**TITLE:**

Analysis of Spinal Cord Blood Supply Combining Vascular Corrosion Casting and Fluorescence Microsphere Technique: A Feasibility Study in an Aortic Surgical Large Animal Model

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**KEYWORDS:**

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**SHORT ABSTRACT:**

This study combines fluorescence microsphere technique and vascular corrosion casting to simultaneously investigate spinal cord blood flow and visualize spinal cord feeding arteries in a large animal model. This model can be employed to investigate morphological vascular alterations and hemodynamic parameters in the same tissue.

**LONG ABSTRACT:**

Spinal cord ischemia after cardiovascular interventions continues to be a devastating problem in modern surgery. The role of intraspinal vascular networks and anterior radiculomedullary arteries (ARMA) in preventing spinal cord ischemia is poorly understood. We are the first to combine the fluorescence microsphere technique and vascular corrosion cast to investigate spinal cord blood supply in a large animal model. Landrace pigs (n= 30, 35.1 ± 3.9 kg) underwent a lateral thoracotomy. Fluorescent microspheres were injected into the left atrium and a reference sample was aspirated from the descending aorta. Repeated measurements of spinal cord and renal cortical blood flow from the left and right kidneys with three different microsphere colors in 5 pigs were taken to validate reproducibility. Spinal cord blood flow to the upper thoracic (T1–T4), mid-thoracic (T5–T8), lower thoracic (T9–T13), and lumbar (L1–L3) levels were determined. After euthanasia, we carried out selective vascular corrosion cast and counted theleft and right ARMAs from levels T1–T13. We observed no alterations in blood flow analysis and fluorescence background noise when using vascular corrosion casting in the same tissue. Repeated measurements of cortical renal blood flow and spinal cord blood flow were reproducible. Blood flow analysis of the left and right kidneys revealed a strong correlation (r = 0.94, *p*<0.001). We detected more left than right ARMAs, with the highest prevalence at T4 (*p*<0.05). The mean number of ARMAs was 8 ± 2. Their number in the upper thoracic region ranged from 2 to 7 (mean of 5 ± 1), while in the lower thoracic region they ranged from 0 to 5 (mean of 3 ± 1 (*p*<0.001)). This study shows that combining fluorescence microsphere technique and vascular corrosion cast is well suited for assessing the blood flow and visualizing the arteries at the same time.

**INTRODUCTION:**

**Microspheres**

Since its introduction by Rudolph and Heymann in 1967, microsphere technique has undergone continuous development1. Today it is the gold standard for measuring regional organ perfusion. Microspheres for blood flow studies are typically 15-µm-diameter particles labeled with colored, radioactive, or fluorescent substances. When injected into the left atrium, they mix into the central circulation and trigger microembolization in small capillaries (“trapping”). Blood flow is proportional to the number of microspheres in the region of interest. Following introduction of the reference sample method, it became possible to calculate absolute blood flow in mL/min/g by comparing the number of microspheres in the reference sample, aspirated at a predefined rate downstream to the injection site, with the number of microspheres in the region of interest2. However, the radioactive microspheres that were first introduced were hazardous for both humans and animals because of the radiation burden. Their expense, especially due to their high disposal costs and large animal experimental models, led to new methods3. Fluorescent microspheres have the advantage of great accuracy, very good spectral separation, high reliability, and low cost compared to radioactive microspheres4,5.

**Vascular Corrosion Casting and Spinal Cord Anatomy**

Vascular corrosion casting has a long history in describing the morphology of vessels and visualizing small vessels that remain otherwise undetectable by the human eye. With the invention of low viscosity resin in 1970, it became possible to study the microvasculature and distribution of small vessels6–8. Modifications in resin's viscosity helped to obtain highly detailed vascular castings. In combination with scanning electron microscopy, this method can provide a precise image of the endothelial surface of the vessels9.

In contrast to these advantages, there are certain sources of error that can affect the casts' reliability. Although modern polymers have improved the quality of casts, there is still some shrinkage. For example, the average shrinking of the polyurethane-based resin (the same one that we used in our experiments) is reported to be 6.8% after one week10. Furthermore, extravasation and changes in the surface and surrounding tissue have been mentioned11. However, these observations have not been made with the resin we used10. Even though combining the fluorescence microsphere technique and vascular corrosion cast is a useful method to describe the anatomy of the vasculature and determine the tissue perfusion in the same model, no simultaneous usage has been reported to our knowledge.

We are the first to combine fluorescence microsphere technique and vascular corrosion casting in an experimental porcine model to determine spinal cord perfusion and visualize ARMA. The ARMAs are branches from segmental intercostal arteries supplying the anterior spinal artery, and vary in number and distribution. 31 somites are formed during embryological development and receive blood from the corresponding segmental arteries through ARMAs, most of which degenerate, and only 4 to 8 of them remain feeding the anterior spinal artery12. They are therefore crucial for supplying adequate blood flow to the anterior two-thirds of the spinal cord and thus motor functions. Our group's recent investigations suggest that ARMAs play a key role in preventing ischemia after cardiovascular surgery interventions13. The Collateral Network Concept introduced by Griepp describes intraspinal vascular networks that can prevent acute ischemic conditions if segmental arteries become occluded14. ARMAs in this case connect the intraspinal collateral system and extraspinal vessels with the anterior spinal artery, thus their number and the maximum distance between them could be an important preoperative risk predictor in aortic surgery15,16. **Figure 1** illustrates the blood supply's schematic to the spinal cord.

**PROTOCOL:**

This study was conducted at the University Medical Center Freiburg, Freiburg, Germany. Institutional Review Board (IRB) approval was obtained before beginning any experiment. The study animals received humane care in compliance with the Guide for the Care and Use of Laboratory Animals and in compliance with the guidelines established by the local German government (Protocol number G 14/39). An experienced veterinarian carried out anesthesia, pain control, perioperative monitoring, and euthanasia.

1. **Preparation for Surgery**
   1. Allow pigs to house in ventilated rooms and fast them 18 h before surgery. Provide water *ad libitum*.
   2. Premedicate the pigs with an intramuscular injection of ketamine (20 mg/kg) and 0.5 mg/kg of body weight (BW) midazolam.
   3. Insert an 18 G intravenous cannula into an ear and deepen anesthesia with propofol (2–4 mg/kg BW) intravenously (i.v.). Carry out orotracheal intubation with a 6.5 Fr tracheal tube. Ensure adequate ventilation and oxygenation by ventilation with a positive end-expiratory pressure (PEEP) of 5 cm H2O, respiratory frequency of 12–14 min-1, and a tidal volume of 8 mL/kg BW.
   4. Maintain anesthesia with isoflurane 1.5–2% in O2/Room Air (FiO2 = 0.6) in combination with fentanyl (5–10 µg/kg/h) and vecuronium (0.2–0.4 mg/kg/h).
   5. Perform electrocardiogram, pulse oximetry, and temperature monitoring. Use vet ointment on eyes to prevent dryness under anesthesia. Carry out adequate pain control with fentanyl (5–10 μg/kg/h) i.v. and monitor heart rate and pain reactions.
   6. Under sterile conditions, dissect free the common carotid artery and external jugular vein carefully using scissors, and cannulate with a 3-French-catheter using the Seldinger technique17. This step is taken to monitor central venous (CVP) and mean arterial pressure (MAP) via pressure transducer and amplifier.
2. **Microsphere Injection** 
   1. While maintaining sterile conditions, carry out a left posterolateral thoracotomy by an incision in the 5/6 intercostal space using a #10 scalpel blade for the initial incision. Open the situs with scissors and fingers. Open the parietal pleura by an incision and anesthetize the intercostal nerves by injecting 1–2 mL mepivacaine (2%, 20–40 mg). Open the situs by introducing a rib spreader.
   2. Dissect the thoracic aorta free using scissors, tweezers, and fingers, and introduce a 3-French-catheter into the aorta to withdraw microsphere reference samples. Connect a three-way-stop-cock for blood sampling.
   3. Open the pericardium using a scissor and insert a 14-G-cannula into the left atrium through the left atrial appendage. Secure the cannula with a 4-0-prolene suture for microsphere injections. Rinse with approximately 10 mL saline to maintain patency for microsphere injection.
   4. Calculate the minimum number of microspheres to be injected using the formula:

Where, N (min)= minimum number of microspheres required for the injection, n = total number of organ pieces, Q (organ)/Q (total) = fraction of total cardiac output supplying the organ of interest.

Note: There should be a minimum number of microspheres in the region of interest to ensure highly accurate measurements18. Here, 2.5 million microspheres were used for the injection.

* 1. Store the vials containing the fluorescent microspheres in a refrigerator at 2–8 °C and protect them from light. Vortex the fluorescence microsphere vials containing 10 mL solution (one million microspheres per mL) for 20 s and place them in a cold ultrasonic water bath for 5 min.

Note: Because the heat generated might damage the microsphere particles, do not leave them in the ultrasonic bath for too long.

* 1. Dilute 2.5 mL (2.5 million) of microspheres with 7.5 mL sodium chloride in a 10-mL plastic syringe.

Note: Carry out injection immediately after aspiration into the syringe. Aggregation of microspheres leads to inaccurate measurements.

* 1. Inject the microsphere solution into the previously introduced left atrial cannula at a steady injection rate lasting 60 s. Inject only in hemodynamically stable pigs to ensure good microsphere distribution in the cardiovascular system and accurate measurements.
  2. Aspirate the reference blood sample through the aortic catheter with a withdrawal pump at a predefined aspiration rate of 4.55 mL/min into a 20-mL syringe.
     1. Start aspiration 15 s before the microsphere injection, and continue for an additional 180 s for a total of 195 s. This step guarantees that all microspheres are “trapped” in the tissue and reference sample, and can be used to calculate blood flow.
     2. Transfer the blood samples into tubes. Rinse the syringe with 5 mL 2% Tween 80 solution and add it to the tube.
  3. Repeat steps 2.5–2.8 with fluorescent microspheres of different colors that to do not exhibit spectral overlap of excitation and emission wavelengths to obtain blood flow at different time points.

Note: The time points can be chosen according to the experimental setup. Up to 7 different microsphere colors can be used in the same model without performing correction calculations19. Adequate postsurgical treatment, including treatment of postsurgical pain and recovery conditions are obligatory for survival strategies and long-term experiments. Do not leave an animal unattended until it has regained sufficient consciousness to maintain sternal recumbency. Do not return an animal that has undergone surgery to the company of other animals until it has fully recovered.

* 1. Perform euthanasia using thiopental (20 mg/kg BW i.v.), potassium (5 mmol/kg BW i.v.), and exsanguination by cutting the inferior vena cava under isoflurane anesthesia.

1. **Vascular Corrosion Casting**
   1. Immediately after sacrifice, place the animals in supine position.
   2. Place a 14-French-catheter in the descending aorta, fix it with a 4-0-prolene suture and flush with 500 mL saline with heparin.
   3. Mix 50 mg blue vascular casting pigment in 50 g casting resin until a dark blue solution is obtained. Mix the dilution solution (74.1 mL ethanol, 10 mL 2-propanol, and distilled water in 100 mL solution) and 5 g hardener into the resin. Adjust the amount of casting material and solvent needed for injection depending on the experimental setup.

Note: Ethylmethylketone or dichloromethane can also be used as a dilution solution. A dilution of up to 40% is recommended.

* 1. Draw the prepared casting material into a 50-mL plastic syringe and immediately inject it manually with high pressure into the aortic catheter.

Note: The use of an injection apparatus enables pressure monitoring. A physiological pressure of 90–120 mmHg is recommended.

3.4.1 During injection, maintain high pressure by closing the catheter manually.Perform adequate suction of casting material through the inferior vena cava vein. After the injection, adjust the operating table for a better distribution into the organ of interest.

1. **Autopsy**

Note: Autopsy is performed the day after the vascular corrosion casting procedure. Store the pigs in a freezer overnight at approximately −10 °C.

* 1. Place the animal in prone position and make a longitudinal incision above the dorsal spine processes. Carryout a midline incision from the cervical region to the sacrum using a #10 scalpel blade.
  2. Dissect the paraspinal muscles off the vertebral column and expose the spinal cord via laminectomies using a bone Rongeur.
  3. After removing fatty tissue in the spinal canal using an anatomical tweezer, count the anterior radiculomedullary arteries from segments T1–T13. Identify the segments through the origins of the spinal nerves.
  4. Dissect the spinal cord at each segment for blood flow analysis using a disposable microtome blade, and put the tissue in 15-mL polypropylene tubes. Perform the dissection in the middle of two consecutive spinal nerves. Do not use polyethylene tubes because the digesting solution used in the tissue processing will also digest the tubes.
  5. Expose the left and right kidneys taking a posterior surgical approach between segment T12 and the iliac crest using a scalpel and scissors. Deepen the incision through the latissimus dorsi muscle, and remove fat and parts of the lumbodorsal facia with a tweezer until reaching the renal fossa.
  6. After the incision into the renal fascia with a scissor, dissect the kidneys free using a scissor and fingers, and remove. Perform this step after removing the paraspinal muscles (step 4.2). Dissect the outer renal cortical part of the left and right kidneys using a #11 scalpel, put them into the tubes for blood flow analysis, and store them in the dark at room temperature.

Note: Perform this step to validate microsphere distribution and reproducibility of blood flow analysis due to the simultaneous usage of casting material in the same tissue.

1. **Tissue Processing**

Note: Blood and tissue samples are processed via a modified sedimentation technique for lipid-rich tissues20.

* 1. Allow the samples to rest for 2 weeks in the dark at room temperature (18–22 °C) for autolysis to occur. The samples need not be stored in solution.
  2. After 2 weeks, place 7 mL of 2.3 M KOH with 0.5% Tween 80 into each tube. Vortex for 20 s, and place in a 50 °C water bath for 48 h.
  3. After 48 h, centrifuge at 2,000 x g for 20 min at 20 °C; the microspheres are pelleted at this step. Remove the supernatant until there is a volume of 1 mL.
  4. Next, add 7 mL of Triton X-100 and vortex again. Centrifuge at 2,000 x g for 20 min at 20 °C and discard the supernatant until a volume of approximately 1 mL is obtained.
  5. To neutralize KOH, add 7 mL of dilute buffer (5.88 g K2HPO4 in 200 mL distilled water and 22.9 g K2HPO4 in 800 mL distilled water; combine the solutions) and vortex the tubes.
  6. Following the next centrifugation at 2,000 x g for 20 min at 20 °C, remove all but approximately 150 μL of the supernatant.

Note: This step is crucial. Execute this step very carefully to minimize microsphere loss.

* 1. Finally, add exactly 3 mL of 2-ethoxyethylacetate and allow the tubes to rest for 5 days in the dark at room temperature. This step will release the fluorescent dyes from the microsphere particles.

Note: An exact volume of 2-ethoxyethylacetate is crucial because the fluorescence-intensity measurements depend on the concentration. The tube should be placed in the dark, because the fluorescent dyes are no longer bound to the particles and the fluorescence intensity will weaken due to light exposure (“quenching”).

* 1. After the last centrifugation step at 2,000 x g for 20 min at 20 °C, take out the supernatant and measure the fluorescence intensity in the spectrometer.

Note: A less time-consuming wavelength program can be used to take repeated measurements at different excitation and emission wavelengths according to the microsphere colors used in the experiment. Excitation (Ex) and Emission (Em) wavelength of red, green, and yellow fluorescent microspheres:Red (Ex/Em), green (Ex/Em), yellow (Ex/Em) **=** 568/595, 455/482, 508/538, respectively.

* 1. Calculate the regional blood flow (mL/min/g) using the following formula:

With RBF: regional blood flow; Ft: fluorescence intensity of tissue sample; Fref: fluorescence intensity of reference sample; R: withdrawal rate of pump; g: tissue weight in grams.

**REPRESENTATIVE RESULTS:**

**Blood Flow Analysis:**

We observed no alterations in the blood-flow analysis results and background fluorescence noise when using corrosion-casting material in the same tissue. To prevent background fluorescence with the combined technique, the microsphere colors and inherent background fluorescence of the casting pigment must not exhibit spectral overlap of their excitation and emission wavelengths. Furthermore, spectral overlap with the solvents used for digesting the tissue must be excluded.

Regional blood flow values are shown in **Figure 2**. Blood flow to the mid-thoracic region in the spinal cord was less pronounced than to the upper thoracic (*p* < 0.05), lower thoracic (*p* < 0.001), and lumbar levels (*p* < 0.05). The absolute blood flow values allow a comparison between different timepoints and regions in in the tissue of interest. Repeated measurements of spinal cord blood flow values are shown in **Figure 3**. We identified no significant differences in spinal cord perfusion at the three timepoints. The microsphere method thus yielded a reproducible blood flow measurement at different timepoints. Regional cortical renal blood flow in the left and right kidneys is shown in **Figure 4**. A strong correlation was detected between blood flow values from the left and right kidneys (r = 0.94, *p* < 0.001). There was no difference in regional renal cortical perfusion among repeated measurements. The high correlation and reproducible blood flow measurements of the kidneys reveal good distribution of microspheres in the cardiovascular system and their high yield in the tissue-digesting process. A strong difference between the kidneys is evidence of a hemodynamically unstable pig during injection, bad pipetting during tissue digesting, or a faulty microsphere injection or withdrawal of the microsphere reference samples.

**Vascular Corrosion Cast:**

ARMAs were well perfused with casting material through their entire length (**Figure 5**). A low penetration of the ARMAs is due to the casting material’s high viscosity or a low injection pressure. A material of low viscosity will penetrate smaller vessels. The anterior spinal artery, however, exhibited some interruptions in the mid-thoracic region. Such interruption is technical due to the viscosity of the casting material that demonstrates less penetration of the anterior spinal arteries of small diameter in the mid-thoracic region. The ARMAs’ number and distribution are shown in **Figure 6**. We counted more left than right ARMAs in all autopsies (*p* < 0.05). Mean number of ARMAs in the pigs was 8 ± 2. The number of ARMAs in the upper thoracic region ranged from 2 to 7 with a mean of 5 ± 1, while in the lower thoracic region they ranged from 0 to 5 with a mean of 3 ± 1 (*p* < 0.001). Selective vascular casting allowed visualizing the distribution of these small vessels of the spinal cord. The technique can be combined with scanning electron microscopy to analyze morphological alterations of small vessels.

**FIGURE LEGENDS:**

**Figure 1: Schematic illustrations of the blood supply to the intraspinal and paraspinal vascular system of the spinal cord.** Branch points of segment arteries connect the paraspinal with the intraspinal system and consecutive intraspinal systems. ARMAs vary in number and distribution and connect the intraspinal and paraspinal system with the anterior spinal arteries. The paraspinal system is the “sleeping reserve” of blood supply activated by arteriogenic stimuli. It serves as a long-term back-up system, as opposed to the intraspinal collateral system, which is the spinal cord’s emergency back-up system as described in reference21. Cervicothoracic and lumbosacral inflows to the spinal cord are parts of the Collateral Network Concept14 (**Illustration 2**) . Watershed = Classical Watershed areas of the poor collateralized mid-thoracic spinal cord at T4/T5 and T8/T922-24. GARMA = great anterior radiculomedullary artery.

**Figure 2: Regional spinal cord blood flows in the upper thoracic (T1–T4), mid-thoracic (T5–T8), lower thoracic (T9–T13), and lumbar (L1–L3) level.** Spinal cord blood flow is less pronounced in the mid-thoracic region. Results are expressed as mean ± SD. Student’s *t*-tests were performed to determine significant differences. *p* < 0.05 was considered as significant.

**Figure 3: Repeated measurements of regional spinal cord blood flow with three different microsphere colors**. Results are expressed as mean ± SD. There is no significant difference in blood flow values between repeated measurements, thus revealing reproducible measurements at different timepoints.

**Figure 4: Repeated measurements of regional cortical renal blood flows (mL/min/g) in the right and left kidneys.** Results are expressed as mean ± SD. A strong correlation (r = 0.94, *p* < 0.001) between the left and right kidneys and reproducible blood flow values indicate good distribution of microspheres in the cardiovascular system.

**Figure 5: Visualizing ARMAs via vascular corrosion casting.** Visualizing the connection between the anterior radiculomedullary arteries and anterior spinal artery via vascular corrosion casting. ARMAs vary in number and distribution and connect intraspinal and extraspinal vessels with the anterior spinal artery. **A** = anterior spinal artery; **B** = anterior radiculomedullary arteries

**Figure 6: Distribution of anterior radiculomedullary arteries**. This graph illustrates all the anterior radiculomedullary arteries identified between T1–T13 in 30 autopsies via vascular corrosion casting. The highest prevalence of left and right ARMAs was found at level T4.

**DISCUSSION:**

We are the first to have combined the fluorescence microsphere technique and vascular corrosion cast in this feasibility study to visualize spinal cord vasculature and determine spinal cord blood flow at the same time.

The spinal cord’s thoracic region has some important features that must be considered in cardiovascular surgery. The anterior spinal artery’s supply of blood through the anterior radiculomedullary arteries leaves watershed areas with decreased blood flow next to the regions in which extraspinal and intraspinal vessels overlap22. The spinal cord’s mid-thoracic region in this case has classic watershed areas vulnerable to ischemic damage around segments T4/T5 and T8/T923–25. Furthermore, the thoracic region reveals the largest space between the ARMAs, and collateral blood flow in this section is reportedly low12,26. The risk for spinal cord ischemia therefore rises when intercostal arteries are occluded, because the collateral system is incapable of providing sufficient blood flow to this area27. Furthermore, the anterior spinal artery is reported to be narrowest in the mid-thoracic region, increasing the risk for infarction in this area.28 The casting material we used penetrated the anterior spinal artery in the mid-thoracic area the least, thus verifying previous findings. The interruptions in our experiments were technical in nature due to the anterior spinal artery’s small diameter in the mid-thoracic region and due to the casting material’s viscosity. In one study, we carried out a simulated “frozen elephant trunk procedure” (FET) by occluding thoracic segment arteries and interrupting collateral inflow into the epidural arcades to investigate histological changes in the thoracic region13. We found out that the 3 h postoperative observation of ischemia was too short to permit the observance of any histological tissue changes. Further long-term experiments could help us better understand the findings previously mentioned.

This study supports the existence of a constant anterior radiculomedullary artery, referred to as the “Artery of von Haller “ at level T4, as opposed to the “Artery of Adamkiewicz”, which often originates between T8–L329,30. This fact should be considered in aortic surgery when segmental arteries in this area are occluded because of the watershed zone downstream of this region23,31. Furthermore, the upper thoracic region has more ARMAs than the mid-thoracic and lower thoracic segments. These findings support the theory of a higher ischemia risk in these regions, as other studies have documented23,24,30,32,33. The regression of ARMAs has been described as being prominent in the caudal region, where the Artery of Adamkiewicz often remains as the largest ARMA27,29,34.

The combined method applied in this study was reproducible in blood flow analyses, although the vascular corrosion cast had been used in the same tissue. The blood flow values we measured in the pig resemble those described before35. The number and distribution of ARMAs in the pig resemble the values documented in humans30. Krucker *et al.* reported some background fluorescence of casting material, but we detected no spectral overlaps with the microsphere colors used in our experiment10. However, blue microspheres are not recommended, as background fluorescence noise has been reported when using the digesting solution to release the microsphere dyes from the particles and blue pigment for vascular corrosion cast5. This combined technique has several limitations that should be addressed. The microsphere method is prone to errors, which can influence the blood flow values calculated. The injection of microspheres in hemodynamically unstable pigs leads to poor distribution of microspheres in the cardiovascular system and therefore inaccurate blood flow values. Furthermore, the reference sample needs to be withdrawn at a steady withdrawal rate for blood flow calculation. Any irregularities in the withdrawal pump lead to inaccurate blood flow calculations. The time-consuming processing of the samples is an important limitation, as each process step can lead to inaccurate blood flow calculations. However, an internal standard can be used with a predefined number of microspheres colors that are not used in the experiments before beginning processing. Low extraction rates of the internal standard can be due to faulty pipetting and an inaccurate digesting-solution volume (step 5.7). However, employing the sedimentation technique enables samples to be processed in one tube, minimizing the loss of microsphere particles20. Finally, the microsphere colors used in the experiment must not exhibit spectral overlap with the vascular casing pigment, the tissue of interest, or the solutions used to process the samples. We recommended making “test samples” with tissue and digesting solution without microsphere particles to measure the tissue’s background fluorescence.

Improvements in perioperative risk management associated with thoracoabdominal aneurysm repair have significantly reduced the incidence of spinal cord ischemia. Cerebrospinal fluid drainage, neuromonitoring using somatosensory-evoked potentials (SSEPs) and motor evoked potentials (MEPs), monitoring of spinal cord perfusion pressure, distal aortic perfusion, and the preoperative visualization of collateral blood flow and ARMAs are important factors for the improving spinal cord risk management. However, preoperative risk management via magnet resonance angiography (MRA) tends to focus on just one ARMA, the great anterior radiculomedullary artery (GARMA). Our group’s recent investigation found that the distance between ARMAs in the thoracic region plays a key role in neurological outcomes after the FET procedure13. A large distance between ARMAs led to insufficient reactive hyperemia after acute ischemic settings. Furthermore, we discovered that the number of ARMAs correlates with the decrease in spinal cord vascular resistance and therefore reactive hyperemia after ischemic conditions (unpublished data). Physiologically, we detected no significant correlation between the number of ARMAs and spinal cord blood flow. ARMAs seem to be the collateral means of providing rapid and sufficient reactive hyperemia when the spinal cord is affected by ischemia. Preoperative visualization of the number and distribution of ARMAs and the collateral pathways could therefore function as an important preoperative risk predictor. In this case assessing the spinal cord blood flow and vasculature is essential for determining the risk. This combined method can be used for preclinical work to investigate tissue blood flow and vasculature. It enables the investigation of absolute blood flow at different time points, but not real-time measurements. Intra-arterial catheter angiography makes highly detailed images to visualize collateral pathways and feeding vessels possible36. However, it is an invasive method associated with the risk for iatrogenic paraplegia itself. Furthermore, it is incapable of visualizing all collateral pathways and ARMAs simultaneously, making more sessions necessary, thus raising the risk for iatrogenic paraplegia37,38. Non-invasive imaging of the GARMA via computer tomography and MRA has improved recently39–41. The assessment of collateral pathways with MRA allowed the assessment of important relations between collateral pathways and spinal cord functions. Backes *et al.* found a significant correlation between the existence of collateral pathways visualized with MRA and a negative predictive value of spinal cord function after cross-clamping in the corresponding aortic area42. Further research on collateral pathways and their visualization could help us create individual risk algorithms preoperatively.

We postulate that the combination of fluorescence microsphere technique and vascular corrosion cast can be used in the same tissue to analyze the vascular system and hemodynamics. Furthermore, we call for more research on the role of the anterior radiculomedullary arteries and intraspinal collateral system to lower the rate of spinal cord ischemia after cardiovascular interventions.

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**DISCLOSURES:**

The authors have no financial or personal relationship to disclose that would create a conflict of interest or bias.

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