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A Simple Critical-Sized Femoral Defect Model in Mice.

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Abstract:	<p>While bone has a remarkable capacity for regeneration, serious bone trauma often results in damage that does not properly heal. In fact, one tenth of all limb bone fractures fail to heal completely due to the extent of the trauma, disease, or age of the patient. Our ability to improve bone regenerative strategies is critically dependent on the ability to mimic serious bone trauma in test animals, but the generation and stabilization of large bone lesions is technically challenging. In most cases, serious long bone trauma is mimicked experimentally by establishing a defect that will not naturally heal. This is achieved by complete removal of a bone segment that is larger than 1.5 times the diameter of the bone cross-section. The bone is then stabilized with a metal implant to maintain proper orientation of the fracture edges and allow for mobility.</p> <p>Due to their small size and the fragility of their long bones, establishment of such lesions in mice are beyond the capabilities of most research groups. As such, long bone defect models are confined to rats and larger animals. Nevertheless, mice afford significant research advantages in that they can be genetically modified and bred as immune-compromised strains that do not reject human cells and tissue. Herein, we demonstrate a technique that facilitates the generation of a segmental defect in mouse femora using standard laboratory and veterinary equipment. With practice, fabrication of the fixation device and surgical implantation is feasible for the majority of trained veterinarians and animal research personnel. Using example data, we also provide methodologies for the quantitative analysis of bone healing for the model.</p>
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30th May, 2014

Dear Editor, *JoVE*,

We would greatly appreciate your consideration of our attached manuscript "*A Simple Critical-Sized Femoral Defect Model in Mice.*" by Clough *et al.* for publication in *JoVE*.

Animal models are frequently employed to mimic serious bone injury in biomedical research, but due to their small size, establishment of stabilized bone lesions in mice are beyond the capabilities of most research groups. This is problematic because mice afford significant research advantages in that they can be genetically modified and bred as immune-compromised strains that do not reject human cells and tissue.

Herein, we demonstrate a technique that facilitates the generation of a segmental defect in mouse femora using standard laboratory and veterinary equipment. With practice, fabrication of the fixation device and surgical implantation is feasible for the majority of trained veterinarians and animal research personnel.

We believe that this methods article will be of great interest to the orthopedic, tissue engineering and regenerative medicine fields and of general interest to the readership of *JoVE*. Thank you for consideration of our manuscript and please feel free to contact me if you have any questions or concerns.

Yours sincerely,

A handwritten signature in blue ink, appearing to read "C. Gregory".

Carl Gregory, Ph. D.

TITLE: A Simple Critical-Sized Femoral Defect Model in Mice.

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SHORT ABSTRACT:

Animal models are frequently employed to mimic serious bone injury in biomedical research. Due to their small size, establishment of stabilized bone lesions in mice are beyond the capabilities of most research groups. Herein, we describe a simple method for establishing and analyzing experimental femoral defects in mice.

LONG ABSTRACT:

While bone has a remarkable capacity for regeneration, serious bone trauma often results in damage that does not properly heal. In fact, one tenth of all limb bone fractures fail to heal completely due to the extent of the trauma, disease, or age of the patient. Our ability to improve bone regenerative strategies is critically dependent on the ability to mimic serious bone trauma in

test animals, but the generation and stabilization of large bone lesions is technically challenging. In most cases, serious long bone trauma is mimicked experimentally by establishing a defect that will not naturally heal. This is achieved by complete removal of a bone segment that is larger than 1.5 times the diameter of the bone cross-section. The bone is then stabilized with a metal implant to maintain proper orientation of the fracture edges and allow for mobility.

Due to their small size and the fragility of their long bones, establishment of such lesions in mice are beyond the capabilities of most research groups. As such, long bone defect models are confined to rats and larger animals. Nevertheless, mice afford significant research advantages in that they can be genetically modified and bred as immune-compromised strains that do not reject human cells and tissue.

Herein, we demonstrate a technique that facilitates the generation of a segmental defect in mouse femora using standard laboratory and veterinary equipment. With practice, fabrication of the fixation device and surgical implantation is feasible for the majority of trained veterinarians and animal research personnel. Using example data, we also provide methodologies for the quantitative analysis of bone healing for the model.

INTRODUCTION:

It is estimated that half of the US population experience a fracture by the age of 65¹. For those patients with fractures treated surgically, 500,000 procedures involve the use of a bone graft² and this number is expected to rise with an increasingly aging population³. Although bone is one of the few organs that has the capacity to completely heal without scarring, there are instances where the process fails^{3,4}. Depending on the circumstances and quality of treatment, 2-30% of long bone fractures fail, resulting in non-union^{3,5}. While there remains some debate on the definition, pseudoarthrosis, critical-sized or non-union bone injuries generally refers to an injury that does not heal over the natural lifetime of the subject⁶. For experimental purposes, this duration is shortened to the average time required for complete healing of an average-sized bone injury. Non-union bone lesions occur for numerous reasons, but major factors include extreme trauma resulting in a critically-sized gap, infection, poor angiogenesis, tobacco use, or inhibited osteoregenerative capacity due to disease or age⁷. Even if non-unions are successfully treated, it can cost in excess of \$60,000 per procedure, depending on the type of injury and the approaches employed⁸.

In moderate cases, autologous bone grafting is employed. This strategy involves recovery of bone from a donor site and implantation at the site of injury. While this approach is extremely effective, the volume of available donor-derived bone is limited and the procedure involves an additional surgery, which results in persistent pain in many patients^{9,10}. In addition, the efficacy of the autologous bone graft is dependent of the health of the patient. Bone substitutes made from synthetic materials or processed cadaveric bone are abundantly available¹¹⁻¹³, but they have significant limitations, including poor host-cell adhesion properties, reduced osteoconductivity, and the potential for immune rejection¹⁴. There is therefore an urgent need for bone regeneration technologies that are safe, effective and widely available.

Our ability to improve bone regenerative strategies is critically dependent on the ability to mimic serious bone trauma in test animals, but the generation and stabilization of large bone lesions is technically challenging. In most cases, serious long bone trauma is mimicked experimentally by establishing a defect that will not naturally heal. Although it can vary with species¹⁵, this is achieved by complete removal of a bone segment that is larger than 1.5 times

the diameter of the bone cross-section¹⁶. The bone is then stabilized with a metal implant to maintain proper orientation of the fracture edges and allow for mobility. Due to their small size and the fragility of their long bones, establishment of such lesions in mice are beyond the capabilities of most research groups. As such, long bone defect models are confined to rats and larger animals. Nevertheless, mice afford significant research advantages in that they can be genetically modified and bred as immune-compromised strains that do not reject human cells and tissue.

For human cell-based applications, immune-compromised mice are attractive to work with because they are physiologically well-characterized, easy to house, cost effective, and easily analyzed radiologically and histologically. Of paramount importance is that immune-compromised mice do not reject cells from different species including humans. Their small size also permits the testing of very small numbers of cells or volumes of experimental scaffolds in orthopedic applications. Several murine orthopedic models have been reported that afford various degrees of bone stability^{17,18}. Those systems that result in very high levels of stability, such as external fixators and locking plates predominantly heal by intramembranous ossification although endochondral healing has been reported¹⁹. In contrast, those that permit some micro- and/or macro-motion, such as those employing unfixed or partially-fixed medullary pins, generally heal with a predominance of endochondral ossification^{20,21}. Delayed union or non-union defects of long bone are particularly difficult to achieve in mice due to the extra level of stabilization required. However, a number of approaches have been reported, including medullary pins with interlocking nails, locking plates and external fixators²². These systems generally work well, but given their complicated design they can be technically challenging to install. For example, Garcia *et al.*²³ devised an elegant interlocking pin system for use in mice, but the procedure involves incisions at two separate sites and extensive modification of the femur to accommodate the pins. These procedures were performed under a dissecting microscope.

Herein, we describe a simple femoral medullary pin with a central collar designed to prevent closing of a 3 mm bone deficit and also delineate the original edges of the defect. While the pin was not fixed to the bone itself, precise sizing of the pin diameter and reaming of the medullary cavity results in sufficient interference to minimize torsional motion (**Fig1**). With careful selection of inbred age, gender and strain-matched mice, the result is a highly reproducible *hypertrophic non-union defect*²² which can be easily evaluated radiologically. Moreover regions of interest can be reproducibly defined after micro-computed tomography (μ CT) for measurement of *de novo* bone formation and histomorphological parameters. The pins were prototyped in our laboratory using readily available tools

[Figure 1 here]

PROTOCOL:

NOTE: This protocol is designed for female nude (Nu/J) mice (18-25 g, 6 weeks) acquired from Jackson Laboratories. Since strains of mice vary slightly in terms of anatomy and growth rate, we advise that the fabrication of pins is optimized to the strain, gender and age of the recipients prior to implantation into live subjects. If the strains are carefully matched, the interference fit between the pin and marrow cavity is highly reproducible. Procedures for housing, diet and general animal husbandry are beyond the scope of this protocol, but all mice were housed in accordance with the *Guide for the Care and Use of Laboratory Animals* (8th Edition) and

institutional policies set by the Institutional Animal Care and Use Committee (IACUC) and Department of Comparative Medicine (DCM) at Scott and White Hospital.

1. Fabrication of pins.

[Figure 2 here]

1.1) Cut a 9 mm length of 22 G stainless hypodermic tubing, and a 3 mm length of 19 G tubing using a 23.8 mm diameter fiberglass reinforced heavy duty cut-off wheel fitted to a rotary tool. Use small fine-tipped pliers to immobilize the tubing (**Fig2A, above**). Wear appropriate eye protection and handle rotary tool with care.

1.2) Place a small amount (approximately 10 μ L) of cyanoacrylate adhesive to the middle of the 9 mm shaft. Pass the 3 mm collar over the 9 mm shaft until in the center and twist to evenly distribute the glue between the collar and shaft. Measure dimensions with a pair of digital calipers and compare with **Fig1**. Allow to set for at least 15 hr (**Fig2A, center**).

1.3) Use a 220 grit emery-impregnated disc to remove burrs and excessive glue.

1.4) Using the rotary tool, polish the pin using a felt polishing disc.

1.5) Rinse with deionized water and dry with compressed air.

1.6) Test integrity by placing a 19 G hypodermic blunt needle over the shaft of the newly made pin and push against the collar. Ensure that the collar can resist approximately 25 g of weight.

1.7) Rinse the pin in sterile-filtered phosphate buffered saline (**Fig2B, top**). Ensure that the shaft of the pin fits snugly into the femoral medullary cavity with the collar flush against the edges of the cut bone (**Fig2C**). Prototype various configurations for the specific purposes of the study and the recipient (**Fig2D**). Make sure that the ends of the pin penetrate into the trabecular bone of the diaphysis so as to maximize fixation and improve the interference fit (**Fig2E**). Note: It is recommended that the fit is tested on bone specimens before implantation in live mice (e.g. **Fig 2C**).

1.8) Use a 4 mm diameter punch-biopsy cutter to cut a cylinder from a 5 mm thick sheet of surgical gelatin sponge. Use a scalpel to trim the cylinder to 3 mm length and pass a 20 G hypodermic needle along the length of the cylinder to generate a hole (**Fig2A, below**). Note: We have found that the positioning of a gelatin or collagen scaffold at the site of the defect improves cell retention and induces longitudinal growth along the axis of the bone.

1.9) Pass the gelatin foam cylinder over the pin and align with the collar (**Fig2B, center**) and autoclave on a dry cycle at 120°C at 15 PSI. The gelatin foam will dry and darken in color (**Fig2B, below**).

2. Surgical technique.

NOTE: The following procedure is written observing all guidelines set by the *Guide for the Care and Use of Laboratory Animals* (8th Edition). Please observe all additional policies set by the local IACUC and ensure an IACUC-approved animal use protocol (or equivalent) is in place before proceeding with the following sections.

[Figure 3 here]

2.1) Select a surgical procedure room or clean laboratory with a closable door and no through-traffic. Sanitize a suitable work surface with a clinical grade quaternary-based disinfectant cleaner.

2.2) While wearing disposable sterile gloves and robe, set up a sterile field of approximately 60 x 90 cm on the sanitized work surface with autoclaved cloth drapes. Note: It is advisable to have an assistant remove the outer packaging and present the sterile materials to the investigator setting up the field.

2.3) Place a sanitized heating pad fitted to a warm water re-circulator on the drape and cover with sterile disposable drapes. Warm a bead sterilizer to operating temperature (250-265 °C, this takes up to 30 min).

2.4) On the sterile field, arrange the surgical kit (**Fig3A**) to provide convenient access to all components. Also, provide sterile cotton gauze (2 x 2 in), sterile Q-tips, a sterile steel bowl (~500 mL) containing sterile saline (0.9% w/v), and chlorhexidine/isopropyl alcohol surgical disinfectant applicators.

2.5) Assemble a small animal anesthesia unit next to the sterile field with an induction chamber and nose-cone assembly in accordance with veterinary guidance and the user manual. Use clinical grade oxygen as the gas supply and isoflurane, USP.

[Figure 4 & 5 here]

2.6) Place a mouse in the induction chamber of the anesthesia system and set the output to 2 liters min⁻¹ O₂ and the isoflurane concentration to 3% (v/v).

2.6.1) Check that the mouse is unconscious within 1 minute; raise the concentration to 4% (v/v) if necessary. Remove the mouse, place on the warm sterile field and apply the nose cone. Transfer flow to the cone, and reduce the isoflurane to 2.5%, wait for a further 20 s, and test for adequate surgical plane in accordance with institutional policy. Typically, lack of a hind limb reflex when gently squeezed is adequate for determining adequate anesthesia.

2.6.2) During the entire process, have an assistant monitor for strong regular breathing and pink coloration of the extremities and mouth region to ensure an appropriate level of oxygenation while unconscious. Adjust anesthesia in accordance with veterinary guidance and institutional policy if necessary. Apply sterile artificial tears lubricant ointment (15% (v/v) mineral oil, 83% (v/v) white petrolatum) to the eyes.

2.7) Turn the mouse onto one side with the hind-limb facing upwards on a new disposable drape. If necessary, remove fur with an electric razor or hair removal cream. Wipe the site with sterile saline and remove the additional drape with excess fur. Place a new fenestrated drape over the mouse so as to cover all parts but the entire hind-limb (**Fig4A**) but maintain view of the face and paw to monitor coloration and breathing.

2.8) Locate the proximal and distal ends of the femur and incise the skin for 5-10 mm along the longitudinal axis (**Fig4B**). Separate the skin layer from the fascia with a #15 scalpel, exposing a lateral approach to the femur via the *biceps femoris* and *vastus lateralis*. Locate where the septa of both muscles meet (it is a line of white tissue against the pink coloration of the muscle). With a scalpel, carefully dissect along the intermuscular boundary until the femur is visible (**Fig4B**).

2.9) Develop the incision with a blunt periosteal elevator so as to expose the entire *diaphysis* (**Fig4C**). Use the elevator to further expose the central two thirds of the femur while taking care to preserve the posterior neurovascular bundle on the medial side (**Fig4D**). Gently scrape soft tissue off of the bone with a scalpel, and dry with a sterile Q-tip or equivalent.

2.10) Locate the center of the femur with calipers if necessary and mark with a sterile scalpel or marker, then mark 1.5 mm proximally and distally from the center. Gently grasp the *femur* using a pair of fine-nosed forceps previously fashioned in the Kern style to prevent excessive pressure on the bone. Note: Exact dimensions for modifications are provided in **Fig3B**. It is advisable to test the forceps on a euthanized specimen prior to use to ensure the bone will not break under pressure required for immobilization during cutting.

2.11) Using a fine drill fitted with a fine diamond-grit coated cutting wheel (8 mm diameter x 0.1 mm width), make the first cut with the elevator in place to protect tissue below (**Fig4E**). Raising the cut femur to 45° while firmly holding the extremity of the *diphysis*, make the second cut, removing a 3 mm segment. Note: Face protection is recommended at this stage.

2.12) With the bone immobilized by forceps, carefully ream the medullary cavities of each end with a blunt 23 G hypodermic needle. Using a pre-made depth-gauge made from a length of 22 G tubing placed in 19 G tubing (**Fig3A, item 8**), assess the depth of the reamed medullary cavity and ensure it is 3 mm (**Fig4F-K**). If the medullary cavity resists the 22 G depth gauge, ream again with a blunt 22 G hypodermic needle.

2.13) Carefully insert the medullary pin into the proximal then distal medullary cavities to bring the femur back out to its original length and establish a stable 3 mm gap (**Fig5A,B**). If needed, apply a small amount of manual stress to achieve a good interference fit of the rod with the cortical bone of the femur. Ensure that the pin fits snugly into the medullary cavities of both sides and the edges of the cut bone are flush with the collar. If there is a gap, ream once again with a 22G blunt needle.

2.14) Reposition the muscle and peripheral tissue over the pin and close with a continuous absorbable 5-0 suture (**Fig5C**). Close skin incision with 5-7 square knot nylon 5-0 sutures and seal with surgical adhesive (**Fig5D**).

3. Postoperative procedures.

3.1) After closing the skin incision, withdraw anesthesia, but allow O₂ to remain flowing until the mouse begins to move; this should take less than 1 minute. If the mouse remains motionless after 5 min of O₂ administration, refer to institutional policies on veterinary intervention.

3.2) When the mouse begins to move, gently transfer it to a cage preferably containing dry, autoclaved bedding.

3.2.1) Place an igloo-type nest in each cage and the mouse will retreat into it, reducing movement. Check that the mouse recovers hind-limb mobility 5-10 minutes after recovery of consciousness.

3.2.2) Perform daily postoperative monitoring in accordance with institutional policies. Provide gelatinized hydration and food on the floor of the cage for the first 5 -7 days and administer analgesia and postoperative monitoring in accordance with institutionally approved policies. Note: We administer 0.05-0.1 mg kg⁻¹ buprenorphine²⁴ with 0.25 mL saline subcutaneously, twice daily for the first 3 days and thereafter if the mouse does not regain normal utility.

3.3) After the first 24 h of recovery, perform live-animal x-ray imaging under anesthesia to visualize pin placement (**Fig4E**). If the pin is dislocated, consider immediate revision surgery.

3.4) At day 7 post-surgery, remove sutures under anesthesia and house in groups in accordance with institutional animal husbandry policies.

3.5) After 2-5 weeks, humanely euthanize animals in accordance with the American Veterinary Medical Association approved methods for euthanasia²⁵. Note: An intraperitoneal injection of commercially available barbiturate-combination euthanasia cocktail is effective and humane, but local institutional policies on euthanasia should be followed.

3.6) Carefully dissect away the hind-limb by exposing the proximal femur and the pelvis from the medial side. Gently press the joint inwards from the lateral side of the limb while detaching the femoral head from the *acetabulum* (the hip socket) with a scalpel. Cut remaining muscle and skin with a sharp scalpel or micro-scissors, releasing the entire limb from the pelvis. With a sharp pair of rongeurs or heavy scissors, cut the lower hind-limb (tibia/fibula) approximately 5 mm below the knee joint.

Note: It is recommended that all specimens are stored in an identical manner prior to analysis.

3.7) Remove skin, but leave muscle in place. Fix the tissue in 10 % buffered formalin supplemented with 10 mM CaCl₂ fixative for 1 week followed by storage in phosphate buffered saline supplemented with 10 mM CaCl₂ for up to 1 month prior to imaging. Perform fixation and storage at 4 °C. Alternatively, scan specimens immediately without fixation.

4. Analysis of specimens.

Note: Bone healing can be assessed by a wide variety of methodologies that are beyond the scope of this protocol. The following is a method that we have successfully employed using a specimen microCT (μ CT) imager. It is recommended that the following parameters are tested initially, then optimized for the specific needs of the project.

4.1) Wrap specimen in a thin layer of plastic sealing film and position it vertically in the instrument chamber. Make sure that the femur is perpendicular to the sample stage during the entire scan. Set the scan to the following parameters; voltage =29 kv, current =661 μ A, power =19 watts, image pixel size (mm) =21.00; 360 degree rotation = yes; frame averaging=on (5); rotation Step (deg)=1.00, random movement= on. Save images as JPEG files in a single destination folder per scan (e.g. **Fig6A**) Note: The scan should be complete in 57 min.

4.2) Utilize the reconstruction software to generate axial images based on the following parameters; smoothing= on (4), misalignment compensation= on, ring artifact reduction= on (5), beam-hardening correction (40 %), CS rotation (deg)=0.00. Set output to 2000-15,000 Hounsfield units. Save images as JPEG files in a single destination folder per scan.

4.3) Using the axial images and analytical software, define the region of interest (ROI) by first setting the proximal and distal edges of the original defect. Achieve this by selecting the sections that encompass the collar only. Because the collar is thicker than the medullary pin, these sections are easily defined (**Fig6B, left**). Exclude the collar from calculations by drawing an exclusion zone around it (with a 100 μ m margin) and transferring the zone to each of the sections in the ROI (**Fig6B, right**). Note: Polar moments of inertia, 3D reconstructions and calculations such as the volume of new bone (**Fig6C,D**) can readily be achieved using the software.

REPRESENTATIVE RESULTS:

Mice typically recover consciousness and hind-limb mobility 5-10 minutes after withdrawal of anesthesia. During the first 5 days, it is advisable to house mice individually and introduce environmental enrichment to prevent excess use of the limb. For this purpose, igloo-type nests reduce the need for nest building and encourage resting. We have also observed that provision of food and hydrogel on the floor of the cage reduces the probability of pin displacement. During the 5-day period, analgesia should be administered as required in accordance with institutionally-approved policies. Weight loss up to approximately 15% of the original pre-operative weight is possible during the 5-day postoperative period. Twenty-four hours after surgery, x-rays of the affected limb are recommended to assess pin-placement. The pins should be completely inserted into the proximal and distal medullary canals with the edges of the defect flush against the collar (**Fig 2C,E Fig5E, and Fig6A**). In rare instances (<5% of cases), pins can become dislocated at early stages of healing and animal use protocols should provide for revision surgery if this occurs. While it is technically challenging to quantify torsional motion on murine femurs, manual palpation of specimens confirmed that torsional and longitudinal motion is marginal after 7 days as connective tissue accumulates around the pin. After 5 days of post-operative monitoring, the mice can be returned to standard communal housing as per institutionally-approved policies.

Without therapeutic intervention, the edges of the defect typically extend 0.5 mm during 21

days but in rare cases, new bone growth can be up to 1 mm (**Fig6A**). Bone growth arrests after this period as the inflammatory and anabolic stages of regeneration cease resulting in a non-union defect. After 14-21 days of healing, the volume of *de novo* bone can be readily determined from axial images generated by μ CT scanning. Using the scanning, axial reconstruction and ROI selection procedures described in the protocol, the volume of new bone generated increases with time, but does not generally exceed a total of 1 mm³ in the absence of therapeutic intervention (**Fig6C**) compared to 6-7 mm³ in an anatomically equivalent region of uninjured femur. While conventional biomechanical testing is technically challenging due to the specimen size and nature of the fixation method, the polar moment of inertia (PMI), an estimation of the ability of a material to resist torsion based on cross-sectional area and density, has been shown to represent a suitable estimation of strength in long bones^{26,27}. Using this method, axial cross-sections at various distances from the lesion edges can be selected for analysis. After 21 days, the PMI of *de novo* bone 0.25 mm from the lesion edges ranges from between 0.05-0.35 mm⁴ compared to 0.02-0.08 mm⁴ at the center of the lesion further confirming the presence of non-union in untreated cases (**Fig6D**). The PMI of uninjured femur at an anatomically equivalent location typically ranges between 0.5-0.7 mm⁴ using the conditions described here.

[FIGURE 6 here]

Decalcification of the tissues typically takes 10-14 days using standard conditions, and is readily monitored by x-ray scanning. It is advisable to retain some musculature on the specimens during decalcification to improve stability during handling. After decalcification, pins can be carefully removed with a sharp scalpel permitting paraffin embedding and histology. Masson's trichrome staining of longitudinal sections permits visualization of endochondral bone outgrowth with a leading edge of cartilage (*ca*) followed by cancellous bone (*cb*) (**Fig6E**). While some damage will inevitably occur during dissection, the histological structure of bone and connective tissue remains clear if the pin is removed carefully. Alternatively, methyl methacrylate embedding and sectioning of non-demineralized sections may be performed with the pin in place (**Fig6F**).

Figure Legends:

Figure 1: Experimental principle. Diagrammatic summary of the segmental defect model. The central 3 mm segment of a 9-10 mm murine femur is excised surgically (*left*). A 3 mm long, 19 gauge surgical steel tube is passed over a 9 mm long, 22 G stainless steel tube and fixed with adhesive at the exact center (*right*). The resultant pin is fitted into the medullary canals of the remaining proximal and distal portions of the femur with the 19 G collar replacing the 3 mm segment of bone (*below, center*).

Figure 2: Pin assembly. Panel a: Photographs of the surgical steel tubing at various stages of assembly and a 4 mm diameter cylinder cut from 5 mm thick Gelfoam sheet. **Panel b:** After polishing the assembled pin (*above*), the Gelfoam cylinder is trimmed, positioned over the steel collar (*middle*), then autoclaved, resulting in a sterile pin coated with dried Gelfoam. This improves cell attachment at the site of injury and maintains the direction of healing (*below*). **Panel c:** An excised femur fitted with the medullary pin. **Panel d:** Examples of pin assemblies at various thicknesses and lengths demonstrating the flexibility of this approach. **Panel e:** μ CT

reconstruction of a pin-stabilized femoral defect illustrating the interaction of the medullary pin with the trabecular bone in the proximal and distal ends of the femur.

Figure 3: Surgical instruments. **Panel a:** Surgical kit. Micro-drill (1), cutting wheel (2), absorbable suture (3), outer suture (4), scalpel blades (5), scalpel handle (6), sterile medullary pins wrapped in foil (7), medullary depth gauge made from hypodermic tubing (8), fine nosed forceps (9), rat-teeth forceps (10), blunt reaming needles (11), needle drivers (12), small hemostats (13), fine scissors (14), periosteal elevator (15), modified Kern forceps (16). **Panel b:** Modifications required to produce Kern-style bone-grips for mice.

Figure 4: Surgical procedure. **Panel a-c:** Approach and exposure of the femur. **Panel d-e:** Elevation and cuts. **Panel f-k:** Reaming and sizing of medullary canals.

Figure 5: Surgical procedure. **Panel a-b:** Installation of pin. **Panel c-d:** Closure. **Panel e:** Typical image of properly positioned pin 24 hr after surgery.

Figure 6: Typical results. **Panel a:** X-ray scans of femurs at day 7, 14 and 21 post-surgery demonstrating limited ingrowth of bone. **Panel b:** Diagrammatic representation of the ROI parameters for volumetric bone measurement. Representative axial cross-section with an exclusion zone (*EX*) over the pin-collar including a 100 μ m margin to exclude measurement of artifacts at the metal-tissue interface (*left*). Full bone scan (*right, top*) demonstrating the longitudinal ROI defined by the sections of bone between the edges of the collar with original bone tissue excluded (*EX*). The original lesion edges are located in the axial sections using the difference between the diameter of the pin and the collar (*right, below*). **Panel c:** Typical volumetric measurements at day 7, 14 and 21 post surgery with no therapeutic intervention (means with standard deviations, n=3). **Panel d:** PMI measurements at axial sections 0.25 mm from the proximal and distal lesion edges and mid-point (means with standard deviations, n=3). **Panel e:** Masson's trichrome-stained paraffin-embedded section (*left*) cut in the longitudinal direction demonstrating bone outgrowth consisting of cartilage (*ca*) and cancellous bone (*b*) (*scale bar: 0.5 mm*). The position of the field is indicated on the x-ray scan (*right*). **Panel f:** Non-decalcified, methyl methacrylate embedded coronal section of 1 day-old defect stained with hematoxylin and eosin (*scale bar: 1.0 mm*).

DISCUSSION:

Herein, we describe a simple method to generate a critical-sized pin-stabilized defect of the murine femur using standard laboratory and veterinary equipment. While the assembly of the pins and the surgical procedure itself requires practice, it is well within the capabilities of a well-trained biomedical research scientist or veterinarian.

The pin is positioned into the medullary canal without additional fixation, making the procedure technically more feasible than more complicated approaches that employ external fixators or interlocking screws. While some torsional motion may occur during the early stages of healing, this is minimized by careful attention to the pin diameter and adequate reaming of the medullary canal so as to attain a firm interference fit between the implant and endosteum. With careful selection of inbred strain and matching of age and gender, the fit becomes reproducibly robust within a few days. Nevertheless, with the advent of 3D printing techniques, it is expected

that torsional motion can be further reduced by more sophisticated versions of the pin that incorporate roughened surfaces and/or barbed attachment sites. The ease of pin fabrication and the availability of a wide variety of hypodermic tubing sizes also permit the optimization of the technique for virtually any adult inbred mouse, irrespective of natural or experimental bone phenotype.

The unique pin-collar design serves two purposes; (i) to prevent aberrant narrowing of the defect and damage of the bone extremities through longitudinal slippage, and (ii) to provide landmarks that define the original edges of the defect. As such, volumetric and PMI measurements can be made easily using a specimen μ CT scanner such as a Skyscan 1174. Indeed, this approach permits a level of quantitation that is not easily obtained with standard non-critical sized fracture techniques that often exhibit variable or poorly defined injuries. While a μ CT unit is preferable for quantitation of healing, evaluation by objective assessment of orthogonal x-ray images or 2D image analysis techniques may represent feasible alternatives. Due to their small size and relatively low mineral content, murine limbs can be readily prepared for histology and mounted as whole specimens for conventional histomorphometry. This dismisses sampling issues frequently faced by researchers performing histomorphometric analyses of large animal fractures.

In the experiments described here, the healing time was relatively short at 3 weeks, which corresponds to the rapid, anabolic phase of bone healing. Thereafter, bone remodeling is a very slow process²⁸. Generally, if bridging is not observed after 4 weeks, healing is unlikely to occur and in agreement, we observe very little additional bone growth after 4 weeks in this system. Furthermore, a 3 mm gap meets the criteria of Key *et al.*¹⁶ for a critical sized defect and Garcia *et al.* demonstrated that a gap as narrow as 1.8 mm does not sufficiently heal after 10 weeks and this could be delayed to 15 weeks with stripped perichondrium²³.

While the size and fragility of their bones present serious technical challenges for orthopedic research, the use of mice is advantageous in numerous ways. For example, there is a variety of immune-compromised strains that permit testing of human cells and proteins without fear of immunological rejection, and their small size reduces the need for excessive amounts of valuable experimental materials, cells or compounds. This is exemplified by our recent study demonstrating the efficacy of adult human stem cells and their extracellular proteins for osteoregeneration²⁹. The relatively short lifespan of mice also present the opportunity for research into aging³⁰ and the wide variety of inbred strains permit the study of global genotype on healing³¹. There are also a number of disease models that are easily established in mice such as diabetes and osteoporosis^{32,33}. Of significant note is the availability of many transgenic mice that may be used with this technique to further our understanding of regenerative bone physiology under conditions of extreme trauma.

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The authors have no competing financial interests.

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Figure
Fig 1: Principle of the model
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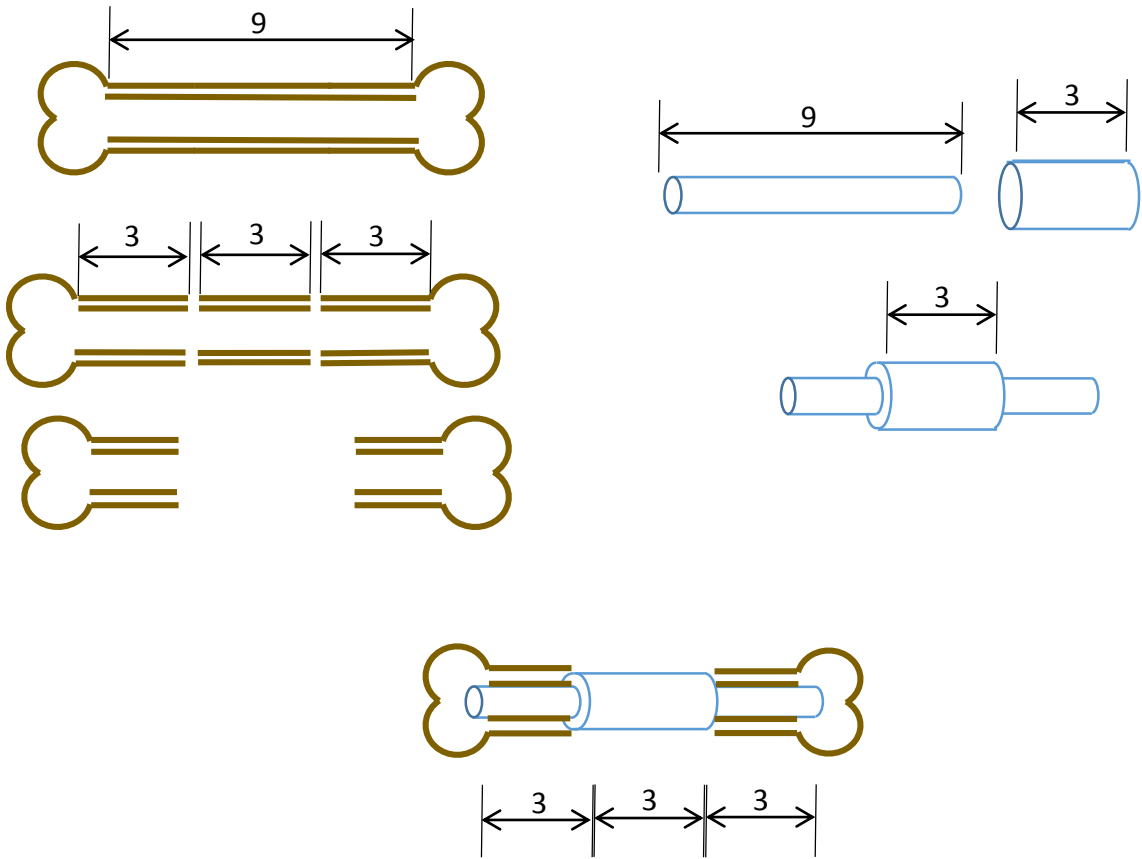


Fig 2: Pin assembly procedure.

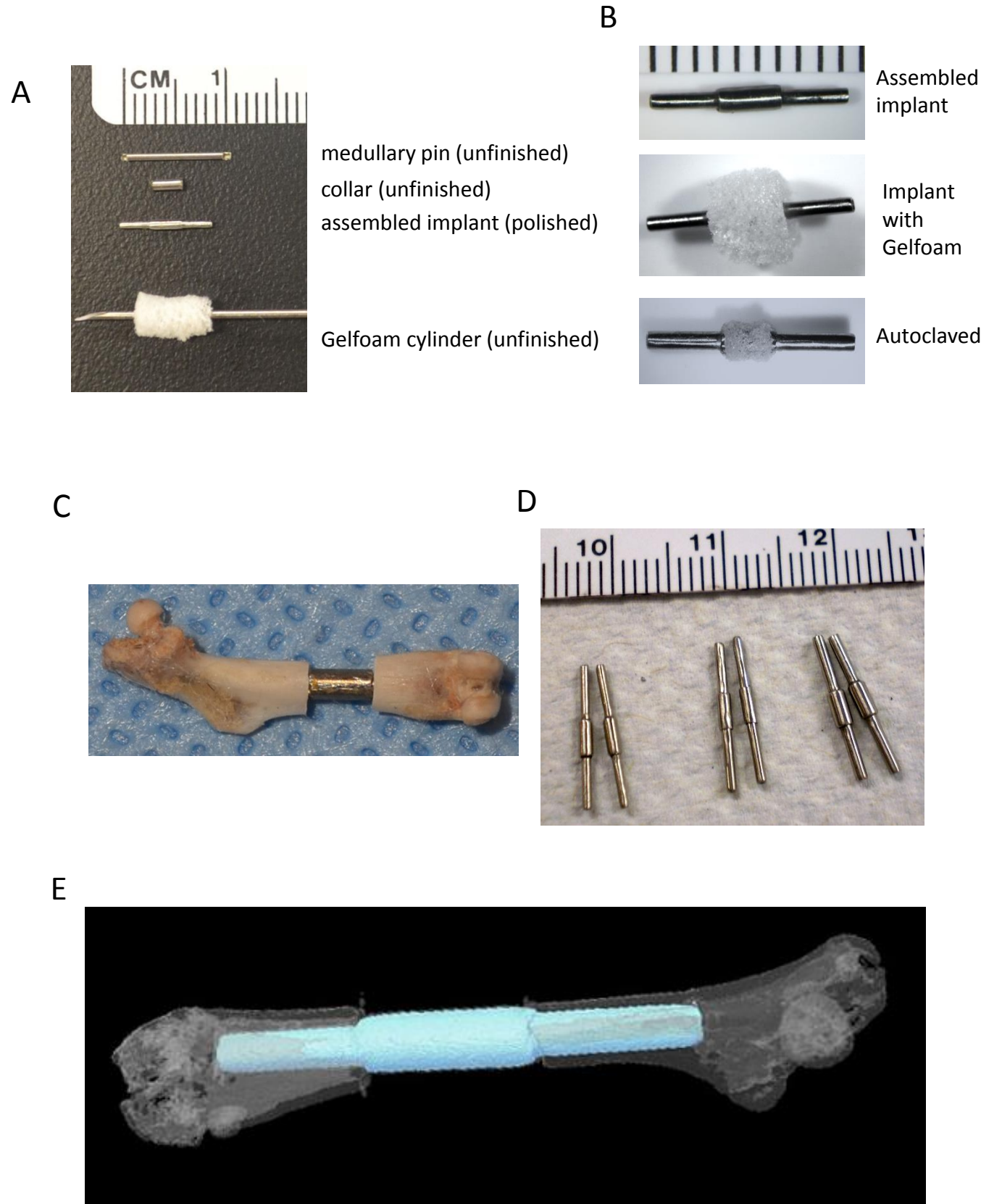


Fig 3: Surgery instruments.

A.



B.

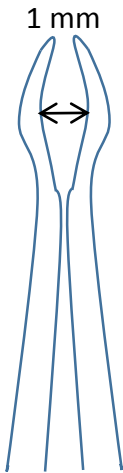


Fig 4: Surgery procedure.

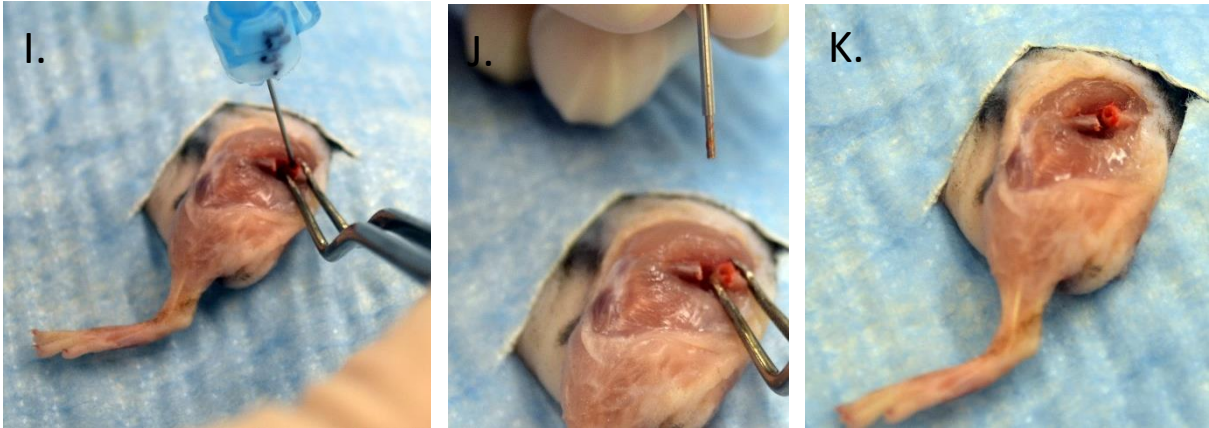
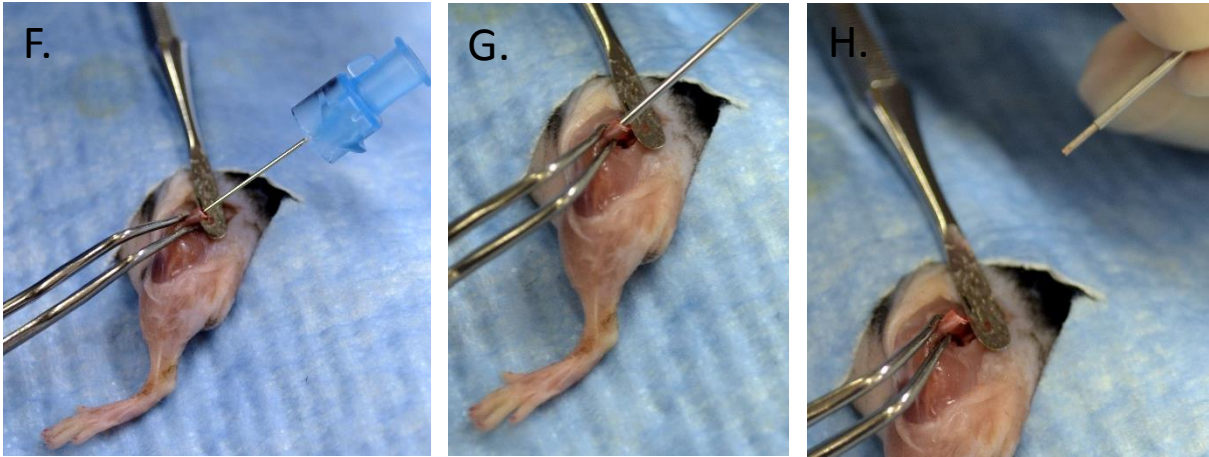
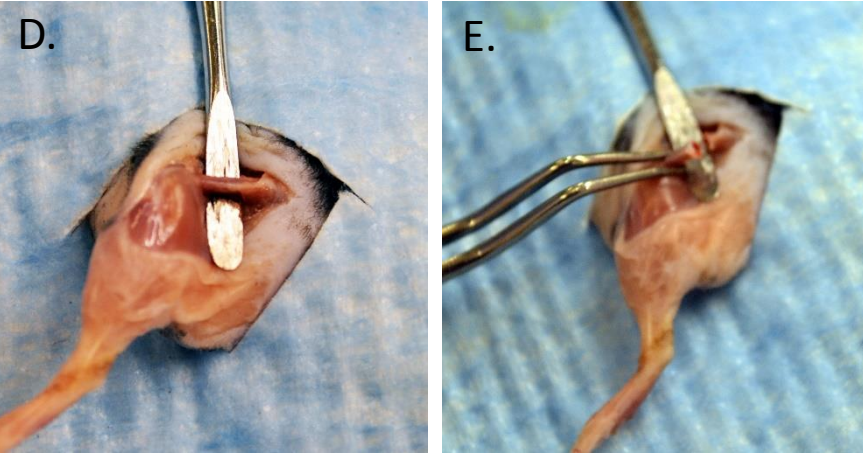
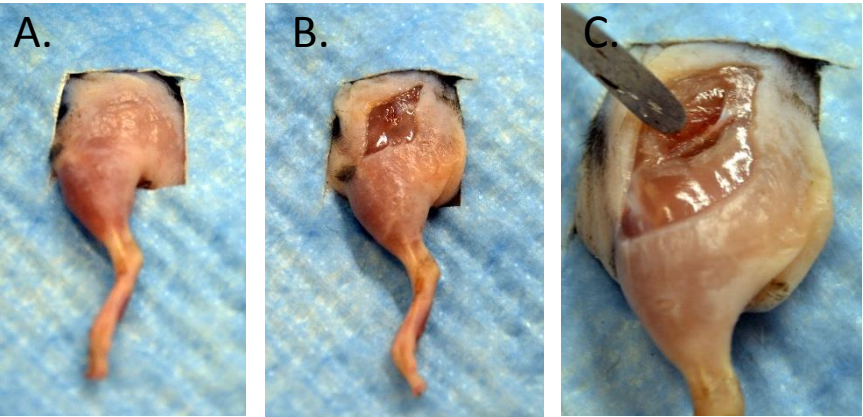


Fig 5: Surgery procedure.

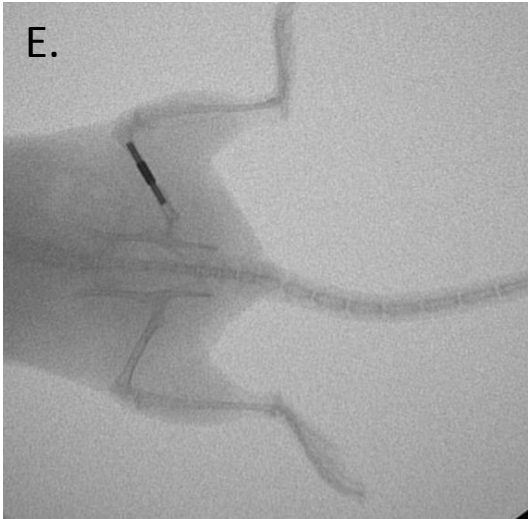
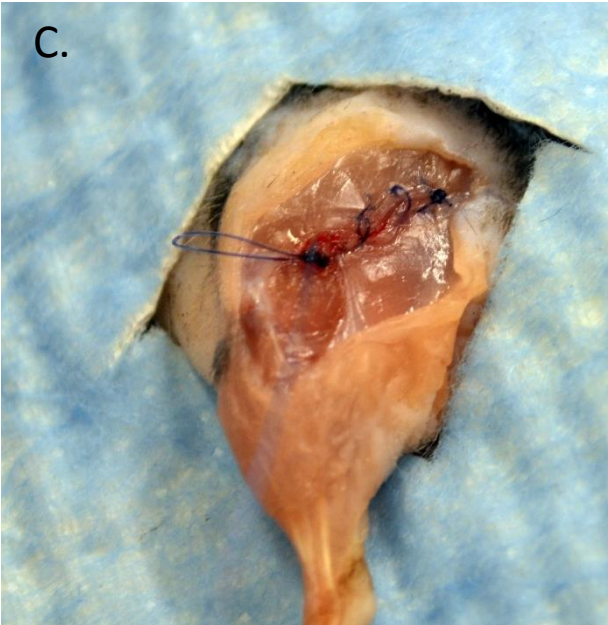
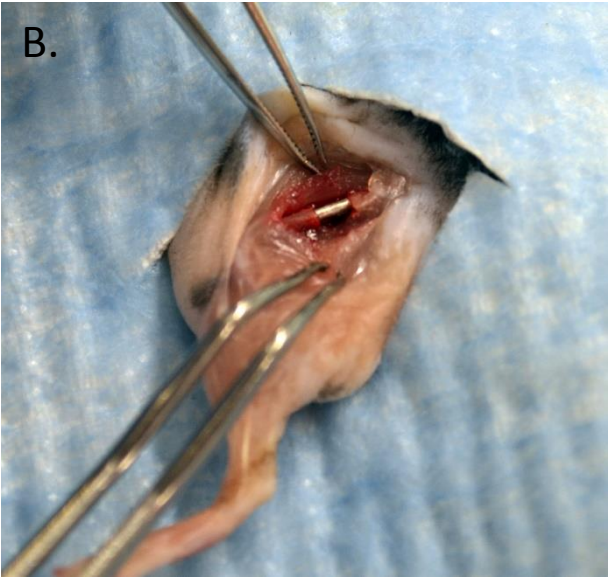
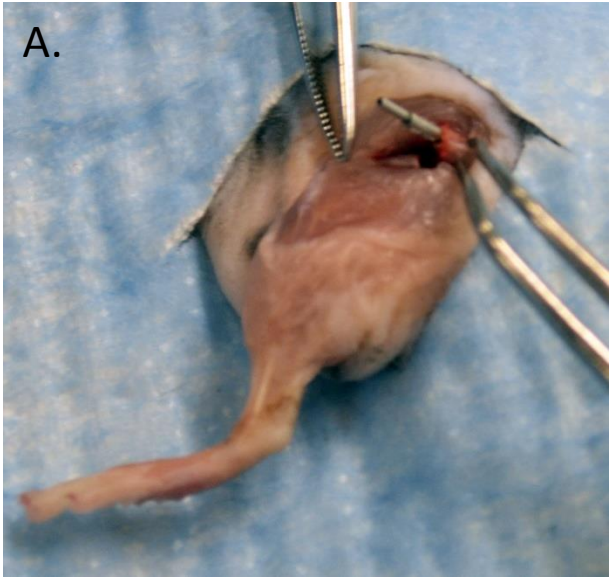
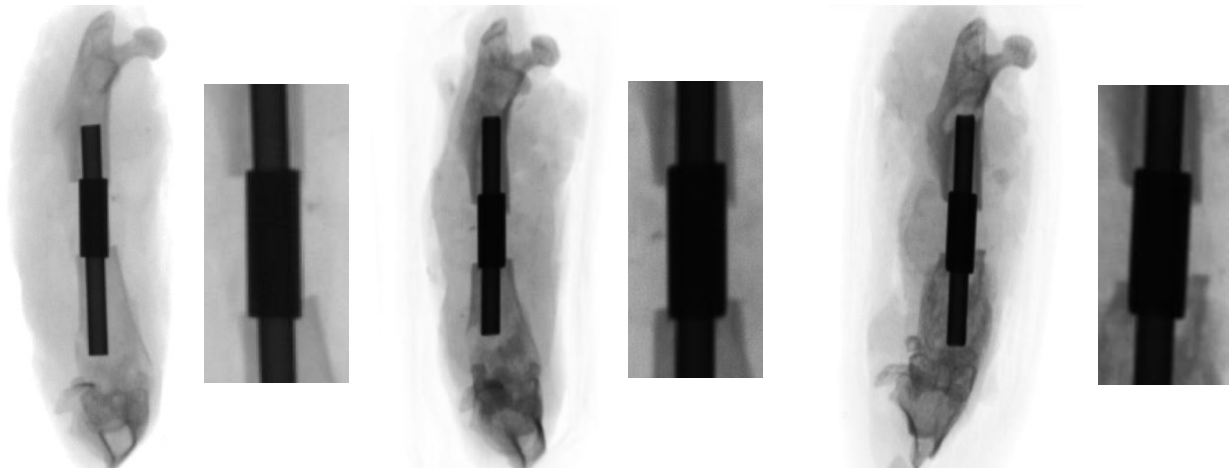


Fig 6: Example data.

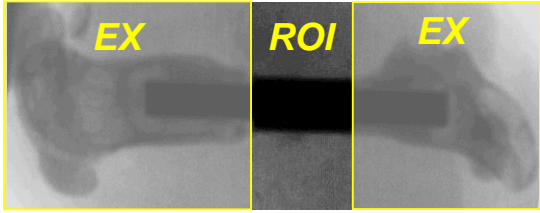
A. day 7

day 14

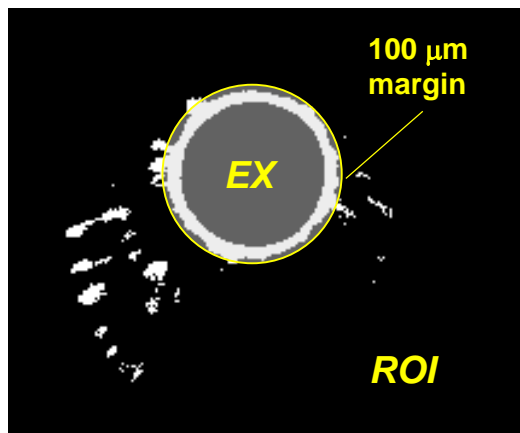
day 21



B. Scan ROI

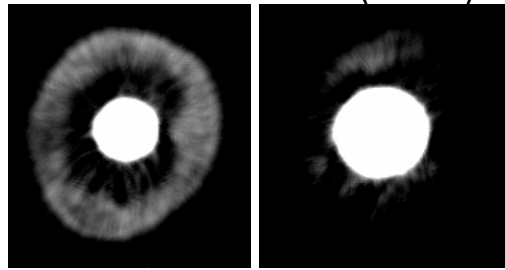


Axial ROI

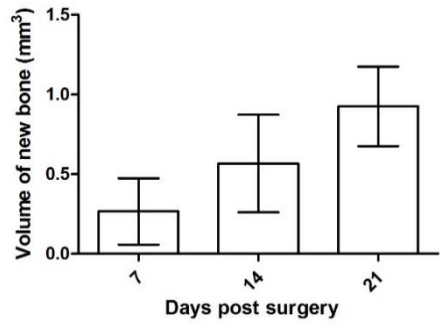


Pin

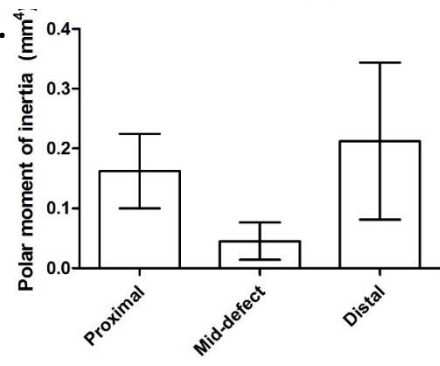
Collar (defect)



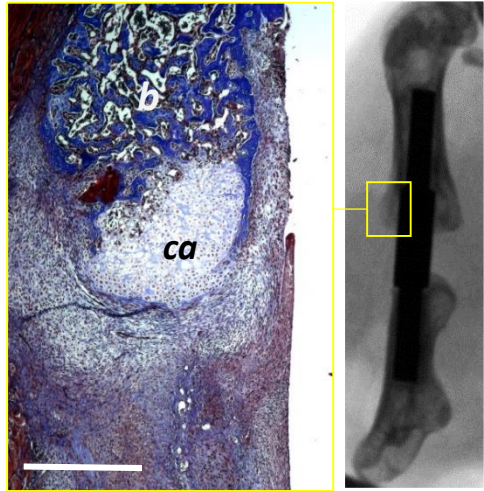
C.



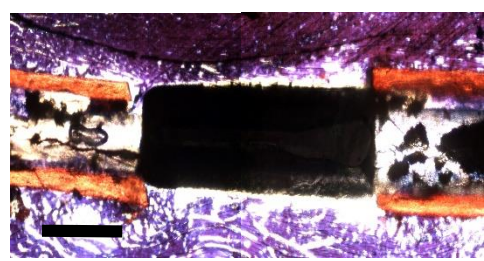
D.



E.



F.



Stage	Name of Equipment/Material*
Pin Assembly	Dremel rotary tool Heavy duty cut off wheel Surgical tubing 19G Surgical tubing 21G Surgical tubing 22G Surgical tubing 23G Cyanoacrylate adhesive Emery disc Rubber polishing point Felt polishing disc Gelatin sponge Punch biopsy cutter
Surgery/post-operative	Warm pad and circulator pump Coverage quaternary spray Bead sterilizer Anesthesia system Isoflurane anesthetic Surgical disinfectant Surgical tools Face protection Rechargeable high speed drill Diamond cutting wheel Absorbable sutures Outer sutures Vetbond Hydration gel Diet gel Buprenorphine Mouse igloos Euthanasia cocktail
Analysis	Live animal imager Micro-CT unit and software Sealing film/Parafilm M
*Generic sources are suitable for all other items such as gauze, drapes, prote	

Company	Catalog or model	Notes
Dremel	8220	or equivalent
Dremel	420	
Small Parts (Amazon)	B000FMZ8LY	OD 1.07mm, ID 0.889mm
Small Parts (Amazon)	B000FMZ8YQ	OD 0.82mm, ID 0.635mm
Small Parts (Amazon)	B000FMYLZS	OD 0.719mm, ID 0.502mm
Small Parts (Amazon)	B000FN0SY0	OD 0.643mm, ID 0.444mm
Loctite	1365882	
Dremel	413	
Dremel	462	
Dremel	414	
Surgifoam/Ethicon	1974	
Miltex	33-34	
Stryker/Thermocare	TP700, TP700C, TPP722	
Steris	1429-77	
Germinator/CellPoint Scientific	Germinator 500	
VetEquip Inc	901806 or 901807/901809	
VETone/MWI	501017, 502017	
Chloraprep/CareFusion	260449	
Fine Science Tools	various	recommend German made
Splash Shield	4505	
Fine Science Tools	18000-17	
Strauss Diaiond	361.514.080HP	
Covidien	UM-213	
Ethicon	668G	or equivalent
3M	1469SB	or equivalent
Clear H2O	70-01-1082	
Clear H2O	72-01-1062	
Reckitt and Benckser	12496-0757-01	controlled substance
Bio Serv	K3328, 3570,3327	
Euthasol/Virbac	710101	controlled substance
Orthoscan	FD Pulse	or equivalent
Bruker	Skyscan1174	or equivalent
VWR or Fisher	100501-338, S37441	

ective clothing, animal care equipment.

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Signature: [Signature] Date: 05/30/2014

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Dear Editors, *Journal of Visualized Experiments*,

We thank the reviewers for their comments regarding our manuscript “A Simple Critical-Sized Femoral Defect Model in Mice.” by Clough *et al.* We have endeavored to address each of the concerns with existing data and observations but were unable to perform additional experiments within the timeframe set by the JoVE editors. We appreciate the reviewers’ understanding in this matter.

Reviewers' comments:

Reviewer #1:

Manuscript Summary:

This paper proposes a novel method for mouse long bone defect model. The small, thin and fragile nature of the femoral bone of mice impedes the establishment of easy, reproducible bone defect model, despite its wide application for gene knock-out/knock-in models. By using self-made prosthesis consisted of only common supplies, the author provided us with useful and relatively easy way to make delayed or non union model of femoral bone.

Major Concerns:

There is no major concerns in this paper.

Minor Concerns:

1. Bone marrow cavity size and shape may vary between individual variability. Polishing metal shaft and reaming femoral cavity to adjust the very same size seems to demand highly sophisticated techniques and this might limit the reproducibility and universality of the methods.

Comparison of this method to intramedullary nails or external fixations might be better to show its superiority, in terms of learning curve, morbidity or mortality rate, if possible.

This is a good question and a valid concern. In fact, have found that the key to reproducibility lies in careful matching of the age, gender and strain of mice rather than the prototyping of the pin, although this should be done carefully.

Regarding comparisons with other methods, we propose that the ability to easily manufacture a pin in-house to the exact specifications of the mice to be studies represents a distinct advantage over established fixation systems.

In response to this concern, we have added the following to the revised manuscript:

INTRODUCTION, page 3, line 119: “With careful selection of inbred age, gender and strain-matched mice, the the result is a highly reproducible *hypertrophic non-union defect*²² which can be easily evaluated radiologically.”

PROTOCOL: page 3, line 133: “Since strains of mice vary slightly in terms of anatomy and growth rate, we advise that the fabrication of pins is optimized to the strain, gender

and age of the recipients prior to implantation into live subjects. **If the strains are carefully matched, the interference fit between the pin and marrow cavity is highly reproducible.**”

DISCUSSION, page 10, line 447: “While some torsional motion may occur during the early stages of healing, this is minimized by careful attention to the pin diameter and adequate reaming of the medullary canal so as to attain a firm interference fit between the implant and endosteum. **With careful selection of inbred strain and matching of age and gender, the fit becomes reproducibly robust within a few days. Nevertheless, with the advent of 3D printing techniques, it is expected that torsional motion can be further reduced** by more sophisticated versions of the pin that incorporate roughened surfaces and/or barbed attachment sites.”

And line 453: “The ease of pin fabrication, the availability of a wide variety of hypodermic tubing sizes also permit the optimization of the technique for virtually any adult inbred mouse, irrespective of natural or experimental bone phenotype.”

2. No adhesives or glues were applied to the interface between the bone cavity and metal implant with smooth surface. Is the friction resistance strong enough to prevent the metal shaft to come out from the bone cavity?

Please refer to our modifications for point 1.

3. Figure 2: The function of gel foam applied to the collar is not described and uncertain in this paper. Is it for cell transplantation?

Sorry for the omission, we have provided clarification:

METHODS, page 4, line 171: “**We have found that the positioning of a gelatin or collagen scaffold at the site of the defect improves cell retention and induces longitudinal growth along the axis of the bone.** Use a 4 mm diameter punch-biopsy...”

FIGURE 2 LEGEND, page 9, line 403: “...Gelfoam cylinder is trimmed, positioned over the steel collar (*middle*), then autoclaved, resulting in a sterile pin coated with dried Gelfoam. **This improves cell attachment at the site of injury and maintains the direction of healing (*below*).**”

Reviewer #2:

Manuscript Summary:

The manuscript describes techniques for generating a segmental defect in the femur of a mouse using a femoral medullary pin for stability. The technique is described in a comprehensive manner that makes it comprehensible to all scientists irrespective of whether they have veterinary training. As one who has performed similar work, I can attest to how difficult it is to generate reproducible bone defects in mice. Therefore, I suspect the article will be very well received and should open the door for a variety of new experimental approaches, such as testing new therapeutics and conducting basic studies using transgenic and knockout mice.

Major Concerns:

There are no major concerns with the manuscript.

Minor Concerns:

The manuscript would be further improved if the authors described several examples of how the technique could be used to test therapeutics, e.g. growth factor, cell-based, or materials-based treatments. Providing a simple example of how one might develop such an experiment, e.g. route and timing of delivery of test agent, and whether differences in bone production would yield significant differences between treatment groups based on the methods of analysis described in the text would be informative.

We also agree that this would benefit the readers of the article. However, experiments involving novel cells, growth factors and scaffolds could be highly variable and subject to very specific requirements. Nevertheless, we have recently utilized the approach to demonstrate efficacy of novel stem cells and stem cell derived scaffolds for femoral healing and the findings have been approved for publication in *Journal of Bone and Mineral Research*. We believe this article would showcase the technique and address many of the concerns raised here. In response to this comment, we have added the citation and the following text.

DISCUSSION, page 11, line 476: “For example, there is a variety of immune-compromised strains that permit testing of human cells and proteins without fear of immunological rejection, and their small size reduces the need for excessive amounts of valuable experimental materials, cells or compounds. **This is exemplified by our recent study demonstrating the efficacy of adult human stem cells and their extracellular proteins for osteoregeneration.**”

Reviewer #3:

The objective of this study is to demonstrate a new simple method to generate a critical-sized pin stabilized defect of murine femur in the standard laboratory. The manuscript claims that the defect 21 days after surgery is a hypertrophic non-union defect. It would be better to follow up the healing process for a longer time period, for instance, 12 weeks. In the previous study, a non-union fracture is defined as failure of healing even after the time period three times longer than that of the normal healing. In this study, the control group is missing. More quantitative data should be added to make the authors' conclusion. Major revision should be made for paper resubmission.

[Editorial comment: We do not require in depth or novel results for publication in JoVE, only representative results that demonstrate the efficacy of the protocol. However, please ensure that all claims made throughout the manuscript are supported by either results or references to published works.]

1, Lines 113-114: The authors state that the superior point to Garsia's is a simple method to generate the defect of the murine femur. Other superior points should be discussed. There are no data to compare with other methods. Comparing with other methods, the present method should be evaluated.

We concede that the primary advantage of our system over others is the simplicity of pin manufacture and implantation (see Introduction, page 3, line 116-124). Another major advantage is that the unique collar permits definition of the defect margins and thus, the region of interest for microCT scanning (Introduction, page 3, line 122-124 and Discussion, page 10, line 453-467). While we believe it is beyond the scope of the manuscript to compare every mouse fixation method in the literature, we appreciate that the method of Garcia *et al.* is the most comparable to ours. As such, we have made the following additions to the text in support of the proposed system and included the citation.

Introduction, page 3, line 112: “For example, Garcia *et al.* [new ref 23] devised an elegant interlocking pin system for use in mice, but the procedure involves incisions at two separate sites and extensive modification of the femur to accommodate the pins. These procedures were performed under a dissecting microscope.”

2, Lines 162-167, Lines 437-444: The reason to fix the pin into the femoral medullary cavity should be described clearly. The torsional motion may occur during the early stages of healing, and the pin became immovable. The statement is difficult to understand. It should be revised. For the osseointegration taking place in the space between the pin and endosteum, the authors should demonstrate that phenomenon scientifically.

Confidential comment to Editor: We are unclear exactly what reviewer 3 is referring to here, but we have attempted to clarify the wording a little more.

Protocol, page 4, line 167: “Make sure that the ends of the pin penetrate into the trabecular bone of the diaphysis so as to maximize fixation and improve the interference fit (Fig2E).”

Results, page 8, line 355: “In rare instances (<5% of cases), pins can become dislocated at early stages of healing and animal use protocols should provide for revision surgery if this occurs. While it is technically challenging to quantify torsional motion on murine femurs, manual palpation of specimens confirmed that torsional and longitudinal motion is marginal after 7 days as connective tissue accumulates around the pin.”

3, Lines 296-299: The follow-up time of healing is too short. Generally mice have a great potential for bone repair and the unstabilised fracture can be healed without any delay. If the authors want to claim that this is a model of permanent bone failure for bone healing, the longer-term follow-up, for instance, 12 weeks, should be performed.

A 12-week experiment is beyond our deadline and also unlikely to be approved by our IACUC given that much of this work has already been done but your point is well taken. We propose the following response to your concern: our assay is designed to assess healing during the anabolic phase of bone which is 3-4 weeks in rodents, thereafter slow bone remodeling takes place which is unlikely to be associated with bridging of the defect. Nevertheless, our defect size (3 mm) conforms to the criteria of Key *et al.* and is much smaller than the 1.8 mm defect used in Garcia's work. Therefore, we predict that the 3 mm defect is critical sized and will remain for up to 12 weeks.

Discussion, page 11, line 468: “In the experiments described here, the permitted healing time was relatively short at 3 weeks, which corresponds to the rapid, anabolic phase of bone healing. Thereafter, bone remodeling is a very slow process²⁸. Generally, if bridging is not observed after 4 weeks, healing is unlikely to occur and in agreement, we observe very little additional bone growth after 4 weeks in this system. Furthermore, a 3 mm gap meets the criteria of Key *et al.*¹⁶ for a critical sized defect and Garcia *et al.* demonstrated that a gap as narrow as 1.8 mm does not sufficiently heal after 10 weeks and this could be delayed to 15 weeks with stripped perichondrium²³.”

4, Lines 378-383: In this study, the pins were removed after decalcification. I am afraid that the removal may lead to the destruction of the surrounding tissue. To demonstrate the immobility of pins, the surrounding tissue should not be destroyed. This point should be discussed.

In response to this concern, we have added the following text and data.

Results, page 9, line 386: “While some damage will inevitably occur during dissection, the histological structure of bone and connective tissue remains clear if the pin is removed carefully. Alternatively, methyl methacrylate embedding and sectioning of non-demineralized sections may be performed with the pin in place (**Fig6F**).”

We have added data in Fig 6 showing an MMA embedded, non-decalcified section with the pin in place.

5, The strain and age of mice to use must affect the healing process of bone fracture. This point should be discussed referring some related research papers.

6, The present procedure is also applicable to the disease models of mice, such as diabetic and ovary-extracted mice. This point should be discussed.

In response to these concerns we have added the following text and references:

Discussion, page 11, line 481: “The relatively short lifespan of mice also present the opportunity for research into aging³⁰ and the wide variety of inbred strains permit the study of global genotype on healing³¹. There are also a number of disease models that are easily established in mice such as diabetes and osteoporosis^{32,33}.”