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Merging Ion Concentration Polarization between Juxtaposed Ion Exchange Membranes for Blocking Propagation of the Polarization Zone

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Abstract:	<p>Ion concentration polarization (ICP) phenomenon is one of the most prevailing methods to preconcentrate low-abundance biological samples. The ICP induces a noninvasive region for charged biomolecules (i.e. ion depletion zone), and we can preconcentrate the targets on this region boundary. Despite the high preconcentration performances with the ICP, it is difficult to find operating conditions of non-propagating ion depletion zones. To overcome this narrow operating window, recently we developed a new platform for spatiotemporally fixed preconcentration. Unlike preceding methods of only using the ion depletion, this platform also utilizes the opposite polarity of the ICP (i.e. ion enrichment) to stop the propagation of the ion depletion zone. By confronting the enrichment zone with the depletion zone, the two zones merge together and stop. In this paper, we describe a detailed experimental protocol to build this spatiotemporally defined ICP platform, and characterize preconcentration dynamics of the new platform by comparing with that of the conventional device. Qualitative ion concentration profiles and current-time responses successfully capture the different dynamics between the merged ICP and the stand-alone ICP. In contrast to the conventional one that can fix the preconcentration location at only ~5V, the new platform can produce a target-condensed plug at a specific location in the broad ranges of operating conditions: voltage (0.5-100 V), ionic strength (1-100 mM), and pH (3.7-10.3).</p>
Author Comments:	Please find the attached cover letter and the response to the editorial review.

Additional Information:	
Question	Response
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To: Jaydev Upponi, Ph.D
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We are hereby submitting a revised manuscript of our rescent submission titled as “Merging Ion Concentration Polarization between Juxtaposed Ion Exchange Membranes for Blocking Propagation of the Polarization Zone” (Manuscript ID: JoVE55313R1). After the editorial and peer reviews, the article was recommended to add detail experimental protocols and refine the wordings. In this letter, we would like to respectfully request you to consider our revised paper for publication in *the Journal of Visualized Experiments*.

As you and the editors recommended, we clarified the raised issues with detailed explanations and new discussions. In this submission, we provided point-by-point responses to both the editorial and peer review comments individually. I would appreciate your careful consideration of our paper.

With Best Regards,
October 10, 2016

A handwritten signature in blue ink, appearing to read 'Rhokyun Kwak', is positioned above the printed name.

Rhokyun Kwak, Ph.D

TITLE:

Merging Ion Concentration Polarization Between Juxtaposed Ion Exchange Membranes to Block the Propagation of the Polarization Zone

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SHORT ABSTRACT:

Protocol for a novel ion concentration polarization (ICP) platform that can stop the propagation of the ICP zone, regardless of the operating conditions is described. This unique ability of the platform lies in the use of merging ion depletion and enrichment, which are two polarities of the ICP phenomenon.

LONG ABSTRACT:

Ion concentration polarization (ICP) phenomenon is one of the most prevailing methods to preconcentrate low-abundance biological samples. The ICP induces a noninvasive region for charged biomolecules (*i.e.*, the ion depletion zone), and targets can be preconcentrated on this region boundary. Despite the high preconcentration performances with ICP, it is difficult to find the operating conditions of non-propagating ion depletion zones. To overcome this narrow operating window, we recently developed a new platform for spatiotemporally fixed preconcentration. Unlike preceding methods that only use ion depletion, this platform also uses the opposite polarity of the ICP (*i.e.*, ion enrichment) to stop the propagation of the ion depletion zone. By confronting the enrichment zone with the depletion zone, the two zones merge together and stop. In this paper, we describe a detailed experimental protocol to build this spatiotemporally defined ICP platform and characterize the preconcentration dynamics of the new platform by comparing them with those of the conventional device. Qualitative ion concentration profiles and current-time responses successfully capture the different dynamics between the merged ICP and the stand-alone ICP. In contrast to the conventional one that can fix the preconcentration location at only ~5 V, the new platform can produce a target-condensed plug at a specific location in the broad ranges of operating conditions: voltage (0.5-100 V), ionic strength (1-100 mM), and pH (3.7-10.3).

INTRODUCTION:

Ion concentration polarization (ICP) refers to a phenomenon that occurs during ion enrichment and ion depletion on a permselective membrane, resulting in an additional potential drop with ion concentration gradients^{1,2}. This concentration gradient is linear, and it becomes steeper as a higher voltage is applied (Ohmic regime) until the ion concentration on the membrane approaches zero (limiting regime). At this diffusion-limited condition, the gradient (and corresponding ion flux) has been known to be maximized/saturated¹. Beyond this conventional understanding, when the voltage (or current) is increased further, an overlimiting current is observed, with flat depletion zones and very sharp concentration gradients at the zone boundary^{1,3}. The flat zone has a very low ion concentration, but surface conduction, electro-osmotic flow (EOF), and/or electro-osmotic instability promote ion flux and induce an overlimiting current³⁻⁵. Interestingly, the flat depletion zone serves as an electrostatic barrier, which filters out⁶⁻⁹ and/or preconcentrates targets^{10,11}. Since there is an insufficient amount of ions to screen the surface charges of charged particles (for satisfying electroneutrality), the particles cannot pass through this depletion zone and therefore line up at its boundary. This nonlinear ICP effect is a generic phenomenon in various types of membranes¹⁰⁻¹⁴ and

geometries^{6,15-21}; this is why researchers have been able to develop various types of filtration⁶⁻⁹ and preconcentration^{10,11} devices using the nonlinear ICP.

Even with such high flexibility and robustness, it is still a practical challenge to clarify the operating conditions for the nonlinear ICP devices. The nonlinear regime of the ICP quickly removes cations through a cation exchange membrane, which causes the displacement of anions moving towards the anode. As a result, the flat depletion zone propagates quickly, which is reminiscent of shock propagation²². Mani *et al.* called this dynamic the deionization (or depletion) shock²³. To preconcentrate targets at a designated sensing position, preventing the expansion of the ion depletion zone is necessary, for example, by applying EOF or pressure-driven flow against the zone expansion²⁴. Zangle *et al.*²² clarified the criteria for ICP propagation in a one-dimensional model, and it highly depends on electrophoretic mobility¹⁷, ionic strength¹⁸, pH²⁵, and so on. This indicates that proper operating conditions will be altered according to the sample conditions.

Here, we present detailed design and experimental protocols for a novel ICP platform that preconcentrates targets within a spatiotemporally defined position²⁶. The expansion of the ion depletion zone is blocked by the ion enrichment zone, leaving a stationary preconcentration plug at an assigned position, regardless of the operating time, applied voltage, ionic strength, and pH. This detailed video protocol is intended to show the simplest method to integrate cation exchange membranes into microfluidic devices and to demonstrate the preconcentration performance of the new ICP platform compared to the conventional one.

PROTOCOL:

1. Fabrication of Cation Exchange Membrane-Integrated Microfluidic Chips

1.1) Preparation of silicon masters

1.1.1) Design two kinds of silicon masters: one for patterning a cation exchange resin and the other for building a microchannel with polydimethylsiloxane (PDMS).

Note: The detail geometry will be described in the steps 1.3.1 and 1.4.1.

1.1.2) Fabricate the silicon masters by using either conventional photolithography or deep reactive ion etching²⁷.

1.1.3) Silanize the micropatterned silicon masters with trichlorosilane (~30 μ L) in a vacuum jar for 30 min.

CAUTION: Trichlorosilane is a pyrophoric liquid that is flammable and has an acute toxicity (inhalation, oral ingestion).

1.2) Preparation of PDMS molds

1.2.1) Mix a silicone elastomer base with a curing agent at a 10:1 ratio and place the cup with this uncured PDMS (30-40 mL for replicating microstructures on a 4-in silicon wafer) in a vacuum jar for 30 min to remove the bubbles.

Note: The silicone base contains siloxane oligomers terminating with vinyl groups and a platinum-based catalyst. The curing agent contains crosslinking oligomers that have three silicon-hydride bonds²⁸.

1.2.2) Pour the uncured PDMS on the silicon masters, remove the bubbles with a blower, and cure the PDMS at 80 °C for 2 h in a convection oven.

1.2.3) Detach the cured PDMS from the silicon masters and properly shape the PDMS with a knife (squared shapes, as shown in **Figure 2a-b, iv**).

1.3) Patterning the cation exchange membranes

1.3.1) Cut half of the PDMS mold perpendicularly to the two parallel microchannels and punch holes at the ends of the PDMS channels with a 2.0-mm biopsy punch.

Note: The PDMS mold for patterning the cation selective membrane has two parallel microchannels (width: 100 μm ; height: 50 μm ; interchannel distance: 100 μm ; **Figure 1a**). The original shape of the mold can be imagined by mirroring the sliced mold along the cutting line. L-shaped microchannels are recommended for punching the two holes without overlapping.

1.3.2) Clean a glass slide and the PDMS mold with tape and a blower and put the mold onto the glass slide to create reversible attachment between them.

1.3.3) According to the microflow patterning technique²⁹, release ~10 μL of a cation exchange resin at the open end of the channel that was sliced in step 1.3.1 (**Figure 1b**). Place the syringe head on the punched holes and pull the plunger (black arrows in **Figure 1b**); a gentle negative pressure will pull the cation exchange resin, and the resin will fill the two channels.

Note: It is recommended that the height of the microchannel is greater than 15 μm , because the high viscosity of the resin requires high pressure to fill the channels. On the other hand, it is better that the height does not exceed 100 μm , because the patterned ion selective membrane will become thicker than 1 μm ; such a thick membrane may create a gap between the membrane and the PDMS channel¹³.

1.3.4) Detach the PDMS mold without touching the patterned resin and place the glass slide on the heater at 95 °C for 5 min to evaporate the solvent in the resin.

Note: The thickness of the patterned membrane is usually less than < 1 μm . The mold is gently detached by hinging the mold to the open-ended side (dotted line and arrow in **Figure 1b**). It is best to detach the mold less than 1 min after filling the resin. If the mold is detached a few minutes later, thicker membranes could be obtained, but they would have a concave shape due to the capillary effect.

1.3.5) Peel off the unnecessary part of the patterned membrane with a razor blade, making two separated line-patterns (**Figure 1c**).

Note: The cation exchange material used here has perfluorinated groups, meaning the pattern is not strongly bonded to the glass. Therefore, the simple blading method can easily remove the unnecessary part of the membrane.

1.4) Integration of the microchannel and the membrane-patterned substrate

1.4.1) Punch two holes at the ends of microchannels and another two holes where the membrane patterns will be located after bonding the PDMS channel to the membrane-patterned substrate fabricated in step 1.3.

Note: The PDMS microchannel has one channel (width: 50-100 μm ; height: 10 μm), but it is bonded to the ends of the neighboring channel (**Figure 1d**).

1.4.2) Bond the PDMS microchannel to the membrane-patterned substrate immediately after oxygen plasma treatment for 40 s at 100 W and 50 mTorr.

Note: Place the patterned membrane perpendicularly on the middle of the microchannel.

2. ICP Preconcentration

2.1) Preparation for the experiment

2.1.1) Prepare various test solutions, including 1-100 mM KCl, 1 mM NaCl (pH \sim 7), the mixture of 1 mM NaCl and 0.2 mM HCl (pH \sim 3.7), the mixture of 1 mM NaCl and 0.2 mM NaOH (pH \sim 10.3), and 1X phosphate-buffered saline.

2.1.2) Add a negatively charged fluorescent dye (\sim 1.55 μM) to the test solutions.

Note: The concentration of the added dye should be much lower than that of the salt ions ($< 10 \mu\text{M}$) so that the charged dyes do not contribute to an electrical current^{30,31}.

2.1.3) Load the sample solution in one reservoir of the channel and apply negative pressure to the other reservoir to fill the channel with the solution. Connect the two reservoirs hydrodynamically by releasing a large droplet to eliminate the pressure gradient along the channel (**Figure 2a**).

2.1.4) Fill the two reservoirs, which are connected to the cation exchange patterns, with buffer solutions (1 M KCl or 1 M NaCl) using a syringe or a pipet to compensate for the ICP effect in the reservoirs.

2.1.5) Place the wires at the reservoirs, across the two patterned membranes (anode on the left reservoir and cathode on the right), and connect them with a source measurement unit (**Figure 2a**).

2.2) Visualization of the ICP phenomenon and ICP preconcentration

2.2.1) Load the ICP device on an inverted epifluorescence microscope. Apply a voltage (0.5-100 V) and measure the current response with a source measurement unit.

2.2.2) Capture fluorescent images with a charge-coupled device camera and analyze the fluorescent intensity using imaging software³².

REPRESENTATIVE RESULTS:

The schematic fabrication steps of a membrane-integrated microfluidic preconcentrator are shown in **Figure 1**. A detailed description of the fabrication is given in the Protocol. The designs

and device images of the spatiotemporally defined preconcentrator²⁶ are contrasted with those of a conventional preconcentrator¹¹ (**Figure 2**). The ICP phenomenon in the spatiotemporally defined preconcentrator was investigated in terms of current-voltage-time responses and fluorescent intensity profiles (**Figure 3-4**). Similar to the ICP phenomenon with a single-membrane preconcentrator^{3,11}, three different regimes (Ohmic, limiting, and overlimiting) were observed in the current-voltage curve: 0.5-1 V (Ohmic and limiting) and 5 V (overlimiting). However, a nonconventional current recovery was detected in the current-time curve as the ion enrichment and the ion depletion zones merged. Next, the ICP preconcentration was tested at different times and voltages with the spatiotemporally defined preconcentrator (**Figure 5**) and the conventional one-membrane device (**Figure 6**). The preconcentration dynamics were quantified by fluorescence images, current-time responses, and fluorescent intensity graphs over different distances and times. When comparing the two platforms, the new ICP platform shows an advantage in always collecting targets (fluorescent dyes) between the two cation selective membrane patterns. In addition, it was confirmed that the preconcentration plug remains the same in different ionic strengths (1-100 mM NaCl) and pH values (3.7-10.3), verifying the high availability of the merging ICP preconcentrator in wide ranges of operating conditions (**Figure 7**). In **Figure 8**, a 10,000-fold protein preconcentration was also demonstrated.

FIGURE LEGENDS:

Figure 1. Fabrication steps of a cation exchange membrane-integrated microfluidic chip.

After a PDMS mold is filled with a cation exchange resin using the microflow patterning technique (a-c)²⁹, the membrane-patterned glass substrate is bonded with a PDMS microchannel by oxygen plasma treatment (d).

Figure 2. Schematics of the spatiotemporally defined preconcentrator (a) and conventional preconcentrator (b).

(a) In the new platform, between two membrane patterns (i), ion depletion/enrichment zones are developed and merged together with linear (Ohmic and limiting regime; ii) or nonlinear (overlimiting regime; iii) concentration profiles. In all three current regimes, the ion enrichment zone blocks the propagation of the depletion zone and targets (hollow circles; i) are preconcentrated at the interface of the ion depletion and enrichment zones (curved, dotted line; i). The wall of the PDMS channel is negatively charged, and this generates electro-osmotic flow (EOF) between the two cation exchange membranes under an electric field. The EOF continuously delivers targets towards the interface of the depletion and enrichment zones. (b) In the conventional platform, only the ion depletion zone is developed near the membrane with linear (Ohmic and limiting regime; ii) and nonlinear (overlimiting regime; iii) concentration gradients. As the EOF delivers the targets, the preconcentration also occurs at the depletion zone boundary, but this zone (and the preconcentrated plug) moves away from the cation exchange membrane (black arrow; i). It is noted that there is no increase in the ion concentration here without the ion enrichment zone (ii-iii). In (a-b), the device images are shown in (iv). C_0 represents the initial ion concentration. V^+ and G indicate the anode and the cathode, respectively. Reprinted from Reference 26t with permission from The American Chemical Society.

Figure 3. Merged ICP phenomenon between two cation exchange membranes. (a) The current-voltage curve shows three distinct regimes (Ohmic, limiting, and overlimiting). The current response is measured by ramping up the voltage at discrete intervals of 0.25 V every

40 s, which is repeated three times. The error bar indicates the standard deviation of the current responses. (b, c) In the three regimes, fluorescence images (b) and intensity profiles along A-A' at the middle of the channel (c) were obtained. Yellow, dotted boxes indicate the locations of the cation selective membranes. 1 mM KCl solution with a 1.55 μM (1 $\mu\text{g/mL}$) negatively charged fluorescent dye was used. Reprinted from Reference 26 with permission from The American Chemical Society.

Figure 4. Transient dynamics of merging ion depletion and enrichment zones. (a, b) In the Ohmic-limiting regimes, the linear concentration gradients grow (< 1 s) from the cation exchange membrane and then overlap together (> 1 s). (c) In the overlmiting regime, the two ICP zones are merged more quickly (< 0.6 s) with the depletion shock (black arrow at 0.2 s). (d-f) The current-time responses show that the current is initially dropped due to the growth of the low-concentration depletion zone, which corresponds to low electrical conductivity. The current drop is then recovered due to a convective transport by vortices confined between two membranes. Reprinted from Referenced 26 with permission from The American Chemical Society.

Figure 5. Spatiotemporally fixed preconcentration at 5, 10, and 20 V. (a-c) Fluorescence images of the merged ICP and the current-time responses (d-f) over time (0-100 s). The yellow, dotted lines indicate the location of the cation exchange membranes. (g) Time-lapse fluorescent intensity profiles are plotted along the microchannel (A-A'). The peak intensities increase as time passes, with fixed locations. (h) The peak intensity fold (*i.e.*, how many times greater than the initial fluorescent intensity). At higher voltages, the faster EOF delivers targets towards the interface of the ion depletion and enrichment zones, so the preconcentration speed increases. A spike at 20 V is induced by the depletion shock (Figure 4c). The fluorescent dyes accumulate on the shock boundary as it pushes the dyes. This initial accumulation is then somewhat dispersed when the depletion shock meets the ion enrichment zone, creating the spike in the peak intensity curve. As can be seen in Figure 4c, at 0.8 s, the peak was wider than it was at 0.4 s. This is probably because the left side of the left Nafion pattern (Figure 2a) was electrically floated, and the accumulated dyes could spread out. Reprinted from Reference 26 with permission from The American Chemical Society.

Figure 6. ICP phenomenon in the conventional ICP preconcentrator at 5, 10, and 20 V. (a-c) Fluorescence images of the ion depletion zone and the current-time response (d-f) over time (0-100 s). The propagation of the depletion zone and the preconcentration plug is clearly visualized in the fluorescence images. Accordingly, the vortices are not confined, so the current recovery does not occur, even in the overlmiting regime. Yellow, dotted lines mark the location of the cation exchange membranes. (g) Time-lapse fluorescent intensity profiles are plotted along the microchannel (A-A'). The peak intensities increase as time passes, but the location moves away from the membrane. (h) Peak intensity fold of the conventional ICP device. In contrast to the merged ICP device (Figure 5h), there is no intensity spike without the confinement of ICP zones, because the fluorescent intensity increased as the dye was preconcentrated. The increase of the peak intensity fold is similar to that of the merged ICP device at the same time (at a given voltage). This indicates that the length of time that the preconcentrated plug is held in place is crucial to the preconcentration performance.

Figure 7. Spatiotemporally defined preconcentration at various ionic strengths (1-100 mM NaCl) and pH values (3.7-10.3). (a) Fluorescence images obtained after 100 s of operation at 50 V. As can be seen, the locations of the preconcentration plugs are still between the two cation exchange membranes (yellow, dotted lines), even though the intensity is weakened under high ionic strength and in a strong acidic or basic solution. (b, c) The location of the peak intensity and its intensity fold (*i.e.*, how many times greater than the initial intensity), mapped under 10, 20, 50, and 100 V. For a single condition (1, 10, 100 mM and/or pH 3.7, 7, and 10), there are four data points corresponding to the four voltage conditions. At higher voltages, there is a higher peak intensity fold in all cases. 100 V was not tested in 1 mM NaCl (pH 7) because the peak intensity already touched the highest values (due to the saturation of the camera) at 50 V. From the peak intensity profile, the peak region is also identified, with 1% below the peak intensity, which is represented by error bars (b, c). A higher voltage and a stronger EOF shift the peak location to the right, with a higher intensity fold and a sharper preconcentration plug. Gray boxes indicate the locations of the cation exchange membranes. The 0 distance (a) represents the origin of the x-axis (b, c), which is on the right edge of the left cation exchange membrane. The origin of the distance is the right edge of the left membrane. Reprinted from Reference 26 with permission from The American Chemical Society.

Figure 8. Demonstration of spatiotemporally fixed protein preconcentration. FITC-albumin (1 $\mu\text{g/mL}$) in 1X phosphate-buffered saline solution was used. 0.1% Tween 20 was also added to prevent nonspecific binding. Since the preconcentration is hardly achieved at a higher ionic strength (Figure 7), we doubled the width of the Nafion pattern (200 μm) and used a narrower PDMS channel (50 μm). In this way, the performance of ICP preconcentration was enhanced by broadening the ion pathway and reducing the absolute amount of ions in the channel. At an applied voltage of 100 V, the peak and averaged fluorescent intensities were traced in the white, dotted box, which is the region between the two cation exchange membranes. Within 10 min of operation, the proteins were preconcentrated up to 10 mg/mL (peak) and ~ 0.1 mg/mL (averaged), indicating 10,000- and 100-fold preconcentrations, respectively. The inset fluorescence images were obtained at 0, 10, and 20 min. In this work, a 20-min operation was enough to preconcentrate the target molecules, so we did not cover longer operating times. Reprinted from Reference 26 with permission from The American Chemical Society.

DISCUSSION:

We have described the fabrication protocol and the performance of a spatiotemporally defined preconcentrator in a range of the applied voltage (0.5-100 V), ionic strength (1-100 mM), and pH (3.7-10.3), achieving a 10,000-fold preconcentration of dyes and protein within 10 min. As like previous ICP devices, the preconcentration performance becomes better at higher voltage and at lower ionic strength. One additional parameter we can consider here is the distance between two cation exchange membranes. If we increase the inter-membrane distance, the electric field decreases under the same applied voltage, resulting in the decrease of the preconcentration speed²⁶.

The microflow patterning technique²⁹ used in this work is a robust method for patterning cation exchange resins, so it has been one of the gold-standard methods for integrating the ion exchange materials into microfluidic systems. Nevertheless, it is necessary to fabricate two juxtaposed cation exchange membranes with a short intermembrane distance (smaller than few hundred

micrometers). In steps 1.3.3-1.3.4, the cation exchange resin is in a liquid phase. Therefore, the resin in the two microchannels can be collapsed, and the remaining resin drop at the open end of the channels can also flood during the mold detachment (step 1.3.4.). To build two cation exchange membranes with high pattern fidelity, we used the resin with a relatively high viscosity (20% of the cation exchange material in the solvents) and carefully set the detachment process with a designated detaching direction.

Even though the high operating flexibility of this platform was demonstrated, the reader might be concerned about determining the optimal conditions from the wide range within the operating window. One representative trade-off is between the preconcentration speed and the stability of the ICP effect. As can be seen in Figure 5 in Kwak *et al.*²⁶, a high applied voltage (> 50 V) can condense targets quickly; however, this also induces strong vortices in the depletion zone (1 mM / pH 7 in Figure 7a), which decreases the stability of the sample preconcentration. Accordingly, the preconcentration speed becomes difficult to predict³³. In the current stage, we recommend experimental conditions with a relatively low voltage (< 30 V) and ionic strength (< 10 mM) for a stable, predictable, and spatiotemporally fixed preconcentration. This trade-off between the preconcentration speed and the stability of the preconcentrated plug is also related to the sources of the nonlinear ICP (surface conduction, EOF, and electro-osmotic instability). The main source of the nonlinear ICP at a relatively small voltage (< 50 V) is EOF, creating a coherent vortex pair in the depletion zone (**Figure 3b**), which leads to a stable preconcentration. At a relatively high voltage (> 50 V), the main source of the nonlinear ICP is changed to electro-osmotic instability, resulting chaotic multiple vortexes, which decrease the stability of the preconcentration.

Recently, paper-based ICP platforms have been developed by Phan *et al.*³⁴, Gong *et al.*¹⁹, and Han *et al.*²¹. These paper devices with microporous structures can suppress electro-osmotic instability^{4,35} and alleviate the stability issue. However, the sizes of the paper channels are generally about 0.5-5 mm, which is much bigger than a conventional microfluidic channel. This wider paper channel with random fiber networks causes irregular motions in the preconcentrated plugs. This has been inevitable in paper-based ICP preconcentrators, because the minimum feature size of wax patterning and paper cutting (*i.e.*, fabrication methods to build paper channels) is about few hundred micrometers.

The ICP preconcentrator has been used in a wide range of biomicrofluidic platforms for preconcentrating various bio-agents; amplifying the signals of various assays; and detecting targets, such as therapeutic proteins³⁶, peptides³⁷, aptamers¹⁷, and enzymes³⁸. These previous works targeted fluorescence-labeled biomolecules. This is because we cannot specify the exact operating conditions (*i.e.*, voltage and flow rate) to maintain the preconcentration site, so we first need to find the proper conditions for the preconcentrator targets. Departing from previous work, the merged ICP phenomenon allows us to always fix the preconcentrated plugs at a broad range of operating conditions while maintaining the high flexibility of the ICP devices. This indicates that we can now extend the applications of ICP preconcentrators to label-free detection techniques without using visualization instruments and tracers. This unique advantage of the spatiotemporal controllability provides a strong commercial opportunity to integrate the ICP device with generic benchtop platforms, such as polymerase chain reaction machines and mass spectrometers.

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DISCLOSURE:

The authors have nothing to disclose.

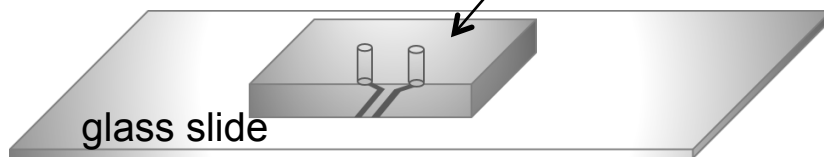
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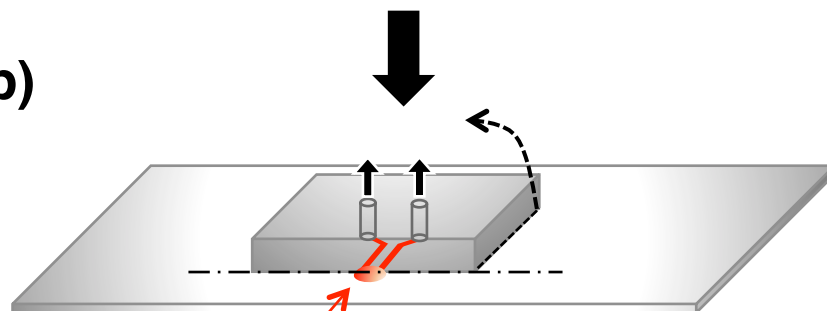
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a) PDMS mold



b)



Nafion resin

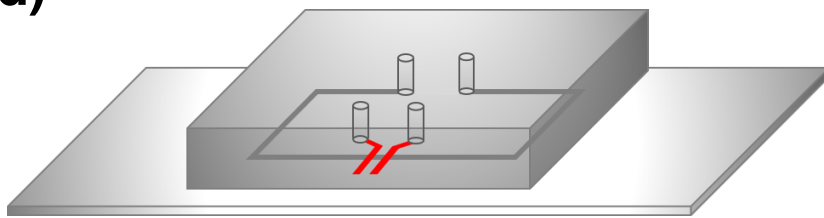
Detach the PDMS mold
Peel off the Nafion residue

c)

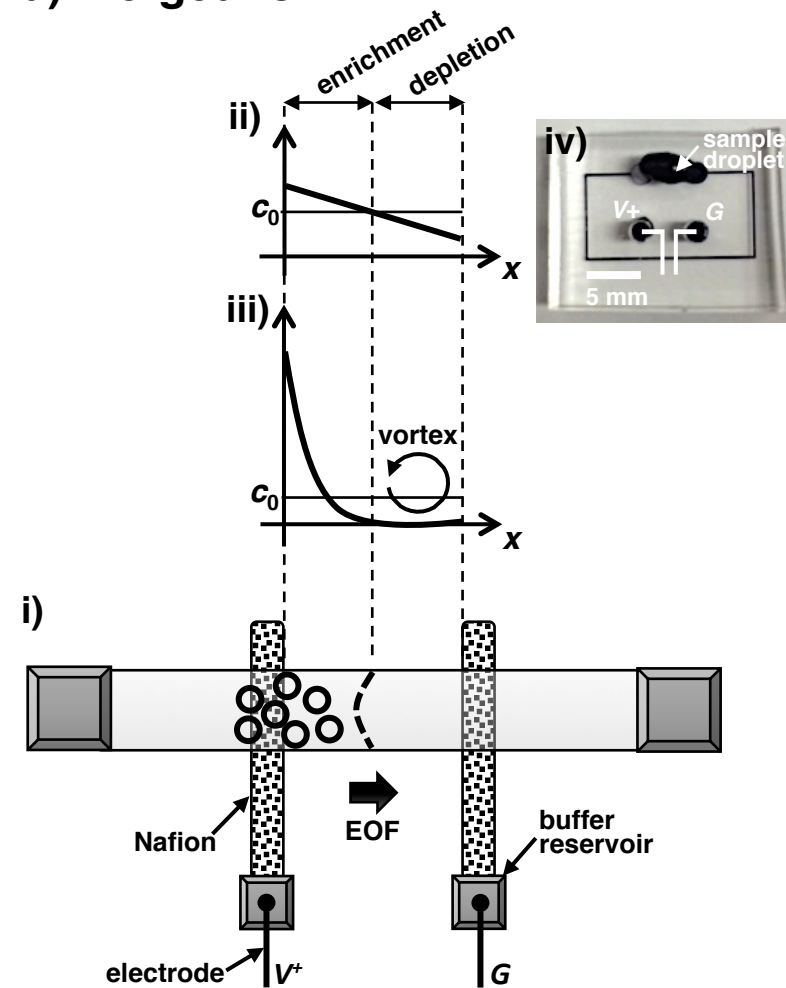


Bond the PDMS channel

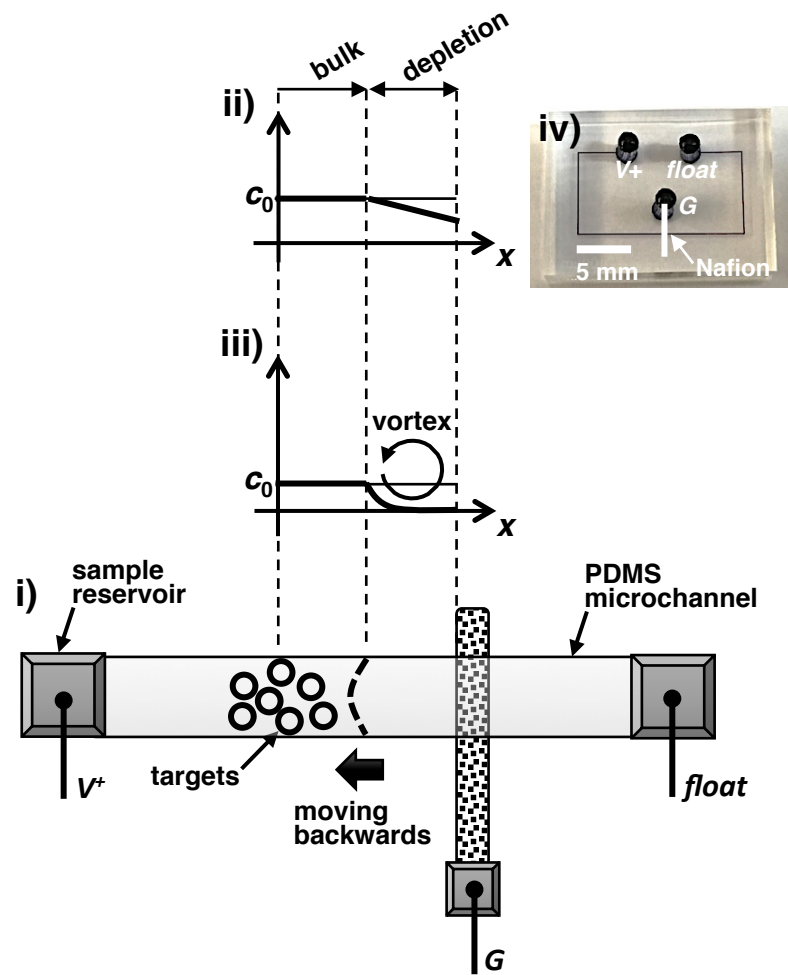
d)



a) merged ICP



b) conventional ICP



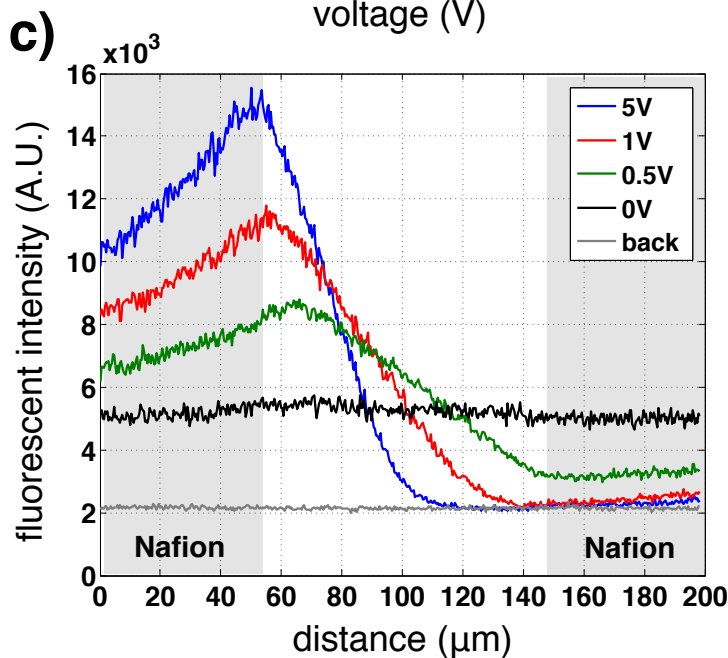
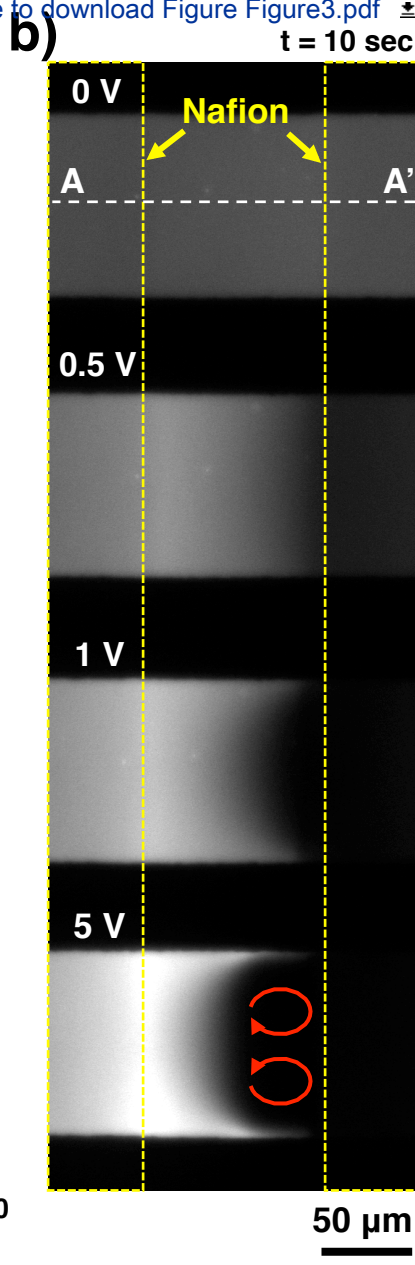
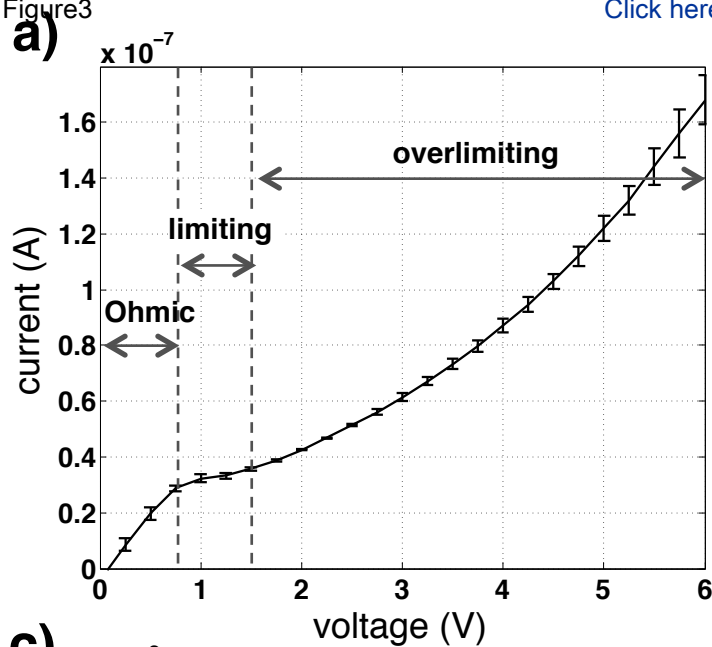
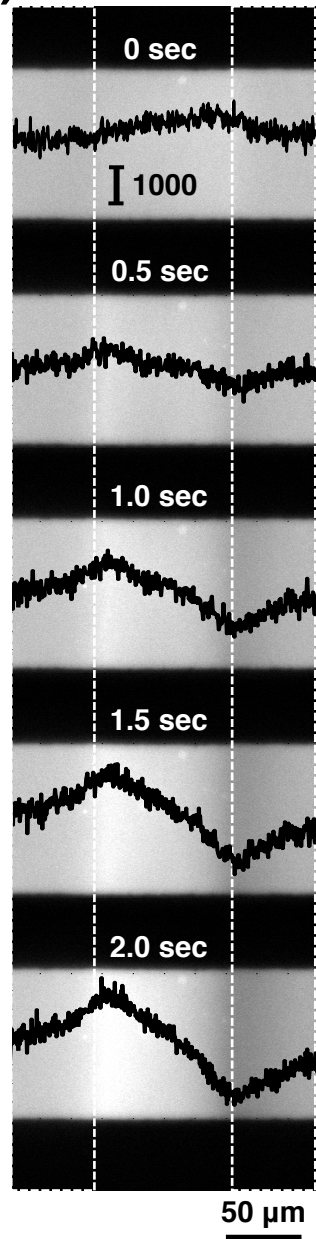
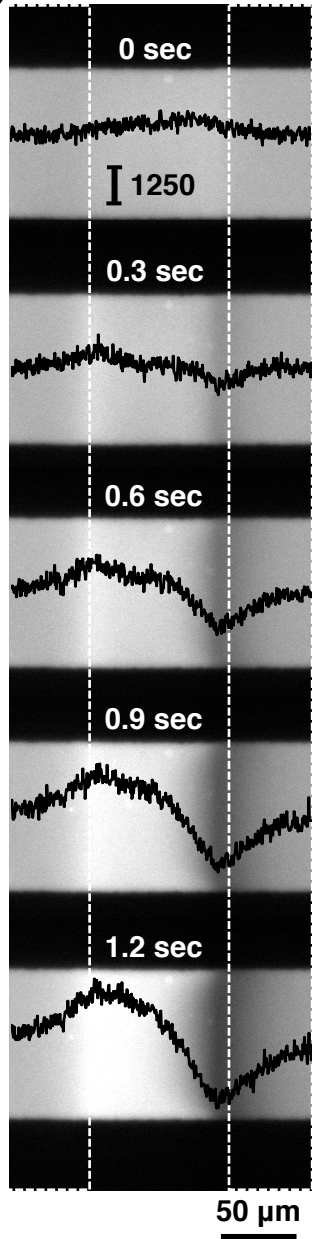


Figure 4

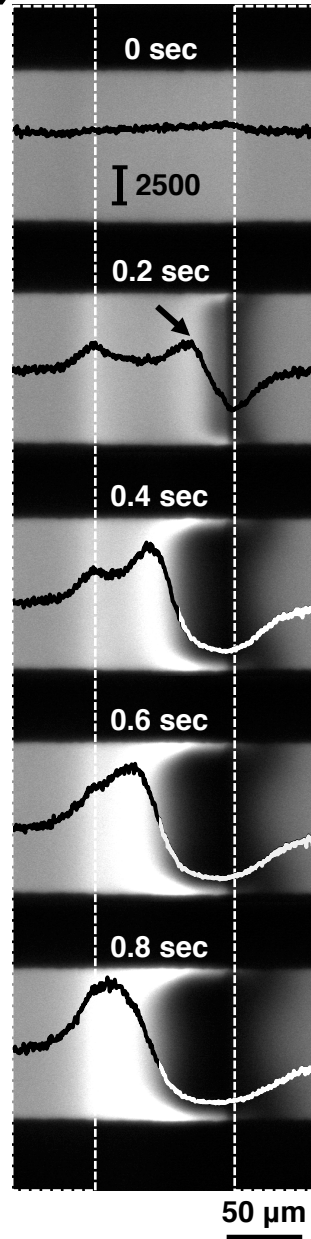
a) 0.5 V



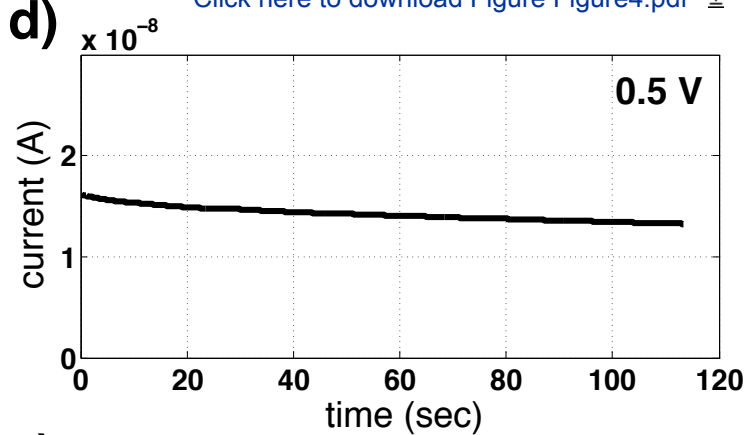
b) 1 V



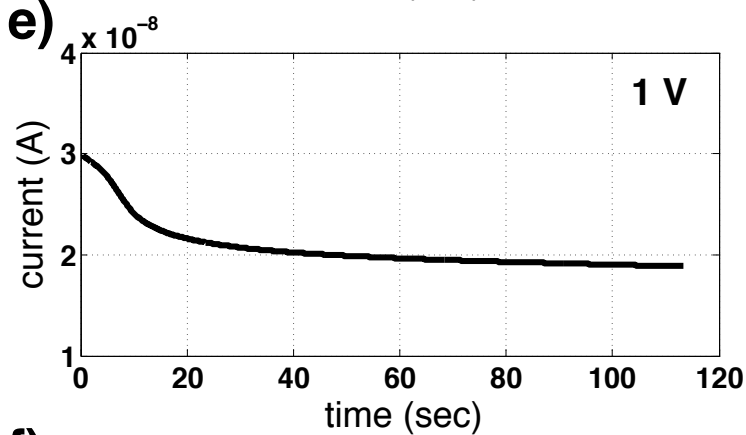
c) 5 V



d)



e)



f)

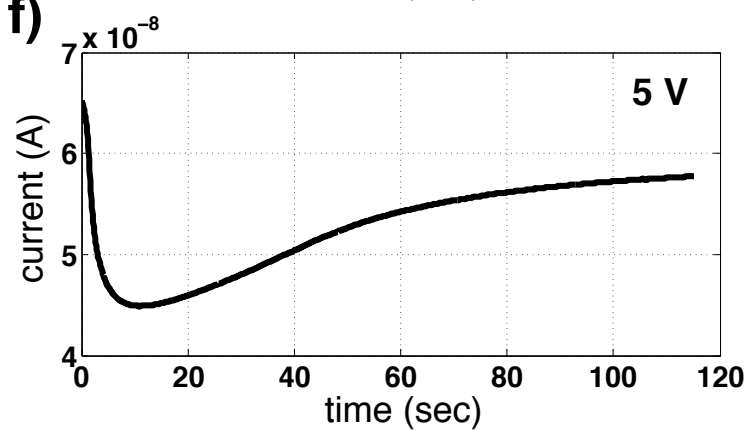
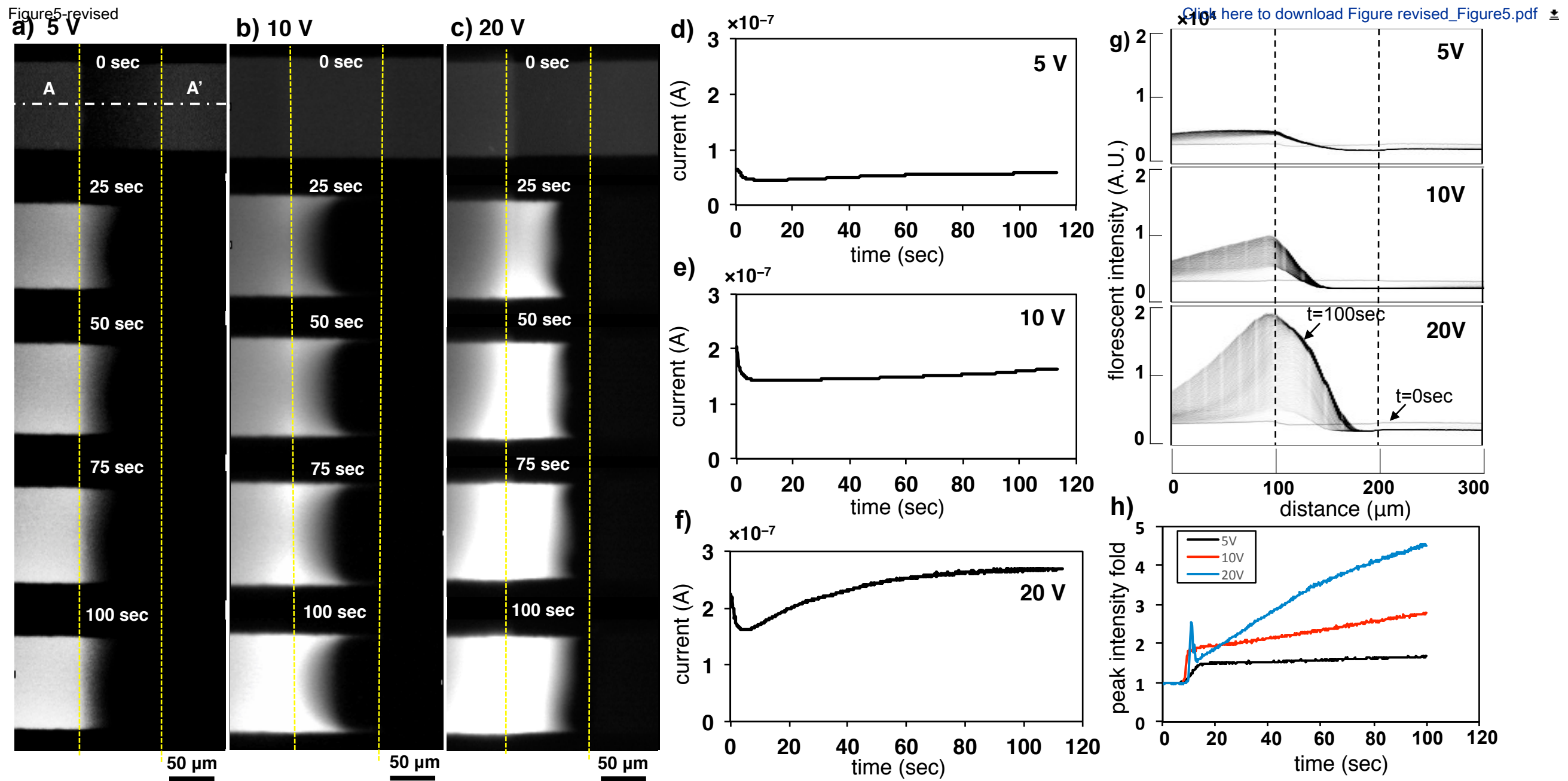
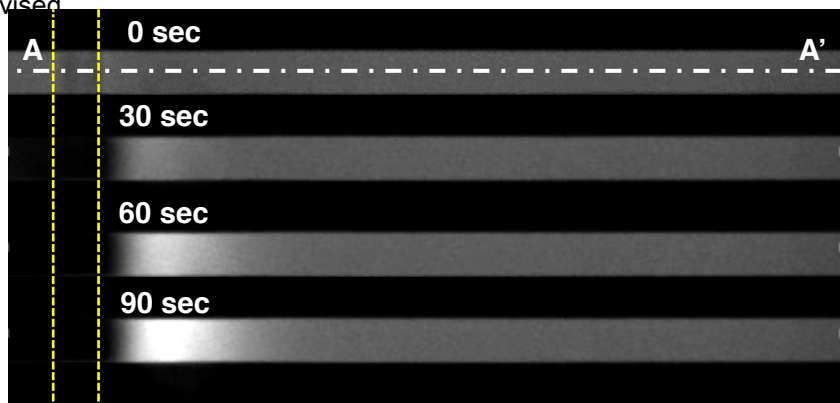


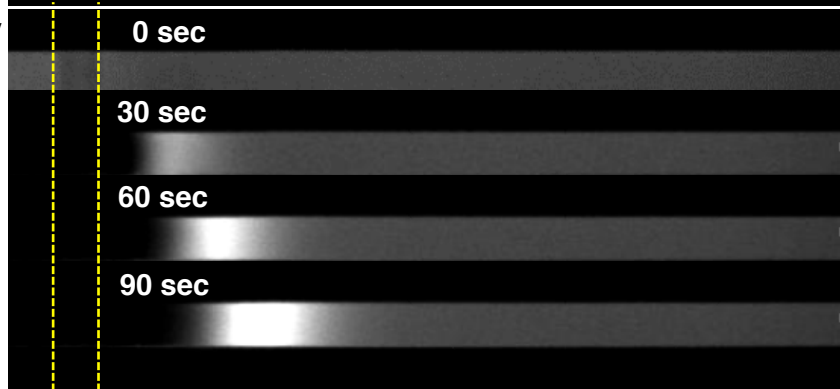
Figure 5-revised



a) 5 V



b) 10 V



c) 20 V

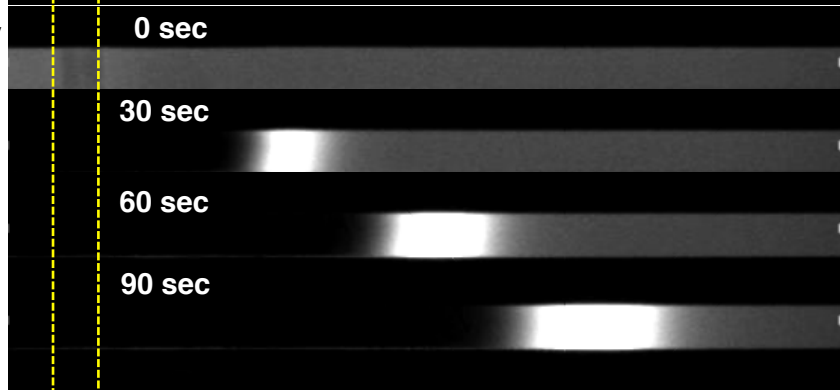
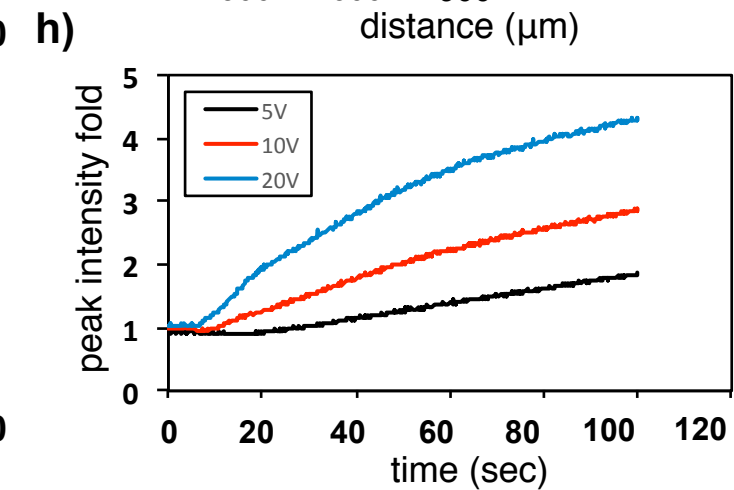
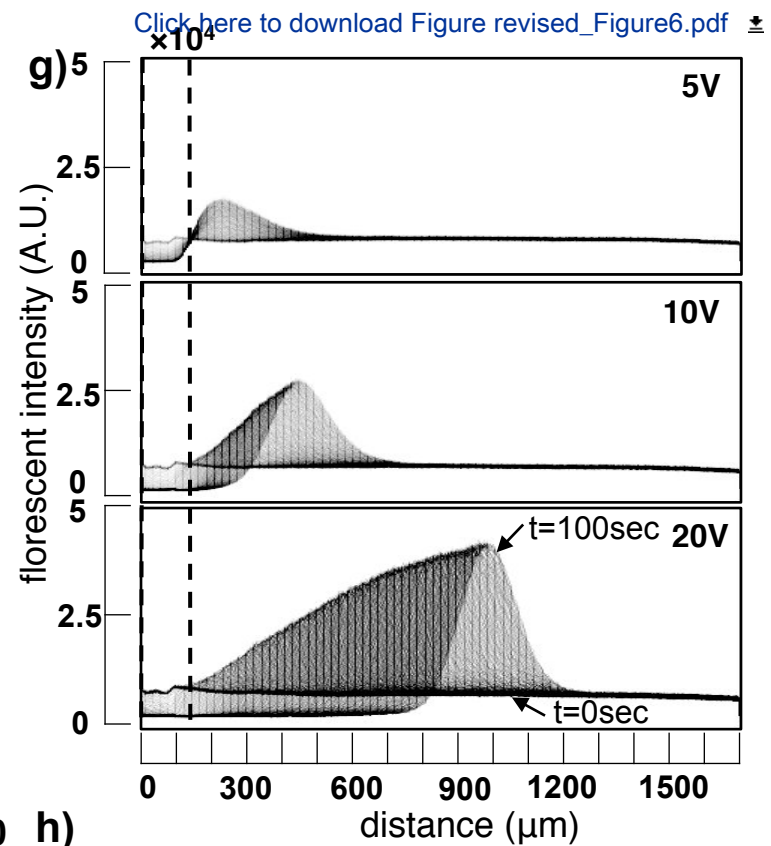
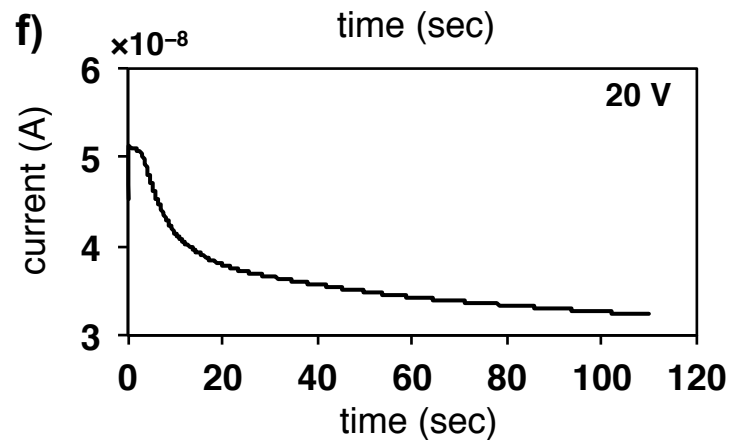
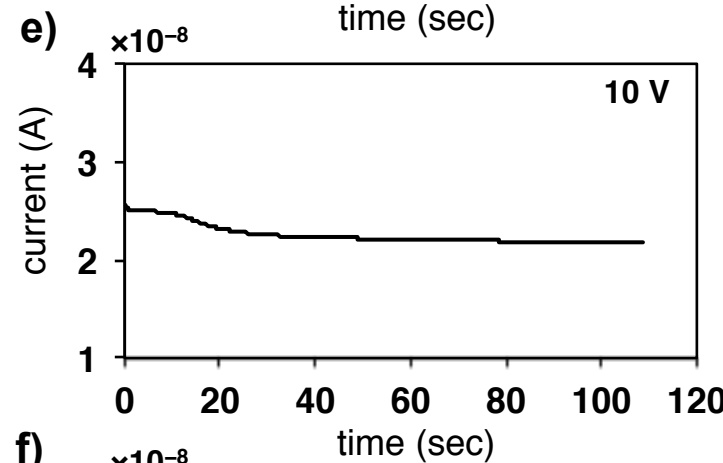
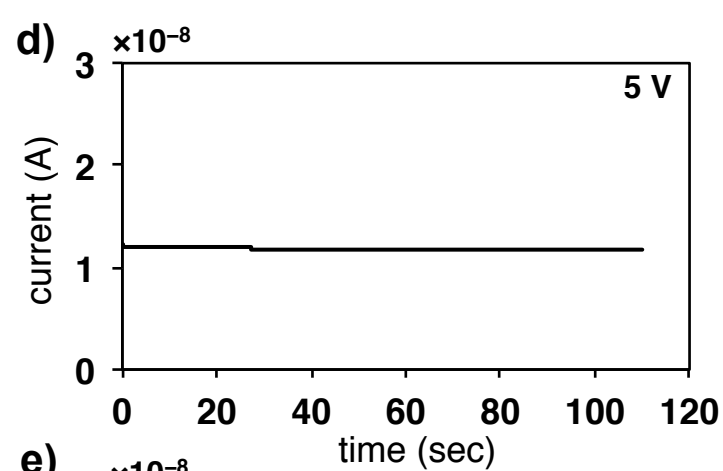
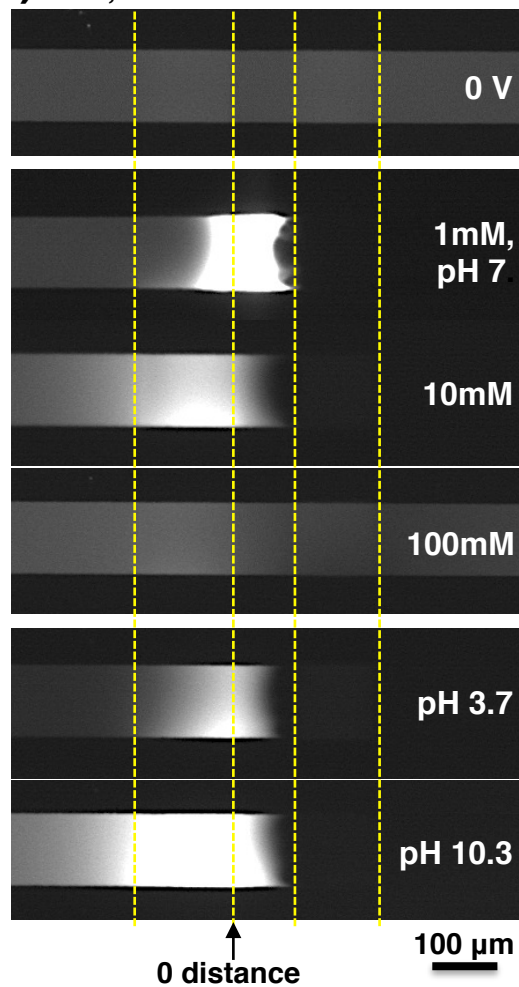
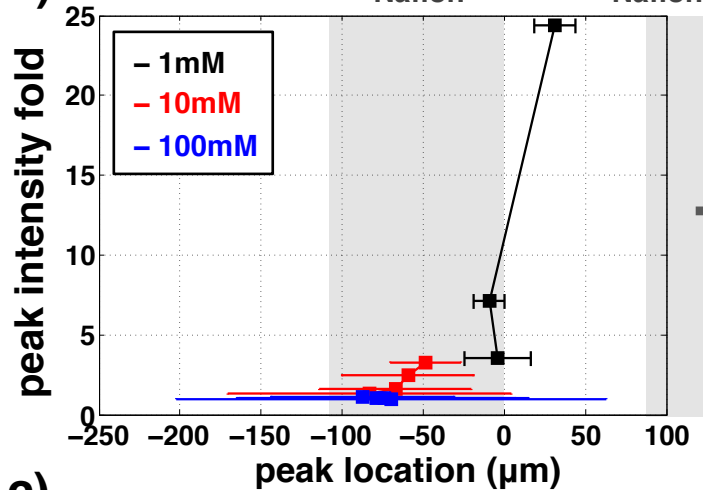
100 μm 

Figure 7

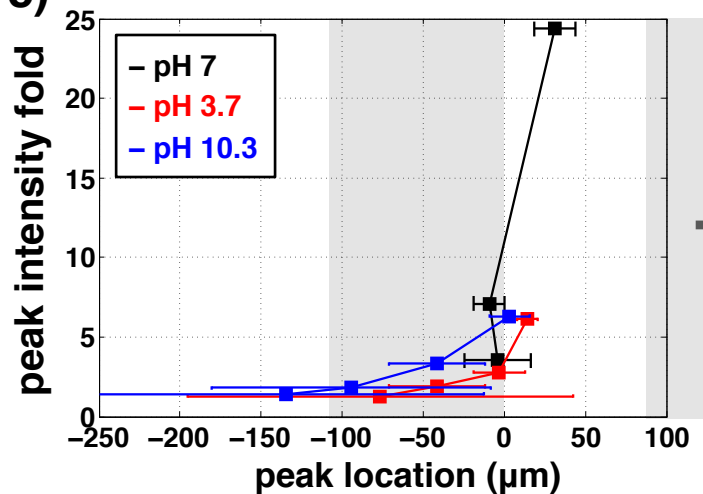
a) 50 V, 100 sec

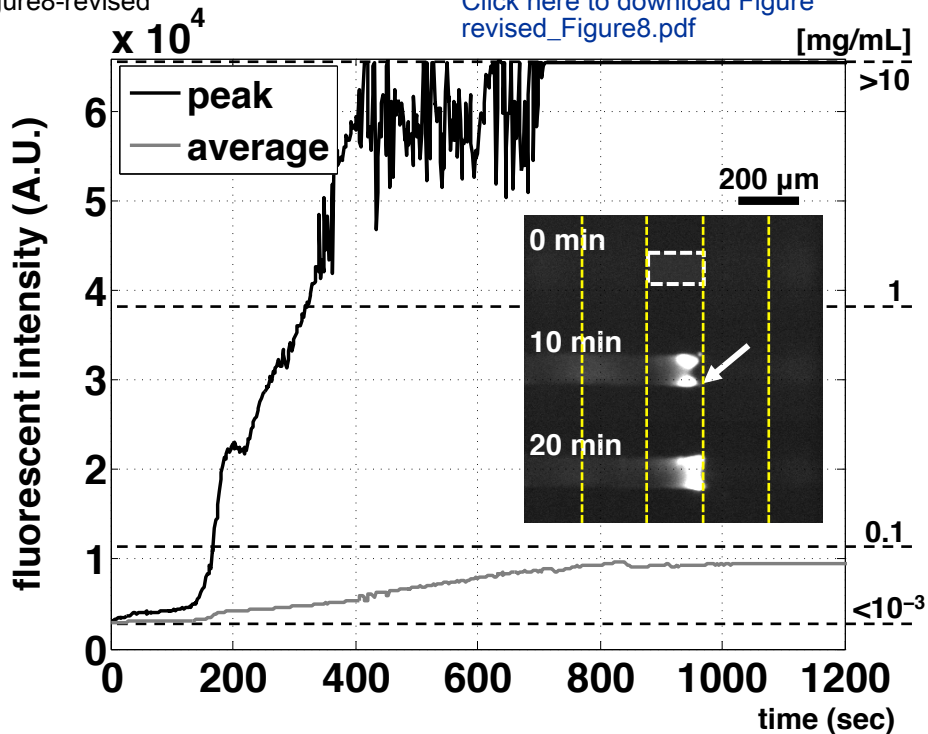


b)



c)





Name of Material/ Equipment	Company	Catalog Number	Comments/Description
Sylgard 184 Silicone Elastomer kit	Dow Corning		
Trichlorosilane	Sigma Aldrich	175552	Highly toxic
Nafion perfluorinated resin, 20 wt%	Sigma Aldrich	527122	
Sodium chloride	Sigma Aldrich	71394	
Potassium chloride	Sigma Aldrich	60121	
Alexa Fluor 488 carboxylic acid, succinyl	Invitrogen	A20000	
Isothiocyanate-conjugated albumin	Sigma Aldrich	A9771	
Phosphate buffer saline, 1X	Wengene	LB004-02	
Tween 20	Sigma Aldrich	P1379	
Epifluorescence microscope	Olympus	IX-71	
Charged-coupled device camera	Hamamtsu Co.	ImageEM X2	
Source measurement unit	Keithley Instruments	2635A	
Covance-MP	Femto Science		



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Response to Editorial Comments (JoVE55313R1)

Merging Ion Concentration Polarization between Juxtaposed Ion Exchange Membranes for Blocking Propagation of the Polarization Zone

by Minyoung Kim, Hyunjoon Rhee, Ji Yoon Kang, Tae Song Kim, and Rhokyun Kwak

1. Please proofread the manuscript for numerous minor grammatical and spelling errors (most occur in the procedures section). Examples include, but are not limited to:

-Line 78: “ion depletion near a permselective membrane”

-1.1.2: “Both etching the silicon wafer by deep reactive ion etching and piling the microstructures on the wafer with a photoresist are available.” – odd phrasing

-1.2.3: “in order to attach on a glass slide”

-1.3.2. “Then they are attached”. Sentences rarely need to begin with “then”.

- 2. “Experiment of ICP Preconcentration” should just be ICP Preconcentration, or ICP Preconcentration Experiment.

-2.1.5: “anode on the left reservoir”

Response 1: We reviewed the manuscript thoroughly, and corrected grammatical and spelling errors.

2. Detail is needed for step 1.2.1: “place the cup with an uncured PDMS in a vacuum jar” - how much PDMS?

Response 2: 30-40 ml of the uncured PDMS is required to replicate microstructures on a 4-inch silicon wafer. We added this detail in the step 1.2.1.

3. Discussion: Please discuss further applications of the demonstrated technique, and it's advantages over any other similar methods.

Response 3: ICP preconcentrator has been used in the wide range of biomicrofluidic platforms for preconcentrating various bio-agents, amplifying the signals of various assays, and finally detecting the targets such as therapeutic proteins [Ouyang et al., *Anal. Chem.*, 2016, **88**, 9669-9677], peptides [Cheow et al., *Anal. Chem.*, 2014, **86**, 7455-7462], aptamers [Cheow and Han, *Anal. Chem.*, 2011, **83**, 7086-7093], and enzymes [Chen et al., *J. Am. Chem. Soc.* 2011, **133**, 10368-10371]. As one can notice, these previous works targeted fluorescence-labeled biomolecules. This is because that we cannot specify the exact operating condition (e.g. voltage and flow rate) to maintain the preconcentration site, so we need to find the proper condition to preconcentrator targets first.

Starting from the same motivation of our work, Yossifon et al. [*Phys. Rev. E*, 2010, **81**, 046301] suggested the device that can focus the electric field geometrically with nanoslits. Although this method successfully slowed down the propagation of the depletion zone, it could not suppress the propagation perfectly, especially at high voltage and long-time operation for preconcentration applications. Senapati et al. and Slouka et al. accumulated nucleic acids in the ion enrichment zones, and directly used an ion exchange membrane as a

sensor[*Biosens. Bioelectron.* 2014, **60**, 92-100; *Talanta* 2015, **145**, 35-42]. This can bypass the problem of the transient depletion zones, but we should hold the membrane material and the sensing spot on the membrane. Therefore, this platform cannot enjoy the enormous modulations of conventional ICP preconcentrators in materials, geometry, and integrations.

Departing from the previous trials, the merged ICP phenomenon allows us to fix the preconcentrated plugs always at broad range of operating conditions, while maintaining the ICP devices' high flexibility. This indicates that now we can extend the applications of ICP preconcentrators for label-free detection techniques without visualization instruments and tracers. This unique advantage on the spatiotemporal controllability would provide a strong commercial opportunity to integrate the ICP device into generic benchtop platforms, such as for polymerase chain reactions and mass spectrometers.

We added this content in DISCUSSION (Page 9).

4. References: Please include DOI for references, where possible.

5. JoVE reference format requires that the DOIs are included, when available, for all references listed in the article. This is helpful for readers to locate the included references and obtain more information. Please note that often DOIs are not listed with PubMed abstracts and as such, may not be properly included when citing directly from PubMed. In these cases, please manually include DOIs in reference information.

Response 4-5: We added the DOI for the references.

6. If your figures and tables are original and not published previously, please ignore this comment. For figures and tables that have been published before, please include phrases such as "Re-print with permission from (reference#)" or "Modified from.." etc. And please send a copy of the re-print permission for JoVE's record keeping purposes.

Response 6: The phrases regarding reprint permission are added in the figure captions. We also attached a copy of the reprint permission in the package of this revision.

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Reviewer #1:

1. The authors have not reviewed the recent advancement in the field of concentration ion polarisation in microfluidics. The fabrication technique presented here has been reported by J Han group at MIT almost 10 years ago. Recent works use paper as microporous material to replace the micro channel and can prevent the instability at the concentration/depletion interface: D.T. Phan et al., Sample concentration in a microfluidic paper-based analytical device using ion concentration polarization, Sensors and Actuators B, Vol. 222, No. 1, 2016, pp. 735-740.

Response 1: Thank you for your insightful comment. We agreed that the fabrication technique presented here (i.e. microflow patterning) was developed almost 10 years ago. Various other techniques have been developed to integrate ion selective materials in microfluidics, however, microflow patterning is still the most easy-to-use method. It has been widely used until recently [Cheow et al., *Anal. Chem.*, 2014, **86**, 7455-7462; Cho et al., *Nanoscale*, 2014, **6**, 4620-4626; Choi et al., *RSC Adv.*, 2015, **5**, 66178-66184; Ouyang et al., *Anal. Chem.*, 2016, **88**, 9669-9677].

Our group also has experiences to build ICP preconcentrators in paper-based microfluidic systems [Han et al., *Lap Chip*, 2016, **16**, 2219-2227; Hong et al., *Anal. Chem.*, 2016, **88**, 1682-1687]. As the reviewer 1 addressed, the microporous structures of the paper may prevent the instability by suppressing electroconvective vortices in ion depletion zones [Rubinstein et al., *Phys. Rev. Lett.*, 2008, **101**, 236101; Kwak et al., *Phys. Rev. Lett.*, 2013, **110**, 114501]. However, the sizes of the paper channels are generally about 0.5~5 mm, which is much bigger than the conventional microfluidic channels. This wider paper channel with random fiber networks makes irregular motions of the preconcentrated plugs, instead of the smooth curved shapes in microfluidic channels (Fig. R1). This has been inevitable in paper-based ICP preconcentrators, because the minimum feature size of wax patterning and paper cutting (i.e. fabrication methods to build paper channels) is about few hundred micrometers. We added this explanation in the revised manuscript (Page 9).

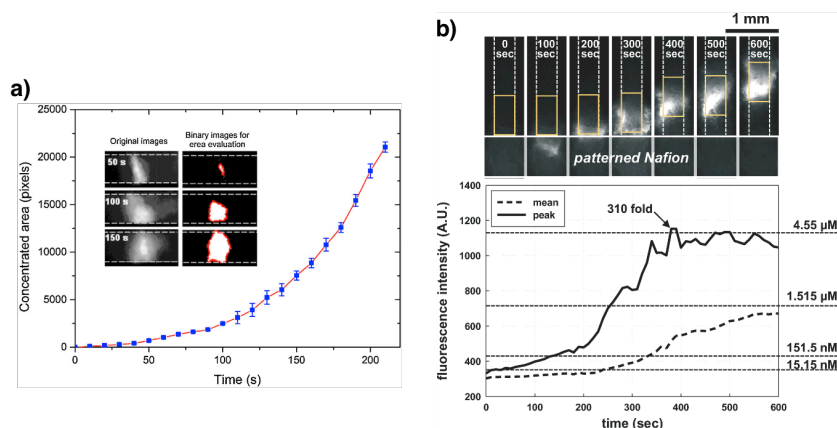


Figure R1. Irregular preconcentrated plugs in paper-based ICP preconcentrators adopted from a) Phan et al. [*Sens. Actuators B* 2016, **222**, 735-740], and b) Han et al. [*Lap Chip*, 2016, **16**, 2219-2227].

Reviewer #3:

1. Usually, the increase of the concentration using ICP is due to the continuous supply of the sample from the reservoir against the ion depletion zone. In the "merged" ICP presented in the manuscript, however, there is no continuous supply of the molecules from the reservoir. It looks like only the molecules confined between the two Nafion membranes get concentrated since there is no continuous supply of molecules from the anodic reservoir. Therefore, the increase is only 4-5 times. However, in Fig. 8, the authors show a 10,000-fold increase which is difficult to understand how. Also, this protein concentration result doesn't correspond to the results presented in Fig. 7 where there is hardly no preconcentration of the dye in 100 mM buffer solution. However, FITC-albumin showed a 100-10,000 fold increase in 1x PBS.

2. in the Discussion section: The first paragraph needs a clarification under which conditions 10,000-fold increase was achieved. In Fig. 7, at 100 mM and pH 3.7, there was hardly any preconcentration achieved. However, in Fig. 8, there was 10,000-fold increase achieved. Why? Any hypothesis?

Response 1-2: As we addressed in the original journal paper [Kwak et al., *Anal. Chem.*, 2016, **88**, 988–996], the wall of the PDMS channel is negatively charged, and this generates electro-osmotic flow (EOF) between two Nafion membranes under an electric field (Fig. 2a; i). The EOF delivers targets toward the interface of the depletion and enrichment zones continuously, and its speed is proportional to the applied voltage. As a result, targets are delivered faster at high voltage, resulting faster preconcentration (Fig. 5 in the manuscript and Fig. R2). We added these detail descriptions in the caption of Fig. 5 (Page 7).

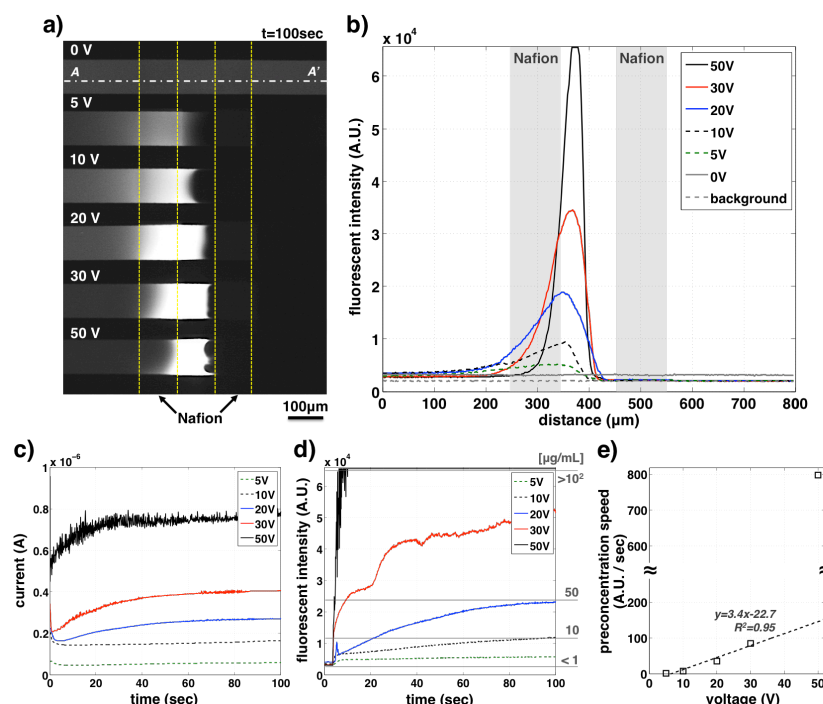


Figure R2. Spatiotemporally defined preconcentration in various operating voltages (5-50V). **a)** Fluorescent images after 100 sec operation, and **b)** fluorescent intensity profiles along A-A'. Yellow dotted boxes indicate the location of Nafions. **c)** In these tests, currents are also fully recovered the initial values. **d)** The peak fluorescent intensities are traced during 100 sec with the reference lines, which indicate the actual concentration of fluorescent dyes (1-100 $\mu\text{g/mL}$ of Alexa Fluor 488 in 1mM KCl solution). **e)** In addition, preconcentration speeds are calculated from the linear regime of the peak intensity-time curves in (d). Under 30V, the preconcentration speed is linearly proportional to the applied voltage (the dotted line is the linear fitting curve), while the speed is much faster at 50V. This figure and contents are adopted from Kwak et al. [*Anal. Chem.*, 2016, **88**, 988–996].

Again, we're sorry to drop important information from the original paper [Kwak et al., *Anal. Chem.*, 2016 **88**, 988–996]. As the reviewer 3 addressed, the preconcentration was hardly achieved in higher ionic strength (Fig. 7). Therefore, to facilitate the preconcentration of FITC-albumin in 1x phosphate buffer saline solution, we doubled the width of the Nafion pattern (200 μm) and used a narrower PDMS channel (width: 50 μm). In this way, ICP phenomenon can be enhanced by broadening the ions pathway but by reducing the absolute amount of ions in the channel. We added these detail descriptions in the caption of Fig. 8 (Page 8).

3. A discussion about the effect of the distance between two Nafion membrane is missing in the discussion section. If you increase the distance between two Nafion membranes, can you expect a higher concentration factor since more molecules trapped in between can be preconcentrated? Would the location of the spatiotemporally predefined region be also the same in front of the enrichment zone?

Response 3: As mentioned in the previous response, target molecules can be delivered by EOF, and then the faster EOF at the higher electric field accelerates the preconcentration speed. Therefore, if we increase the distance between two Nafion membranes d , the electric field E decreases under the same applied voltage V ($E=V/d$), resulting the decrease of the preconcentration speed (Fig.R3). We added this discussion in Page 8.

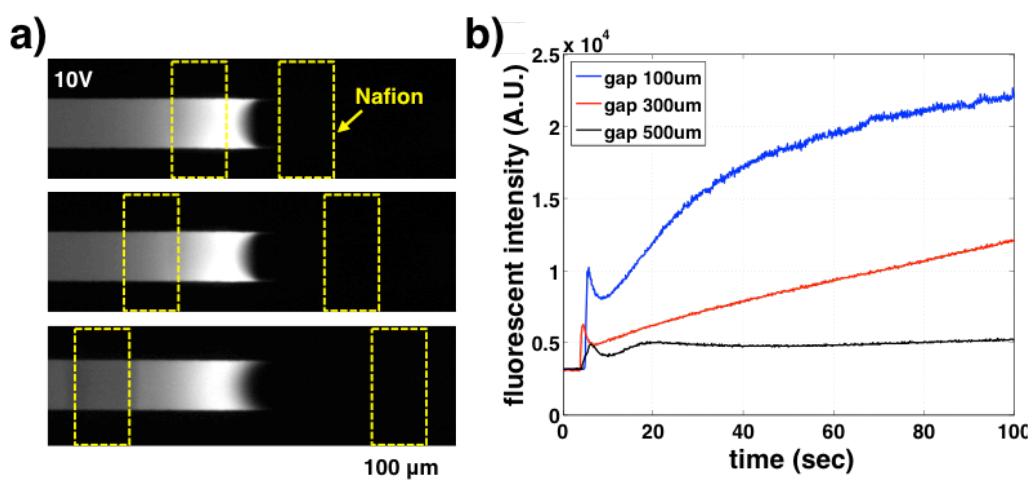


Figure R3. a) Merged ICP preconcentration with various inter-Nafion distances (100, 300, and 500 μm) under 10 V. Yellow boxes indicate the location of the patterned Nafions. b) The peak fluorescent intensities at the applied voltage 10V. The preconcentration plugs are always between the Nafions. However, longer inter-Nafion distances induce weaker preconcentration performance. This figure and contents are adopted from the Figure S2 in Kwak et al. [*Anal. Chem.*, 2016, **88**, 988–996].

4. It is claimed that the location of the plug is spatiotemporally predefined using the merged ICP. What is the longest preconcentration time tested using the merged ICP device? 20 min. are not really a long time for preconcentration. Even using the conventional ICP, a more or less stable plug at the same location can be achieved for ~20 min.

Response 4: Thank you for your valuable comment. Indeed, the longest preconcentration time in our experiments with the merged ICP platform is 20 min (Fig.8). In the FITC-albumin test, we decided that 20 min operation was enough because we achieved 10,000-fold already, and the general operating time in previous works also around few ten minutes [Cheow et al., *Anal. Chem.*, 2014, **86**, 7455-7462; Ouyang et al., *Anal. Chem.*, 2016, **88**, 9669-9677].

We agreed that our experiments could not cover the cases with longer operating times, and addressed this limitation in the caption of Fig. 8 (Page 8).

5. on page 5, under 1.3.4): Should the PDMS mold be detached right after filling the Nafion resin in the channel? Or is it better to wait a little bit in order to minimize the loss of Nafion stuck on the PDMS surface?

Response 5: In our experiment, the PDMS mold was detached right after filling the Nafion resin. We recommend the detachment time within one minute after filling the resin, but it is not necessary. If we detach the mold few minutes later, we may obtain the thicker Nafion patterns, but the pattern would have a concaved shape; the thickest point would occur at the edge of the pattern because of the capillary effect. We added this content in the Protocol 1.3.4.

6. in the figure caption of Fig. 2: Why is there no increase of the ion concentration in the conventional platform without the ion depletion zone? Is it because there is not enough EOF generated in the channel since the Nafion is grounded and not the right outlet that is floating? What if the right outlet is grounded like the membrane? Would there be a concentration increase in front of the Nafion membrane in conventional ICP? In Fig. 6a, however, there is an increase of the concentration in the form of a plug using the conventional ICP platform. The statement seems to be contradictory. Please clarify this.

Response 6: We addressed that there is no increase of the “ion” concentration in the conventional platform without the ion “enrichment” zone. In this platform, one Nafion pattern rejects ions in the channel, generating only ion depletion zone where ion concentration drops. In this situation, there is no source of ions, so no increase of the ion concentration occurs. This is also directly observed in previous works [Kim et al., *Nanoscale*, 2012, 4, 7406-7410] (Fig.R4). Also, in Fig. 6a, ion concentration did not increase even the fluorescent dyes were preconcentrated. It is noted that the concentration of a fluorescent dye (and target biomolecules) is not representing the concentration of ions.

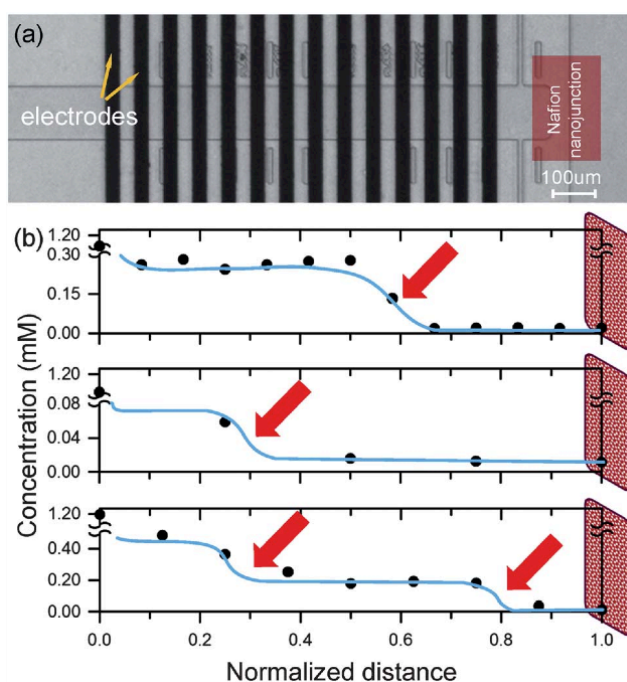


Figure R4. (a) Straight and single micro-nano-microchannel device with microelectrode pairs (black bars) for conductivity measurement experiments. (b) Conductivity drops as a function of normalized distance between ICP interface and Nafion membranes. The y-axes have a break since the concentration steeply decreased right inside ICP layer. The three measurements have different points (denoted by arrows) where the stepwise changes of the electrolyte concentration occurred with multiple vortices in the ion depletion zone. This figure and contents are adopted from Kim et al. [*Nanoscale*, 2012, 4, 7406-7410].

7. in the figure caption of Fig. 5: why is the depletion shock only observed when the second Nafion membrane is present? A reference would be great if one would like to know more about this depletion shock.

Response 7: Thank you for your valuable comment. We believe that there would be a similar depletion shock in the conventional platform, but it would not make the spike in the peak intensity curves (Fig.5h and Fig.6h).

At high voltage, the flat depletion zone is developed in a moment, and propagates as the ions are rejected through the ion selective membrane continuously. The propagation of the flat depletion zone is reminiscent of the shock propagation, so Mani et al. called this dynamics as the deionization (or depletion) shock [Mani et al., *Phys. Rev. E*, 2011, **84**, 061504].

According to our observations, the fluorescent dyes were accumulated on the shock boundary as it pushes the dyes (Fig.4c). In the conventional platform, this initial accumulation was not identified in the peak intensity curves (Fig.6h); because the fluorescent intensity was keep increasing as the dyes was preconcentrated. However, in the new platform with two Nafion patterns, the initial accumulation was somewhat dispersed when the depletion shock met the ion enrichment zone. As can be seen in Fig.4, the width of the peak at 0.8 sec was wider than that at 0.4 sec. This is probably because the left side of the left Nafion pattern (Fig. 2a) was electrically floated, and the accumulated dyes could spread out. Indeed, in Fig.5g, the slope of the dye concentration was steeper on the right side of the intensity peak than on the left side. We added this content in the caption of Fig. 5-6 (Page 7).

8. in Fig. 6: the ticks on the x- and y-axis are missing in d), e), f). (see Fig. 5d, e, f)

Response 8: We added the ticks on the axis in the revised manuscript.

9. in Fig. 7: why are the yellow dotted boxes are used here while in all other figures, just the dotted lines are used? Use the dotted lines to indicate the Nafion membrane in order to be consistent. What is "0 distance"? In the figure caption of Fig. 7, it says that 10,20, 50 and 100 V were used to map the location of peak intensity. Are the graphs in Fig. 7b) and 7c) based on the results at 50V?

Response 9: Thank you for your specific comment. We changed the word “dotted boxes” to “dotted lines” in Fig. 7. The 0 distance in Fig. 7a represents the origin of the x-axis in Fig. 7b-c, which is on the right edge of the left Nafion membrane.

Next, the data in Fig. 7b-c shows the peak intensity locations and folds under four different voltages (10, 20, 50, and 100 V). For one case (6 cases: 1, 10, 100 mM and/or pH 3.7, 7, and 10), there were four data points corresponding to the four voltage conditions. At higher voltage, we have higher peak intensity fold in all cases. We revised the caption of Fig. 7 for more clear description (Page 7).

10. in Fig. 8: the unit for x-axis [sec.] is missing. Please indicate the location of the Nafion membranes using yellow dotted lines.

Response 10: We added the unit for x-axis, time (sec), and indicated the location of the Nafion membranes with yellow dotted lines.

11. Violent vortices -> strong vortices

Response 11: We changed the word in the revised manuscript.

12. Can you please add a short discussion about how this technique can be applied to enhance the detection sensitivity of a biosensor immobilized with capture molecules in the Discussion section? Plasma bonding of the PDMS chip with a glass slide will compromise the immobilized capture molecules.

Response 12: Thank you for the insightful comment. Indeed, plasma bonding can compromise immobilized capture molecules. Therefore, various protocols and devices have been developed to immobilize molecules after microfluidic channels are built through plasma bonding. There are three representative methods: i) adding target molecules and capture molecules together, and preconcentrating both of them together [Sarkar et al., *Lab Chip*, 2011, **11**, 2569-2576], ii) loading microbeads which holds immobilized molecules [Cheow et al., *Anal. Chem.*, 2010, **82**, 3383-3388], and iii) building one bifurcated channel to immobilize capture molecules near the Nafion membrane while the main channel is closed by a valve [Liu et al., *Lab Chip*, 2010, **10**, 1485-1490]. We added this discussion in Page 9.