION:
The crayfish has proven to be an excellent model due to its ability to survive under non-natural conditions. There is easy access to *in vivo* and *in vitro* electrophysiological analyses. In addition, crustaceans are a favorable group for neurobiological research in the field of comparative chronobiology[21].

In this paper, the study of desensitization and recovery of the light-activated transduction-

current of crayfish photoreceptor cells is shown using the intracellular recording technique. However, we believe that the same technique could be adapted to other invertebrate visual systems as long as it is possible to access photoreceptor cells.

To obtain acceptable experimental results, it is important to consider some critical steps in the protocol, including eliminating electrical noise by grounding all equipment, building an electrode with a sufficiently fine tip, and ensuring that the photoreceptor cell is completely dark-adapted before the two-pulse protocol begins.

Despite the limitations of intracellular recording such as the damage of membrane, it is possible to go further and obtain detailed information about the biophysical mechanism underlying crayfish (or another animal) photoreceptor electrical signal. As in other invertebrate photoreceptors, in crayfish photoreceptors, light triggers a graded depolarization, or receptor potential, produced by the activation of a cationic conductance. The light-activated conductance begins after a lag or latency, and after reaching its maximal amplitude, it slowly drops following an exponential time course, as the channels enter an absorbing desensitized state.

The kinetics of recovery from desensitization of the light-elicited ion conductance of crayfish were obtained using a two-light flash protocol (similar to the standard two-voltage pulse protocol used to study recovery from inactivation of voltage-gated channels)[20]. Interestingly, and in contrast to the well-known case of voltage-gated channels, not only the peak amplitude, but also all the current parameters (I_p, L, T) change after the first light stimulus, recovering with characteristic exponential time courses to the original, first flash values, as reported elsewhere[20]. This variation of all the parameters that characterize the current indicates the participation of second messengers in the visual transduction system of crayfish[1, 2, 22-24].

Additionally, and interestingly, as **Figure 8** shows, recovery of L, I_p, and T depends on the circadian time at which experiments are realized. Further studies are needed to determine the molecular basis of this phenomenon. Of course, it is possible to obtain similar information using another technique, such as patch clamp. However, the intracellular milieu can be greatly disturbed in other techniques, and this could be critical, if, for example, internal elements like proteins, amino acids, nucleotides, among many others, play a relevant role in the electrical signal generation or in the interaction with hormones or neuromodulators.
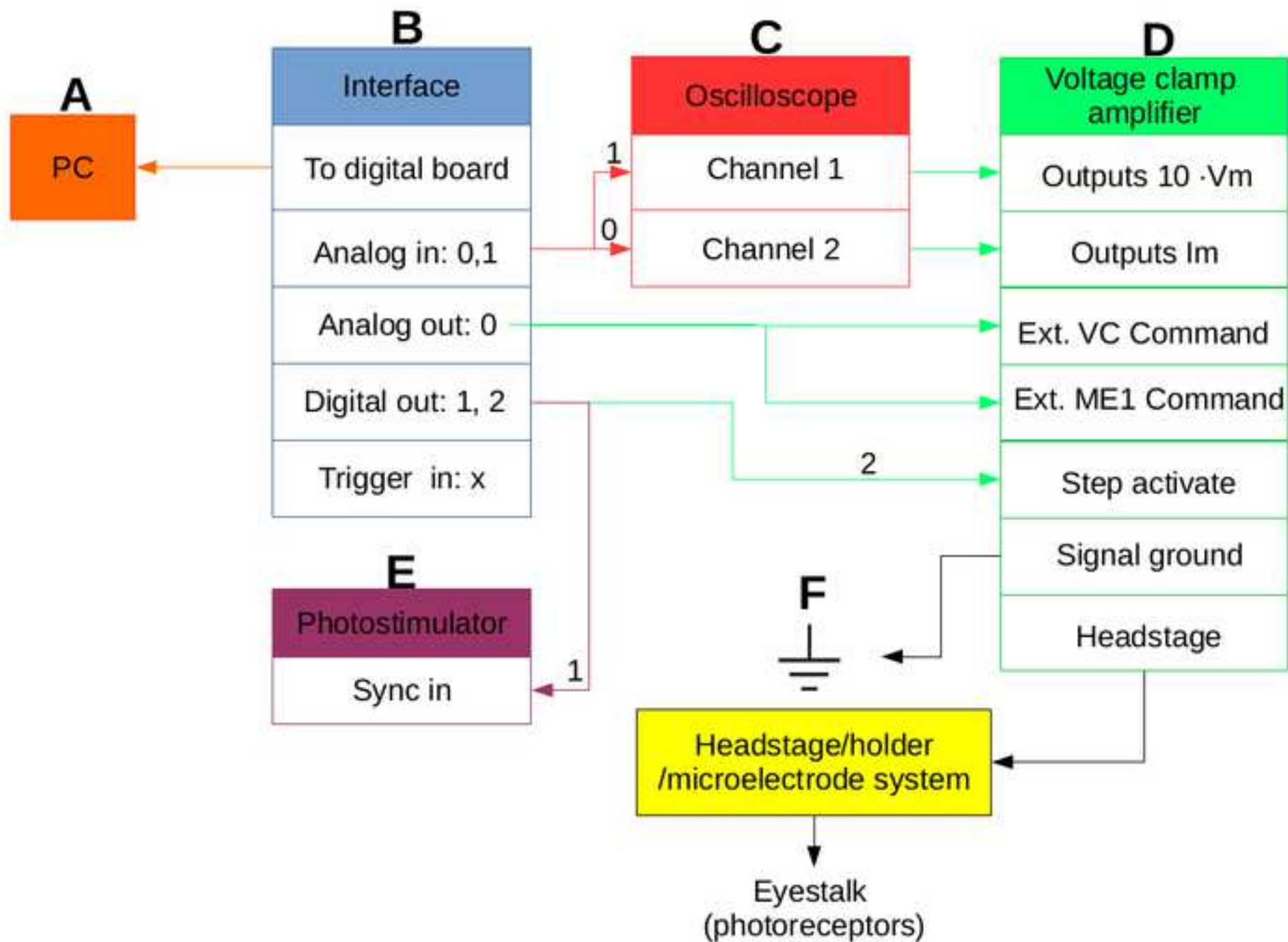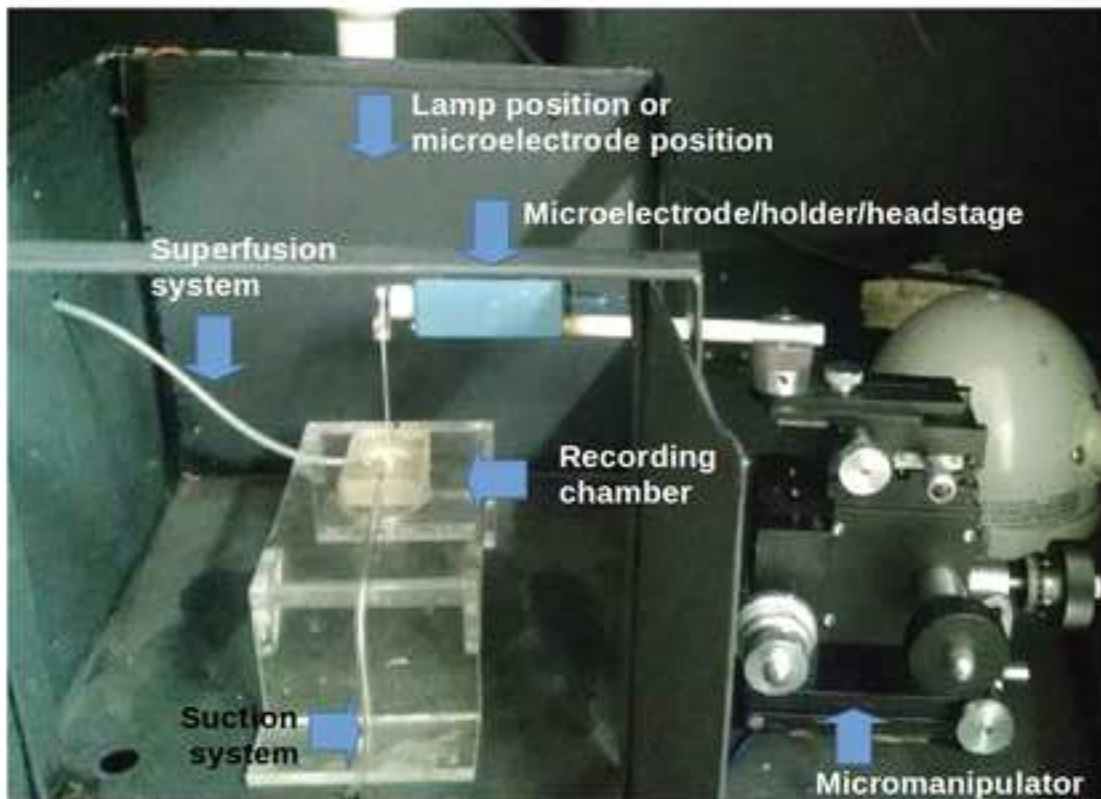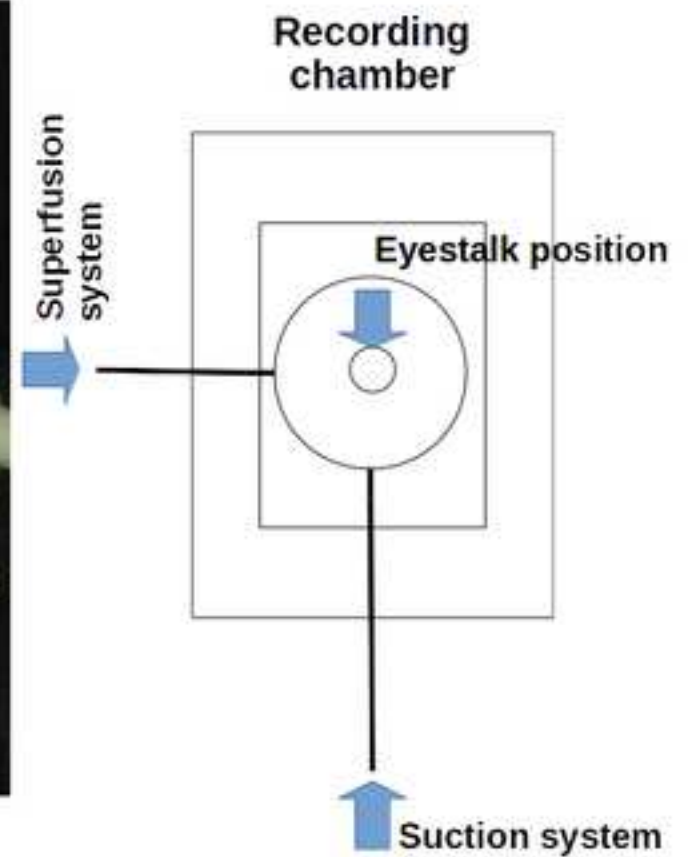
DISCLOSURE:
We have nothing to disclose.

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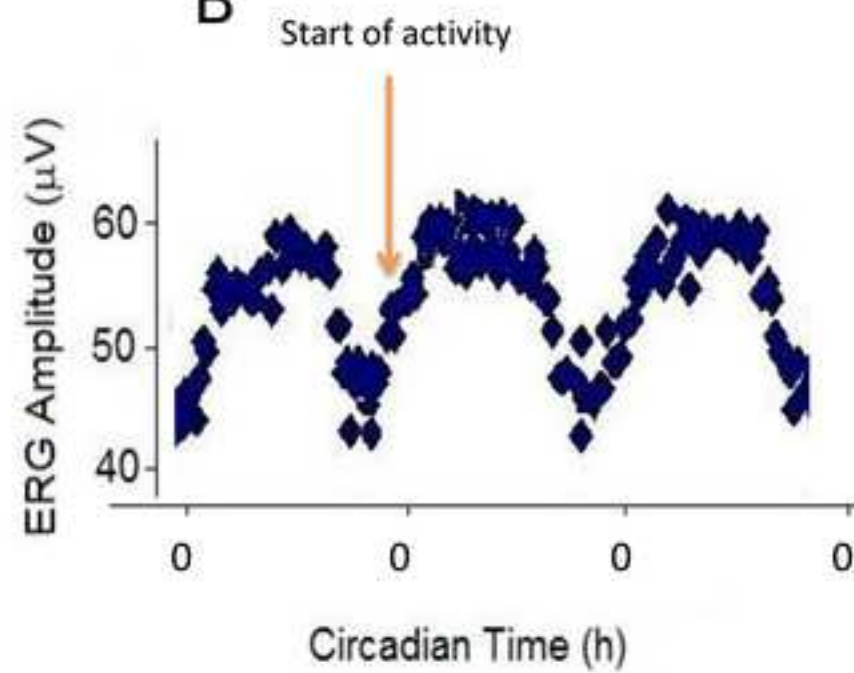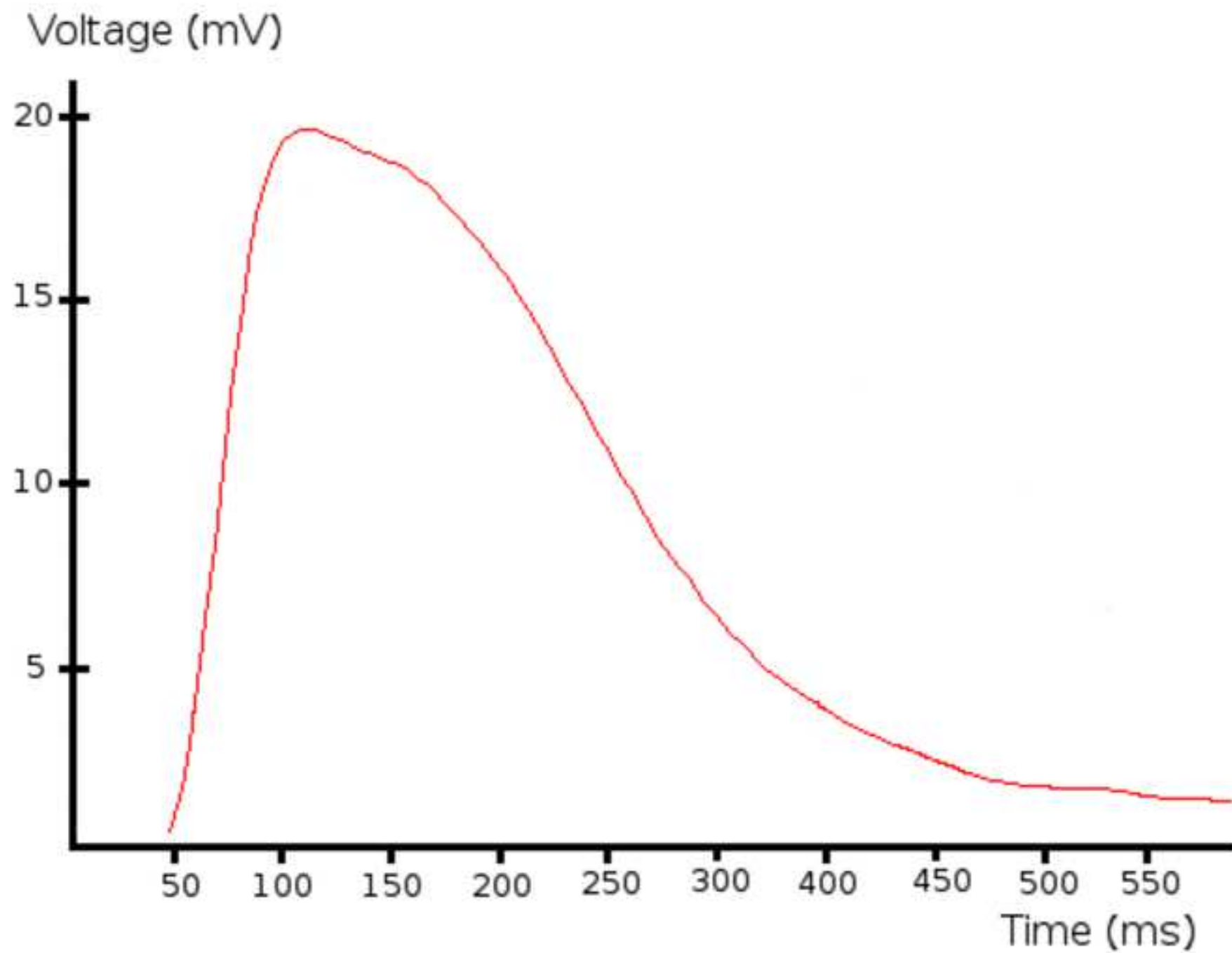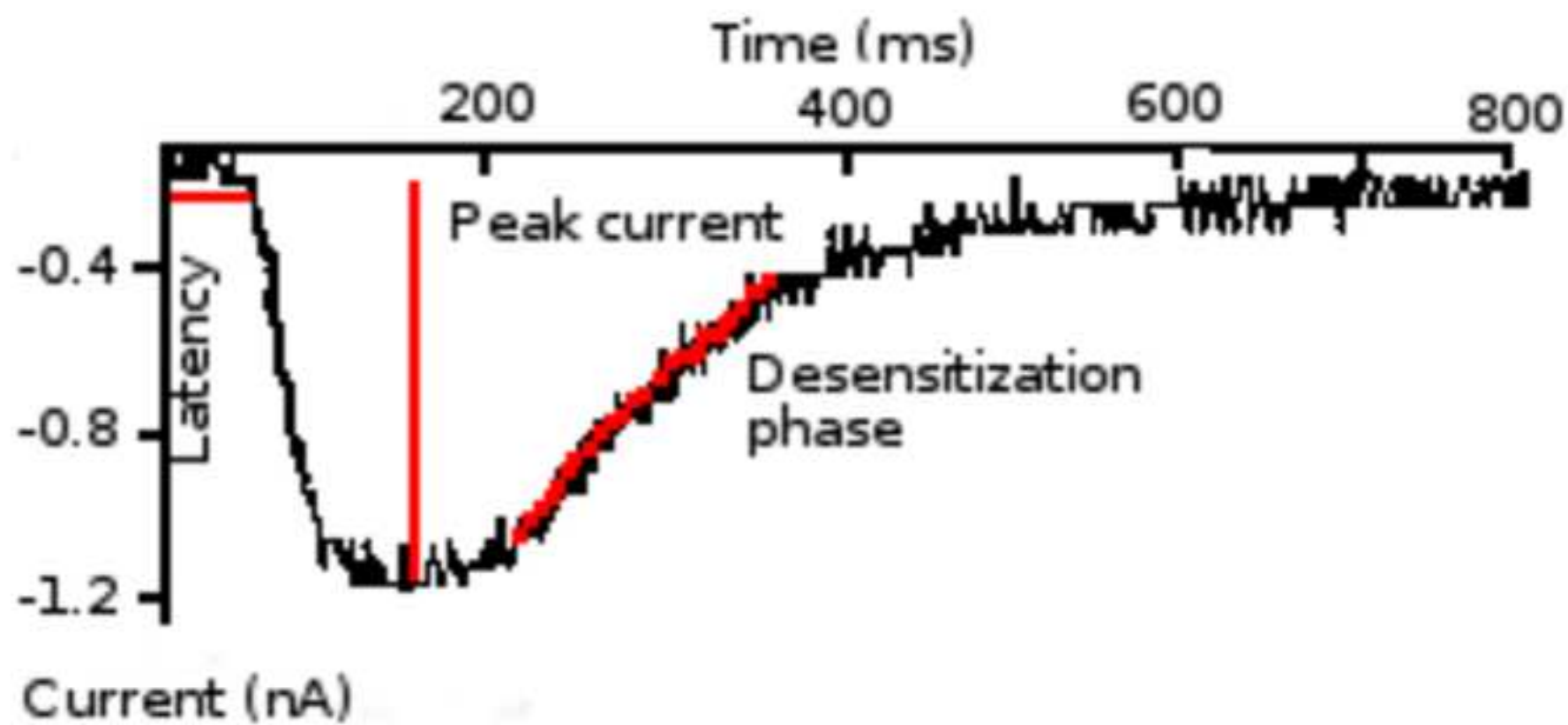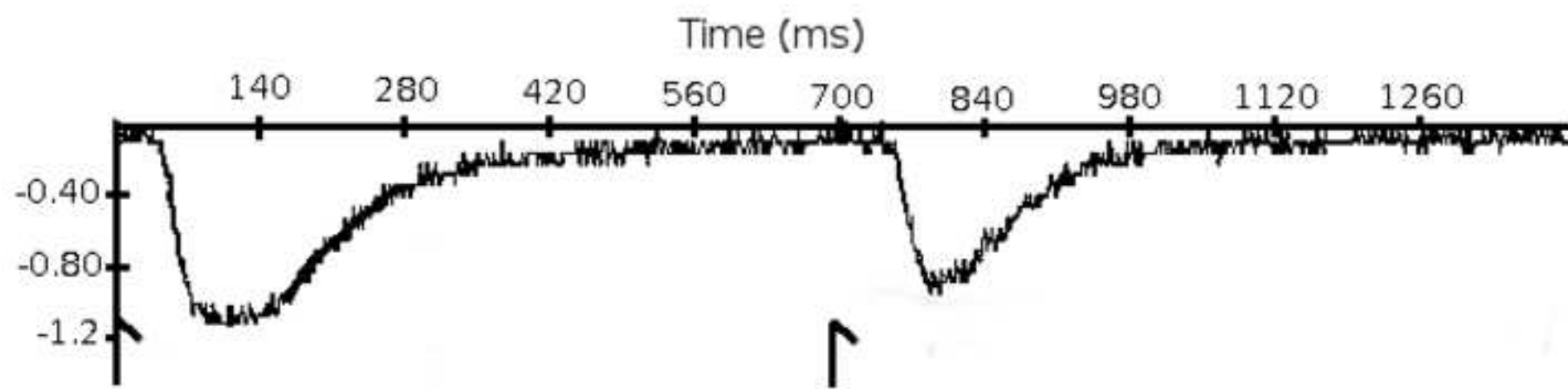
A

Lamp position or microelectrode position

Microelectrode/holder/headstage

Superfusion system

Recording chamber

Suction system

Micromanipulator

B

Recording chamber

Superfusion system

Eyestalk position

Suction system

A

B
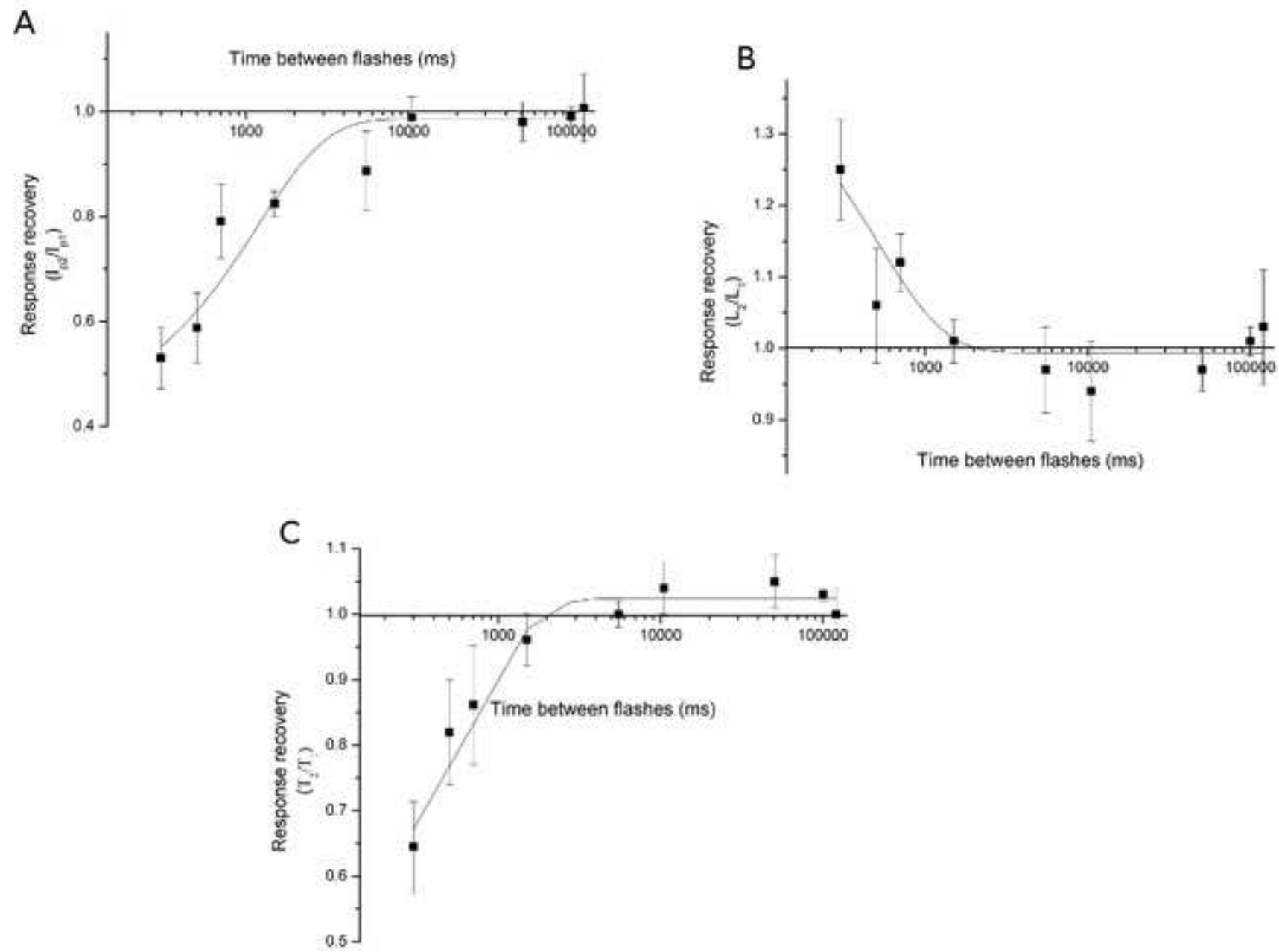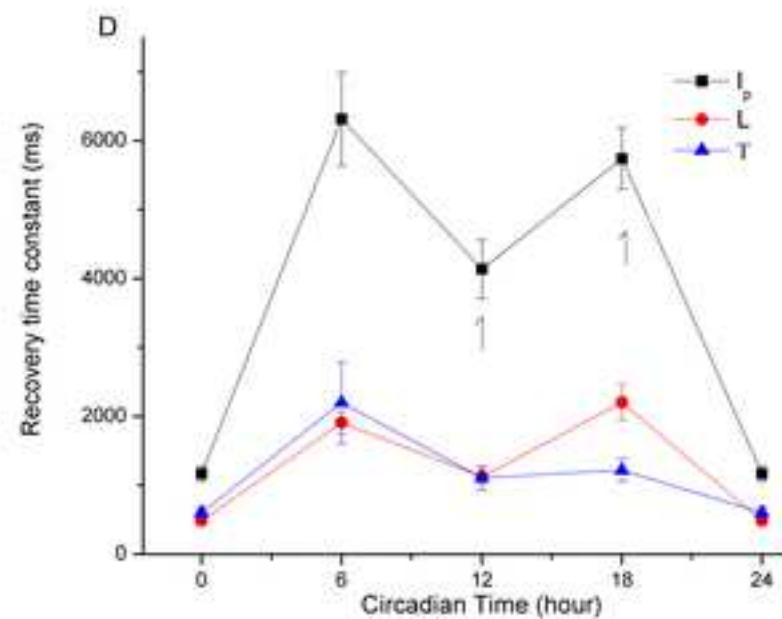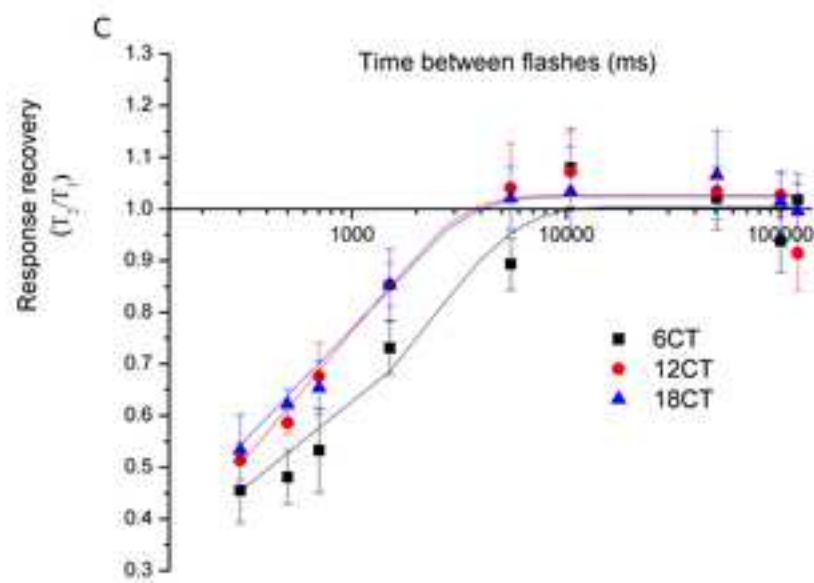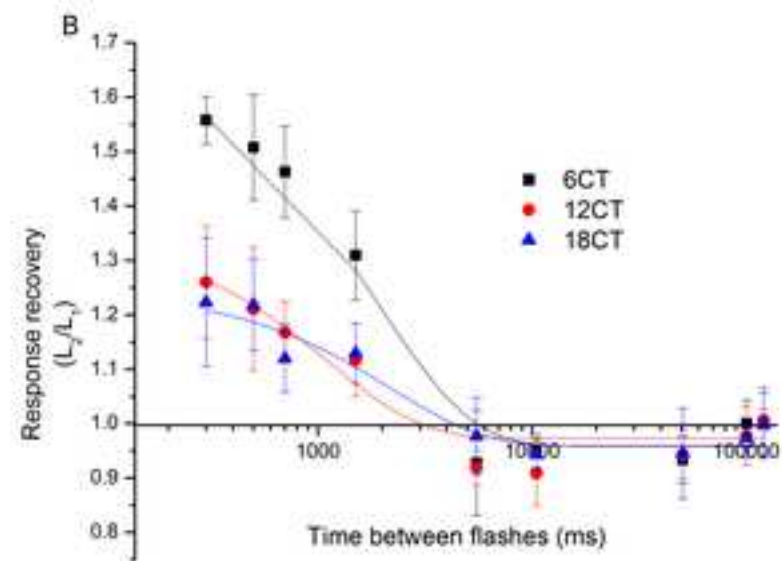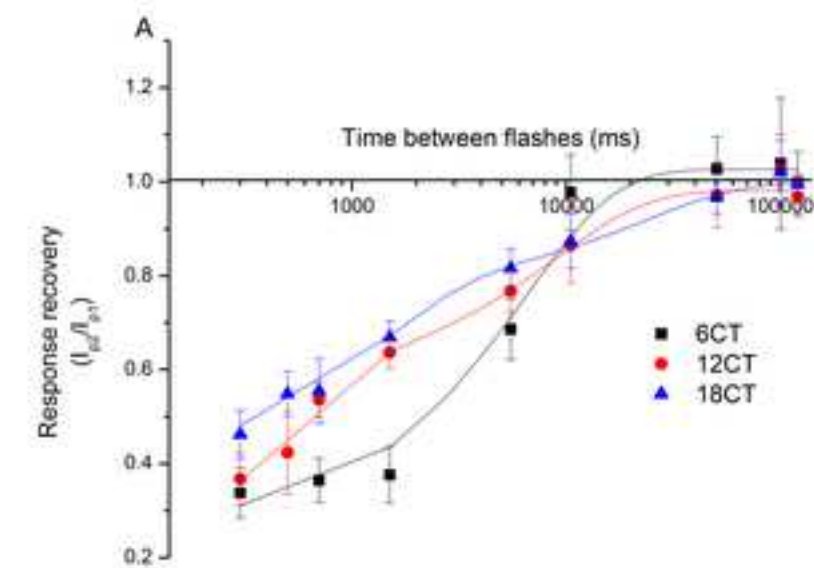
Name of Material/ Equipment	Company	Catalog Number	Comments/Description
Axoclamp2A	Axon Instruments Inc		Amplifier
Digidata 1200 Interface	Axon Instruments Inc		Digitizer
Oscilloscope TDS430A	Tektronix		Analogic Oscilloscope
Photostimulator PS33 Plus	Grass		Lamp
Puller PC-100	Narishige		Micropipette Puller
Puller P-97	Sutter Instruments		Micropipette Puller
Glass Capillary Tube Kimax-51	Kimble Products	34502	0.8, 1.10, 100 mm
HS-2 Headstage	Axon Instruments Inc		Headstage
Micromanipulator MX-4	Narishige		Mechanical Micromanipulator
Stereoscopic Microscope	Zeiss		Microscope
pClamp	Axon Instruments Inc		Data acquisition software for digidata 1200 interface
Clampfit	Axon Instruments Inc		Analysis software linked to pClamp
Origin	OriginLab Corp.		Data analysis and graphing software
Sodium Chloride	Sigma	S7653	>99.5%
Potassium Chloride	Sigma	P-9333	Minimum 99%
Magnesium Sulfate	Sigma	M7506	Minimum 99.5%
Calcium Chloride	Sigma	C5080	Minimum 99.0%
Hepes	Sigma	H7523	>99.5%
Sodium Hydroxide	Sigma	S8045	98.00%
Sodium hypochlorite solution	Sigma	425044	Available chlorine, 10-15%

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Author(s): BARRIGA -MONTOYA C, de la O-MARTINEZ A etal

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CORRESPONDING AUTHOR:

Name: Froylán Gómez-Lasunas

Department: Fisiología, Facultad de Medicina

Institution: Universidad Nacional Autonoma de Mexico, UNAM

Article Title: ON The DESENSITIZATION AND SENSITIVITY ----

Signature: *Froylán Misrad Gómez Lasunas*   Date: 3-17-2017

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Dear Editor,

Please receive the revised manuscript JoVE56258R1 "On desensitization and recovery of crayfish photoreceptors upon delivery of a light *stimulus*." to be considered for publication in the JoVE.

We satisfactorily answered all the comments and modify the article and figures to totally fulfill their requests.

The list detailing the changes made to the manuscript is:

1. Please ensure that all text in the protocol section is written in the imperative tense as if telling someone how to do the technique (e.g., "Do this," "Ensure that," etc.). **The actions should be described in the imperative tense in complete sentences wherever possible.** Any text that cannot be written in the imperative tense may be added as a "Note."
All text in the protocol is written in the imperative tense or was added as a Note.

2. Figure 1: Please align different panels in this Figure and label all panels, e.g. A, B, C, etc.
We align and label different panels.

3. Figure 2: Please align two panels in this Figure and label two panels. Please use 'h' instead of 'hours'.
We suppose it corresponsd to figure 3. We align two panels and use h instead of hours.

4. Figure 3, 4, 5, 6 and 7: Please add x, y axes with scales and their corresponding symbols for this Figure.
We add x an y axes with scales.

5. For each figure, please provide a title and a short description.
Each figure has a title (in bolds) and a short description

6. Please remove 'Place Figure X here' in the manuscript.
There are no more 'Place Figure X here' in the manuscript.

7. Please use focused images of uniform size/resolution (at least 300 dpi).
We use images of at least 300 dpi

8. Please abbreviate all journal titles for references.
We abbreviate all journal titles for references.

Additionaly,
Section 1.3.1. We corrected the reaction
Sections 1.4., 4.2. We do not upper case all letters.

Sincerely,

Dr. Froylán Gómez-Lagunas

Software parameters for measuring electrode resistance (BRIDCAP), receptor potential (RP), and [LEC?] current (LEC)

	BRIDCAP	RP
ACQUISITION		
Number of trial to perfrom (−1 for continuous)	−1	1
Number or runs/trial (runs are averaged) (≤65536)	1	1
Number of episodes/run (if no conditioning pulses)	1	60
Perform interepisode data write: 0=No, 1= Yes (Set future trials>0)	0	0
Starting episode number (normally 1)	1	1
Number of 512–sample segments/episode (1..4)	1	1
Number of channels to sample (1..4)	2	2
Trigger mode: 0=Internal, 1=External, 2=Space bar, 3=Ext–No waveform	0	0
Time between start of episodes (s) (0 for maximum rate)	1	120
First clock interval (samples 1–256) (≥8µs)	100	2000
Second colck interval (samples 257–512) (µs)(0 to use 1st clock)	0	0
Delay between scope trigger and episode start	0	0
SUBTRACTION		
Number of P/N sub–pulses: 0=None, –N=Add, +N=Substract	0	0
ADC channel number	0	0
Subpulse holding amplitude (mV)	0	0
Settling time after change of holding amplitude (ms)	0	0
Time interval between subpulses	0	0
WAVEFORM ON ANALOG OUTPUT CHANNEL #0		
Holding amplitude (mV)	0	0
A Epoch type: 1_step, 2=ramp	1	1
Amplitude initial value (mV)	0	0
Amplitude increment (mV)	0	0
Duration initial value (samples)	10	0
Duration increment (samples)	0	0
B Epoch type: 1_step, 2=ramp	1	1
Amplitude initial value (mV)	0	0
Amplitude increment (mV)	0	0
Duration initial value (samples)	10	0
Duration increment (samples)	0	0
C Epoch type: 1_step, 2=ramp	1	1
Amplitude initial value (mV)	0	0
Amplitude increment (mV)	0	0
Duration initial value (samples)	0	0
Duration increment (samples)	0	0
D Epoch type: 1_step, 2=ramp	1	1
Amplitude initial value (mV)	0	0
Amplitude increment (mV)	0	0
Duration initial value (samples)	0	0
Duration increment (samples)	0	0
Inter–episode amplitude: 0=Holding, 1=Last epoch amplitude	0	0
TRIGGER OUTPUTS		
Duration and polarity of pulse on trigger channel #1 (samples)	0	10
Sample number at which start pulse	0	10
Duration and polarity of pulse on trigger channel #2 (samples)	250	0
Sample number at which start pulse	20	0
First episode at which trigger channels #1 and #2 fire	1	0
Last episode at which trigger channels #1 and #2 fire	500	500

CONDITIONING TRAIN		
Number of pulses in train (0 for none)	0	0
Pre–conditioning pulse duration (ms)	0	0
Pre–conditioning pulse amplitude (mV)	0	0
Conditioning pulse duration (ms)	0	0
Conditioning pulse amplitude (mV)	0	0
Post–conditioning train duration (ms)	0	0
Post–conditioning train amplitude (mV)	0	0
DISPLAY DATA		
ADC ch. #3: amplification factor (not 0)	1	1
Display offset: fraction of full screen	0	0
ADC ch. #2: amplification factor (not 0)	1	1
Display offset: fraction of full screen	0	–5
ADC ch. #1: amplification factor (not 0)	20	40.95
Display offset: fraction of full screen	0	0.7
ADC ch. #0: amplification factor (not 0)	20	50
Display offset: fraction of full screen	–0.2	0
Segment number to display (0..1) (0 for all)	0	0
Skip factor: plot every nth point (1..1)	1	1
Display averaged data: 0=After each episode, N=After each N runs	0	0
Autoerase: 0=No, 1=Yes	1	0
Graph style: 0=Points, 1=Lines	1	1
UNITS OF MEASURE		
ADC ch. #3	mV	mV
ADC ch. #2	mV	mV
ADC ch. #1	mV	mV
ADC ch. #0	uA	pA
DAC ch. #0	mV	mV
PEAK DETECTION		
Search mode: 0=None, 1=A, 2=B, 3=C, 4=D, 5=All, 6=Use sample number	0	0
Optional sample number to measure, negative for negative peaks	0	0
Channel number to search	0	0
Number of samples averaged in search (1–20) (0 for default 5)	0	0
Baseline: 0=Average first 6 samples, 1=Average interval A	0	0
Display: 0=Screen, 1= File&screen	0	0
HARDWARE CONFIGURATION		
DAC ch. #0: gain from DAC to cell (mV@cell/V@DAC)	20	20
ADC ch. #3: gain from cell to ADC (V@ADC/mV@cell)	1	1
ADC ch. #2: gain from cell to ADC (V@ADC/mV@cell)	1	1
ADC ch. #1: gain from cell to ADC (V@ADC/mV@cell)	0.01	0.01
ADC ch. #0: gain from cell to ADC(V@ADC/pA@cell)	1	1
ADC range, ±V	10.24	10.24
DAC range, ±V	10.24	10.24
Autosample Axopatch–1: 0=Manual, 1=Yes, 2=Yes (inverted), 3= Disabled	0	0
Gain multiplier	1	1
Filter cutoff frequency	10,000	100,000
TIMES		
Start time for this data file		
Elapsed time for this data file		
Date this data file acquired		

light-elicited

LEC
1
1
11
0
1
1
1
0
120
700
0
0
0
0
0
0
0
Membrane Potential
1
Membrane Potential
0
500
0
1
0
0
0
0
1
0
0
0
0
1
0
0
0
0
0
−10
1
−20
1
1
24

0
0
0
0
0
0
0
1
0
1
0
1
0
25
0
0
1
0
0
1
mV
mV
mV
nA
mV
0
0
0
0
0
0
20
1
1
0.01
0.115
10.24
10.24
0
1
10,000