

Journal of Visualized Experiments

Phosphorus-31 magnetic resonance spectroscopy: a tool for measuring in vivo mitochondrial oxidative phosphorylation capacity in human skeletal muscle --Manuscript Draft--

Manuscript Number:	JoVE54977R3
Full Title:	Phosphorus-31 magnetic resonance spectroscopy: a tool for measuring in vivo mitochondrial oxidative phosphorylation capacity in human skeletal muscle
Article Type:	Methods Article - JoVE Produced Video
Keywords:	magnetic resonance, spectroscopy, phosphorus, mitochondrial oxidative phosphorylation capacity, skeletal muscle, dynamic
Manuscript Classifications:	3.18.452: Metabolic Diseases; 5.1.370.350.500: Magnetic Resonance Imaging (MRI); 5.5.196.867.519: Magnetic Resonance Spectroscopy; 7.3.495.790.550: Oxidative Phosphorylation
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Abstract:	Skeletal muscle mitochondrial oxidative phosphorylation (mOXPHOS) capacity, which is critically important in health and disease, can be measured in vivo in humans, noninvasively via phosphorus-31 magnetic resonance spectroscopy (31PMRS). However, the approach has not been widely adopted in translational and clinical research, with variations in methodology and limited guidance from the literature. Increased optimization, standardization, and dissemination of methods for in vivo 31PMRS would facilitate the development of targeted therapies to improve mOXPHOS capacity and could ultimately favorably impact cardiovascular health. 31PMRS produces a direct, in vivo measure of mOXPHOS capacity in human skeletal muscle, rather than alternative measures obtained from explanted and potentially altered mitochondria via muscle biopsy, and relies upon only modest additional instrumentation beyond what is already in place on magnetic resonance scanners available for clinical and translational research at most institutions. In this work we outline a method to measure in vivo skeletal muscle mitochondrial function. The technique is demonstrated using a 1.5 Tesla whole body MR scanner equipped with suitable hardware and software for 31PMRS along with a simple and robust protocol

	for in-magnet resistive exercise to rapidly fatigue the quadriceps muscle. Reproducibility and feasibility are demonstrated in volunteers as well as patients over a wide range of functional capacities.
Author Comments:	
Additional Information:	
Question	Response
If this article needs to be "in-press" by a certain date to satisfy grant requirements, please indicate the date below and explain in your cover letter.	

TITLE:

Phosphorus-31 magnetic resonance spectroscopy: a tool for measuring *in vivo* mitochondrial oxidative phosphorylation capacity in human skeletal muscle

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KEYWORDS:

magnetic resonance, spectroscopy, phosphorus, mitochondrial oxidative phosphorylation capacity, skeletal muscle, dynamic

SHORT ABSTRACT:

This work demonstrates the feasibility of an *in vivo* phosphorus-31 magnetic resonance spectroscopy (³¹PMRS) technique to quantify mitochondrial oxidative phosphorylation (OXPHOS) capacity in human skeletal muscle.

LONG ABSTRACT:

Skeletal muscle mitochondrial oxidative phosphorylation (OXPHOS) capacity, which is critically important in health and disease, can be measured *in vivo* and noninvasively in humans via phosphorus-31 magnetic resonance spectroscopy (³¹PMRS). However, the approach has not been widely adopted in translational and clinical research, with variations in methodology and limited guidance from the literature. Increased optimization, standardization, and dissemination of methods for *in vivo* ³¹PMRS would facilitate the development of targeted therapies to improve OXPHOS capacity and could ultimately favorably impact cardiovascular health. ³¹PMRS produces a noninvasive, *in vivo* measure of OXPHOS capacity in human skeletal muscle, as opposed to alternative measures obtained from explanted and potentially altered mitochondria via muscle biopsy. It relies upon only modest additional instrumentation beyond what is already in place on magnetic resonance scanners available for clinical and translational research at most institutions. In this work, we outline a method to measure *in vivo* skeletal muscle OXPHOS. The technique is demonstrated using a 1.5 Tesla whole-body MR scanner equipped with the suitable hardware and software for ³¹PMRS, and we explain a simple and robust protocol for in-magnet resistive exercise to rapidly fatigue the quadriceps muscle. Reproducibility and feasibility are demonstrated in volunteers as well as subjects over a wide range of functional capacities.

INTRODUCTION:

The goal of this work is to outline a reproducible method to noninvasively measure *in vivo* skeletal muscle mitochondrial function in individuals possessing a wide range of abilities. Aberrant mitochondrial impairment is a hallmark of a wide range of metabolic syndromes and genetic diseases, from common conditions such as aging and diabetes to rare disorders such as Friedreich's ataxia.

Metabolic syndrome and mitochondrial dysfunction

Metabolic syndrome has been shown to disrupt mitochondrial function, depress skeletal muscle OXPHOS, and lead to ectopic lipid storage in skeletal muscle^{1,2}. As critical organelles regulating metabolic and energy homeostasis, mitochondria are implicated in the pathophysiology of obesity^{3,4}, insulin resistance⁵, Type 2 Diabetes Mellitus (T2DM)^{6,7}, diabetes-related micro-⁸⁻¹¹ and macrovascular complications^{12,13}, and non-alcoholic fatty liver disease (NAFLD)¹⁴⁻¹⁶, among others. Insulin resistance is characterized by profound changes in skeletal muscle mitochondrial activity, including decreased mitochondrial tricarboxylic acid (TCA) flux rate, ATP synthesis rate, and citrate synthase and NADH:O₂ oxidoreductase activity⁵. One hypothesis is that these alterations could be due to the accumulation of free fatty acid (FFA) metabolites in the muscle, which are markedly augmented during obesity and other obesity-related diseases^{2,17}. The exposure of muscle to elevated FFAs and lipid intermediates can decrease the expression of genes in the lipid oxidative pathway as well as the TCA cycle and electron-transport chain (ETC)¹⁸. This reduction in mitochondrial skeletal muscle OXPHOS capacity in the setting of a lipid overload is accompanied by a decline in the quantitative (content and biogenesis of mitochondria)¹⁹ and qualitative function of skeletal muscle mitochondria²⁰. Exposing skeletal muscle and myocytes to FFAs leads to severe insulin resistance, and increased FFA uptake in muscle is associated with insulin resistance in both humans and rodents²¹. The lipid intermediates ceramide and diacylglycerol (DAG) have been shown to directly inhibit the insulin signaling pathway by altering the activity of kinases, such as protein kinase C and protein kinase B²¹. Therefore, lipid-derived molecules appear to play a prominent role in the development of skeletal muscle insulin resistance and T2DM. However, it remains unclear whether changes in mitochondrial capacity are a cause or a consequence of insulin resistance²².

Friedrich's ataxia and mitochondrial dysfunction

Decreased OXPHOS can also arise from genetic defects. Friedrich's ataxia (FA), the most common form of hereditary ataxia, is a genetic disorder caused by a mutation in the frataxin (FXN) gene, resulting in intra-mitochondrial iron accumulation, reactive oxygen species production, and abnormalities of oxidative phosphorylation²³⁻²⁶. This important discovery has led to the development of targeted therapies, which aim to improve mitochondrial function at the sub-cellular level. Despite this understanding, there has been limited development of *in vivo*, reproducible biomarkers for FA clinical research. In fact, a critical barrier in the effective evaluation of targeted therapies in FA is the inability to track changes in mitochondrial function. Current functional measures, for example, can identify decreased cardiac output; however, they are incapable of determining the level at which the dysfunction occurs (Figure 1). The development of a reliable marker of mitochondrial function that can be used to identify and evaluate disease progression in Friedrich's ataxia is crucial to gauge the relevant mechanistic impact of targeted therapies.

Impaired OXPHOS and cardiac dysfunction

Aberrant mitochondrial function, either acquired or genetic, could contribute to the development or progression of cardiac dysfunction. Under the conditions of pressure overload

and heart failure, the primary energy substrate preference switches from FFA to glucose. This is associated with decreased ETC activity and oxidative phosphorylation²⁷. The pathophysiology of mitochondrial bioenergetics in cardiac dysfunction can be different depending on the primary origin of the mitochondrial defect. Diabetes and metabolic syndrome results in mitochondrial abnormalities in myocardium, such as impaired biogenesis and fatty acid metabolism, which lead to reduced substrate flexibility, energy efficiency, and eventually, diastolic dysfunction^{28,29}. In FA, on the other hand, a frataxin deficiency results in significant mitochondrial iron accumulation in cardiomyocytes^{30,31}. Iron accumulation leads to the production of free radicals via the Fenton reaction³² and increases the chance of free radical-induced cardiomyocyte damage. Intra-mitochondrial iron accumulation is also associated with an increased sensitivity to oxidative stress and a reduced oxidative capacity^{30,31}. Iron accumulation and subsequent aberrant mitochondrial function, due to frataxin deficiency, may therefore be responsible for the impaired cardiac energetics and cardiomyopathy observed in FA^{33,34}. It is also interesting to note that the reduced oxidative capacity in skeletal muscle mitochondria parallels the exercise intolerance and reduced metabolic capacity in heart failure (HF)³⁵. Measurement of skeletal muscle OXPHOS capacity, as detailed herein, is readily implementable and robust; coupled with the significance of skeletal muscle OXPHOS in HF, these features make it an appealing biomarker in comprehensive studies of heart disease³⁶.

Impaired OXPHOS and the accompanying cardiac dysfunction is not an inconsequential aspect of metabolic and mitochondrial disease. Subjects with diabetes and metabolic disease are at a higher risk of developing cardiovascular disease and have excess mortality after myocardial infarction (MI)³⁷⁻⁴¹; over half of FA subjects have cardiomyopathy, and many die of cardiac arrhythmia or heart failure⁴². Therefore, quantification of reduced OXPHOS could not only allow for early detection and treatment of cardiac dysfunction, but it could also alleviate a major clinical burden in these diseases.

Targeted therapies to directly increase OXPHOS capacity is a promising area to improve the treatment of subjects, whether the cause of metabolic dysfunction is genetic or acquired. Currently, the development of novel targeted drugs that either alleviate abnormal mitochondrial function⁴³ or correct the primary genetic defect⁴⁴ can improve the deranged bioenergetics characteristic of FA. In the case of acquired mitochondrial dysfunction, increased physical activity can improve mitochondrial function⁴⁵⁻⁴⁷.

³¹Phosphorous magnetic resonance spectroscopy as a non-invasive biomarker of mitochondrial function

Regardless of the tested therapy, an integrated *in vivo* assessment of skeletal muscle bioenergetics is a crucial tool to assess the impact of targeted interventions, especially in subjects with severe exercise intolerance or the inability to undergo conventional metabolic testing. Magnetic resonance spectroscopy tuned to phosphorous (³¹PMRS), an endogenous nucleus found in various high-energy substrates within cells throughout the body, has been used to quantify mitochondrial oxidative capacity using a variety of approaches, including in-magnet exercise-recovery protocols and muscle stimulation protocols⁴⁸. The exercise-recovery protocols rely upon a variety of apparatus ranging in complexity from MRI-compatible

ergometers that regulate and measure workload to simple configurations of straps and pads allowing for burst-type resistive and quasi-static exercise. One of the primary goals of any of these protocols is to produce an energy imbalance for which the demand for adenosine triphosphate (ATP) is initially met through the enzymatic breakdown of phosphocreatine (PCr) through the creatine kinase reaction⁴⁹. Upon cessation of exercise, the rate of ATP production is dominated by oxidative phosphorylation and represents the maximum *in vivo* capacity of the mitochondria⁵⁰. Furthermore, OXPHOS during post-exercise recovery can be described by a first-order rate reaction⁵¹. The post-exercise recovery of PCr can therefore be quantified by the fitting of an exponential time constant (τ_{PCr}), with smaller values of τ_{PCr} representing greater capacities for oxidative ATP synthesis. Significant efforts have been made to validate ³¹PMRS against *ex vivo* and more direct measures of OXPHOS and demonstrate the potential clinical applicability of this technique⁵²⁻⁵⁵.

Notably, the protocol described in this work can be implemented on clinically-available scanners, and it has been widely validated as a noninvasive biomarker of mitochondrial function⁵⁶. However, an exercise ³¹PMRS protocol optimized for application to individuals with varying severities of neuromuscular impairment or mobility has not been well established⁵⁷. A well-defined, broadly-applicable exercise protocol and ³¹PMRS technique would be particularly useful in the evaluation of diseases with fundamental abnormalities in mitochondrial function.

Several prior studies have explored the applications of non-invasive techniques to quantify mitochondrial function in subjects. For instance, these techniques have shown impaired OXPHOS in subjects with type 2 diabetes³⁶. Lodi *et al.* first tested the feasibility of PMRS techniques in subjects with FA and found that 1) the fundamental genetic defect in FA impairs skeletal muscle OXPHOS and 2) the number of GAA triplet repeats is inversely proportional to skeletal muscle OXPHOS³³. More recently, Nachbauer *et al.* used PMRS as a secondary outcome measure in an FA drug trial with 7 subjects. PCr recovery times were significantly longer in subjects compared to controls, reaffirming Lodi's earlier work and indicating that the effects of aberrant frataxin expression in FA can result in a decline in mitochondrial capacity that is detectable using PMRS techniques⁵⁸.

Reliable methods to adequately define *in vivo* skeletal muscle function in a feasible, cost-effective, and reproducible manner are critical to improving subject outcomes in a range of diseases that affect mitochondrial function.

This work outlines a robust procedure for obtaining *in vivo* maximum oxidative capacity of skeletal muscle using ³¹PMRS. The in-magnet exercise protocol is well tolerated by individuals spanning a wide range of physical and functional abilities and affords a simplified subject setup using inexpensive and widely-available equipment.

PROTOCOL:

This protocol is approved by and follows the guidelines of the Ohio State University Institutional Review Board for human subjects research. It is critically important that all procedures involving MR equipment are performed by adequately trained personnel adhering to the highest

standards of MR safety⁵⁹.

1. Materials and Preparation

1.1) Ensure that all necessary materials are available prior to the experiment (Figure 2).

1.2) Plug the ³¹P coil into the in-table coil connector at the end of the exam table closest to the bore. Place a large triangle foam cushion near the head of the MR exam table, but not directly on the ³¹P coil. Place a head pillow at the other end of the MR exam table, farthest from the bore, for subject comfort.

2. Subject Positioning (Figure 3a)

2.1) Instruct the subject to lie supine, feet first on the MR table. Place a foam cushion under the knees to support the leg in a partially flexed position.

2.2) Position the subject close to the right side of the table (the subject's right) in order to center the left thigh as closely to the magnet isocenter as possible, thus ensuring optimal B0 homogeneity in the thigh muscle under examination. Provide the subject with ear plugs and/or headphones.

2.3) Position the ³¹P RF coil on the left quadriceps at approximately the midpoint between the patella and the femoral head, and secure to the leg using straps. Place the coil over the lateral portion of the leg, above the vastus lateralis.

2.4) Secure the baby oil to the medial aspect of the thigh with the same straps used to secure the coil to the leg. This facilitates scan localization.

2.5) Bind the subject's legs together with a strap placed below the coil and above the knee. Secure the subject's legs to the MR table with additional straps, one above the knee and one midway between the knee and ankle.

2.6) Use the laser light guide to delineate the center of the coil and move the table to the magnet isocenter using this centering landmark.

3. Exercise Protocol

3.1) Explain to the subject that the exercise protocol consists of three phases: an initial, baseline phase; a short, intense exercise phase; and a recovery phase.

3.2) Instruct the subject to lie still and relax their leg muscles during the baseline and recovery phases of the spectroscopy acquisition in order to minimize motion artifacts.

3.3) Provide a countdown to the subject indicating the start of exercise. At this point, have the subject initiate knee extension/flexion as forcefully and as rapidly as possible against the resistance of the straps.

NOTE: The quadriceps muscles are used to move the left lower leg up and down, until instructed to stop.

3.4) Terminate exercise after a 30% drop in the PCr peak height.

3.4.1) Observe the PCr peak height in the acquisition viewer window, and also view it upon completion of the exercise sequence.

NOTE: A general guideline is that an approximate 30% drop in PCr peak height corresponds to a Pi peak that is 50% of the height of the PCr peak. If PCr depletion is not occurring rapidly enough to achieve a 30% drop during the exercise phase of the exam, encourage the subject to kick harder or faster while exercising.

NOTE: Cessation of exercise is determined by monitoring the PCr peak height and duration of exercise. This may result in slightly different durations of exercise in different patients and can be accounted for in the analysis.

4. Scan Protocol

4.1) Acquire a tri-plane localizer to verify proper subject positioning and identify the location of the ^{31}P coil.

NOTE: The localizer sequence begins automatically and centers at the indicated position using the laser light guide (step 2.9)

4.2) Acquire a second tri-plane localizer.

4.2.1) Open the slice view on the first tri-plane localizer images.

NOTE: This process may be different for different software and hardware systems.

4.2.2) Center and rotate the slice orientation by left-clicking and holding on the slice group. Rotate the slice group. Ensure that the final orientation of slices matches with the position of the baby oil.

4.2.3) In the sequence routine window, increase the number of slices to cover the entire leg in the axial and sagittal images (Figure 3b).

4.3) ^{31}P spectroscopy sequence:

4.3.1) Use the following non-localized pulse-acquire sequence parameters: TR: 1,000 ms; TE: 0.34 ms; spectral width: 2,000 Hz; flip angle: 90 degrees; acquired data points: 1,024; 4 averages resulting in a time resolution of 1 spectrum every 6 s.

4.4) ^{31}P shim box placement:

4.4.1) Using a mouse, drag the second triplane localizer images into the viewing window at the top of the screen. Drag the spectroscopy sequence into the protocol window and double-click to open.

4.4.2) Use the position tool bar to visualize the shim voxel (select the black rectangle with horizontal lines). After selecting this option, observe a green box on the localizer images.

NOTE: This is the shim voxel.

4.4.3) Move the voxel by left-clicking and holding the voxel in the center. Change the size and rotate the orientation of the voxel by left-clicking and holding the voxel at the corner of the box. Place the shim box so as to ensure B0 field homogeneity directly below the coil and parallel to the plane of the quadriceps.

NOTE: This is to ensure proper shimming within the sensitive region under the coil, which is the volume of tissue directly below the center of the coil.

4.4.4) Use the tri-plane localizer images to identify the sensitive region of the coil and adjust the shim box to encompass this region within the quadriceps muscle.

NOTE: The shim box can be larger than the true coverage of the surface coil in order to ensure B0 homogeneity within the data acquisition voxel (Figure 3c).

4.4.3) ³¹P test acquisition:

4.4.3.1) Open the acquisition viewer window and select the head icon in the acquisition tool bar. This will allow for viewing of the spectroscopy acquisition in real time.

4.4.3.2) After placement of the ³¹P shim voxel, run the sequence to obtain a single spectrum by clicking the “run” button at the top of the protocol window.

4.4.3.3) Examine the quality of B0 shimming. Observe the resulting spectrum in the acquisition window. Observe a prominent PCr peak centered at 0 ppm and no significant noise (Figure 4a, left).

NOTE: Troubleshooting: If the spectrum appears noisy, ensure that the shim box is placed within muscle. Adjust the size and position of the shim box to improve the signal-to-noise ratio. Repeat the test acquisition as needed.

4.4.3.4) In order to see the PCr peak height, open the spectrum in the spectroscopy tool (“Applications” → “Spectroscopy”). Open the patient’s folder (folder tree icon), select the appropriate scan, and double-click to load the spectrum.

4.5) Pre-exercise T1 image:

4.5.1) Obtain a single-slice axial T1-weighted image at the center of a coil.

4.6) ³¹P pre-exercise acquisition:

4.6.1) Copy the sequence from step 4.4 (that produced the best spectral quality) by left-clicking and dragging the sequence in the protocol window. Use this sequence for all subsequent measurements.

4.6.2) In the sequence routine window, increase the number of measurements from 1 to 10. Select run to acquire 10 measurements while the subject is at rest.

4.7) ³¹P exercise acquisition:

NOTE: Make careful note of the start and end exercise times, as this will be important for analysis.

4.7.1) Rest: Apply the shim settings from the previous scan and set the sequence to acquire 20 measurements. Instruct the subject to begin kicking after a countdown. Instruct the subject to remain at rest for 2 measurements.

4.7.2) Exercise: Ask the subject to perform the knee extension exercise for ~30 s (or the time required to achieve a 30% decrease in the PCr peak amplitude). After the subject achieves sufficient PCr depletion, ask them to rest.

4.8) ³¹P post-exercise acquisitions:

4.8.1) Acquire an additional 20 measurements at rest. Ensure that the post-exercise acquisitions begin immediately following the exercise sequence, without pause or shimming (Figure 4a, right).

NOTE: The subdivision of this recovery period into two separate acquisitions permits the analysis of the initial 20 dynamic spectra during the acquisition of the second 20 dynamic spectra, allowing the operator to avoid acquisition of the full recovery period if the exercise needs to be repeated.

4.9) Ensuring exercise quality:

4.9.1) Compare the PCr peak heights at the beginning and end of exercise. High-quality exercise sessions result in a ~30% decrease in the PCr concentration.

4.9.2) Verify that the PCr peak height is the same at beginning of rest and at the end of recovery (typically, < 10% difference is desired). This ensures that there was negligible loss of field homogeneity during acquisition.

NOTE: If the PCr breakdown is insufficient, or if there has been a loss of field homogeneity, then repeat the exercise/recovery portion of the exam (taking care to avoid fatigue), ensure that the coil and straps are securely attached, and extend the duration of exercise and/or encourage more vigorous exercise (Figure 4b).

NOTE: A comparison of the images obtained in steps 6 and 11 permits an additional quality control step to visualize any displacement of the thigh and coil due to the exercise, thus ensuring that minimal motion occurred during the protocol, which could significantly affect the acquired data.

4.10) Following post-exercise T1 imaging, repeat the pre-exercise axial T1 imaging (step 4.5) using the same acquisition parameters.

4.10.1) In addition to sufficient depletion of PCr, measure the end exercise pH to ensure that the exercise did not induce acidosis of the muscle.

4.10.2) Perform this by measuring the chemical shift between Pi and PCr (δP_i) and using the following equation⁶⁰:

$$\text{pH} = 6.77 + \log[(\delta P_i - 3.29)/(5.68 - \delta P_i)]$$

NOTE: The pH should remain greater than 6.8⁶¹. If the PCr breakdown is sufficient but the pH is too low, repeat the exercise bout for a shorter duration and/or with a decreased intensity.

4.11) Saving Data:

4.11.1) Save all acquired spectra as DICOM files and export them for processing using JMRUI.

4.11.2) If using a scanner, select all spectroscopy acquisitions in the “Navigator” window.

4.11.3) Under “Applications,” select “Dicom Tools” → “Export MR Spectroscopy,” and save the DICOM (*.dcm) files to C:/User/MedCom/temp/CDROFFLINE (the tool automatically chooses this location).

4.11.4) Under “Transfer,” select “Export to Offline.” Save to the desired location.

5. Data Processing and Analysis⁶²

5.1) Analyze the MR spectra with freely-available JMRUI software (version 5.2; <http://www.jmrui.eu/>).

5.2) Apodize and phase shift the spectra to ensure uniformity over all acquired time points (Figure 5). The PCr peak will be centered at 0 ppm in the spectra.

5.3) Use the built-in AMARES algorithm to quantify the amplitude of the PCr peak in each acquired spectrum. The peak amplitude represents the concentration of PCr within the sensitive region of the surface coil at that particular time point.

5.4) In the computational software, plot the PCr concentrations as a function of acquisition time. Using the built-in computational software curve-fit tool, fit the PCr recovery period data

to the following equation^{52,63}:

$$PCr(t) = PCr_0 + PCr_{\Delta} * e^{-\frac{1}{\tau}}$$

5.5) Record the values of the baseline PCr ($PCr_0 + PCr_{\Delta}$), the lowest PCr (PCr_{Δ}), and the recovery time(τ).

5.6) Ensure that the appropriate conditions are met during the exercise session by calculating the PCr depletion, the percent difference between the baseline PCr and the lowest PCr. Ideal exercise sessions result in a 20-50% depletion.

NOTE: The quality of the curve fitting can be ensured by verifying that the R^2 value is greater than 0.75. R^2 values are automatically calculated by the fitting software.

REPRESENTATIVE RESULTS:

Reproducibility study

Six volunteers (4 men and 2 women; mean age: 24.5 ± 6.2 years) with no self-reported heart, metabolic, or mitochondrial disease underwent sessions of the described ^{31}P MRS exercise and imaging technique on 2 different days within 1 week to evaluate technique reproducibility (Figure 6a). The studies performed on normal volunteers confirm the reproducibility of the ^{31}P MRS study in the quantification of mitochondrial function. A Bland-Altman analysis of PCr recovery time demonstrates a mean difference \pm standard deviation of 1.03 ± 4.83 s and a between-trials coefficient of variation of 4.66 (Figure 6b). No changes to the acquisition or analysis protocol described in the methods section were required to obtain good-quality data, as described in step 4 of the protocol. These results demonstrate the reproducibility of the acquisition and analysis techniques described in this work.

Technique evaluation in non-ambulatory participants with Friedrich's ataxia

Four participants (2 men and 2 women; mean age: 35) underwent a single session of the ^{31}P MRS exercise and imaging technique described in this work to evaluate its feasibility in a non-ambulatory population with FA. These subjects were capable of performing the in-magnet exercises for obtaining sufficient depletion of PCr to fit the recovery parameters shown in step 5.6. However, longer exercise times (60-90 s) were required to sufficiently deplete the PCr levels. Additionally, oscillations around the fit that were caused by the progressive loss of muscle control, which is characteristic of this disease, were noted (Figure 7). For these subjects, we used two additional resistive straps between the knees and ankles, giving a total of three straps, to limit unwanted motion. These results demonstrate the feasibility of the acquisition and analysis technique to obtain PCr recovery times in non-ambulatory subjects. However, the modifications required to obtain good-quality data indicate that further evaluation and standardization studies are necessary.

Feasibility study

Nine volunteers with no self-reported cardiovascular disease and 15 subjects referred to a program of cardiac rehabilitation and secondary prevention (CRSP) were enrolled in a local

institutional review board (IRB)-approved study. We obtained some clinical values as indicators of cardiovascular health and severity of metabolic syndrome. The left ventricular ejection fraction was preserved in CRSP subjects ($56 \pm 10\%$). The maximum cardiovascular exertion ability, measured before starting CRSP, was similar in subjects with and without diabetes (3.05 ± 0.6 versus 3.4 ± 0.8 metabolic equivalents METs, $p = 0.4$). Prior to starting CRSP, each enrolled subject underwent the ^{31}P MRS exercise and imaging technique, described in this work, and the intramuscular fat quantification imaging, described previously⁶⁴. The time constant of PCr recovery was longer (41.9 ± 1.4 versus 32.1 ± 7.4 s, $p = 0.05$), and the intramuscular fat percentage was higher in CRSP subjects versus controls (8.7 ± 2.9 versus $2.54 \pm 0.6\%$, $p < 0.001$). The percentage of intramuscular fat was similar in CRSP subjects with and without diabetes ($p = 0.4$), and the time constant of PCr recovery tended to be longer in subjects with diabetes versus in those without diabetes and in controls ($p = 0.03$ for the trends across groups). Preliminary follow-up data suggest a considerably worse improvement in METs post-CRSP in subjects with diabetes compared to those without ($\Delta = 1.0 \pm 0.8$ versus 4.0 ± 2.4 , $p = 0.06$; Figure 8). These results demonstrate the feasibility of this technique to quantify differences in skeletal muscle OXPHOS between subjects with and without known metabolic disease.

FIGURE TITLES AND LEGENDS:

Figure 1. Mitochondria, skeletal muscle, and cardiopulmonary systems

A representation of the link between mitochondria, skeletal muscle, cardiac output, ventilation, and functional capacity is shown. Reproduced from Milani *et al*⁶⁵.

Figure 2. Materials

The required materials include 1) a triangle cushion, 2) a 10-cm ^{31}P -tuned transmit-receive surface coil, 3) table-to-table connecting resistive straps, 4) a self-connecting resistive strap, and 5) a small bottle of baby oil.

Figure 3. Positioning

A) Subjects are imaged in a supine, feet-first position. The ^{31}P coil is placed on the left quadriceps. Resistive straps are placed above and below the knee and attached to the table. A single strap is used to bind both legs together above the knee. B) The slice positioning is shown for the second localizer. Note that the slices are centered at the location of the baby oil bottle, and slices cover the entire quadriceps. C) The shim box placement for ^{31}P MRS is shown. This volume is placed directly below the coil in the quadriceps and covers a depth that insures sufficient signal and appropriate shimming within the area of the surface coil.

Figure 4. Data acquisition

A) A representative ^{31}P acquisition at rest is shown. The PCr is the large single peak, and there is minimal noise (left). A typical acquisition during the exercise portion of the protocol results in two large peaks, Pi and PCr (right). As exercise progresses, the Pi and PCr peaks will increase and decrease, respectively. B) Comparison of the PCr peak height at rest and post-exercise should reveal at least a ~30% decrease. This calculation should be done at the scanner console in order to ensure the successful completion of the exercise study.

Figure 5. Analysis

The phase correction and apodization of a representative spectrum is shown. A) A raw spectrum showing an un-phased peak and the presence of noise that obscures the peaks. B) A spectrum showing 0th- and 1st-order phase correction. The PCr peak located at the center frequency is easily identifiable, but other metabolite peaks are still obscured. C) The spectrum after apodization with a Lorentzian line shape, resulting in a reduction in noise and better visualization of the 3 ATP peaks and the PDE and Pi peak. This spectrum is ready for peak quantification with the AMARES tool.

Figure 6. ³¹PMRS in healthy subjects

A) This figure shows the recovery of the phosphocreatine (PCr) concentration after its depletion with rapid quasi-static knee extension exercise. The line represents the fit of the exponential recovery function described in step 5.6, with the recovery time constant τ shown; this time constant is a well-established biomarker of mitochondrial oxidative function. B) The Bland-Altman analysis of the ³¹PMRS technique reproducibility demonstrates a mean difference \pm standard deviation of 1.03 ± 4.83 s for the PCr recovery time between trials; the coefficient of variation is 4.66.

Figure 7. ³¹PMRS in non-ambulatory subjects

A representative PCr recovery curve from the ³¹PMRS examination of a non-ambulatory subject is shown. Note that a PCr depletion of 64% was attained with this exercise protocol.

Figure 8. ³¹PMRS in CRSP subjects

A comparison of PCr recovery times demonstrates sequentially poorer mitochondrial oxidative capacity in control, non-diabetic, and diabetic subjects. The error bars represent the standard deviation.

DISCUSSION:

This paper describes a standard protocol for ³¹PMRS examination that affords serial and noninvasive *in vivo* measurement of skeletal muscle mitochondrial function. The protocol holds considerable appeal when considering the breadth of investigations targeting the growing burden of metabolic syndrome and its resulting morbidity and mortality. This ³¹PMRS protocol requires a minimal amount of scanner time and can be incorporated into comprehensive metabolic investigations in subjects at any center with commercially-available MRS facilities.

Critical steps within the protocol

Contraindications- Prior to MR examinations, it is crucial to screen subjects for potential contraindications. In addition to typical MR exclusion criteria, the following should be considered before implementing this protocol: 1) ipsilateral knee or hip implants (regardless of MR compatibility) to avoid artifacts, 2) conditions that restrict blood flow or oxygen delivery to the lower limbs (*e.g.*, peripheral artery disease), 3) an inability to perform resistive quadriceps extension exercise, and 4) an inability to lie supine for approximately 30 min.

Motion artifact reduction- The movement of the ^{31}P coil with respect to the subject's quadriceps and the movement of the subject's thigh relative to the table should be minimized. Ensure that the coil is securely fastened to the subject's leg and that the resistive straps are securely fastened to the exam table. Test this by ensuring that the subject's heel rises no more than 5 in. off the exam table during kicking and that there is no rotation of the coil during the exercise.

Acquisition

Exercise quality- The subject should exercise to achieve at least a 30% depletion in the PCr. For this protocol, we have determined that 30 s of exercise for ambulatory subjects and 60 s for non-ambulatory subjects achieves this target. We have observed that non-ambulatory subjects exert less force per kick and therefore require a longer interval for sufficient depletion.

Analysis- The methods described here provide a framework to minimize the subjectivity and maximize the automation. Selection of user input parameters for the analysis of the spectra should be made carefully in order to ensure reproducibility.

Modifications and troubleshooting

Quality of spectrum- If the spectrum appears noisy, ensure that the shim box is placed within muscle. Adjust the size and position of the shim box to improve the signal-to-noise ratio. Repeat the test acquisition as needed.

Quality of exercise- If the initial exercise results in insufficient PCr depletion, there are several modifications that can be used to troubleshoot: 1) the straps can be tightened, to increase resistance; 2) the subject can be instructed to kick faster, which increases exertion; or 3) the duration of sustained exercise can be increased. However, note that over-exercise can result in altered pH and could lead to acidosis, which can inhibit the OXPHOS recovery kinetics⁶¹. This can be avoided by limiting the exercise time to a maximum of 3 min.

Limitations of the technique

A muscle biopsy analysis permits the measurement of specific mitochondrial characteristics, such as mitochondrial content and size, as well as the mitochondrial maximum ATP synthesis rate. However, it is important to note that the *in vivo* measurement using ^{31}P PMRS represents an aggregate of these direct measures, in addition to extra-mitochondrial factors, such as the microvascular supply of oxygenated blood to the muscle. Thus, in situations where the status of the microvasculature is in question due to reduced oxygen supply or other factors, it would not provide an unambiguous indicator of mitochondrial status. Rather, it would indicate the *in vivo* status of the maximum oxidative ATP synthesis of muscle, which may reflect some combination of OXPHOS and microvascular issues.

A limitation of the exercise ^{31}P PMRS protocol detailed in this work is the lack of standardization of work output. This lack of standardization simplifies the apparatus required, and thus the implementation of this protocol. However, it comes at the expense of not permitting the quantitative evaluation of other parameters, such as strength and fatigability, and their

relationship to metabolic measures. As a result, varying levels of exertion could impact the PCr recovery time beyond the severity of the underlying mitochondrial defect. One can minimize these effects by ensuring sufficient PCr depletion and can further standardize the work output by using MR-compatible ergometers with adjustable resistance and measurable work outputs.

Significance of the technique with respect to existing or alternative methods

The ability to directly quantify mitochondrial function in skeletal muscle is the main advantage of the ^{31}P MRS technique when compared to standard metabolic exercise testing. Invasive muscle biopsy affords measurements in single fibers⁶⁶, though with attendant risks that make it less appealing for investigations requiring serial assessment. Approaches based on near-infrared spectroscopy⁶⁷ may be limited by penetration depth, particularly in obese patients, where as little as 5 mm of fat attenuates the NIRS signal by 20%⁶⁸. Furthermore, the technique does not lend itself to the multidimensional assessment of muscle and other systems afforded by MR-based techniques. Additionally, unlike invasive biopsy methods for quantifying muscle energetics, this non-invasive and non-destructive measure permits repeated measures of the metabolic status in intact muscle, making it advantageous for the evaluation of subject populations and therapeutic interventions.

Future applications

Potential applications after mastering this ^{31}P MRS technique include the evaluation of diseases with specific mitochondrial defects or any of a broad range of metabolic disorders. In patients with poor cardiac output, current techniques can identify impaired functional capacity but cannot establish the level at which the dysfunction occurs (*e.g.*, the skeletal muscle, heart, or lungs). It would be particularly interesting to develop integrated protocols that combine ^{31}P MRS with metabolic measures and cardiopulmonary assays to identify the root causes of subject-specific reduced capacity in order to facilitate personalized therapies.

We have detailed examples of important targeted therapies and interventions that would benefit from the use of *in vivo* markers of mitochondrial function. A standardized ^{31}P MRS exercise protocol, such as the one detailed above, is an important step for more widespread use of this important *in vivo* marker of skeletal muscle mitochondrial capacity in both basic and intervention studies.

ACKNOWLEDGMENTS:

This work was supported in part by a Davis Heart and Lung Research Institute Trifit Award, as well as by the Intramural Research Program of the NIH National Institute on Aging.

DISCLOSURES:

The authors have nothing to disclose.

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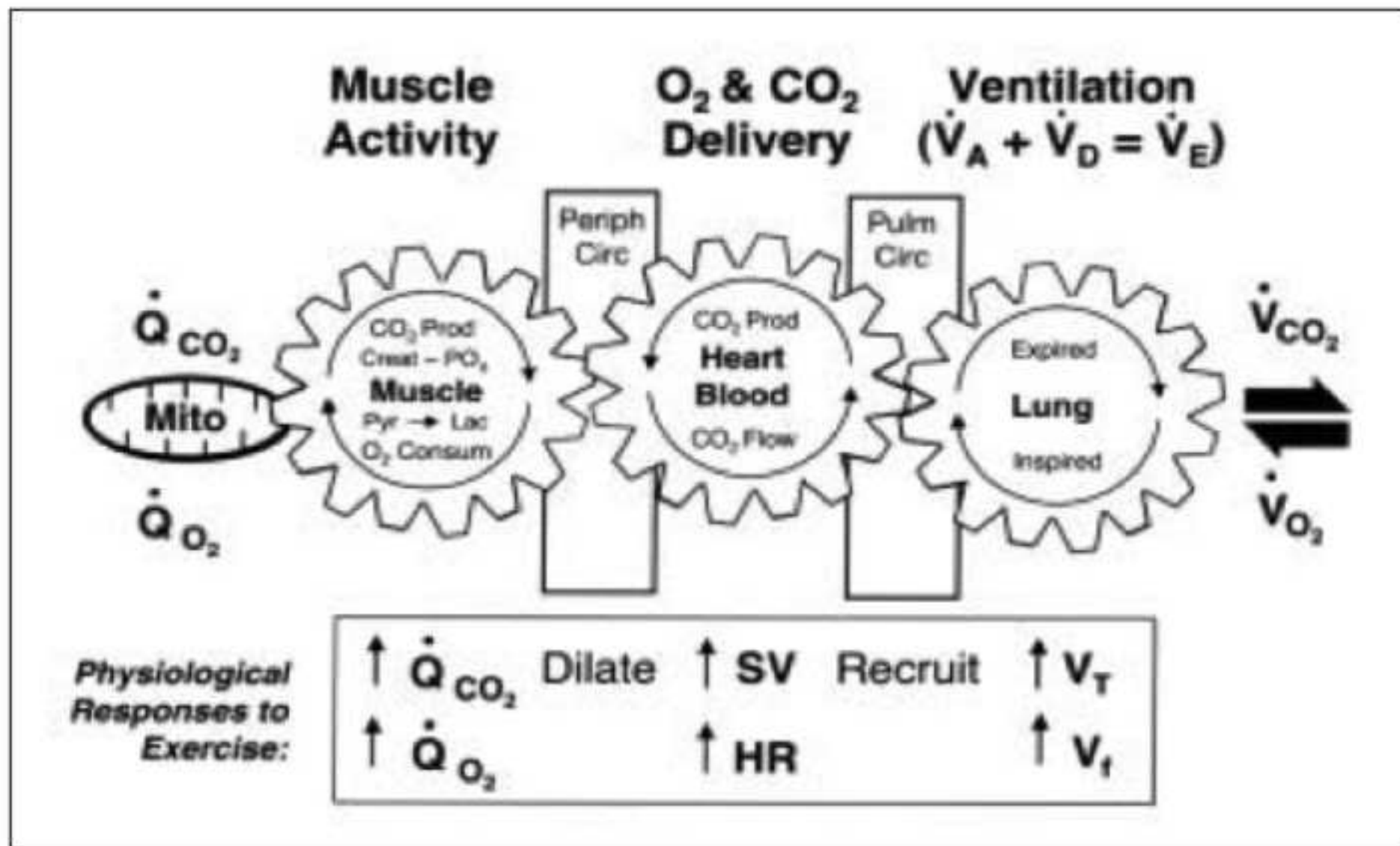
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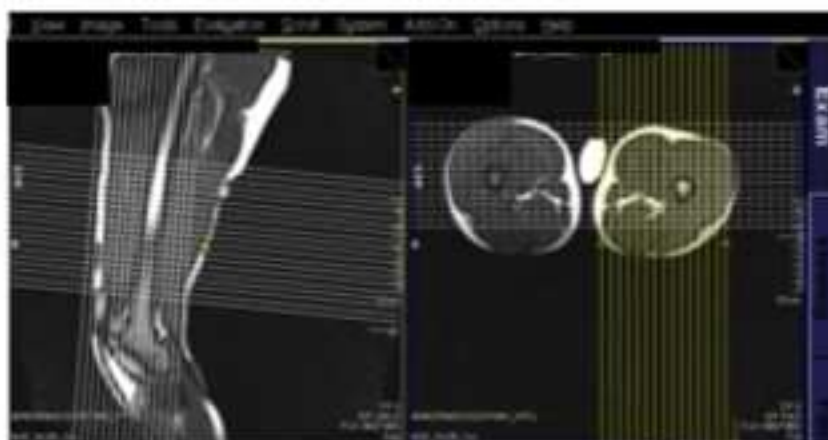




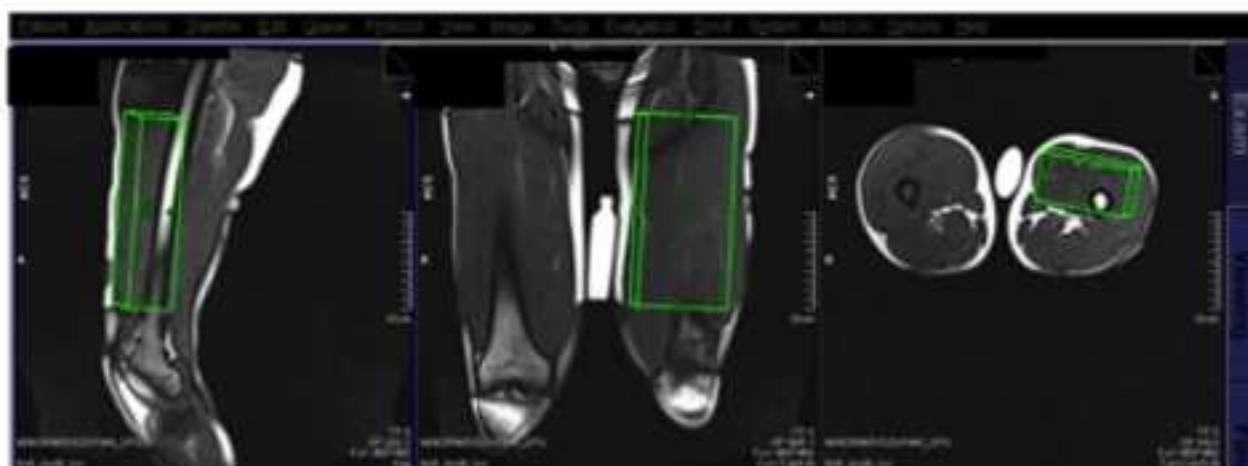
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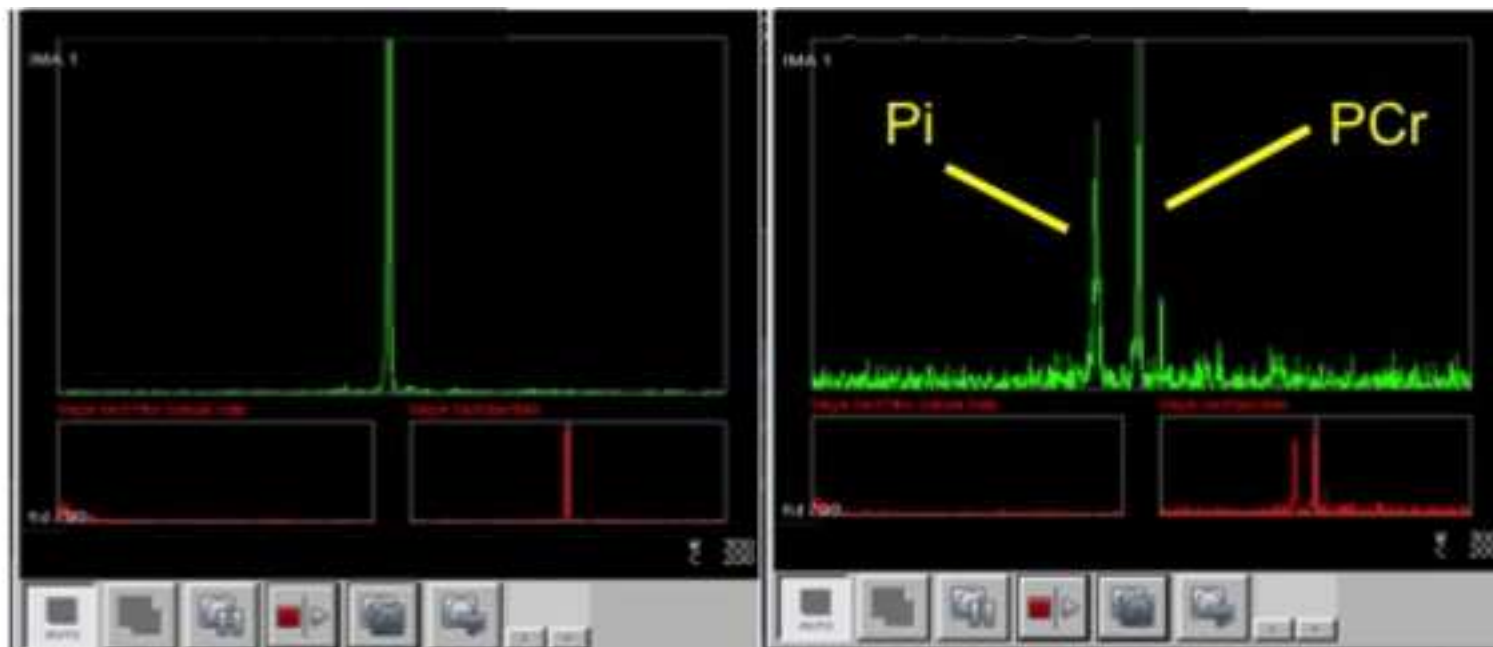
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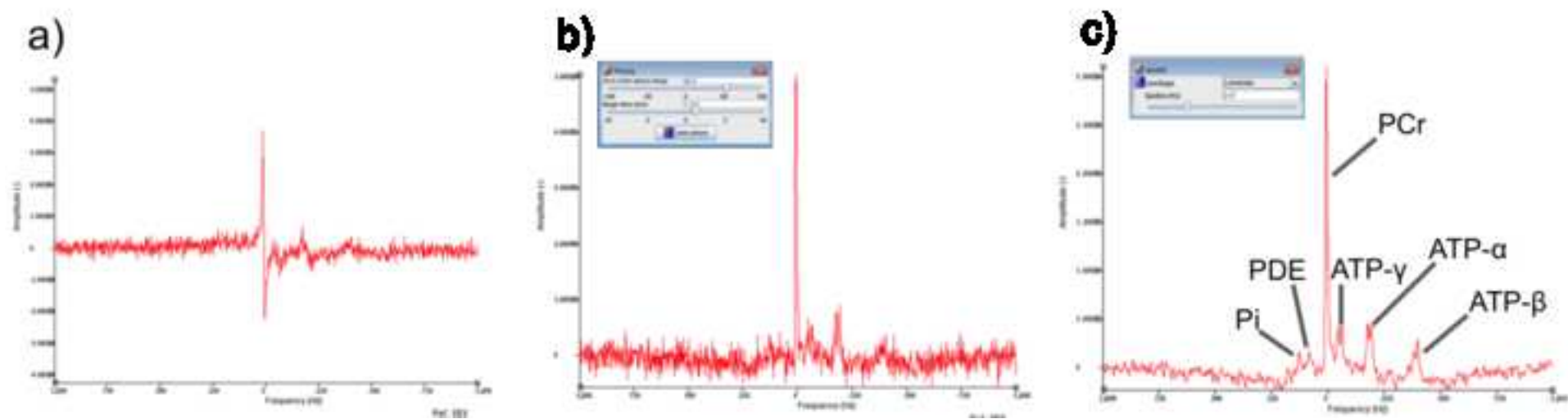


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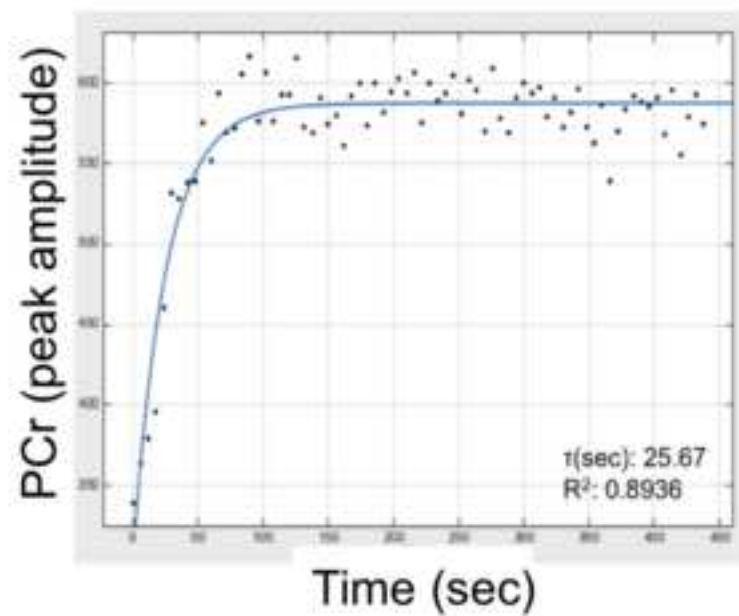


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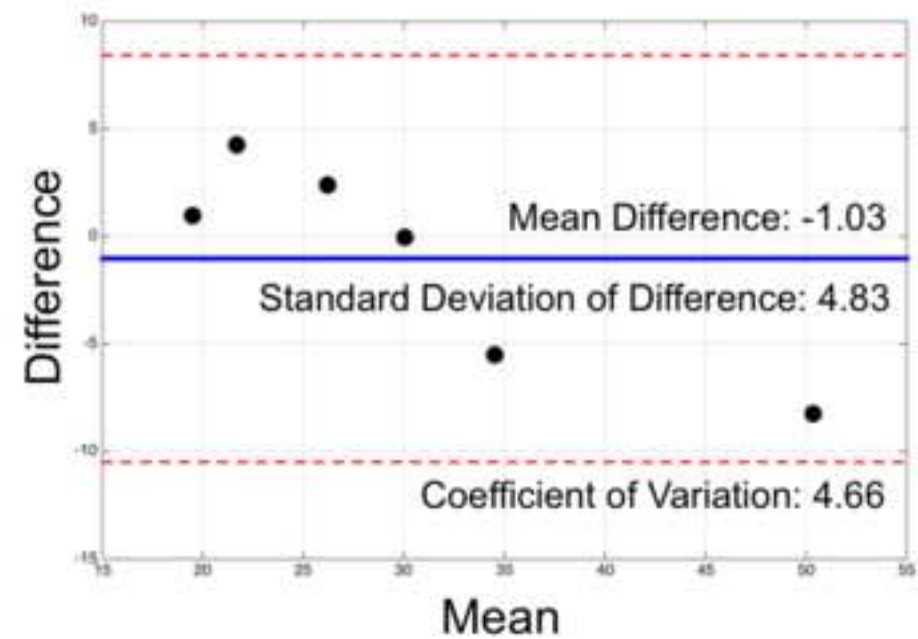




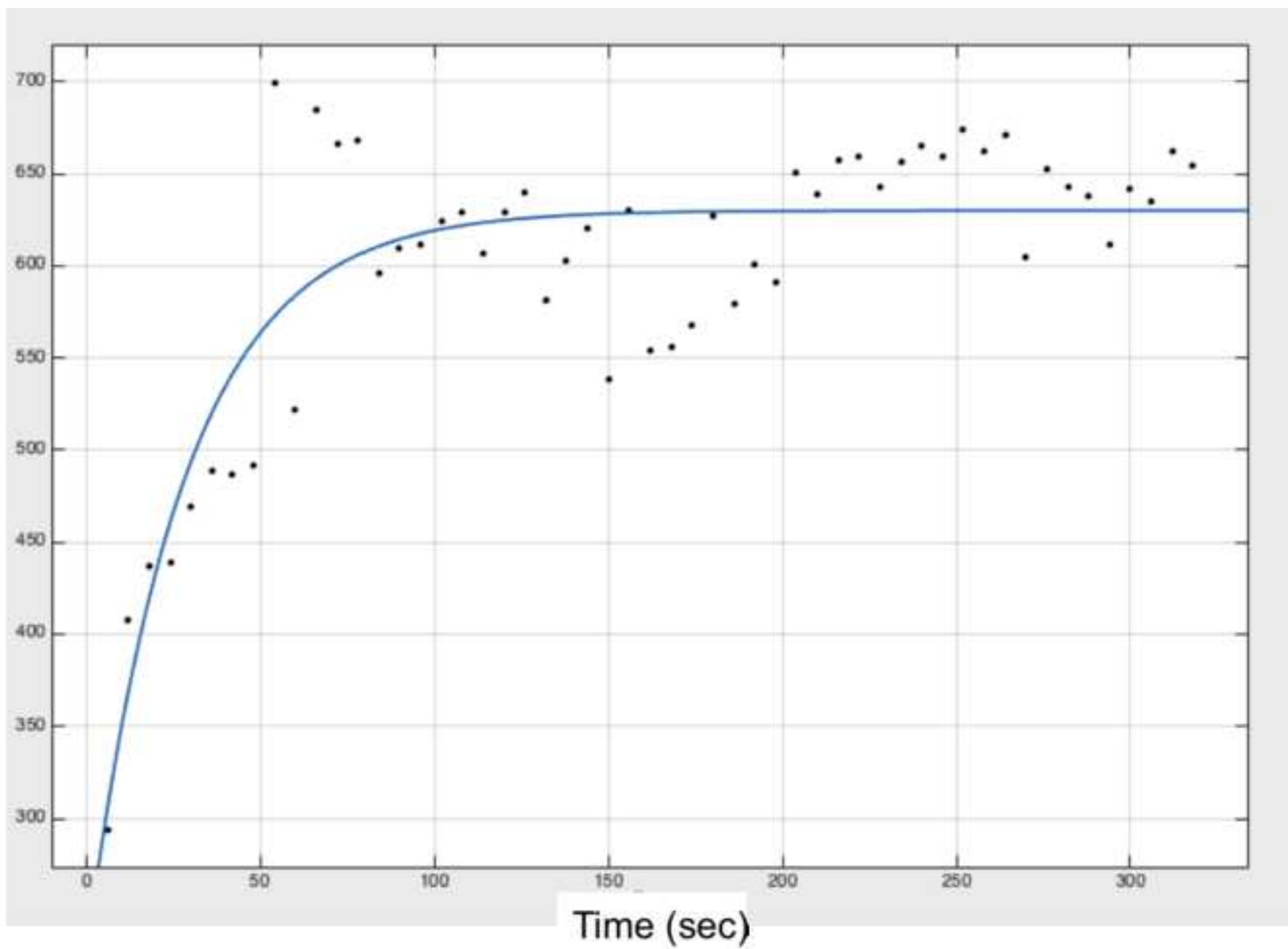
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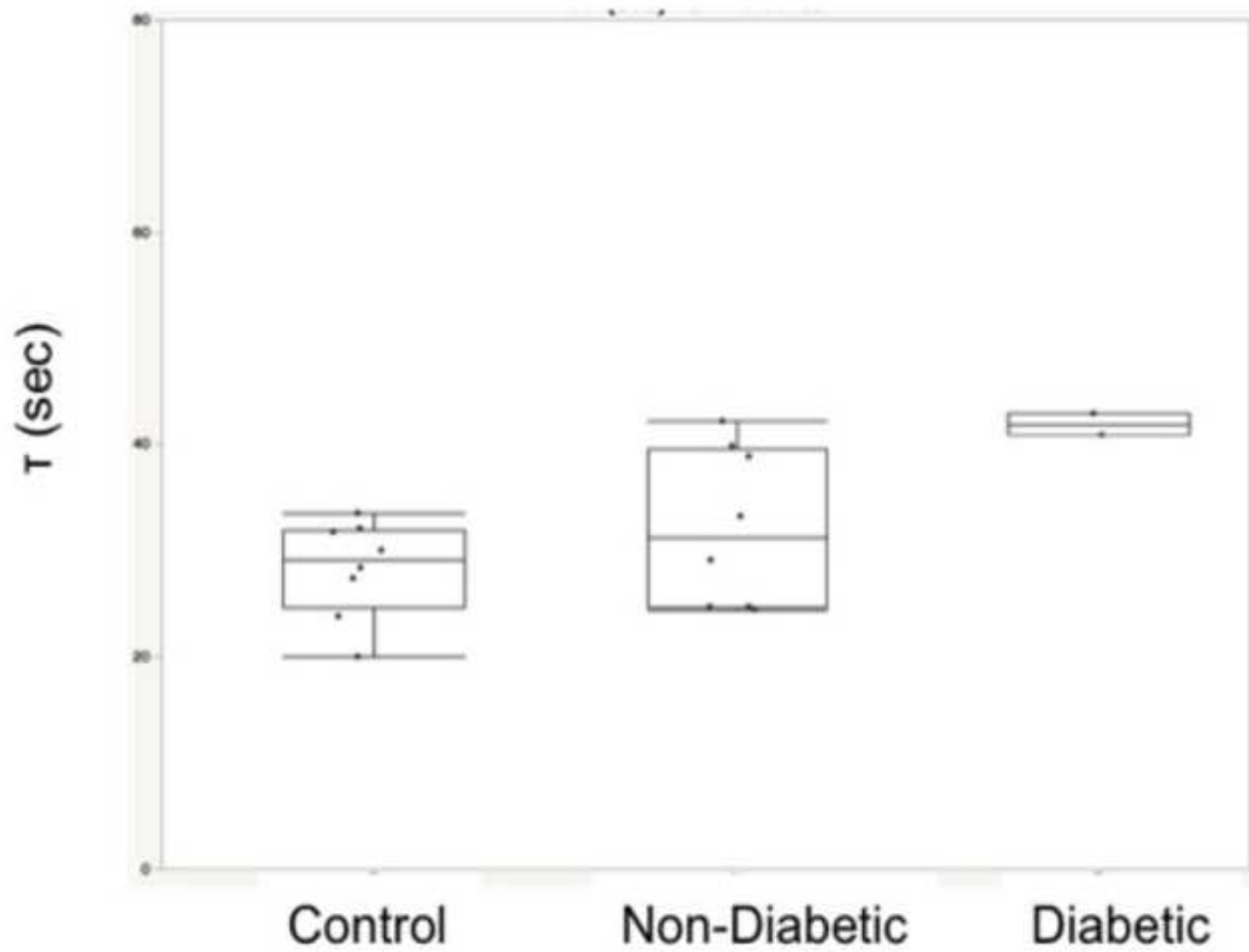


b)



PCr (peak amplitude)





Name of Material/ Equipment	Company	Catalog Number	Comments/Description
1.5 T MR Scanner	Siemens		manufacturer will not affect results
10 cm 31P transmit-receive coil, 1.5T compatible	PulseTeq		manufacturer will not affect results
3 fl oz Baby Oil	Johnson & Johnson		manufacturer will not affect results
Foam triangle cushion (Knee)	Siemens		manufacturer will not affect results
(3) plastic buckle resistive straps; table to table	Siemens		manufacturer will not affect results
(1) plastic buckle resistive strap; self-connecting	Siemens		



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- **Please keep the editorial comments from your previous revisions in mind as you revise your manuscript to address peer review comments. For instance, if formatting or other changes were made, commercial language was removed, etc., please maintain these overall manuscript changes.**
- **Formatting:**

-Please do not use duplicate sentences in the short and long abstracts.

No sentences are duplicated in the short and long abstracts.

-1.2 – Please make 31 superscript.

We have corrected this line to read: “Plug the ³¹P coil into the in-table coil connector at the end of the exam table closest to the bore.”

-4.10 – Which step? Is this step 4.6?

The instruction refers to step 4.5; the text now states this more clearly: “Post-exercise T1 image: repeat the pre-exercise axial T1 image (step 4.5) using the same acquisition parameters.”

-Please include spaces between all bullet points in the protocol. See 4.11.1 and 4.11.2.

We have included spaces between all steps and sub-steps.

-Please use size 12 font. Parts of the results are in a different font and size from the rest of the document.

The font and size have been corrected to Calibri, size 12 for the entire document.

-All latin phrases (ie in vivo, in vitro) should be in italics.

All latin phrases have been changed to italics

•Grammar:

-Please make sure all sentences end with a period (see 1.1, 4.11.2, 4.11.3).

All sentences end with a period.

-3.1 – “Explain the subject”

This line has been corrected and now reads: “Explain to the subject that the exercise protocol consists of three phases: an initial baseline phase, a short intense exercise phase, and a recovery phase.”

-3.4 – “PCR”

This has been corrected and now reads : “Observe the **PCr** peak height in the acquisition viewer window, and also view it upon completion of the exercise sequence.”

-4.10 – Please clarify – the phrase at the beginning of the sentence seems out of place.

This instruction has been clarified and now reads: “Post-exercise T1 image: repeat the pre-exercise axial T1 image (step 4.5) using the same acquisition parameters.”

-Line 547 – “?MOXPPOS”

This line has been corrected “OXPHOS”. We also have replaced ‘mOXPHOS’ with ‘OXPHOS’ throughout, to be more consistent with widely used and accepted terminology.

•Additional detail is required:

-2.6 – Where is the baby oil placed?

This instruction has been clarified: “**Secure the baby oil to the medial aspect of the thigh** with the same straps used to secure the coil to the leg. This facilitates scan localization.
”

-4.1, 4.2 – How does one acquire this? Are these steps performed by software? If so, how?

4.2.1 – How is the orientation adjusted?

-4.4.1 – How does one place the shim box?

4.4.2 – How are images used for this? What should one see to identify the “sensitive region?” Then how is the shim box adjusted? Is it moved or are the coordinates adjusted?

-4.4.3.1 – How is a spectrum obtained?

-4.6.1 – What example settings are used here?

Comments on steps 4.1 to 4.6.1: These are very basic steps in MR scanning, and can be easily performed without further clarification by anyone with nominal technical training allowing use an MR scanner. We expect those without prior MR experience will perform these experiments under the supervision of a trained MR technician.

-4.7.1 – How long does the subject kick here? Or are they actually beginning to kick in the next step? This is not clear – actions should be mentioned in the order in which they occur.

This is a rest step, and the subject does not kick during this time. The instructions have been clarified in the manuscript: “**Rest:** Apply the shim settings from the previous scan and set the sequence to acquire 20 measurements. Instruct the subject to begin kicking after a countdown. Subject remains at rest for 2 measurements.”

•Results: Please define the error bars (SD, SEM, etc.) in Figure 8.

The caption for Figure 8 is now: "Comparison of PCr recover times demonstrates sequentially poorer mitochondrial oxidative capacity in control subjects, non-diabetic and diabetic subjects. Error bars represent standard deviation."

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- **NOTE:** Please include a line-by-line response letter to the editorial and reviewer comments along with the resubmission.

Reviewers' comments:

Reviewer #1:

Manuscript Summary: This manuscript addresses the need for non-invasive techniques to assess mitochondrial function and metabolism. 31P MRS has a long pedigree in the context of exercise physiology and has improved our understanding of healthy muscle energetics. Alternatives for painful biopsy are needed, particularly for patients with genetic or acquired myopathies who often require longitudinal follow-up to assess the effectiveness of therapies on muscle metabolism. While not new, the protocol suggested by the authors offers a relatively straightforward approach for introducing 31P MRS into the clinic. The authors provide reproducibility data from healthy volunteers; the clinical feasibility of the technique is demonstrated in small groups of patients with genetic (Friedrich's ataxia) or acquired (metabolic syndrome) pathologies.

Major Concerns: None.

Minor Concerns:

-1. Materials and Preparation

1.1) (pg 5, line 216): "prior to the experiment" rather than "prior to experiment"

This line (line 256) has been corrected: "Ensure that all necessary materials are available prior to the experiment. (Figure 2)"

1.4) (pg 6, line 224): "farthest" rather than "furthest"

This line [\(line 264\)](#) has been corrected: **“Place a head pillow at the other end of the MR exam table, farthest from the bore, for subject comfort.”**

2. Subject Positioning

2.1) (pg 6, line 228): "lie supine" rather than "lay" (this should be checked throughout the manuscript, eg line 258)

We have corrected this throughout the manuscript.

-2.9) (pg 6, line 251): "centering light" might not be the conventional term here; "laser light guide" might be preferable?

We have corrected this. The line [\(line 291\)](#) now reads: “Use the **laser light guide** to delineate the center of the coil, and move the table using this centering landmark to magnet isocenter.”

3. Exercise

3.4) (pg 7, line 271): consider replacing the idiom 'rule-of-thumb' with 'general guideline' (or something less colloquial)

We have changed the line [\(line 316\)](#) to read: “NOTE: A **general guideline** is that an approximate 30% drop in PCr peak height corresponds to a Pi peak that is 50% of the height of the PCr peak.”

4. Scan Protocol

4.7.2 (line 327): the note to record the start and end of each exercise interval is important; should this note appear earlier in the protocol, e.g., beginning of 4.7?

We have moved this note to the beginning of the section [\(line 370\)](#).

-4.11 Saving Data

4.11.2 (line 369): "If using a scanner" ? Is this in reference to a specific scanner/vendor?

We have indicated that these instructions are specific for a Siemens scanner. “If using a Siemens scanner, select all spectroscopy acquisitions in the Navigator window.” [\(line 426, step 4.11.2\)](#)

-Results and Fig 6B: reproducibility; the authors indicate a mean difference and stdev of 1.03 +/- 4.83s. I presume this refers to the mean difference and stdev of the recovery time constant, but this should be stated explicitly in the Results section (pg 10, line 406) and in the caption for figure 6B.

The line [\(line 466\)](#) in the results section has been modified and now reads: “Bland-Altman analysis of PCr recovery time demonstrates a mean difference±standard deviation of 1.03±4.83s and between trials coefficient of variation of 4.66.”

The caption for 6b has been modified: “B) Bland-Altman analysis of ³¹PMRS technique reproducibility demonstrates mean difference±standard deviation of 1.03±4.83s for the PCr recovery time between trials the coefficient of variation is 4.66. ”

-Results, pg 10, lines 417-418: "Additionally, note oscillations around the fit that are caused by the progressive

loss of muscle control characteristic of this disease." Does this comment refer to the sinusoidal pattern in the recovery curve depicted in Figure 7? If so, please move the reference to Fig 7 from line 420 to the end of this sentence on line 418.

Yes, this refers to the sinusoidal pattern and the reference has been moved as suggested. [\(line 481\)](#)

-With respect to the oscillation observed in the participants with ataxia, is there any advantage to removing the oscillation (detrend) prior to fitting the curve to obtain the recovery time constant?

This is an interesting consideration that warrants evaluation in a larger cohort of patients with ataxia.

-Results, pg 10: very minor style suggestion: the latter part of the Feasibility Study section (lines 434-437) would benefit from the addition of articles ("the"): e.g. "The PCr recovery time constant..." instead of "Time constant of PCr recovery..." "The percentage of intramuscular fat..." instead of "Intramuscular fat percentage..." etc.

All of the suggested modifications have been made.

Additional Comments to Authors: N/A

Reviewer #2:

Manuscript Summary: The manuscript describes a simple method for estimating quadriceps ³¹P MRS PCr recovery kinetics following exercise as an estimator of skeletal muscle mitochondrial oxidative capacity (mOXPHOS). This method is relative old (~ 30 years) but is not widely used, largely due to the availability of ³¹P capable MRS scanners. The manuscript describes the technique adequately. However, the limitations and assumptions inherent in inferring mOXPHOS capacity from PCr kinetics are not well described. Simple reproducibility studies are provided for healthy participants as well as some comparative data between patients and controls

Major Concerns: Overall more emphasis needs to be placed on how this method can be quality controlled. For example, how accuracy can be known when cellular PO₂ is not measured, or how between site precision could be controlled or a multisite clinical study.

1. I disagree that ³¹P MRS measurement provided is a "direct measure of OXPHOS capacity". It measures PCr resynthesis following exercise which contains at least two assumptions: 1) PCr is resynthesized through the ATP hydrolysis by the creatine kinase reaction using ATP solely provided by oxidative phosphorylation; and 2) that the P/O₂ ratio is constant. While in all likelihood these assumptions are met under the conditions of the experiment; the method is not direct. A direct method would assess intramuscular O₂ consumption recovery e.g. as seen measured in single fibers by Wust et al., J Physiol. 2013 Feb 1;591(3):731-44; or possibly by near-infrared spectroscopy e.g. Ryan et al. J Physiol. 2014 Aug 1;592(15):3231-41. These papers should be discussed and cited in the main text.

³¹P MRS is described as 'direct' in this manuscript to differentiate this technique from clinical functional measures, like VO₂ measurements, which indirectly measure mitochondrial activity. However, the authors agree with the point that ³¹P MRS does not measure oxidative phosphorylation directly, and have modified line 74 appropriately: " ³¹PMRS produces a **noninvasive**, *in vivo* measure of OXPHOS capacity in human skeletal muscle, rather than alternative measures obtained from explanted and potentially altered mitochondria via muscle biopsy, and relies upon only modest additional instrumentation beyond what is already in place on magnetic resonance scanners available for clinical and translational research at most institutions."

The goal of this manuscript is to thoroughly describe a ^{31}P MRS technique that can be used *in vivo* in humans with illustration of potential applications of this technique. We have added mention of the two other methods in the main text under 'Significance of the technique with respect to existing/alternative methods', noting potential limitations of the single fiber assay (invasive with attendant risks that make it less appealing for investigations requiring serial assessment) and NIRS-based approaches (penetration depth may be limited, particularly in obese patients where as little as 5 mm of fat attenuates the NIRS signal by 20% (Hamaoka T *et al*, Philos Trans A Math Phys Eng Sci. 2011), and the technique does not lend itself to the multidimensional assessment of muscle and other systems afforded by MR-based techniques).

2. An additional crucial assumption, which is not addressed, is that mitochondrial O₂ delivery is not limiting to OXPHOS and therefore to PCr recovery. It has been shown using lower body positive pressure and hypoxic gas breathing that the PCr recovery rate constant is sensitive to O₂ delivery: PCr recovery after exercise is slowed by hypoxia or reduced blood flow. The recovery kinetics are also complicated during a metabolic acidosis. These need to be mentioned and any method needs to be able to account for or monitor adequate O₂ supply.

We have designed this exercise protocol to avoid metabolic acidosis, and have provided methods to ensure appropriate pH throughout the study. Impaired oxygen delivery could certainly impact the measurement; we have added to the text the exclusion of patients with "conditions that restrict blood flow or oxygen delivery to the lower limbs (e.g. peripheral artery disease)" (line 578) that our group and others use to minimize any confounding effect of impaired O₂ delivery. The limitations section also emphasizes that the PCr recovery rate constant is sensitive to O₂ delivery "Thus, in situations where the status of the microvasculature is in question, due to reduced oxygen supply or other factors, it would not provide an unambiguous indicator of mitochondrial status but rather represent an indicator of the *in vivo* status of the maximum oxidative ATP synthesis of muscle that may reflect some combination of OXPHOS and microvascular issues." (lines 618-622)

3. The sentence starting on line 180 is underdeveloped. You need to discuss: 1) by how much PCr flux is "dominated" by OXPHOS (not lactate-associated ATP production or other non-oxidative phosphorylative process), and 2) why PCr recovery kinetics represent OXPHOS capacity. This latter assumption only holds true for a first-order rate reaction (Michaelis-Menten reaction). OXPHOS control in muscle appears to be dominated in recovery by M-M first order kinetics (e.g. see Korzeniewski and Rossiter J Physiol. 2015 Dec 15;593(24):5255-68.), therefore the assumption is valid, but this needs to be proposed and discussed.

We have cited the suggested work amongst additional references (line 207) that support: 1) a major component of PCr recovery can be attributed to OXPHOS and a smaller component (7-10%) from other sources, 2) PCr recovery can be modeled using a monoexponential model, and 3) OXPHOS control in muscle is dominated by the first-order Michaelis-Menten reaction.

4. mOXPHOS is actually linearly related to the rate constant (k) of PCr recovery not the time constant (line 182). $k=1/\tau$. Therefore OXPHOS capacity is, in theory, hyperbolically-related to τ of VO₂ (and by implication τ PCr). This theory was proven in single cells in the presence of unlimited O₂ by Wust et al., J Physiol. 2013 Feb 1;591(3):731-44. 5. Line 202 and onwards. There is little discussion of alternative methods such as biopsy and NIRS assessments. Please highlight the advantages/disadvantages of each method.

With the preponderant use of the time constant (τ) in the literature on *in vivo* muscle PMRS, we respectfully adhere to the use of τ in describing PCr recovery rather than switch to the rate constant. The specifics of the model are discussed later in the text (line 447). These are excellent references that we have now incorporated into the text (lines 636-647).

Minor Concerns: Line 74 see major comment 1

We have expanded the discussion on alternative techniques as described under the response to major comment 1.

88 specialized equipment.

Line 88 (now line 86) is: “The goal of this work is to outline a reproducible method to measure *in vivo* skeletal muscle mitochondrial function in individuals possessing a wide range of abilities.”

Mitochondrial impairment is 89 Friedrich's Ataxia is a bizarre condition to highlight, without mentioning far more common conditions abnormality in muscle OXPHOS capacity such as chronic heart, lung or kidney diseases, cachexia, mitochondrial myopathies etc. How about simple healthy aging?

The overall goal of this manuscript is to describe a method with many potential applications, some more common and of greater interest to certain investigators than others. We along with the patients with FA whom we serve take issue with its characterization as a ‘bizarre condition’. Rather, FA as a condition whose distinct mitochondrial defect produces phenotypic changes similar to a broad range of disorders (e.g. diastolic heart failure, diabetes) makes it extremely relevant to this work. We have also highlighted other, more common disorders (i.e. aging, diabetes) as suggested (lines 102-123).

104 How then do you explain the common finding in animal models that OXPHOS capacity is increased on exposure to a high fat diet? E.g. Jian et al. Diabetes. 2014 Jun;63(6):1907-13.

The intent of line 104 (now line 112) is to describe a potential reason for reduced OXPHOS in the setting of lipid overload. There are instances of exceptions, and paradoxical findings (i.e. the athletes paradox, or the study referenced above). These interesting phenomena demonstrate the need for more accurate *in vivo* techniques with which to better understand instances where obesity does vs. does not associate with increased risk of cardiovascular disease.

105 I don't agree with the concept of "number" of mitochondria. Mitochondria are a reticular conjoined structure. Their number is a meaningless construct.

We have modified line 106 (now line 115) to read “This reduction in mitochondrial skeletal muscle OXPHOS capacity in the setting of lipid overload is accompanied by a decline in the quantitative (content and biogenesis of mitochondria) and qualitative...”

113 changes in mitochondrial oxidative capacity are

Line 113 is “However, it remains unclear whether **changes in mitochondrial capacity are** a cause or a consequence of insulin resistance.”

124 cardiovascular capacity for what? Oxygen transport and utilization? Blood flow? What? Please be specific.

We have changed ‘cardiovascular capacity’ to ‘cardiac output’.

155-157 I am worried here that you are mixing the notions of cardiac mOXPHOS and skeletal muscle mOXPHOS. These two require very different approaches for measurement.

The authors understand and acknowledge that the particular technique described here cannot be used for evaluation of OXPHOS in cardiac mitochondria. However, “Measurement of skeletal muscle OXPHOS capacity as detailed herein is readily implemented and robust; **coupled with the significance of skeletal muscle OXPHOS in**

heart failure, these features **makes it an appealing biomarker in comprehensive studies of heart disease³⁶.**" (line 161) The authors believe that this is a crucial, and often overlooked point prompting emphasis in the manuscript.

181 see major comment 3

We have cited additional references demonstrating that 1) a major component of PCr recovery can be attributed to OXPHOS and a smaller component (7-10%) from other sources and 2) PCr recovery can be modeled using a monoexponential model. (line 200-207)

192 impaired mitochondrial oxidative capacity in. [N.B. mitochondria have several roles in the cell; you need to say which capacity you are talking about. You could be talking about calcium retention capacity for example].

We have clarified this line: "For instance, these techniques have shown impaired OXPHOS in subjects with type 2 diabetes." (line 217)

234 Why left leg? Why not dominant or non-dominant leg in all participants?

While our setup uses the left leg, we have removed specification of 'left' when mentioning the leg in this protocol.

271. see major comment 2. This type of severe intensity ballistic exercise can drive down PO₂ very rapidly and therefore may limit PO₂ availability for PCr resynthesis during exercise recovery. This may provide an artifact for extrapolation to OXPHOS capacity. Simply requiring a 30% drop in PCr peak height may still be accompanied by O₂ delivery limitation.

We have added mention of excluding patients with: "2) conditions that restrict blood flow or oxygen delivery to the lower limbs (i.e. peripheral artery disease)" (line 578) to minimize any confounding effect of impaired O₂ delivery. Our lab and others have found that intact blood flow and avoidance of acidosis should prevent O₂ delivery limitation, though adding perfusion imaging is certainly a technique that can be added to the MR protocol if this is a concern for a given study population.

315 An improved protocol would acquire unsaturated GREs with full relaxation to first determine resting PCr peak area with unsaturated acquisitions. This allows the assumption of PCr:bATP peak ratio area to be applied (often 8.2 mM bATP is used) and estimate quantitative resting and exercise PCr concentrations.

Thank you for this suggestion. We will explore this approach in future work.

334 6 averages is not a whole number fraction of 20 seconds. How can the acquisitions during exercise be controlled so that the exercise is terminated exactly at the point at which one set of 6 acquisitions is complete and the other about to start. Not clear.

We use 4 averages; the 6 was a typographic error.

340 PCr depletion is not a measure of quality control. Signal to noise (variability) or precision (versus some known value) would be a suitable measure of quality control. The 'quality' of the protocol should be judged on the basis of some quantitative indicators of precision and accuracy of the method.

This step refers to the quality of the exercise itself, not spectral or data quality. Steps to ensure quality of the overall acquisition are described in step 4.9.2 **“Verify that PCr peak height is the same at beginning of rest and end of recovery (typically <10% difference is desired).** This ensures that there was negligible loss of field homogeneity during acquisition.”

391 why not fit this equation with k in the exponent? k is directly linearly proportional to OXPHOS capacity.

We use tau given the preponderance of literature using the time constant rather than k.

403 where these studies repeated on different days or the same day. Different days would be preferable.

Studies were repeated on different days (within 1 week); this has been added to line 456.

409 this only described reproducibility in healthy volunteers. In patients with O2 delivery constraints this protocol may be invalid for reasons discussed above.

We have included an additional exclusion criterion for “2) conditions that restrict blood flow or oxygen delivery to the lower limbs (i.e. peripheral artery disease)” (line 578).

518 the rationale for this 30% depletion target is not explained.

One rationale for this target depletion is that reliable fits of the exponential recovery require sufficient dynamic range of PCr loss during exercise. We have empirically determined that a general guideline of ~30% depletion is sufficient for this purpose on our typical signal-to-noise ratio.

542 mitochondrial number is not a valid variable. Volume-density perhaps? 548 ?

We have modified line 106 to read: “This reduction in mitochondrial skeletal muscle OXPHOS capacity in the setting of lipid overload is accompanied by a decline in the quantitative (content and biogenesis of mitochondria) and qualitative...”

560 see major point 1. Discuss NIRS

Done.

Additional Comments to Authors: N/A

Reviewer #3: *Manuscript Summary:* This manuscript from Kumar and colleagues describes the use phosphorus magnetic resonance spectroscopy to assess skeletal muscle oxidative capacity in vivo in human participants. ³¹P-MRS has been extensively used in both rodents and humans to assess skeletal muscle metabolism, and thus this experimental video will provide a useful tool for the rookie MRS user, although instrumental differences between magnets will make exact replication more difficult.

Introduction -Line 86-88: Can you really claim this this technique doesn't require specialized equipment? It is required that you have a magnet capable of multi-nuclear spectroscopy (not always the case especially in clinical situations) and a tuned coil for phosphorous detection.

In this case, specialized equipment refers to MR-compatible ergometers and other additional equipment beyond the necessary materials for phosphorous spectroscopy. The authors understand that access to MR and spectroscopy equipment is limited, and we have deleted this portion of the sentence.

-Line 93-113: While mitochondria have been associated with many disease states, impaired maximal capacity for oxidative phosphorylation is rarely the cause for disease. This is particularly evident in the case of insulin resistance/T2D where oxidative capacity is not impaired during the development of insulin resistance, but appears only with chronic T2D, suggesting this is not causative (See work from Fisher-Wellman et al. Diabetes 2014). Furthermore, the description of decreased oxphos capacity causing lipid accumulation is misleading and not well supported by the literature. Most cells, particularly skeletal myocytes, normally function with a basal energy demand which is far lower than the oxidative capacity. It is not clear how the authors link modest reductions in the maximal capacity associated with T2D would result in lipid accumulation. Wouldn't there have to be alterations in the basal 'energy balance' for this to occur? Clearly this is not the point of this methods paper, but these topics are often misconstrued in the literature.

The use of this technique is more to observe changes in mitochondrial function in the setting of T2D and other diseases, rather than determining a mechanism for these changes. We agree that statements regarding causation could be potentially misleading and have taken care to avoid this in the manuscript.

Line 130-149: It is unclear why there is a paragraph discussing mitochondria and cardiac dysfunction since the methodology described cannot be used to assess cardiac mitochondria function. Granted there are capabilities for ³¹P-MRS in cardiac metabolism, the exercise/recovery protocol is not possible. It is suggested that this paragraph be removed.

The authors understand and acknowledge that the particular technique described here cannot be used for evaluation of OXPHOS in cardiac mitochondria. However, "Measurement of skeletal muscle OXPHOS capacity as detailed herein is readily implemented and robust; **coupled with the significance of skeletal muscle OXPHOS in HF**, these features **makes it an appealing biomarker in comprehensive studies of heart disease.**" (line 161-164) The authors believe that this is an often-overlooked point.

Line 172: phosphorus in ATP does not contain 'high energy'. This is an enormous misconception in bioenergetics. In bioenergetics, the potential energy for cellular work comes from the extent to which the observed mass action ratio is displaced from equilibrium (i.e. Δ GATP), which in the case of skeletal myocyte cytoplasm is ~-60kJ/mol. This is where the driving force for cellular work is derived, not the 'phosphate bond'.

We describe phosphorous as a component of high-energy substrates. The line does not imply that phosphorous itself contains the energy to do useful, cellular work. Line 172: "Magnetic resonance spectroscopy tuned to **phosphorous (³¹PMRS), an endogenous nucleus found in various high-energy substrates** within cells throughout the body". (line 186)

Line 180: The authors should more clearly describe the energetic model used in this protocol. Upon cessation of exercise, ATP production is primarily driven by mitochondrial oxidative phosphorylation. This ATP is 'shuttled' from the mitochondrial matrix to the cytoplasm where it can be utilized by CK to resynthesize PCr until the cellular equilibrium for PCr/tCr is reached (resting). The authors should also mention the potential for other sources to contribute ATP during the recovery phase (see work from Sean Forbes and Ron Meyer which shows ~7-10% contribution from glycolytic sources).

Thank you for these excellent references. We have referenced the work of Forbes and Meyer in lines 202 & 207.

Line 185: Several pivotal validation studies are not cited including: Meyer (1988) Am J Physiol McCully (1993) J Appl Physiol Larson-Meyer (2000) Muscle and Nerve Lanza (2011) J Magnetic Resonance Imaging Layac (2016) AJP Endocrinology and Metabolism

We have included references to these important validation studies in line 207.

Line 182-184: There are several approaches for modeling this approach including the very simple calculation of a time constant. It is recommended that the authors provide a discussion regarding the various analytical approaches and briefly the benefits and limitations. See elegant work from Gwenaél Layec and Russ Richardson.

We have included references to these studies in the manuscript. Further discussion of the model and calculation of the time constant has been included in the methods step 5.4.

Protocol

General: It is suggested that the authors provide some general background regarding the safety of MR testing. Many safety precautions are taken to ensure that participants can have MRI testing and all equipment used and personnel involved in testing are cleared. Clearly the testing will occur under the supervision of an MR technician, but I think it is critically important to provide a little background on this given its importance.

Thank you for this important point. We have added this at line 296-297: "It is critically important that all procedures involving MR equipment must be performed by adequately trained personnel adhering to the highest standards of MR safety," and cited MR safety guidelines.

Line 239: These instructions should be described for a surface coil. Volume coils will be slightly different. It should also be noted that testing of other muscle (besides the VL) is possible depending on the positioning of the surface coil.

The instructions in this manuscript are specific to the equipment indicated (i.e. 10 cm surface coil). The exercise method described in this manuscript is specific to the VL and therefore we did not include a discussion of testing other muscles. Testing of different muscle groups could be an interesting follow-up to this publication.

Line 243: Unsure what 'baby oil' is used for? Localization can be easily performed with scout images...

The baby oil is used to mark the position of the coil for localization on the proton image. This position is used to guide the selection of the shim volume for B0 field homogenization. Some phosphorous coils come equipped with a fiducial marker. This is a simple alternative approach for coils that do not.

Line 277: Actually, using the recovery kinetics approach for PCr, it is not necessary to account for differences in exercise duration because the mono-exponential model is used for fitting (i.e. first-order metabolic system). The only aspect that needs checking is to see if pH has changed too much...

The duration of exercise is important to this technique because it informs us of the exact end of exercise PCr measurement, which is crucial for analysis.

-Line 288: These sequence parameters will be specific for their equipment. This should be noted here for readers/viewers. It is also possible to measure PCr kinetics with faster time resolution which might be required for those participants with faster PCr recovery.

We have generalized the descriptions in this section to ensure that any specific values can be replicated on different systems (even if the technique to set those values may be different). We have also ensured that any system specific instructions have been noted as such in the text.

Line 293: The authors should be clear here regarding shimming. Typically shimming occurs using the proton coil and signal from water within cells. Moreover, the practice of shimming involved more than moving the

box, it involves small changes to the magnetic field coils to make the signal most homogenous.

We fully appreciate that the physics of proton shimming involve more than moving a box. For this practical methods paper, we have detailed the steps necessary to acquire good quality phosphorous spectra, and have omitted, due to scope, a discussion regarding the physics of proton shimming.

General comment: The authors suggest making several scans in which 20 spectra are acquired. In most cases, this protocol is run using a single scan with multiple spectra acquisitions (for example acquiring spectra every 6 sec for 5 min). Having to start new scans during and after exercise will result in a loss of some signal as PCr is being resynthesized while the next scan protocol is sent to the scanner.... Moreover, it is important to recognize that the number of scans required for accurate exponential fitting will depend on the recovery time constant. For example, the slower the recovery the more scans will be required to properly and accurately fit the data mathematically to an exponential.

The method described in the protocol ensures **“that post-exercise acquisitions begin immediately following the exercise sequence, without pause or shimming”** (step 4.8.1). Splitting of the recovery scans is to allow for dynamic observation of depletion and recovery, which is only possible after acquisition is complete on our particular system.

Line 334: I would disagree with the author's comment regarding splitting the recovery if exercise needs to be repeated. It is vitally important that enough time is given for the muscle to fully recover from exercise as calcium and other ions can alter mitochondrial bioenergetics and bias the results. Typically, we allow for a 10min rest period between exercise/recovery measurements to ensure this does not occur.

We completely agree that sufficient recovery is important if repeating the exercise after insufficient effort. In light of inescapable time constraints on *in vivo* MR experiments, particularly in human subjects, our proposed scheme allows us to interleave other scans in the exam during the recovery before the next exercise bout. We have now clarified this in the text.

-Line 358: The authors should note why it is important to measure pH. Tell the readers what impact this can have on the results...

We have included a brief note on the significance of pH in OXPHOS recovery, along with a reference to the work by Jubrias *et al.* J Physiol 2003. (line 653)

Line 384: The AMARES algorithm does not calculate Peak heights, but rather calculated the 'area under the peak', which is more accurate for calculating absolute concentrations of metabolites.

We thank the reviewer for highlighting this confusing nomenclature of the jMRUI software. We have clarified in the manuscript that the AMARES peak area, referred to as “amplitude”, is used in the analysis.

General comment: The authors do not describe any quality control measures taken to assure curve fitting is of high quality. The software will always force a curve fit and produce a time constant, but this may not be an accurate representation of the muscle oxidative capacity. This is an important point of discussion especially considering the large introduction suggesting the use of this approach for testing the efficacy of therapeutics...

We have included step 5.7 that describes a method to obtain goodness-of-fit measures.

Line 555: Varying levels of PCr depletion do NOT impact to the recovery of PCr. In fact, the main benefit of this

modeling approach is the recovery kinetics (1st order exponential) are completely independent of the amount of PCr depletion. (see work from Ron Meyer 1988 and 1989 Am J Physiol).

We thank the reviewer for helping us clarify this point. We did not intend to suggest recovery kinetics were directly related to the degree of depletion but rather that the fitting of noisy data to an exponential recovery curve can be impacted by this and so sufficient dynamic range of the signal is important in the realm of limited signal-to-noise. We have now clarified this in the text.

-General comment: The major limitation of ³¹P-MRS is that if a defect in oxphos is indicated, this approach does not provide any mechanistic insight. The same goes for potential therapies. Its major benefit is the easy and repeatability of measuring human participants.

We thank the reviewer for providing these comments. We have emphasized the idea that this technique may not provide specific mechanistic insight into the development of disease, but rather offers a useful biomarker of disease status. "It is important to note that unlike muscle biopsy analysis, which permits the measure of specific mitochondrial characteristics such as mitochondrial content and size as well as the mitochondrial maximum ATP synthesis rate, the *in vivo* measure using ³¹PMRS represents an aggregate of these direct measures in addition to extra-mitochondrial factors such as microvascular supply of oxygenated blood to the muscle." (line 657-661)

Figures

Figure 1: Not sure this figure is all that relevant to this approach. Small musculature exercise does not result in the same systemic effects as whole body exercise. I think it would be better to provide a metabolic model for the PCr model used within. This will make is easier for readers/viewers to understand how this measurement works and the assumptions made regarding the bioenergetic system.

Figure 1 helps put these methods into what we feel is highly relevant context for investigators seeking a technique to better understand integrative physiology *in vivo* in humans with a broad spectrum of cardiovascular and metabolic disorders.

Major Concerns: N/A

Minor Concerns: N/A

Additional Comments to Authors: N/A